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## IV.研究成果の刊行物・別冊

## Controlled Release of Bone Morphogenetic Protein-2 Enhances Recruitment of Osteogenic Progenitor Cells for *De Novo* Generation of Bone Tissue

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The objective of this study was to evaluate the cellular contribution to the phenomenon of *de novo* generation of bone tissue induced by the controlled release of bone morphogenetic protein-2 (BMP-2). Gelatin hydrogels (2 mg) incorporating BMP-2 (3 µg) with different water contents were subcutaneously implanted into the back of enhanced green fluorescent protein-chimeric mice to induce the ectopic *de novo* generation of bone tissue. The hydrogels incorporating BMP-2 could release BMP-2 at different time profiles. When evaluated radiologically and histologically, the ectopic *de novo* generation of bone tissue was induced by the controlled release of BMP-2 from the hydrogels around the hydrogel-implanted site. The relative percentage number of green fluorescent protein- to osteocalcin-positive cells recruited into the *de novo* generated bone tissue depended on the BMP-2 release profile. The higher the percentage, the stronger was the *de novo* generation of bone tissue. These findings indicate that bone marrow-derived osteoblast progenitor cells were recruited from the blood circulation by BMP-2 release and consequently contributed to the ectopic *de novo* generation of bone tissue. It is conceivable that the local concentration of BMP-2 modifies the recruitment profile of progenitor cells with an osteogenic potential around the release site of BMP-2, resulting in regulated volume of *de novo* generated bone tissue.

### Introduction

**T**ISSUE ENGINEERING has been vigorously investigated over the last 20 years to experimentally demonstrate the biomedical feasibility of regeneration in medical therapy. The key components are cells, the scaffolds for cells attachment, proliferation, or differentiation, and biosignaling molecules for cell proliferation and differentiation. Various precursor or stem cells have been extensively studied and the mechanisms of their differentiation into specific cell lineages have been clarified recently.<sup>1,2</sup> Among the well-recognized mechanisms, it has been demonstrated that several soluble factors interact with their cellular receptor and subsequently start the intracellular signals required for specific gene expression. In addition, the matrix present around cells, so-called extracellular matrix, also plays an important role in the activation of signals and their biological functions.<sup>3-5</sup>

Recently, some research reports strongly suggest that stem or precursor cells circulating in the blood and body are originally present for hematopoiesis, vascularization, or mesenchymal tissue regeneration.<sup>6-15</sup> Therefore, it is highly

conceivable that a promoted recruitment of cells that are inherently present in the body to a body site results in cell-based tissue regeneration at the site. If the *in vivo* recruitment or fate of cells can be regulated by making use of their recruitment mechanism, tissue regeneration based on the cells present in the body can be achieved. We have developed gelatin hydrogels for the controlled release of various biosignaling molecules, such as growth factors, chemokines, and genes, and succeeded in the regeneration and repairing of various tissues.<sup>16</sup> Among them, it is well-known that bone morphogenetic protein-2 (BMP-2) is a strong inducer of bone tissue formation through mesenchymal cell infiltration, differentiation of mesenchymal cells into chondrocytes, diminishment of chondroid tissue, and generation of bone tissue.<sup>17-19</sup> Many researches have been reported for the complete regeneration of bone tissue with BMP-2.<sup>20</sup> In addition, it has been reported that BMP-2 is able to enhance the cells' mobilization.<sup>21</sup> This activity is promising and useful from the viewpoint that tissue regeneration can be achieved through the recruitment of cells originally present in the body.

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The objective of this study was to evaluate BMP-2-induced *de novo* generation of bone tissue in terms of cell recruitment. Previous research reports have demonstrated the contribution of bone marrow for bone fracture healing through hematoma formation.<sup>22-25</sup> Although they indicated the possible contribution of growth factors in hematoma or bone marrow cells to fracture healing, the characterization of cells contributing for *de novo* generation of bone tissue was not clarified. In this study, BMP-2 was incorporated into gelatin hydrogels with different degradabilities for the controlled release in different profiles. After the hydrogels incorporating BMP-2 were implanted subcutaneously, ectopic *de novo* generation of bone tissue was evaluated by radiological and histological examinations. We examined the effect of BMP-2 release profile on the recruitment of bone marrow-derived osteoblast progenitor cells at the release site of BMP-2 and the consequent *de novo* generation of bone tissue.

## Materials and Methods

### Materials

A gelatin sample with an isoelectric point of 9.0 was isolated from the porcine skin by an acidic process of collagen (Nitta Gelatin, Osaka, Japan). Na<sup>125</sup>I (NEZ-033H, >12.95 GBq/mL) was purchased from Perkin-Elmer Life Sciences (Boston, MA). Other chemicals were obtained from Wako Pure Chemical Industries (Osaka, Japan) and used without further purification.

### Preparation of gelatin hydrogels

Chemically crosslinked gelatin hydrogels with glutaraldehyde (GA) were prepared according to a previously reported method.<sup>26</sup> Briefly, aqueous solution of 3 wt% gelatin (pH 5.0) was mixed with GA at a final concentration of 0.16 and 0.09 wt%, respectively, followed by incubation at 4°C for 12 h for gelatin crosslinking. The gelatin hydrogel crosslinked was treated with 0.1 M glycine solution to block the residual aldehyde groups. After washing with double-distilled water for three times, the hydrogels were freeze-dried. The crosslinking extent of prepared hydrogels was evaluated by measuring the water content according to a previously described method.<sup>27</sup> The water contents of hydrogels prepared with higher and lower GA concentrations were 97.5 ± 0.1 and 99.3 ± 0.0 wt%, respectively.

### In vivo release test of BMP-2 from gelatin hydrogels

All the animal experiments were performed according to the Institutional Guidance of Kyoto University on Animal Experimentation and with permission from the Animal Experiment Committee of the Institute for Frontier Medical Science, Kyoto University. All the surgical procedures were performed under continuous inhalation anesthesia using isoflurane (Forane®; Abbott Japan, Osaka, Japan) with 400 Anesthesia Unit (Univentor, Zejtun, Malta).

Human recombinant BMP-2 (Yamanouchi Pharmaceutical, Tokyo, Japan) was radioiodinated through the conventional chloramine T method as previously described.<sup>28</sup> Briefly, 5 µL of Na<sup>125</sup>I was added to 200 µL of BMP-2 solution (150 µg/mL) in 0.5 M potassium phosphate buffer (pH 7.5) containing 0.5 M sodium chloride. Then, 0.2 mg/mL of chloramine-T in the same buffer (100 µL) was added to the

solution mixture. After agitation at room temperature for 2 min, 100 µL of phosphate-buffered saline (PBS; pH 7.4) containing 0.4 mg of sodium metabisulfate was added to the reaction solution to stop radioiodination. The reaction mixture was passed through a PD-10 desalting column (GE Healthcare Life Sciences, Giles, UK) to remove the uncoupled, free <sup>125</sup>I molecules from the <sup>125</sup>I-labeled BMP-2 (9.0 µg/mL; removal ratio of free <sup>125</sup>I = 97.0%).

PBS containing <sup>125</sup>I-labeled BMP-2 (27.4 µL, 9.0 µg/mL) and PBS containing nonlabeled BMP-2 (2.6 µL, 1 mg/mL) were mixed and dropped onto 2 mg of freeze-dried gelatin hydrogels, followed by incubation at 4°C for 12 h, to allow to swell into the hydrogel. Following the implantation of gelatin hydrogels incorporating <sup>125</sup>I-labeled BMP-2 into the back subcutis of 6-week-old, female ddY mice (18–20 g body weight; Shimizu Laboratory Supply, Kyoto, Japan), tissue around the implanted site was extracted at different time intervals after hydrogel implantation, and the tissue radioactivity was counted by a gamma counter to estimate the *in vivo* time profiles of BMP-2 release (*n* = 3, at each time point).

### Preparation of green fluorescent protein-chimeric mice

C57BL/6 transgenic mice that ubiquitously express enhanced green fluorescent protein (GFP) under the Cytomegalovirus (CMV) early enhancer/chicken β actin (CAG) promoter were provided by RIKEN BRC through the National Bio-Resource Project of the MEXT, Japan. Preparation of chimeric mice was performed according to a previously reported procedure.<sup>29</sup> Briefly, bone marrow cells were isolated from 8- to 10-week-old, male transgenic mice under sterile conditions.<sup>30</sup> The cells were incubated with CD90.2 microbeads (no. 130-049-101; Miltenyi Biotec, Auburn, CA) and RPMI 1640 medium at 8°C for 20 min and passed through large depletion (LD) column with Midi MACS system (no. 130-042-901; Miltenyi Biotec) for depletion of CD-90.2-positive T cells and prevention of subsequent autoimmune attack. Eight- to 10-week-old, female C57BL/6 mice were irradiated lethally with 10 Gy of gamma ray. For total bone marrow transplantation, 5 × 10<sup>6</sup> of bone marrow cells prepared from GFP transgenic mice was intravenously administered to recipient irradiated mice. After the transplantation, the mice were bred for 10 weeks to complete the replacement of bone marrow cells to GFP-positive cells. The replacement ratio of bone marrow cells was 93.2% ± 1.5% when evaluated by the fluorescence-associated cell sorter method (FACS Calibur; BD Bioscience, Franklin Lakes, NJ).

### In vivo assay of *de novo* generation of bone tissue

BMP-2 was dissolved in PBS at 100 µg/mL and the solution (30 µL) was dropped on the gelatin hydrogel (2 mg) to allow it to swell into the hydrogel. After incubation of the hydrogels incorporating BMP-2 at 4°C for 12 h, the hydrogels were implanted to the back subcutis of GFP-chimeric mice. As a control, gelatin hydrogels incorporating PBS were similarly implanted to the back of the mice. Then, the tissue around the implanted sites was extracted at different time intervals after hydrogel implantation, and the fluorescent images of tissues were obtained by a digital microscope (Multiviewer System VB-S20; Keyence, Osaka, Japan). *De novo* generation of bone tissue was radiologically exam-

ined by a soft X-ray machine (Hitex-100; Hitachi, Tokyo, Japan) at 54kV and 2.5mA for 20s. Then the extracted tissues were fixed with 4% paraformaldehyde at 4°C for 48 h, and the bone tissue was decalcified with PBS containing 9 wt% ethylenediamine tetraacetic acid disodium salt and 10 wt% ethylenediamine tetraacetic acid tetrasodium salt (EDTA solution) at 4°C for 6 days. The EDTA solution was changed every other day. After decalcification, the pellets were equilibrated in PBS containing 15 wt% sucrose for 12 h and then in PBS containing 30 wt% sucrose for 12 h, embedded in Tissue-Tek OCT Compound (Sakura Finetek, Tokyo, Japan), frozen on dry ice, and stored at -80°C. For the histological examinations, 6- $\mu$ m-thick sections were cut with a cryostat (Leica Microsystems AG, Wetzlar, Germany) at the portion of implanted site as central as possible, followed by staining with hematoxylin and eosin. The area of newly formed bone tissue was assessed in terms of histological image analysis using the computer program Image-Pro Plus 3.01 (Media-Cybernetics, Silver Spring, MD).

#### Immunofluorescence staining

After washing with PBS, the sections (6 $\mu$ m thickness) were blocked with a normal goat serum for 1 h at room temperature before incubation with a rabbit polyclonal anti-mouse osteocalcin antibody (1:250; Takara Bio, Shiga, Japan) for 1 h at room temperature. Then the sections were stained with a tetramethylrhodamine-isothiocyanate-conjugated goat anti-rabbit IgG (Molecular Probes, Eugene, OR) for 1 h at room temperature. After washing with PBS, the sections were mounted with Vectashield<sup>®</sup> (Vector Laboratories, Burlingame, CA). Fluorescent images were obtained using an epifluorescent microscope (AX-80; Olympus, Tokyo, Japan), and the relative percentage number of GFP-positive cells to osteocalcin-positive cells in each image was calculated manually by observing the images. Three areas of interest (100 $\times$ 100 $\mu$ m<sup>2</sup>) were chosen randomly from each fluorescent image (at least four images per each experimental group) and the number of GFP- and osteocalcin-positive cells were counted.

#### In vitro migration assay

Bone marrow cells (3 $\times$ 10<sup>6</sup> cells/cm<sup>2</sup>) isolated from the transgenic mice described earlier were plated onto cell culture dish (no. 430167; Corning Incorporated, Corning, NY) with alpha minimum essential medium ( $\alpha$ MEM; Sigma-Aldrich, St. Louis, MO) containing 15 vol% fetal bovine serum (FBS) and cultured at 37°C and 5% CO<sub>2</sub>-95% air atmospheric pressure. The cells were flushed with PBS at 3 days after seeding to remove unattached blood cells and cultured till subconfluent condition for further experiment. The medium was changed to  $\alpha$ MEM without serum at 24 h before the migration assay experiment. The cells were trypsinized and plated onto the HTS<sup>®</sup> fluoroblok inserts (1.3 $\times$ 10<sup>3</sup> cells/mm<sup>2</sup>; Falcon no. 351552 with 8- $\mu$ m-diameter pore; Becton Dickinson, Franklin Lakes, NJ) with  $\alpha$ MEM containing 0.5 vol% FBS. The bottom side of the inserts contacted  $\alpha$ MEM containing 15 or 0.5 vol% FBS, 100 ng/mL of recombinant human stromal cell-derived factor-1 (SDF-1; no. 350-NS/CF; R&D systems, Minneapolis, MN), BMP-2, or recombinant human placental growth factor (PIGF; no. 264-PG; R&D systems) with 0.1 vol% bo-

vine serum albumin. After 24 h culture, cells that migrated to the bottom side were counted from fluorescent photographs taken by an epifluorescent microscope (IX-70; Olympus). The number of cells in six images (0.594 mm<sup>2</sup> per each image) were counted.

#### Statistical analysis

All the results were statistically analyzed by the unpaired Student's *t*-test and *p* < 0.05 was considered to be statistically significant. Data were expressed as the mean  $\pm$  standard deviation.

## Results

### De novo generation of bone tissue by gelatin hydrogels incorporating BMP-2

Figure 1 shows the time profiles of *in vivo* radioactivity remaining after implantation of gelatin hydrogels incorporating <sup>125</sup>I-labeled BMP-2 with different water contents. The gelatin hydrogels with higher water content released BMP-2 faster than those with lower water content.

Figure 2 shows the soft X-ray radiophotographs of implanted sites at 2 weeks after the implantation of gelatin hydrogels incorporating 3  $\mu$ g of BMP-2 or PBS. A radio-opacity portion was observed at the center of tissues implanted with gelatin hydrogels incorporating BMP-2, although the influence of water content on the extent was not observed. On the contrary, no radio-opacity was observed for the BMP-2-free gelatin hydrogels.

Figure 3a-c shows the histological images of the implanted site at 2 weeks after implantation of the gelatin hydrogels incorporating 3  $\mu$ g of BMP-2 or PBS. Figure 3d shows the histological image of the implanted site at 7 weeks after implantation of the gelatin hydrogel incorporating BMP-2.

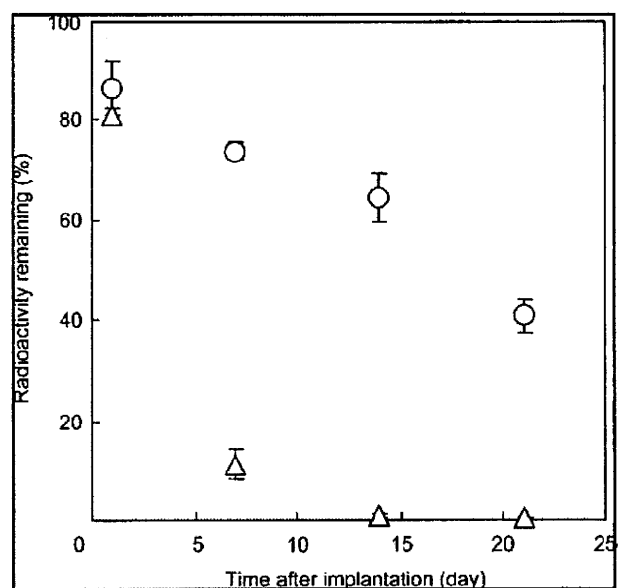
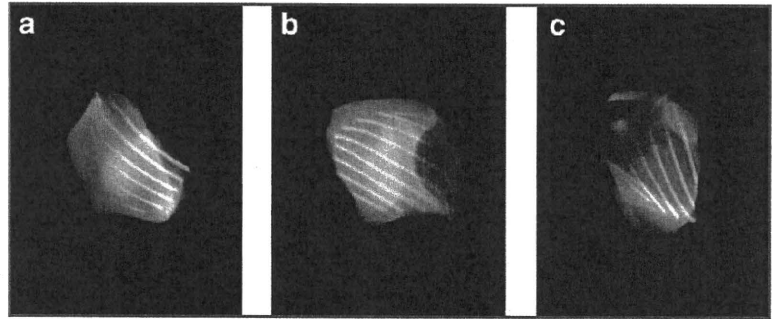


FIG. 1. *In vivo* release profiles of BMP-2 from gelatin hydrogels with water content of 97.5 wt% (○) and 99.3 wt% (△). BMP, bone morphogenetic protein.

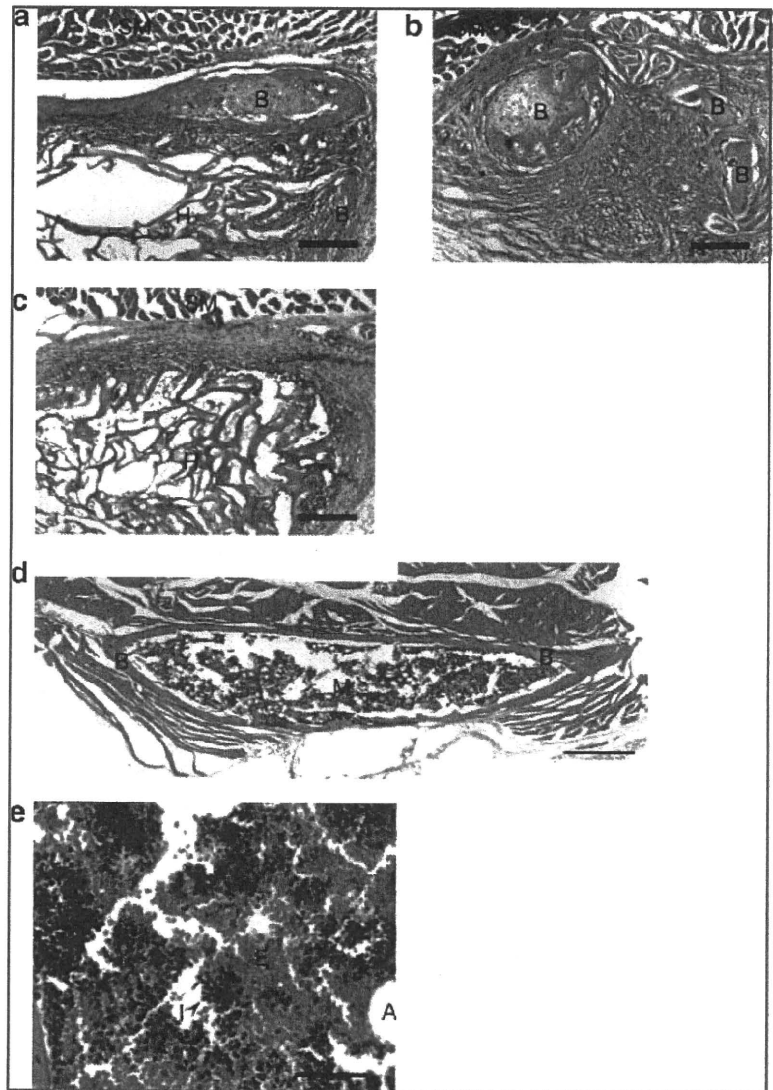
**FIG. 2.** Soft X-ray radiophotographs of tissues around the implanted site at 2 weeks after implantation of (a) the gelatin hydrogel incorporating BMP-2 (3  $\mu$ g) with a water content of 97.5 wt%, (b) the gelatin hydrogel incorporating BMP-2 (3  $\mu$ g) with a water content of 99.3 wt%, and (c) the gelatin hydrogel incorporating PBS with a water content of 97.3 wt%. PBS, phosphate-buffered saline.



After implantation, mature bone tissues with a bone marrow-like structure containing many inflammatory cells, blood cells, and adipocytes (Fig. 3e) were observed. The implanted gelatin hydrogel was completely degraded and was not detected in the section. Figure 4 shows the area of newly formed bone tissue at the implanted site of gelatin hydrogels incorporating BMP-2. After the implantation of

gelatin hydrogel incorporating BMP-2 with a water content of 99.3 wt%, the *de novo* generation of bone tissue was observed only at 2 weeks, but thereafter the tissue disappeared. On the contrary, the implantation of hydrogels incorporating BMP-2 with a water content of 97.5 wt% induced significant *de novo* generation of bone tissue and the bone tissue was retained even at 7 weeks after implantation.

**FIG. 3.** (a–c) Histological image of tissues around the implanted site at 2 weeks after implantation of (a) the gelatin hydrogel incorporating BMP-2 (3  $\mu$ g) with a water content of 97.5 wt%, (b) the gelatin hydrogel incorporating BMP-2 (3  $\mu$ g) with a water content of 99.3 wt%, and (c) the gelatin hydrogel incorporating PBS with a water content of 97.5 wt%. B, bone tissue; M, bone marrow-like structure; SM, subcutaneous muscle tissue; H, remaining gelatin hydrogels. (d) Histological image of tissues around the implanted site at 7 weeks after implantation of gelatin hydrogel incorporating BMP-2 (3  $\mu$ g) with a water content of 97.5 wt%. Scale bar = 500  $\mu$ m. (e) Higher magnification image of bone marrow-like structure inside the implanted site. Scale bar = 50  $\mu$ m. I, inflammatory cells; E, blood cells; A, adipocyte. Color images available online at [www.liebertonline.com/ten](http://www.liebertonline.com/ten).



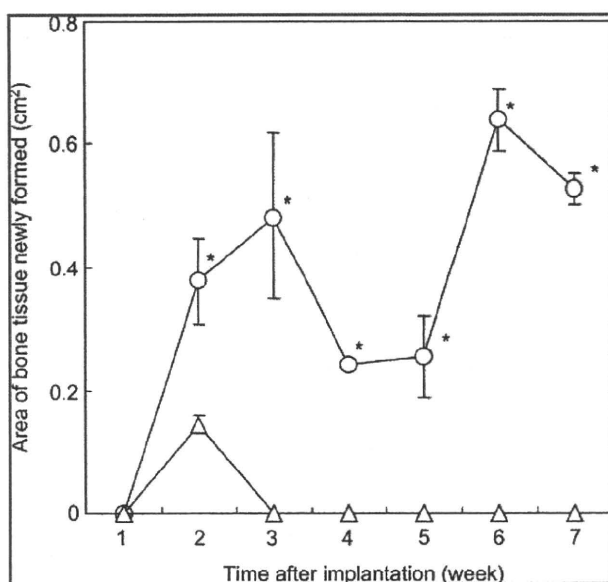


FIG. 4. Area of newly formed bone tissues after implantation of gelatin hydrogels incorporating BMP-2 (3  $\mu$ g) with a water content of 97.5 wt% (O), gelatin hydrogels incorporating BMP-2 (3  $\mu$ g) with a water content of 99.3 wt% ( $\Delta$ ). \* $p < 0.05$ , significant against the area after implantation of gelatin hydrogels incorporating BMP-2 (3  $\mu$ g) with a water content of 99.3 wt% at the corresponding time.

#### Recruitment of cells by gelatin hydrogels incorporating BMP-2

Figure 5 shows the fluorescent images of tissues around the implanted site at 2 weeks after the implantation of gelatin hydrogels incorporating BMP-2 or PBS. Irrespective of the experimental groups, a green fluorescence was detected in the implanted sites, which indicates the accumulation of bone marrow-derived cells.

Figure 6 shows the immunofluorescent images of tissues around the implanted site at 2 weeks after implantation of gelatin hydrogels incorporating BMP-2 or PBS. Cells with green fluorescence were observed in all images, and the cells were of round and spindle shape. For the gelatin hydrogels incorporating BMP-2, many red-stained cells were observed around the implanted site (Fig. 6a, b). On the contrary, no cells with red fluorescence were observed around the implanted site of gelatin hydrogels without BMP-2 (Fig. 6c). Figure 7 shows the relative percentage number of

GFP-positive cells to osteocalcin-positive cells around the implanted site at 2 weeks after implantation of gelatin hydrogels incorporating BMP-2 or PBS. The implantation of gelatin hydrogels incorporating BMP-2 with different water contents increased the relative percentage number of GFP-positive cells to osteocalcin-positive cells around the implanted site. And the relative percentage for the gelatin hydrogel incorporating BMP-2 with a water content of 97.5 wt% was significantly higher than that of hydrogels with a water content 99.3 wt%. After this time point, it was practically impossible to compare the accumulation of bone marrow-derived cells between the implanted sites of the gelatin hydrogel incorporating BMP-2 with water contents of 97.5 and 99.3 wt%. This is due to the disappearance of the newly formed bone tissue around the implanted site of the latter gelatin hydrogel incorporating BMP-2.

#### In vitro cell migration

Figure 8 shows the number of cells that migrated to the bottom side of the inserts at 24 h after incubation with  $\alpha$ MEM containing BMP-2 or other factors. No activity as a chemoattractant to bone marrow cells was observed for BMP-2. The migration level was the same as that of the negative control (0.5 vol% FBS). However, a strong chemoattractant activity was observed for SDF-1 and PIGF, which was the same as that of the positive control (15 vol% FBS). The activity by PIGF was significantly higher than that by SDF-1 and 15 vol% FBS.

#### Discussion

This study demonstrates that the BMP-2 release profile affected the extent of accumulation of bone marrow-derived cells and the consequent *de novo* generation of bone tissues. The hydrogel water contents of 97.5 and 99.3 wt% indicated that the weight ratio of gelatin molecules to total hydrogel were 2.5 and 0.7 wt%. The difference in gelatin molecule fraction and crosslinking density of hydrogels caused the difference in hydrogel degradation and the consequent BMP-2 *in vivo* release profiles (Fig. 1). The BMP-2 release for a longer time period enabled strong accumulation of GFP-positive bone marrow-derived osteoblast progenitor cells which are also stained with the anti-osteocalcin antibody, even at 2 weeks after implantation. It is apparent from Figure 5 that the accumulation of bone marrow-derived cells was observed by the implantation of gelatin hydrogels with or without BMP-2. However, from the double-staining assay, for the hydrogel without BMP-2, no osteocalcin-positive cells were detected around the implanted site (Figs. 6 and 7). As

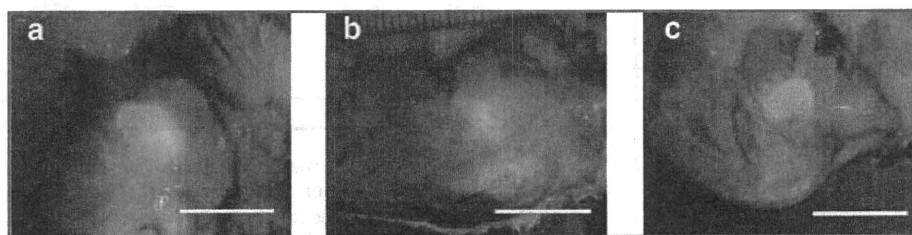
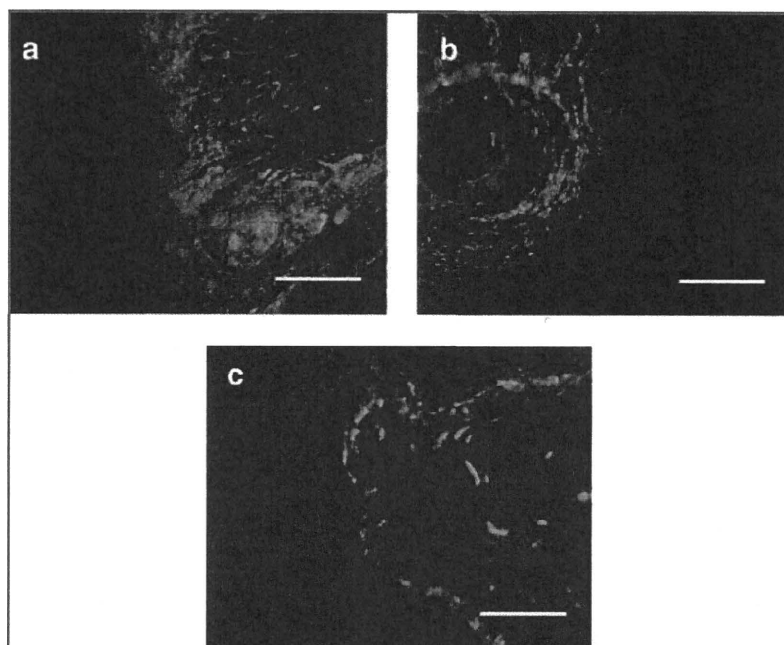


FIG. 5. Fluorescent images of the area surrounding the implant at 2 weeks after implantation of (a) the gelatin hydrogel incorporating BMP-2 (3  $\mu$ g) with a water content of 97.5 wt%, (b) the gelatin hydrogel incorporating BMP-2 (3  $\mu$ g) with a water content of 99.3 wt%, and (c) the gelatin hydrogel incorporating PBS with a water content of 97.3 wt%. Scale bar = 1 cm. Color images available online at [www.liebertonline.com/ten](http://www.liebertonline.com/ten).

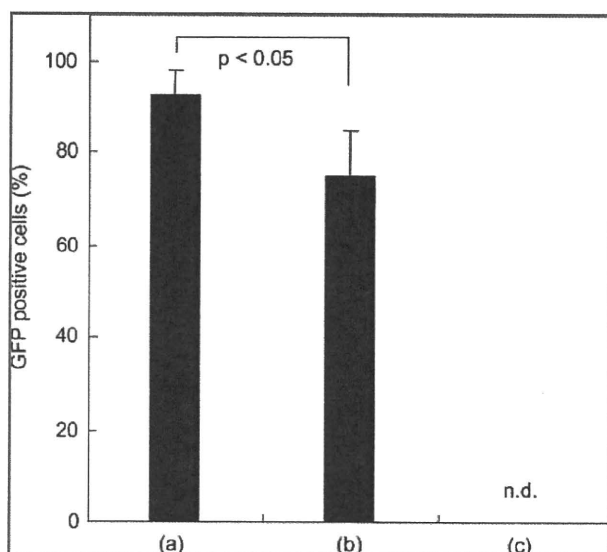
**FIG. 6.** Immunofluorescence staining images of tissue around the implanted site at 2 weeks after implantation of (a) the gelatin hydrogel incorporating BMP-2 (3  $\mu$ g) with a water content of 97.5 wt%, (b) the gelatin hydrogel incorporating BMP-2 (3  $\mu$ g) with a water content of 99.3 wt%, and (c) the gelatin hydrogel incorporating PBS with a water content of 97.3 wt%. Red fluorescence: osteocalcin; green fluorescence: green fluorescent protein. Scale bar = 200  $\mu$ m. Color images available online at [www.liebertonline.com/ten](http://www.liebertonline.com/ten).



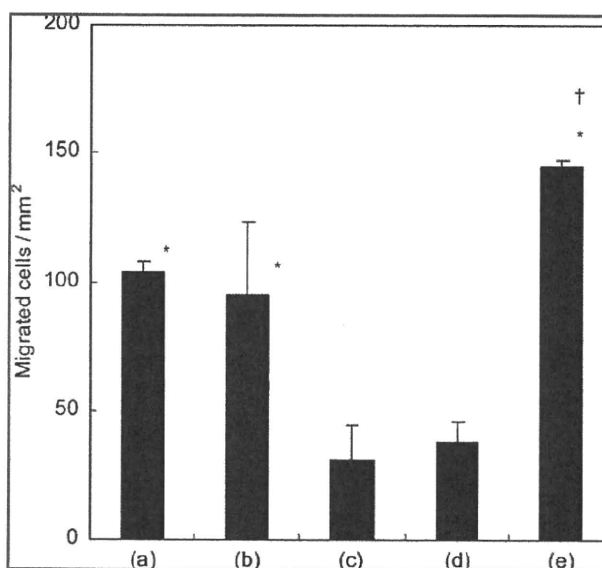
the osteocalcin-expressing cells are generally osteoblastic cells with bone formation activity, we can say with certainty that the BMP-2 release increased the recruitment of osteogenic cells around the release site.

The extent of *de novo* generation of bone tissue depended on the water content of gelatin hydrogels. This finding was experimentally confirmed in a previous study<sup>26</sup> and the present results are also in accordance to it even after ex-

tended time course (7 weeks after implantation). The decrease in the *de novo* generated area was observed in 4 or 5 and 3 weeks after implantation for gelatin hydrogels with water contents of 97.5 and 99.3 wt%, respectively (Fig. 4). This time profile can be explained in terms of that of BMP-2 release. For the gelatin hydrogel, the time profile of BMP-2 release was well correlated to that of hydrogel degradation. The hydrogel that is degraded for 4–5 weeks would release



**FIG. 7.** Relative percentage number of GFP-positive cells to osteocalcin-positive cells around the implanted site at 2 weeks after implantation of (a) gelatin hydrogels incorporating BMP-2 (3  $\mu$ g) with a water content of 97.5 wt%, (b) gelatin hydrogels incorporating BMP-2 (3  $\mu$ g) with a water content of 99.3 wt%, and (c) gelatin hydrogels incorporating PBS with a water content of 97.5 wt%. n.d., not detected; GFP, green fluorescent protein.



**FIG. 8.** Migration of bone marrow cells through the transwell membrane at 24h after incubation with  $\alpha$ -minimum essential medium containing (a) 15 vol% fetal bovine serum, (b) 100 ng/mL stromal cell-derived factor-1, (c) 100 ng/mL BMP-2, (d) 0.5 vol% fetal bovine serum, and (e) 100 ng/mL placental growth factor. \* $p < 0.05$  against the groups (c) and (d); † $p < 0.05$  significant against the groups (a) and (b).

BMP-2 for 4–5 weeks. It is possible that for this range, the BMP-2 release results in the BMP-induced *de novo* generation of bone tissue. However, the cessation of release would suppress bone tissue induction, resulting in the disappearance of bone tissue. The area of *de novo* generated bone increased again from 6 weeks after implantation. The cells recruited by the released and remaining BMP-2 may be able to further promote *de novo* generation of bone tissue. This reason is not clear at present.

Significant difference in the accumulation of osteocalcin-positive cells between the gelatin hydrogels with water contents of 97.5 and 99.3 wt% was observed (Fig. 6). This experimental result indicates that the profile of BMP-2 release affects the recruitment of bone marrow-derived cells. It is conceivable that BMP-2 release for a longer time period induces the recruitment of cells for a long time period, resulting in enhanced accumulation of cells. BMP-2 can accelerate bone tissue formation<sup>18</sup> through osteoblast migration,<sup>31</sup> by promoting osteogenic differentiation of mesenchymal stem cells,<sup>32,33</sup> angiogenesis,<sup>34</sup> apoptosis of osteoblast,<sup>35</sup> and recruitment of osteoblast progenitor cells.<sup>21,29</sup> It has been demonstrated that BMP-2 could induce the expression of PIGF. The enhanced expression of PIGF promoted the recruitment of progenitor cells from the bone marrow.<sup>36–38</sup> In addition, fibrous tissue and hypertrophic cartilage formation was observed in a fracture healing model of PIGF-deficient mice.<sup>37</sup> The chemoattractant study revealed that PIGF accelerated the migration of isolated bone marrow cells, in contrast to BMP-2 (Fig. 8). It is highly conceivable that BMP-2 functions as a trigger molecule to induce PIGF for the migration of bone marrow-derived cells. Further analysis is needed to understand the effect of BMP-2 release on cell recruitment.

This study clearly indicates that the BMP-2-releasing materials enhance cell accumulation for *de novo* generation of bone tissue. This activity could be modified by the release profile. This finding opens a new strategy of tissue engineering to achieve tissue regeneration by induction of cells present in the body.

#### Disclosure Statement

No competing financial interests exist.

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# Serum Anti-BPAG1 Auto-Antibody Is a Novel Marker for Human Melanoma

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## Abstract

Malignant melanoma is one of the most aggressive types of tumor. Because malignant melanoma is difficult to treat once it has metastasized, early detection and treatment are essential. The search for reliable biomarkers of early-stage melanoma, therefore, has received much attention. By using a novel method of screening tumor antigens and their auto-antibodies, we identified bullous pemphigoid antigen 1 (BPAG1) as a melanoma antigen recognized by its auto-antibody. BPAG1 is an auto-antigen in the skin disease bullous pemphigoid (BP) and anti-BPAG1 auto-antibodies are detectable in sera from BP patients and are used for BP diagnosis. However, BPAG1 has been viewed as predominantly a keratinocyte-associated protein and a relationship between BPAG1 expression and melanoma has not been previously reported. In the present study, we show that bpag1 is expressed in the mouse F10 melanoma cell line *in vitro* and F10 melanoma tumors *in vivo* and that BPAG1 is expressed in human melanoma cell lines (A375 and G361) and normal human melanocytes. Moreover, the levels of anti-BPAG1 auto-antibodies in the sera of melanoma patients were significantly higher than in the sera of healthy volunteers ( $p < 0.01$ ). Furthermore, anti-BPAG1 auto-antibodies were detected in melanoma patients at both early and advanced stages of disease. Here, we report anti-BPAG1 auto-antibodies as a promising marker for the diagnosis of melanoma, and we discuss the significance of the detection of such auto-antibodies in cancer biology and patients.

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## Introduction

Melanoma is one of the most aggressive tumors due to its strong capacity to metastasize. In the United States, there were an estimated 62,480 new melanoma cases and 8,420 deaths caused by melanomas in 2008 [1]. Although the 5-year survival rate of patients with early stage localized melanoma is greater than 90%, survival rates drop to less than 20% once the melanoma has metastasized to distant sites [1]. In general, early diagnosis of cancers greatly improves the survival of patients. Therefore, great efforts have been made to screen tumor markers for early diagnosis. Several melanoma markers (e.g. gp100, MART-1 and tyrosinase) have been detected and proposed for immunotherapy approaches [2,3,4]. With regards to melanoma markers in serum, S100 protein, 5-S-cysteinyl dopa and 6-hydroxy-5-methoxyindole-2-carboxylic acid can be useful although levels tend to be more up-regulated in advanced melanomas. As such, these particular markers are not suitable for the early detection of malignant melanoma [5]. Glypican-3 (GPC3), however, is overexpressed in melanoma and its serum concentration can serve as an early stage melanoma diagnostic marker [6,7]. Nevertheless, from a practical prospective, use of only one biomarker may lack sensitivity and specificity and diminish clinicopathologic value. The availability of multiple markers would make the diagnosis of melanoma more

reliable, and thus there is a need to identify and assess additional melanoma markers.

In the present study, we developed a screening method to detect tumor markers recognized by auto-antibodies to these proteins in serum. Using this method, we found that bullous pemphigoid antigen 1 (BPAG1) was expressed in both melanoma cell lines and normal melanocytes. BPAG1 is a plakin family protein that anchors keratin filaments to hemidesmosomes [8]. Another protein BPAG2, a transmembranous collagen, is also expressed in the skin and is a component of hemidesmosomes [8]. Deletion of the *dst* gene, that encodes bpag1, disrupts hemidesmosomes structure, resulting in the failure of hemidesmosomes to associate with keratin filaments [9]. Both BPAG1 and BPAG2 can serve as auto-antigens in bullous pemphigoid (BP) [10,11,12]. Auto-antibodies to BPAG1 and BPAG2 maybe detected in the sera of BP patients, and assessment of antibody levels can be used for BP diagnosis and clinical management. While passive transfer experiments have shown that BPAG2 antibodies have pathogenic relevance to BP, the clinicopathological significance of BPAG1 antibodies, has not yet been fully elucidated [13]. It has been hypothesized that anti-BPAG1 auto-antibodies might interfere with hemidesmosome integrity, but this has not been proven [9].

Here, we show that the level of auto-antibodies against BPAG1 in the sera of melanoma patients, at both early and advanced

stages, was significantly higher than levels in the sera of healthy volunteers. These findings identify anti-BPAG1 auto-antibodies as a novel and promising tumor biomarker in the detection of melanoma.

## Materials and Methods

### Libraries, bacteria and helper phage

The human single-fold scFv libraries I + J (Tomlinson I + J), *E. coli* TG1 and HB2151, and KM13 helper phage were all kindly provided by the Medical Research Council (MRC). The scFv library was prepared as previously described [14]. The scFv library was cloned into the pIT2 expression vector, which contains a lac promoter and a pelB leader sequence upstream of the VH-(G<sub>4</sub>S)<sub>3</sub>-VL insert; the insert is followed by 6×His and myc tags, an amber stop codon and the gene encoding the pIII phage coat protein. Thus, in a suitable non-suppressor strain (HB2151), addition of isopropyl-thio-β-D-galactoside (IPTG) induces only scFv and not scFv-pIII fusion expression.

### Mice

Female C57BL/6N mice (6 weeks old) were studied (Charles River Laboratories Japan, Inc., Japan) Animal experiments were performed in accordance with the guidelines of the Osaka University Graduate School of Medicine.

### Cell lines and culture

Mouse melanoma cell line F10, mouse fibroblast cell line NIH-3T3, human melanoma cell lines A375, G361 and human epidermoid carcinoma A431 were obtained from the American Type Culture Collection (ATCC, USA). Normal human keratinocyte (NHK) cells and melanocyte (NHM) cells were obtained from Lonza (USA). F10, NIH-3T3, A375, G361 and A431 cells were maintained in Dulbecco's modified Eagle's medium (DMEM) (Nacalai Tesque Inc., Japan). DMEM was supplemented with 10% fetal bovine serum (FBS) (Biowest, France), 100 units/ml penicillin and 0.1 mg/ml streptomycin (penicillin-streptomycin mixed solution) (Nacalai). NHK and NHM cells were maintained in keratinocyte growth medium (KGM) (Lonza) and melanocyte growth medium (MGM-4) (Lonza), respectively.

### Preparation of tumor lysates and the isolation of sera from tumor-bearing mice

F10 cells ( $5 \times 10^6$ ) were intradermally injected into the backs of C57BL/6N mice. After 4 weeks, tumors were excised, and protein was extracted using T-PER Tissue Protein Extraction Reagent (Pierce, USA), according to the manufacturer's instructions. At the same time as the tumor excision, whole blood was collected, and the sera were isolated using Capiject Capillary Blood Collection Tubes (Terumo Corp., Japan).

### In vivo screening of tumor-homing phages and isolation of the tumor-binding scFv

F10 cells ( $5 \times 10^6$ ) were intradermally injected into the backs of C57BL/6N mice. After tumors reached 7 to 8 mm in diameter, we injected the phage library ( $1 \times 10^{13}$  CFU) dissolved in 100 μl saline into the tail veins of tumor-bearing mice. After 15 min, the animals were sacrificed by an overdose of anesthetic and perfused via the heart with 100 ml of PBS [15]. Next, the tumor tissue was snap-frozen in liquid nitrogen and homogenized in a mortar. Tumor-homing phages were eluted by using 500 μl of 0.1 M glycine (pH 2.2) for 15 min, and then the solution was neutralized with 50 μl of 2 M Tris-HCl (pH 8). Next, 50 μL of Protein A (GE

Healthcare, USA) was added to the neutralized phage solution, and the mixture was rotated for 1.5 h at 4°C. After washing with PBS to remove unbound phages, phages bound to protein A were used to infect log-phase HB2151 for 1 h at 37°C; then, the cells were plated on 2×YT agar plates containing 100 μg/ml carbenicillin. After 16 h of incubation at 37°C, a nitrocellulose membrane soaked in 100 mM IPTG (Takara Bio Inc., Japan) for 10 min was placed on the 2×YT plate for 4 h at 37°C. The plate was stored at 4°C as a master plate for *E. coli* recovery. The membrane was washed 3 times with PBS containing 0.1% tween 20 and blocked 30 min with PBS containing 5% skim milk (Nacalai). Then, the membrane was incubated with tumor lysate followed by tumor-bearing mouse serum. The complexes of auto-antibodies bound to tumor proteins were detected with the anti-mouse IgG horseradish peroxidase-conjugated antibody (GE Healthcare) followed by ECL Western Blotting Kit (GE Healthcare).

### Identification of tumor antigen with MALDI-TOF mass spectrometry

Positive clones that were recovered from the stored 2×YT agar plate were re-plated onto a fresh 2×YT agar plate and incubated for 16 h at 37°C. Next, a nitrocellulose membrane soaked with 100 mM IPTG was placed onto the 2×YT agar plate for 4 h at 37°C. After washing with PBS containing 0.1% tween 20, the membrane was blocked 30 min with 0.5% polyvinylpyrrolidone K30 (Nacalai), and then the membrane was incubated with tumor lysate. The scFv-tumor protein complexes were stained with 0.5% ponceau (Wako Pure Chemical Industries, Ltd., Japan)/5% acetic acid in distilled water, and the membrane around the area was excised. The protein on the excised membrane was digested with 100 ng/ml trypsin (Sigma-Aldrich, USA)/40 mM ammonium bicarbonate (Nacalai) for 6 h at 37°C. Then, the solution was dried up, and saturated α-cyano-4-hydroxy cinnamic acid (Wako), 1% trifluoroacetic acid, and 50% acetonitrile was added. After desalting with a ZipTip C18, the solution was analyzed using an Ultraflex MALDI-TOF/TOF instrument (Bruker Daltonik, Germany). The mass spectrometry data were analyzed with the Mascot search engine (<http://www.matrixscience.com>).

### RT-PCR and real-time PCR

RNA was extracted using Isogen (Nippon Gene, Japan), and 1 μg of total RNA was converted to cDNA with SuperScript III (Invitrogen, USA), according to the manufacturer's instructions. Mouse bullous pemphigoid antigen 1 (bpag1), TBC1 domain family member 13 (tbc1d13), uncharacterized protein C7orf30 homolog (c7orf30), and β-actin were amplified using SYBR Premix Ex Taq (Takara Bio) and an ABI Prism 7900 sequence detector (Applied Biosystems, USA). Human BPAG1, BPAG2, and β-actin were amplified with TaKaRa Ex Taq Hot Start Version, and PCR products were analyzed by electrophoresis on 1% agarose gels. All procedures were performed according to the manufacturer's instructions.

The primers were as follows:

Mouse bpag1-f:5'- TTGGAACAGACCTGGAGACC-3'  
 Mouse bpag1-r:5'- GTTCAGCCTTTCCATTTCCA-3'  
 Mouse tbc1d13-f:5'- AGGCCAACATGGGTGTATTC -3'  
 Mouse tbc1d13-r:5'- AGGGTTTGGGTTTCAGAGGAT-3'  
 Mouse c7orf30-f:5'- GAGGGGAAGGACGCTGAC -3'  
 Mouse c7orf30-r:5'- TGGAAGCATCAAATGGATCA-3'  
 Mouse β-actin-f:5'- CCCTGCCCCTCCTCTTCC-3'  
 Mouse β-actin-r:5'- CTCGTTGCCAATAGTGATGACCTG -3'  
 Human BPAG1-f:5'- CCAGCCCGGTTAACTATTGA -3'