

of the yeast-based procedure for GPCR mutagenesis has been proven.

Human formyl peptide receptor like-1, which was originally identified as an orphan GPCR, has been used to isolate agonists for GPCRs of unknown function [77]. Histidine prototrophic selection by the *FUS1-HIS3* reporter gene was performed with secreted random tridecapeptides as a library and a mammalian/yeast hybrid $G\alpha$ subunit which allows functional coupling with the receptor. As a result, surrogate agonists as peptidic candidates have been successfully screened, and the promoted activation of formyl peptide receptor like-1 expressed in human cells has been validated with synthetic versions of the peptides.

Pheromone signaling-based screening systems – protein–protein interactions

Yeast–mammal chimeric $G\alpha$ system

Medici et al. [78] constructed an intelligent system for analysis of protein–protein interactions by managing heterotrimeric G-protein signaling in yeast (Fig. 3A). They initially found that a fusion protein between the yeast Ste2p receptor lacking the last 62 amino acids of the cytoplasmic tail and the full-length Gpa1p transduced the signal in response to the binding of α -factor in cells devoid of both endogenous *STE2* and endogenous *GPA1*. Subsequently, a yeast–mammal chimeric $G\alpha$ composed of the N-terminal 362 amino acids of Gpa1p and the C-terminal 128 amino acids of rat $G\alpha_s$ was prepared. The chimeric $G\alpha$ is able to interact with the yeast $G\beta\gamma$ complex, but is not able to interact with the yeast Ste2p receptor, and it was fused to the truncated Ste2p receptor. Although a *gpa1Δ* yeast strain harboring the yeast–rat chimeric $G\alpha$ does not respond to pheromone, a *ste2Δ gpa1Δ* yeast strain expressing the Ste2p–Gpa1p– $G\alpha_s$ fusion protein that is covalently linked to Ste2p and the chimeric $G\alpha$ displayed a strong pheromone response in the presence of α -factor. These results suggest that the specific interaction of the receptor with the C-terminus of $G\alpha$ is necessary to bring the two proteins into close proximity. This hypothesis was applied to the analysis of protein–protein interactions. It was demonstrated that the interaction of Gpa1p– $G\alpha_s$ fused to protein X and Ste2p receptor fused to protein Y permitted pheromone response signaling through the contact between Ste2p and Gpa1p– $G\alpha_s$, using the interaction between Snf1 and Snf4, which form a kinase complex regulating transcriptional activation in glucose deprivation, or between Raf and the constitutively active form of Ras (Table 1). In this system, a *gpa1Δ* haploid strain harboring the

plasmid, which complements Gpa1p function to capture Ste4p/Ste18p subunits, or a *GPA1/gpa1Δ* diploid yeast strain was used to avoid lethality by spontaneous signaling from the liberated Ste4p/Ste18p subunits.

$G\gamma$ interfering system

The $G\gamma$ interfering system (it was called a G-protein fusion system in the original literature) has been developed to monitor integral membrane protein–protein interactions and to screen for negative mutants with loss of the interaction capacity (Fig. 3B) [79]. The yeast $G\gamma$ -subunit Ste18p was genetically fused to the C-terminus of cytoplasmic protein X, and the protein X– $G\gamma$ fusion protein and integral membrane protein Y in its native form were coexpressed in a *ste18Δ* strain. The interaction between protein X– $G\gamma$ and protein Y inhibits pheromone signaling through the $G\beta\gamma$ complex, in spite of the presence of α -factor, whereas a lack of interaction between protein X and protein Y normally leads to signaling. This event might be attributed to the fact that restrictive localization or structural interruption by trapping of the $G\beta\gamma$ complex at the position of protein Y on the membrane disturbs the contact with its subsequent effector. In one example, interactions of attractive drug target candidates, syntaxin 1a and nSec1 or fibroblast-derived growth factor receptor 3 and SNT-1, were monitored, and nSec1 mutants that lost the ability to bind to syntaxin 1a were successfully identified by taking advantage of growth arrest induced through the protein–protein interaction [79] (Table 1).

$G\gamma$ recruitment system

The above-described systems for analysis of protein–protein interactions using pheromone signaling are proven techniques for selecting target proteins involved with membrane proteins. However, they might generate relatively high background signals, making them unfavorable for screening candidates by growth selection, because the machinery for distinguishing interactions does not always ensure complete inactivation of signaling in the presence of pheromone.

The $G\gamma$ recruitment system has recently been developed using the pheromone signaling pathway, and is a dependable system that completely eliminates background signals for noninteracting protein pairs in the presence of pheromone (Fig. 3C) [80]. This system can be used to investigate cytosolic–cytosolic or cytosolic–membrane protein interactions. A yeast strain with a mutated $G\gamma$ lacking membrane localization ability

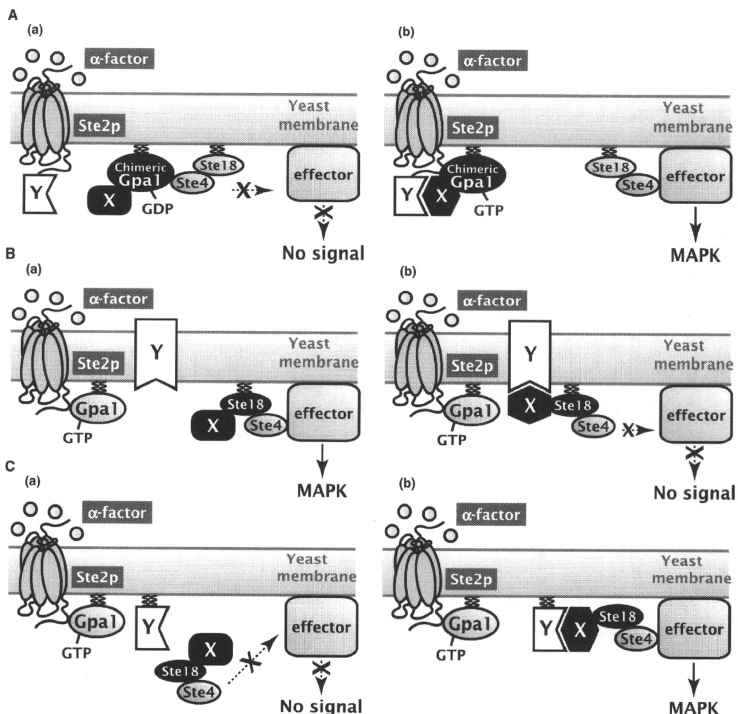


Fig. 3. Schematic illustration of pheromone signaling-based screening systems for protein-protein interaction analysis. (A) The yeast-mammalian chimeric G α system uses chimeric Gpa1p, which is able to interact with the yeast G $\beta\gamma$ complex, but not with the yeast Ste2p receptor. Chimeric Gpa1p is fused to protein X, and yeast Ste2p receptor is fused to protein Y. (a) Noninteracting protein pairs are unable to activate the pheromone signaling pathway. (b) Interacting protein pairs bring Ste2p and chimeric Gpa1p into close proximity, and permit physical contact between the two, resulting in activation of pheromone signaling. (B) The Gy interfering system can screen for negative mutants that do not interact. Ste18p genetically fused to the C-terminus of cytoplasmic protein X and integral membrane protein Y are coexpressed in a *ste18 Δ* strain. (a) Noninteracting protein pairs are unable to activate the pheromone signaling pathway, owing to the interruption of contacts between the G $\beta\gamma$ complex and its effector. (b) Interacting protein pairs are able to activate the pheromone signaling pathway, owing to the interruption of contacts between the G $\beta\gamma$ complex and its effector. (C) The Gy recruitment system can completely eliminate background signals for noninteracting protein pairs. Mutated Ste18p lacking membrane localization fused to cytoplasmic protein X and membrane-associated protein Y are coexpressed in a *ste18 Δ* strain. (a) Noninteracting protein pairs completely lack pheromone signaling, owing to the release of the Ste4p-Ste18p complex into the cytosol. (b) Interacting protein pairs restore signaling, owing to the recruitment of the G $\beta\gamma$ complex onto the plasma membrane.

(G γ_{cyto}) should be prepared by deletion of the dual lipid modification sites in the C-terminus of Ste18p, because yeast pheromone signaling strictly requires the localization of the G $\beta\gamma$ complex to the plasma

membrane [41,42]. The release of Ste18p into the cytosol eliminates the signaling ability mediated by the Ste4p-Ste18p complex [41], and this technique therefore leads to absolute interruption of background

signals. One test protein must be soluble and fused with $G_{\gamma_{\text{cyto}}}$ to be expressed in the cytosol but not the membrane, whereas the other may be soluble but should have an added lipid modification site to allow association with the inner leaflet of plasma membrane, or it may be an intrinsically hydrophobic integral membrane protein or lipidated element of a membrane-associated protein. Consequently, when the cytosolic protein X- $G_{\gamma_{\text{cyto}}}$ fusion protein and the membrane-associated protein Y are expressed in a *ste18A* haploid strain in the presence of α -factor pheromone, the interaction between protein X and protein Y restores signaling, owing to the recruitment of the $G\beta\gamma$ complex onto the plasma membrane, which can be monitored, but a lack of interaction between protein X and protein Y results in no background signaling.

In an original report, the ZZ domain derived from protein A of *Staphylococcus aureus* and the Fc portion of human IgG, which are both soluble proteins, were used as a model interaction pair (Table 1). The ZZ domain is a tandemly repeated Z domain that binds to human Fc protein and displays higher affinity than a Z domain monomer [81]. The interaction between the ZZ domain with an attached dual lipidation motif in its C-terminus and Fc fused to the C-terminus of $G_{\gamma_{\text{cyto}}}$ was easily detected with a transcriptional assay using the pheromone response *FIG1* promoter and a *GFP* reporter gene or a halo bioassay by growth arrest, whereas background signals from noninteracting pairs were never observed, owing to the loss of localization of the yeast $G\beta\gamma$ complex at the plasma membrane.

The wild-type and two variants of the Z domain that each possess a single mutation and exhibit different affinity constants were expressed as additional interaction pairs for the Fc fusion protein [82]. All variants with a wide range of affinity constants, from 8.0×10^3 to $6.8 \times 10^8 \text{ M}^{-1}$ [83], were clearly detectable, and moreover, the relatively faint interaction with an affinity constant of $8.0 \times 10^3 \text{ M}^{-1}$ was successfully detected because of the complete elimination of background signal for noninteracting pairs (Table 1). Surprisingly, a logarithmic proportional relationship between affinity constants and fluorescence intensities measured by the transcriptional assay was observed, suggesting that this approach may facilitate the rapid assessment of affinity constants.

Finally, the $G\gamma$ recruitment system has more recently been improved by the expression of a third cytosolic protein that competes with the candidate protein [102]. The competitor-introduced $G\gamma$ recruitment system could specifically isolate only affinity-enhanced variants from libraries containing a large majority of

original proteins, clearly indicating the applicability of this new approach to directed evolution.

Concluding remarks

Yeast-based approaches with the G-protein signaling machineries presented here are remarkably useful for the detection and screening of interactions of proteins involved in various biological processes. These systems are essentially comparable to the Y2H systems that have been predominantly used to screen protein-protein interaction partners from large-scale libraries and to estimate the relative strengths of interactions, but are additionally able to detect activation or inactivation associated with the switching machinery of signaling molecules, such as major pharmaceutical targets of GPCRs. Yeast-based and signaling-mediated screening systems are obviously powerful and practical tools with which to quickly screen for possible candidates. In the future, we can be sure that they will be improved, with more powerful and user-friendly advanced modifications, and will be widely applied to various fields, such as protein engineering.

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Review

Potential uses of titanium dioxide in conjunction with ultrasound for improved disinfection

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ABSTRACT

The inactivation of hazardous microorganisms is an important subject for water treatment. While the most widely used methods in water treatment systems are chlorination, ozonation, and ultraviolet ray irradiation, the drawbacks of these techniques surpass their efficacy. The potential formation of carcinogenic chemical byproducts has been reported as a drawback of chemical disinfection methods, hence there is a need to develop some alternate disinfection techniques. Ultrasonic (US) irradiation is well known as a useful technique for microbial inactivation due to its chemical and physical factors. Our recent studies indicated that the presence of titanium dioxide (TiO₂), known as a photocatalyst, accelerates the generation of hydroxyl (OH) radicals during US irradiation, and that the process is mediated through the induction of cavitation bubbles in irradiating solutions. This review describes a disinfection method that utilizes US irradiation of contaminated solution in the presence of TiO₂, a so-called "sonocatalytic disinfection" method. The significant role of OH radicals in the mechanism of cell-killing is discussed.

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1. Introduction

While water has been disinfected by various chemical and physical methods, the drawbacks of these techniques surpass their efficacy [1–4]. Chlorine has been used widely as a disinfectant, but it results in the formation of mutagenic and carcinogenic compounds in water and wastewater effluent [5,6]. Further, some microorganisms produce colonies and spores that agglomerate in large clusters. Chemical treatment of such clusters may kill microorganisms on the surface but leave the organisms under the surface intact. In the case of ultraviolet (UV) light, disinfection is affected by suspended solid particles, because microorganisms can be shielded from UV light and the formation of organic fouling on the UV lamps suppresses disinfection [7,8]. Thus, there is a need to develop some alternate techniques for water disinfection.

An ultrasonic (US) system has been used as an alternative disinfection method and has been used to oxidize contaminants in water as well as to inactivate cells [9–16]. US has been found capable of producing cell lysis and other damaging effects, such as membrane impairment, DNA degradation, organelle damage, and miscellaneous functional and biochemical changes. As illustrated in Fig. 1(A), mechanism for the inactivation of microbial cells by the US system is based on the acoustic cavitations created as a result of the growth and adiabatic collapse of bubbles in the liquid. As a result of cavitation bubble implosions, extreme temperatures and pressures are generated at the center of the collapsed bubble. One of the factors for microbial inactivation is these extreme temperatures and pressures (“physical factor” in Fig. 1(A)). Another factor for microbial inactivation is hydroxyl (OH) radicals, hydrogen peroxide, and other oxidants produced via dissociation of water molecules caused by extreme temperatures in the collapsed bubble (“chemical factor” in Fig. 1(A)) [17–19].

Recently, Shimizu and co-workers [20–22] reported that microbial cells were inactivated more effectively by US irradiation with addition of titanium dioxide (TiO₂), and that the OH radical has been shown to be responsible for the sterilization effect. This review therefore focused the disinfection by this US/TiO₂ system, and sum-

marized the following points: the enhancement of the OH radical generation by the US/TiO₂ system, the applicability of this US/TiO₂ system to degradation of organic compound and inactivation of microbial cells, membrane damage of microbial cells by US/TiO₂ system, and the possible mechanism of OH radical generation and microbial inactivation by the US/TiO₂ system.

2. Generation of OH radicals during US irradiation in the presence of TiO₂

The TiO₂ photocatalyst has been used in the degradation of different chemicals under UV light illumination since the first report of Fujishima et al. on the application of semiconductors to oxidation processes [27]. Those findings indicated that TiO₂ can catalyze the production of OH radicals and other oxidizing agents on its surface in photochemical reactions [28–31].

The application of TiO₂ under US seemed to be an efficient method for enhancing the degradation of hazardous materials [24–26]. While the detailed mechanisms have not been clarified yet, the possible roles of OH radicals in the US/TiO₂-induced degradation of hazardous materials were proposed using several OH radical scavenging agents. These agents significantly suppressed degradation, possibly due to the quenching of the OH radicals. While these results may indicate the possibility that OH radicals play important roles in degradation mechanisms, the successful application of TiO₂ in the US system first requires the clarification of the augmentation of OH radical formation in this system.

2.1. Effect of TiO₂ addition on OH radical generation under US irradiation

The OH radical has a very short half-life due to its high reactivity, and is present at extremely low concentrations. Therefore, in general, OH radical generation has been evaluated based on the measurement of aromatic molecules hydroxylated by OH radical using HPLC-ECD [32,33]. Salicylic acid has been mainly used as highly selective OH radical trapping reagent, because of the high reaction rate ($2.7 \times 10^{10} \text{ M}^{-1} \text{ s}^{-1}$) [34] and the stability of result-

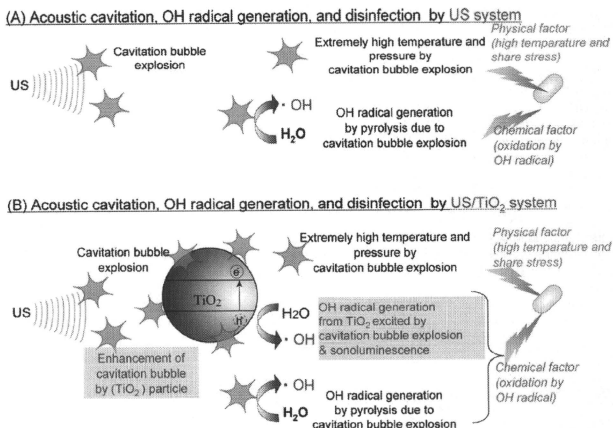


Fig. 1. Conceptual illustration for the mechanism of cavitation bubble formation and implosion, OH radical generation, and microbial inactivation by US system (A) and US/TiO₂ system (B).

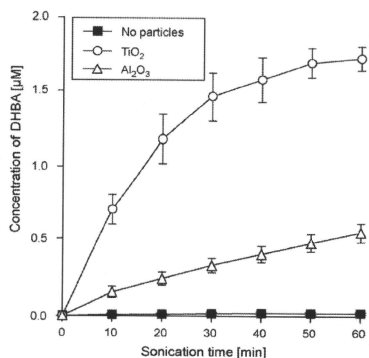


Fig. 2. Changes in DHBA concentrations during 60 min of US irradiation in the presence of TiO₂, Al₂O₃, or neither [35].

ing hydroxylated products 2,3-dihydroxybenzoic acid (DHBA) and 2,5-DHBA.

To evaluate effect of TiO₂ addition on the OH radical generation under US irradiation, the time course of the total DHBA concentration (2,3-DHBA plus 2,5-DHBA) was studied by irradiating US (frequency of 36 kHz and with a rated output power of 200 W) to the salicylic acid solution with addition of TiO₂ (2.0 mm diameter). Moreover, total DHBA concentration in the presence of TiO₂ was compared with that in the presence of Al₂O₃ (2.0 mm diameter) in order to elucidate the specificity of the sonocatalytic effects of TiO₂ [35]. As shown in Fig. 2, total concentration of DHBA changed only slightly in the absence of any particles (0.02 µM after 60 min irradiation). However in the presence of TiO₂, total DHBA concentration increased significantly with elapsed time of US irradiation, reaching plateau of 1.73 µM after 60 min. DHBA formation was significant also in the presence of Al₂O₃ particles, and the total concentration of DHBA was 0.54 µM at the 60-min irradiation period. However, the increased level was significantly lower than that of the concentration induced by TiO₂. These results demonstrate that the combination of TiO₂ plus US plays a specific role in the generation of OH radicals.

2.2. Effects of OH radical scavengers on OH radical generation by US/TiO₂ system

The oxidation mechanism was studied by employing the selected radical scavengers for this process. Dimethylsulfoxide (DMSO), methanol, and mannitol were tested as OH radical scavengers to evaluate the role of OH radicals in the oxidation of salicylic acid [36–38]. Fig. 3 compares the total concentration of DHBA produced after a 10-min irradiation period in the presence of each of these scavengers. The addition of each scavenger into the irradiating solution suppressed the formation of DHBA significantly. DMSO had the highest suppressive effect, at 200 µM. These results suggested that OH radicals were surely generated by the US/TiO₂ system.

2.3. Effects of deaeration on OH radical generation by US/TiO₂ system

The next experiment was conducted to determine whether or not the deaeration of the salicylate solution affected DHBA for-

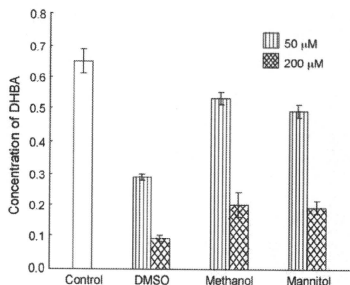


Fig. 3. Significant suppression of DHBA formation by several OH radical scavenging compounds [35]. The concentration of DHBA was measured after 10 min US irradiation with TiO₂ and salicylic acid in the presence of DMSO, methanol, or mannitol. The control indicates US irradiation with TiO₂ and salicylic acid in the absence of scavenger.

mation. Fig. 4 indicates the effect of deaeration pressure on the dissolved oxygen (DO) concentration (A) and the formation of DHBA (B) measured at 30 min after sonication began. The DO concentration of air-saturated aqueous solution was 8.5 ppm, which decreased linearly as the deaeration pressure increased. The DO concentration became almost null after 96 kPa negative pressure was applied for 30 min. The DHBA concentration decreased linearly as the deaeration pressure increased, and became almost null after 96 kPa negative pressure was applied. From the data in Fig. 4, the deaeration pressures corresponding to the half-decay concentration of DO and DHBA were estimated to be 50.0 and 51.3 kPa, respectively. These results suggest that the formation of cavitation bubbles may play an important role in the formation of OH radicals by the US/TiO₂ system.

2.4. Effects of dissolved gases on OH radical generation by US/TiO₂ system

The phenomenon of acoustic cavitation – the nucleation, growth, and collapse of small gas bubbles in liquids – is the basis of a variety of US-induced mechanical and chemical processes [18]. It is recognized that the core temperatures of cavitation bubbles are very high (several thousand Kelvin) and are affected by the properties of the gases dissolved in aqueous solution. Assuming an adiabatic collapse, the final temperature of the gas bubble (T_{ad}) can be estimated by the following equation [19]:

$$T_{ad} = T \left(\frac{R_{init}}{R_{fin}} \right)^{3(\gamma-1)}$$

where T is the temperature of the liquid, ($\gamma = C_p/C_v$) is the ratio of the specific heat at constant pressure to the specific heat at constant volume of the gas inside the bubble, and R_{init} is the initial radius of a bubble that collapses to a final radius of R_{fin} . To clarify the hypothesis that the core temperature of the cavitation bubbles may affect the sonocatalytic formation of OH radicals, we examined Xe, Ar, O₂, and N₂ with different γ values. It can be seen that the power of the dissolved gases on the formation of OH radicals was in the order Xe > Ar > O₂ > N₂. This order was consistent with the previous results of sonoluminescence [19]. Our results suggest the possibility that cavitation bubbles that collapse at higher temperature are more effective for the sonocatalytic formation of OH radicals with TiO₂. The γ values for Xe, Ar, O₂, and N₂ are 1.66, 1.67, 1.40, and 1.40, respectively. Because there

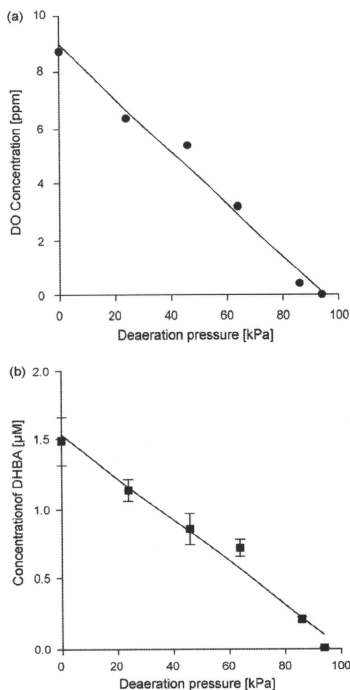


Fig. 4. The effects of deaeration pressure on the concentrations of dissolved oxygen (DO) and DHBA [35]. DO concentration (A) or formation of DHBAs (B) was measured at 30 min after the initiation of sonication.

are few differences between γ values for Xe and Ar, the final temperature seems to be almost the same under Xe and Ar atmospheres, although OH radical formation was significantly higher in the former than in the latter. Cavitation thresholds increase with increasing frequency, ambient pressure, and liquid viscosity but decrease with increasing gas content and liquid temperature [39]. The solubility of Xe is three times that of Ar, which also supports the present results, thus suggesting that OH radical formation was significantly higher under the Xe atmosphere than under the Ar atmosphere. These results also suggest that cavitation bubbles implosion may be a key for OH radical generation by the US/TiO₂ system.

3. Applicability of US/TiO₂ system to the degradation of organic compounds and microorganisms

The combined irradiation of UV and US toward TiO₂ seems to enhance the degradation ratio of organic pollutants due to the increase in the generation of OH radicals. In fact, the combination of UV and US irradiation has been reported to have a positive effect on the degradation ratio of the hazardous chemical substances in the presence of TiO₂ [40–43]. For example, it was demonstrated that

the US had a synergistic effect on the photocatalytic degradation of salicylic acid and formic acid [42], while the detailed mechanisms have not been clarified yet.

Recent observations have indicated that TiO₂ particles can enhance the oxidizing power of US even in the absence of UV irradiation [25,26]. In the following sections, applied studies of this US/TiO₂ system to the degradation of chemical substance and microbial inactivation were presented, and it was discussed that the OH radical generated by US/TiO₂ system was contributed to the disinfection.

3.1. Degradation of methylene blue by US/TiO₂ system

Following US irradiation to methylene blue solution containing TiO₂ (2 g/ml) and H₂O₂ (50 mM), the temporal changes in the spectral features of the solution were studied by monitoring the absorbance of UV–vis spectra at 665 nm [45]. Fig. 5 shows a typical absorption spectral pattern and photographs of the methylene blue solution (0.3 mM). US irradiation for 30 min significantly decreased absorbance at 665 nm, and absorbance almost disappeared after 60-min irradiation (Fig. 5(A)). As shown in Fig. 5(B), the color of the methylene blue solution containing TiO₂ and subjected to 60-min irradiation faded completely, whereas the solution of methylene blue containing Al₂O₃ showed no significant color change. This result suggested that the combination of TiO₂ plus US plays a specific role in the degradation of methylene blue. This effect could not be attributed to the adsorption of methylene blue on the surface of TiO₂ because there was no significant reduction in the methylene blue concentration during several days of incubation in the presence of TiO₂ and without any treatment. These results further indicated that the addition of H₂O₂ to the solution enhanced methylene blue degradation, and this may have been due to the fact that H₂O₂ was a more effective electron acceptor than O₂ in the solution.

3.2. Inactivation of *Legionella* by US/TiO₂ system

Diluted cell suspension of *Legionella* was treated in an US bath in the presence or absence of TiO₂ [21]. The concentrations of viable cells were then measured, based on the number of colonies formed on BCYE plates. Fig. 6 shows the effect of the presence of TiO₂ on the concentration of viable cells after the US treatment. Inactivation of *Legionella* in the absence of TiO₂ indicated that only 18% of the initial viable cells were killed after 30 min of treatment. However, the addition of TiO₂ pellets to the solutions significantly increased the disinfection power. The concentration of viable cells was reduced to 3% of the initial value in the presence of 1.0 g/ml TiO₂ after a 30-min treatment period. This enhancing effect cannot be attributed to the aggregation or adsorption of cells. When no treatment was provided, there was no reduction in cell concentrations during the incubation of *Legionella* in the presence of TiO₂.

Disinfection efficiency in the presence of TiO₂ was compared with that in the presence of Al₂O₃ in order to elucidate the specificity of the sonocatalytic effects of TiO₂. The same size and amount of Al₂O₃ pellets (diameter = 2.0 mm) that were used for TiO₂ were added to the treatment solutions, followed by a 15-min treatment period. Fig. 7 shows the relative concentrations of viable cells after 15 min of treatment in the presence of 0.3 g/ml of Al₂O₃ and TiO₂. These results indicate that the inactivation efficiency of *Legionella* was larger in the presence of TiO₂ compared with that in the presence of Al₂O₃, indicating that there is the sonocatalytic effects observed specifically in the case of TiO₂. The possible scenario for the sonocatalytic effect will be explained in the following section.

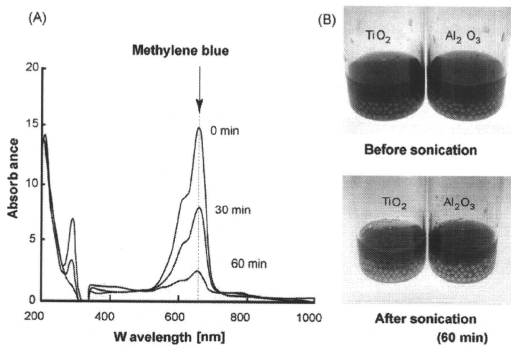


Fig. 5. (A) Temporal spectral changes in methylene blue solution containing TiO_2 and H_2O_2 under US irradiation [45]. The 665 nm absorption band was selected to monitor the temporal concentration changes of methylene blue dye. (B) Degradation of methylene blue solution containing TiO_2 pellets after 60-min US irradiation.

3.3. Effects of radical scavenging compounds

The mechanism of microbial inactivation by US/ TiO_2 system was investigated by examining the effects of selected radical scavengers on the cell-killing process. It has been reported that glutathione can inhibit the photodynamic DNA strand-breaking activity of TiO_2 [46]. In addition, an *in vivo* elevation in glutathione concentrations in the rat brain has been reported to reduce the protein oxidation induced by OH radicals [47]. Therefore, glutathione was tested as a scavenger of OH radicals to evaluate the role of such radicals in this process. Different concentrations of this glutathione were added to the treatment solutions, and *Legionella* concentrations were measured after a 15-min treatment period. The results clearly show that the presence of glutathione suppresses the disinfection process at concentrations above 10 mM and that the scavenging effect is proportional to the concentration of glutathione in the applied range (data not shown). From these results, it was confirmed that the OH radical generation by US/ TiO_2 system was contributed to the microbial inactivation, as suggested in Fig. 1(B).

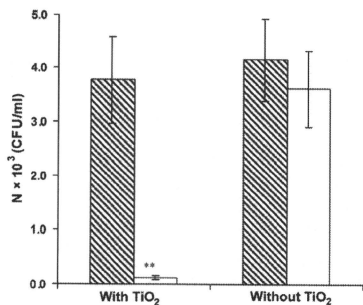


Fig. 6. The effect of TiO_2 on the number of remaining viable *Legionella* cells before (shaded columns) and after a 30-min US treatment (open columns) at a concentration of TiO_2 of 1.0 g/ml [21]. **Significantly different from the control ($p < 0.01$, one-way ANOVA).

4. Microbial membrane damage following disinfection by US/ TiO_2 system

Maness and co-workers [23] reported for the first time that the lipid peroxidation reaction is the mechanism underlying the death of *E. coli* by photocatalytic TiO_2 reaction. Therefore, microbial membrane damage and DNA leakage during disinfection by sonocatalytic TiO_2 reaction was examined to investigate the killing mechanisms.

4.1. Membrane damage by US/ TiO_2 system

To investigate damage of cellular membrane by US/ TiO_2 system, a fluorogenic assay method was applied and the release of 4-methyl-7-hydroxycoumarin upon cell lysis was measured by a fluorescence spectrophotometer [22]. In this method, 4-methylumbelliferyl- β -D-glucuronide (MUG) was added to *E. coli* culture and was incubated at 37 °C for 4 h. MUG was taken up by *E. coli*

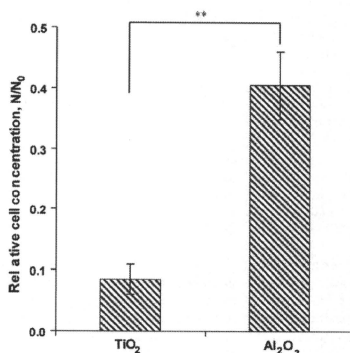


Fig. 7. Inactivation of *Legionella* in the presence of Al_2O_3 or TiO_2 after a 15-min treatment period [21]. Initial cell concentration, 4.0×10^3 CFU/ml. ** $p < 0.01$ (one-way ANOVA).

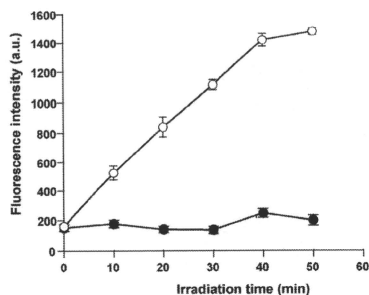


Fig. 8. The effects of TiO₂ on the release of 4-methyl-7-hydroxycoumarin during US irradiation of *E. coli* solution [22]. Open circles, US irradiation in the presence of TiO₂; filled circles, US irradiation without TiO₂.

during this period and converted to 4-methyl-7-hydroxycoumarin by β -glucuronidase intracellularly. This compound has fluorescent characteristics and can be detected by a fluorescence spectrophotometer upon leakage from *E. coli* cells. Fig. 8 shows the variation in the fluorescence intensity of irradiated samples during US irradiation that indicates the leakage of this compound into the solutions. US irradiation in the absence of TiO₂ was found to have no considerable increase in the amount of leaked fluorescent agent. Also, the results obtained in the blank samples containing TiO₂ and in the silent condition did not show any cell lysis during the incubation period. However, the amount of 4-methyl-7-hydroxycoumarin leaked during the irradiation period in the presence of TiO₂ was increased significantly, suggesting a high cell lysis rate under this condition.

4.2. Leakage and subsequent degradation of DNA by US/TiO₂ system

The effect of TiO₂ on cell lysis was further studied by analyzing the leakage and the subsequent degradation of DNA during US irradiation. Sonicated samples were pretreated to separate the leaked DNA and then were analyzed by agarose gel electrophoresis. The results of electrophoresis are shown in Fig. 9, which compares DNA fragments obtained in the samples, which were irradiated ultrasonically in the presence of TiO₂, with the extracted intact DNA of *E. coli*. DNA leakage and degradation were obvious during the irradiation period, and the resultant fragments indicated that the degradation was preceded by an irradiation period. This may be an indicative of a high rate of cell lysis during US irradiation in the presence of TiO₂. DNA fragmentation was clearly taking place within 5 min of irradiation, after which the degradation of DNA resulted in smaller fragments. This amount of degradation indicates a high ratio of cell lysis during the 5-min irradiation period, compatible with the high ratio of cell-killing under these conditions.

The results of electrophoresis were compared with the samples that were irradiated ultrasonically with no particles. US irradiation's effect on the release and degradation of DNA was not significant in the samples containing no particles. In addition, the results indicate that US irradiation to *E. coli* in the presence of Al₂O₃ resulted in cell lysis followed by degradation of leaked DNA during the irradiation period. Al₂O₃ particles may also induce a high degree of cavitation in the US system, resulting in high rates of cell lysis and disinfection. However, TiO₂ particles have been reported

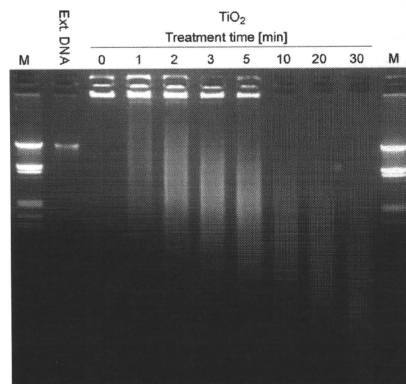


Fig. 9. Agarose gel electrophoresis analysis of DNA leaked from *E. coli* during US irradiation in the presence of TiO₂ [22]. Initial concentration of *E. coli* was 3.8×10^8 cells/mL. M, DNA size marker; Ext. DNA, extracted chromosomal DNA from *E. coli*.

to exert higher biocidal effects in US systems compared to Al₂O₃ particles [20]. To elucidate the difference between the effects of these two kinds of particles, a quantitative analysis was applied to determine the synergistic effect of TiO₂ in this process.

4.3. Quantitative analysis of DNA leaked by US/TiO₂ system

For quantitative comparison between the results obtained in the presence of TiO₂ and Al₂O₃ particles, the absorbance of leaked DNA in the irradiated solutions was determined at 260 nm. US irradiation in the presence of TiO₂ caused the leakage of more DNA into solution, indicating a higher cell lysis rate under these conditions. Also, leakage depended on time, and the absorbance of samples increased during the sonication period. However, these increases were leveled off after 15 min of irradiation; this is likely due to the termination of degradation of the leaked DNA in the solution.

US irradiation in the presence of Al₂O₃ also increased cell lysis and consequently promotes leakage. However, DNA leakage was significantly lower than in the solutions containing TiO₂. The study also compares the effects of these particles with those of blank samples without any particles. In the absence of any particles, the effect of US irradiation on cell lysis was negligible under these conditions.

4.4. Effects of radical scavenger on DNA release

The mechanism of cell lysis was further studied by investigating the effects of radical scavengers on the concentration of DNA leaked in the irradiated solutions. It has been reported that glutathione can inhibit the photodynamic DNA strand-breaking activity of TiO₂ [47]. The suppressing effects of this scavenger on *E. coli* inactivation were also reported in the previous paper [20]. Therefore, the effects of different concentrations of glutathione on the concentration of DNA leaked during US irradiation were studied. Glutathione was found to suppress the leakage of DNA during US irradiation, likely showing the suppression of cell lysis too. This suppressive effect was found to be concentration-dependent as well. Therefore, these results may indicate that OH radicals have a primary role in the degradation of DNA as well as cell lysis.

5. Possible mechanisms of enhanced OH radical formation and disinfection by US/TiO₂ system

The results reported herein indicate that the presence of TiO₂ accelerates OH radical formation and microbial inactivation during US irradiation even in the absence of UV irradiation. The results also lead us to propose the possible mechanisms for enhancement of OH radical formation and microbial inactivation by US/TiO₂ systems as illustrated in Fig. 1(B). The details are explained in the following sections.

5.1. Mechanisms of enhanced OH radical formation by US/TiO₂ system

The enhancement of OH radical formation by US/TiO₂ system may be mediated through the induction of cavitation bubbles in irradiating solutions, because the degassing of the irradiation solution completely blocked the formation of OH radicals in US/TiO₂ systems (Fig. 4). The presence of heterogeneous particles seems to increase the formation rate of cavitation bubbles by providing additional nuclei [44,50–53]. Cavitation increased due to the heterogeneous nucleation of bubbles would cause the induction of hot spots in the solution, resulting in the OH radical generation via pyrolysis of water. Although similar enhancements were obtained even in the presence of inert particles such as Al₂O₃, the oxidizing power obtained in the presence of TiO₂ was significantly higher than that obtained with Al₂O₃. This might be due to the OH radical generation via TiO₂ excitation under US irradiation, in addition to that via pyrolysis [48,49].

One possible reason for TiO₂ excitation under US irradiation might be very high temperatures (>5000 K) in the hot spots caused by cavitation bubble implosion, which can produce thermally excited positive holes on the TiO₂ surface. Mizuguchi et al. revealed the complete decomposition of polycarbonate mixed with TiO₂ when the mixture was heated to about 500 °C [54–56]. The mechanism was thought to be the successive decomposition of molten polycarbonate due to thermally excited positive holes at the TiO₂ surface. A large number of positive holes are expected to appear on the surface of high-temperature TiO₂. Nakajima et al. further demonstrated that the addition of TiO₂ was more effective than SiO₂ for the decomposition of 1,4-dioxane in water [57]. After examining the temperature change of water or TiO₂ suspension during sonication, they suggested that an endothermic process occurred in the TiO₂-added water, and that the thermal excitation of TiO₂ is the most plausible explanation of such a process.

Another possible reason for TiO₂ excitation under US irradiation might be the flushes of single-bubble sonoluminescence (SBSL) caused by bubble implosion. The SBSL involves intense UV light, which may induce the excitation of TiO₂ in the US system. Recent study indicated that the activation of TiO₂ photocatalyst by SBSL caused a significant decomposition of phenol and 2,4-dinitrophenol [58]. These observations may propose the possibility that US irradiation over a TiO₂ enhances the generation of OH radicals, and this effect is mediated by mechanisms similar to those of TiO₂ photocatalysis.

5.2. Mechanisms of enhanced disinfection rate by US/TiO₂ system

The improvement of disinfection rate by US/TiO₂ system may be attributed to the synergistic action of the enhancing the physical and chemical factor for cell inactivation, as shown in Fig. 1(B). With regard to the physical factor, the frequency of hot spot increased associating with the extreme high temperature and shear stress, since cavitation bubble formation and implosion increased due to the addition of TiO₂, which serve as nuclei of cavitation bubble. For the chemical factor, generation of OH radical increased via both

the sonocatalytic excitation of TiO₂ and the enhancing pyrolysis of water molecules by extreme temperature and sonoluminescence derived from cavitation bubble implosion, as described in the foregoing section.

Based on the present and previous findings, we propose a more detailed mechanism for the bactericidal effect of the TiO₂ sonocatalytic reaction. The initial oxidative damage occurs on the cell wall, where the TiO₂ sonocatalytic surface makes first contact with intact cells. Cells with damaged walls are still viable. After the wall is no longer protected, oxidative damage occurs on the underlying cytoplasmic membrane. Sonocatalytic action progressively increases cell permeability and subsequently allows the free efflux of intracellular contents, leading eventually to cell death. Free OH radicals may also gain access to cells that have damaged membranes, and the subsequent direct attack on the intracellular components can accelerate cell death. Evidence for the molecular targets of attack in the cell envelope is the subject of an upcoming report from our laboratory, in which we demonstrate that lipid peroxidation can be initiated via a TiO₂ sonocatalytic reaction and may be an important cause of cell death. The OH radicals are primarily involved in this process.

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Construction of protein-modified TiO₂ nanoparticles for use with ultrasound irradiation in a novel cell injuring method

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ABSTRACT

Recently, our group discovered an alternative titanium dioxide (TiO₂) activation method that uses ultrasound irradiation (US/TiO₂) instead of ultraviolet irradiation. The pre-S1/S2 protein from hepatitis B virus, which recognizes liver cells, was immobilized to the surface of TiO₂ nanoparticles using an amino-coupling method. The ability of the protein-modified TiO₂ nanoparticles to recognize liver cells was confirmed by surface plasmon resonance analysis and immuno-staining analyses. After uptake of TiO₂ nanoparticles by HepG2 cancer cells, the cells were injured using this US/TiO₂ method; significant cell injury was observed at an ultrasound irradiation intensity of 0.4 W/cm². Together with these results, this strategy could be applied to new cell injuring systems that use ultrasound irradiation in place of photodynamic therapy in the near future.

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Titanium dioxide (TiO₂) is a photocatalyst and reactive oxygen species (ROS) can be generated on the surface of TiO₂ by ultraviolet irradiation ($\lambda < 390$ nm).^{1,2} Because ROS strongly catalyze reactions that result in degradation of many harmful chemicals, the killing of microorganisms,^{3,4} and injury of mammalian cells,^{5,6} TiO₂ has been used as a photocatalyst in sanitization processes to maintain clean environments in hospitals.⁷ Recently, our group discovered an alternative TiO₂-activation method that uses ultrasound irradiation (US/TiO₂) instead of ultraviolet irradiation.⁸ The US/TiO₂ method produced an OH radical upon combination with methylene blue—a typical substrate for photocatalytic reactions—and other various radical scavengers. Although ultrasound irradiation in aqueous media is known to produce various ROS, including OH radicals and superoxide anion oxygen radicals (O₂⁻), it was assumed that production of ROS, including OH radicals, was enhanced using the US/TiO₂ method. Furthermore, production of ROS using the US/TiO₂ method with pellet-type TiO₂, such as ceramics, had been previously applied to chemical degradation^{9–10} and to killing microorganisms such as an *Escherichia coli*^{11,13} and *Legionella* strains.¹² The advantage of the US/TiO₂ method over the typical photo-excitation and ultraviolet irradiation methods is that it can be used on non-transparent media. Because sound waves generated by ultrasound can

transmit through non-transparent media, TiO₂ located within non-transparent media, such as the human body, can be activated by ultrasound, but not by photo-excitation or ultraviolet radiation.

Photodynamic therapy (PDT) is well-known as a novel approach to cancer treatment based on the produced ROS. Typical PDT is carried out using the combination of a photosensitizer, such as porphyrin IX, and an activator, typically a laser. PDT works by producing ROS that result in cell injury or death. However, the application of PDT is limited to the laser-irradiated area, so the clinical use of PDT has been restricted to cases of skin cancer.^{14,15}

Because the ROS generated on the surface of TiO₂ have very short half-lives,¹⁶ a large portion of the ROS disappear during diffusion in aqueous media without participating in any cell injuring or killing. Therefore, delivery of TiO₂ nanoparticles to specific target tissues is required for effective cell injuring using the US/TiO₂ method. However, TiO₂ has no cell-recognition potential. Moreover, the OH residues on the surface of TiO₂ nanoparticles easily associate with each other at neutral pH, resulting in aggregation of nanoparticles.¹⁷ After aggregation occurs, the nanoparticles are no longer able to transfer into blood and therefore have no adaptation to clinical utility. Sonezaki et al. constructed TiO₂ nanoparticles that remained in suspension at neutral pH by surface modification of the nanoparticles with polyacrylic acid (PAA) at high temperature.¹⁸ Because the dissociation constant of the carboxylic acid group of PAA is approximately $pK_a = 4.0$,¹⁹ the carboxylic acid group of PAA can dissociate

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into anionic ion in neutral pH solution, and these electric charge assist of stable formation of TiO₂ nanoparticle. In addition, the carboxylic acid group of PAA allows an immobilization of proteins to the nanoparticles via covalent bond with amino groups.

Therefore, based on the concept of ROS utilization in cancer therapy, in sanitation, and in methods of modifying TiO₂ nanoparticles, the purpose of the present study was to apply the US/TiO₂ method to mammalian cell killing or injuring via ROS production. To achieve this goal, the ability of protein-modified TiO₂ nanoparticles targeted to specific tissues was investigated. In particular, the pre-S1/S2 protein, which is part of the L protein from hepatitis B virus²⁰ and recognizes hepatocytes, was immobilized on the surface of TiO₂ nanoparticles. Subsequently, the ability of the protein-modified TiO₂ nanoparticles to produce OH radicals was investigated.

Escherichia coli BL21(DE3) (Merck KGaA Novagen, Darmstadt, Germany) was used for the recombinant protein expression. The plasmids, pGEX-GFP-pre-S1/S2 and pGEX-GFP²¹ were used for production of the fusion recombinant proteins, GST-GFP-pre-S1/S2 and GST-GFP, respectively. Using the production of GST-GFP-pre-S1/S2 as an example, a single colony of the transformant, harboring the pGEX-GFP-pre-S1/S2 plasmid, was inoculated into a test tube containing 3 ml of LB medium [1% (w/v) tryptone, 0.5% (w/v) yeast extract and 0.5% (w/v) NaCl] supplemented with 100 µg/ml ampicillin and incubated at 37 °C for 8 h with shaking (200 rpm). The culture medium (1 ml) was then seeded into a flask containing 200 ml LB medium with 100 µg/ml ampicillin, and incubated at 37 °C for approximately 3 h. When the absorbance at 600 nm of the culture medium reached 1.0 by spectrophotometer (U-3000, Hitachi, Tokyo, Japan), the cultivation temperature was decreased to 17 °C and IPTG was added to the culture medium at a final concentration of 0.1 mM for inducing of recombinant protein production. After 12 h of incubation, the cells were collected by centrifugation at 10,000g for 10 min, rinsed twice with running buffer (20 mM HEPES buffer (pH 8.0)), and suspended in 30 ml of running buffer containing 100 µg/ml PMSE as a protease inhibitor. The cytoplasmic fraction was extracted by ultrasonication on ice for 5 min (output = 100 W, duty = 40%, frequency = 20 kHz), and the supernatant was collected by centrifugation at 10,000g for 10 min. The pellet containing the inclusion body fraction was washed twice with 10 ml of wash buffer (20 mM HEPES, 0.5% (v/v) Triton X-100, and 1 mM EDTA, pH 8.0), re-suspended with folding buffer (20 mM HEPES, 1 mM DTT, and 1 mM EDTA) containing 8 M urea, and incubated at room temperature for 1 h. After centrifugation, the supernatant containing the denatured recombinant protein was dialyzed with folding buffer containing 4 M urea for 3 h at 4 °C. Subsequently, the supernatant was dialyzed with folding buffer containing 2 M urea for 3 h at 4 °C, and then dialyzed with folding buffer overnight at 4 °C. The sample then was centrifuged at 10,000g for 10 min, and the supernatant containing the recombinant GST-GFP-pre-S1/S2 protein was immobilized on PAA-TiO₂ nanoparticles as follow: Polyacrylic acid-modified TiO₂ particles (PAA-TiO₂, average diameter of 102 nm) were constructed as previously described¹⁸ using a MPT-422 TiO₂ suspension (Ishihara Sangyo Kaisha, Ltd, Osaka, Japan) as the starting material. GST-GFP-pre-S1/S2 and GST-GFP were immobilized onto the surface of the TiO₂ nanoparticles by chemical coupling at the carboxyl residue. The PAA-TiO₂ suspension (1.5% (w/v), 2.5 ml) was gently mixed with 0.5 ml of activating solution (0.2 M 1-ethyl-3-(3-dimethyl-aminopropyl)carbodiimide hydrochloride (ECD) and 0.05 M *N*-hydroxy succinimide (NHS)), and the mixture was incubated at room temperature for 1 h. Then, the PAA-TiO₂ suspension was applied to a PD-10 column (GE Healthcare Bio-Science AB, Uppsala, Sweden) to exchange the buffer solution for 20 mM HEPES buffer (pH 8.0), and remove un-reacted ECD and NHS. An eluted sample (3.5 ml) of the activated PAA-TiO₂ suspension was

mixed with 2.5 ml of the recombinant protein solution (approximately 1–2 mg/ml), and the mixture was incubated at 4 °C overnight. Subsequently, 1.0 ml of 0.1 M ethanolamine solution was added to block activated carboxyl residues and the mixture was incubated at 4 °C for an additional 30 min. The reacted mixture was separated using size exclusion chromatograph equipped with a AKTA FPLC (GE Healthcare Bio-Science AB, Uppsala, Sweden). In detail, 2.0 ml of sample was subjected to a Sephacryl S-500 HR column (16 × 300 mm, total bed volume 64 ml (GE Healthcare Bio-Science AB, Uppsala, Sweden)) that had been pre-equilibrated with 20 mM HEPES buffer (pH 7.4). Elution was performed with 0.5 ml/ml, and a sample was collected every 8 min (4 ml/tube). The size distribution of the protein-modified TiO₂ nanoparticles in each fraction was measured using a high performance particle size (HPP5001, Sysmex, Kobe, Japan). Immobilization of the recombinant protein on the TiO₂ nanoparticles was confirmed by surface plasmon resonance (SPR) analysis and sodium dodecyl sulphate polyacrylamide gel electrophoresis (SDS-PAGE). The weight of the TiO₂ particles was determined by the difference in particle weight before and after drying at 65 °C for 30 min. SPR analysis of the protein-modified TiO₂ nanoparticles was carried out using a BIACORE2000 (Biacore Life Sciences, Uppsala, Sweden). Anti-pre-S1 protein (80 µl) monoclonal antibody (0.5 mg/ml, Institute of Immunology Co., Ltd, Tokyo, Japan) was immobilized onto the CM-5 chip by chemical coupling with EDC and NHS according to the manufacturer's instruction manual. The interaction between GST-GFP-pre-S1/S2 protein-modified TiO₂ nanoparticles and the antibody was analyzed. The interactions of BSA-modified and unmodified TiO₂ nanoparticles with the antibody also were analyzed. In addition, for topographic observation of TiO₂ nanoparticles using atomic force microscopy (AFM), 10 µl of GST-GFP-pre-S1/S2 protein-modified TiO₂ nanoparticle suspension (0.002% (w/v)) was dropped onto a cover glass (Matsunami, Japan) and dried under an air atmosphere. The topographic observation and average particle size analysis were performed using the dynamic force mode of AFM (SPA400 equipped with Nanonavi computer station, SIINT, Tokyo, Japan) with SI-DF20 as a cantilever.

Recombinant GST-GFP-pre-S1/S2 protein was recovered from the inclusion body fraction of cultivated transformant *E. coli* and refolded to form the soluble protein by dialyzing with folding buffers containing graded concentrations of urea (8 M to 0 M). The recovered sample was confirmed to be a single protein, approximately 72 kDa in size, by SDS-PAGE analysis (data not shown), and the purified protein concentration was estimated to be 2.98 mg/ml using the Bradford method. The GST-GFP-pre-S1/S2 protein was immobilized on the surface of the TiO₂ nanoparticles (average diameter 102 nm, see Table 1) by chemical coupling between the terminal amino group of the protein and the terminal carboxyl group of polyacrylic acid. The protein-modified TiO₂ nanoparticles were purified by size exclusion chromatography. The protein-modified TiO₂ nanoparticle suspended in 20 mM HEPES buffer was eluted in the void fraction and was completely separated from the unbound free protein (data not shown). The protein-modified TiO₂ nanoparticle suspension was stable in culture medium for at least 2 days (Table 1), although there was slight

Table 1
Average particle size of GST-GFP-pre-S1/S2-modified TiO₂ nanoparticles

Particle type	Average size (nm)
PAA-TiO ₂	102
GST-GFP-pre-S1/S2 immobilized TiO ₂ (immediately)	120 ^a
GST-GFP-pre-S1/S2 immobilized TiO ₂ (after 1 day)	136 ^a
GST-GFP-pre-S1/S2 immobilized TiO ₂ (after 2 days)	174 ^a

^a The particle size distribution analysis was performed after re-suspension in DMEM.

particle aggregation after static incubation at 4 °C. Furthermore, AFM analysis of GST-GFP-pre-S1/S2-modified TiO₂ nanoparticles showed protein-modified TiO₂ nanoparticles were of similar diameter (Fig. 1), and the average particle size based on topographic measurements was estimated to be 152 nm (data not shown). Each evaluation result was well agreed, and strongly indicated that the protein-modified TiO₂ nanoparticle form 100 to 150 nm scale size nanoparticle without particle aggregation. The molecular interaction between the anti-preS1 antibody and the protein-modified TiO₂ nanoparticles was investigated using a SPR sensor. First, a solution of free GST-GFP-pre-S1/S2 protein was applied to a CM-5 chip coated with anti-pre-S1 antibody equipped with BIACORE2000 (Fig. 2A). The resonance unit was increased in a dose-dependent manner and the antibody immobilized on the chip recognized pre-S1 protein. Next, GST-GFP-pre-S1/S2-modified TiO₂ nanoparticles were applied to the same chip (Fig. 2B). Although the immobilized protein concentration of the TiO₂ nanoparticle suspension was 0.8 μM, a significant interaction was observed. As a control, TiO₂ nanoparticles were modified with the same concentration of bovine serum albumin (BSA); there was no significant increase in the resonance unit. Therefore, it was concluded that the GST-GFP-pre-S1/S2 protein was covalently bound by chemical coupling to the surface of the TiO₂ nanoparticles without any denaturation of the protein.

Human hepatoma HepG2 cells were cultured in Dulbecco's modified Eagle medium (DMEM, Nakarai Tesqu, Kyoto, Japan), supplemented with 10% (v/v) fetal bovine serum (FBS; Invitrogen GIBCO, Carlsbad, CA, USA), 60 μg/ml penicillin (Nakarai Tesqu, Kyoto, Japan), and 100 μg/ml streptomycin (Nakarai Tesqu, Kyoto, Japan). The cells were maintained at 37 °C and under a 5% CO₂ atmosphere. Approximately 2×10^5 HepG2 cells, counted by hematology, suspended in 2 ml DMEM were seeded in 35-mm culture dishes and incubated for 24 h. Then, the recombinant protein-modified TiO₂ nanoparticles suspension were added to the culture medium at a final concentration of 0.01% (w/v) (=0.1 g/l) of TiO₂ and cultured for an additional 6 h because it was reported about the complete uptake of BNC was attained within 6 h in HepG2.²⁰ After additional cultivation, the culture dishes were washed twice with 500 μl of PBS(-) buffer. To immobilize the cells, 500 μl paraformaldehyde (PFA) solution (4%) was added to the dish, followed

by incubation at room temperature for 15 min. After removal of the PFA solution, cells were permeabilized with 500 μl of 0.25% (w/v) Triton X-100 in PBS(-) buffer for 15 min. Then, the primary antibody solution (500 μl of 1 μg/ml anti-pre-S1 or 4.4 μg/ml anti-GFP monoclonal antibody (Nakarai Tesqu, Kyoto, Japan)) in PBS(-) buffer was added to the dish, followed by an overnight incubation at 4 °C. After washing three times with 0.03% (w/v) Triton X-100 in PBS(-) buffer, the secondary antibody solution (500 μl, 4 μg/ml Alexa Fluor 555 goat anti-mouse IgG antibody (Invitrogen, Carlsbad, CA, USA)) was added to the dish, followed by incubation at room temperature for 1 h. After washing three times with 0.03% (w/v) Triton X-100 in PBS(-) buffer, uptake of protein-modified TiO₂ nanoparticles by HepG2 cells was observed using a fluorescent microscope (BZ-8000, KEYENCE, Osaka, Japan). After incubation of HepG2 cells with protein-modified TiO₂ nanoparticles for 6 h, the uptake of TiO₂ nanoparticles was observed by fluorescent microscopy (Fig. 3). Cell morphology was unchanged by incubation with TiO₂ nanoparticles (Fig. 3A, C, G, and I) or with free protein (Fig. 3B and H). Free GST-GFP-pre-S1/S2 protein recognized HepG2 cells, and its clearance was nearly complete after a 6-h incubation period (Fig. 3E and K). The uptake of GST-GFP-pre-S1/S2-modified TiO₂ nanoparticles also was observed by staining with anti-preS1 and anti-GFP monoclonal antibodies (Fig. 3D and J). The fluorescence signal was observed proximal to the cell membrane. The GST-GFP-pre-S1/S2-modified TiO₂ nanoparticles appeared to adhere to the cell membrane, but did not translocate into the cytosol fraction. As a negative control, the uptake of GST-GFP-modified TiO₂ nanoparticles also was investigated (Fig. 3F and L); there was no evidence of GST-GFP-modified TiO₂ nanoparticle uptake. In addition, there was no evidence of non-specific endocytosis of TiO₂ nanoparticles by HepG2 cells (Fig. 3L). Based on these observations, it was assumed that the GST-GFP-pre-S1/S2-modified TiO₂ nanoparticles specifically recognized the HepG2 cells.

Aminophenyl fluorescein (APF, Daiichi Pure Chemicals Co., Ltd, Tokyo, Japan) was used to quantify OH radicals. The APF solution (1 μM) was prepared with PBS(-) buffer. APF solution (2 ml) was added to each dish, and subsequently, protein-modified TiO₂ nanoparticles were added at a final concentration of 0.01% (w/v). Then, each dish was irradiated with high frequency ultrasound (1 MHz) at intensity varied between 0 and 2.0 (W/cm²) for 30 s. The amount of fluorescein generated from the reaction of APF with OH radicals was measured using a multi-well plate reader CytoFluor 4000 (Applied Biosystems, Foster City, CA, USA) at an excitation wavelength of 490 nm and an emission wavelength of 515 nm. OH radical generation from both rutile and anatase TiO₂ particles using ultrasound irradiation has been confirmed.⁸ This method has been established for killing of various microorganisms, such as *E. coli* and *Legionella*.^{11–13} Based on these previous findings and on the targeting potential of protein-modified TiO₂ nanoparticles, effective cell injuring using the combination of ultrasound irradiation and TiO₂ nanoparticles was investigated. First, the OH radical generation ability of TiO₂ nanoparticles in the absence of cultured cells was measured by high frequency ultrasound irradiation (1 MHz) (Fig. 4). Although ultrasound irradiation itself has OH radical-generating potential, the additional PAA-TiO₂ nanoparticles enhanced OH radical production 1.3–1.5-fold at intensity of 0.4 W/cm². In addition, the capacity of protein-modified TiO₂ nanoparticles to generate OH radicals exhibited the same response (data not shown). Therefore, it was assumed that PAA-TiO₂ nanoparticles had the potential to generate OH radicals.

For evaluating of cell injury resulting from the combination of TiO₂ nanoparticles and ultrasound irradiation, after incorporating protein-modified TiO₂ nanoparticles, HepG2 cells were washed three times with fresh DMEM (2 ml) and were then re-suspended in 2 ml DMEM. Ultrasound irradiation was performed as follows:

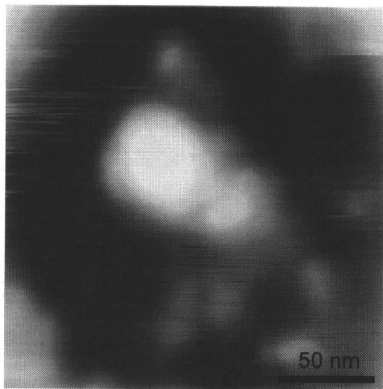


Figure 1. Topographic observation of GST-GFP-pre-S1/S2-modified TiO₂ nanoparticles using AFM. Scale bar indicates 50 nm.

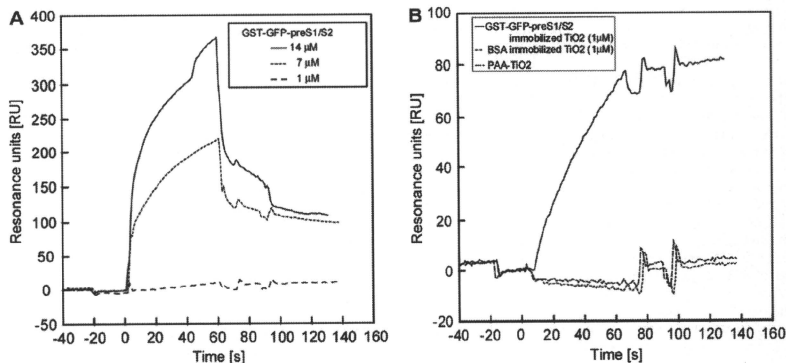


Figure 2. Confirmation of GST-GFP-preS1/S2 immobilization on the surface of TiO₂ nanoparticles. The sensorgram of free GST-GFP-preS1/S2 (A) and GST-GFP-preS1/S2-modified TiO₂ nanoparticles (B) using anti-preS1 antibody was analyzed using BIACORE2000.

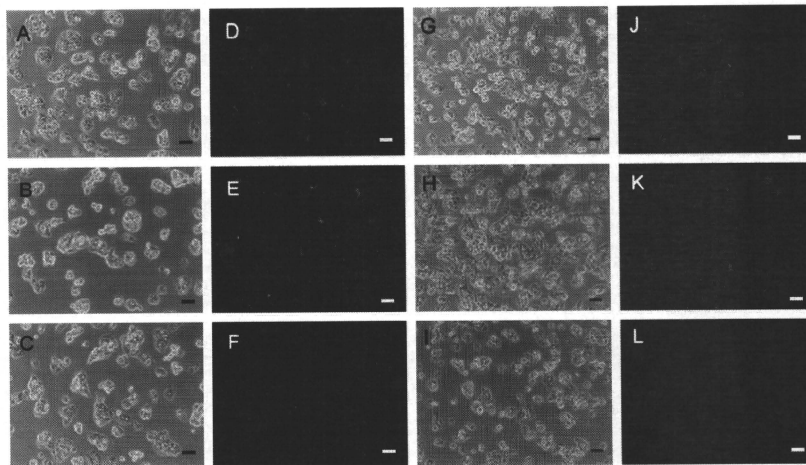


Figure 3. Immuno-staining of HepG2 for uptake of GST-GFP-preS1/S2-modified TiO₂ nanoparticles. The uptake of GST-GFP-preS1/S2-modified TiO₂ nanoparticles (A, D, G, J), free GST-GFP-preS1/S2 protein (B, E, H, K) and GST-GFP-modified TiO₂ nanoparticles (C, F, I, L) was confirmed by fluorescent microscopy after staining with anti-preS1 monoclonal antibody (A–F) and anti-GFP monoclonal antibody (G–L), respectively. Phase-contrast images are shown in panels A–C and G–I and fluorescent images are presented in panels D–F and J–L. Each scale bar indicates 50 μm.

frequency, 1 MHz; duty, 50%; and, irradiation time, 30 s. After irradiation, lactose dehydrogenase (LDH) activity leaked from damaged cells into the culture medium was measured using a CytoTox-One homogeneous membrane integrity assay kit (Promega, Madison, WIS, USA). In brief, the fluorescence intensity of the final product, resorufin, which is produced by a sequential reaction involving LDH, was measured using a multi-well plate reader, CytoFluor 4000, at an excitation wavelength of 560 nm and an emission wavelength of 590 nm. Cell-injury was performed using the US/TiO₂ method and cell damage was monitored by measuring

the amount of LDH that leaked out of the cell (Fig. 5). At 0.6 W/cm², the fluorescent intensities, which were indicative of leaked LDH, were saturated in each experimental condition; therefore, it was assumed that most cells were killed. In contrast, there were no significant differences among the three conditions at intensity of 0.2 W/cm². Therefore, this irradiation intensity was deemed insufficient for significant cell injury, as OH radicals were not generated under this condition (Fig. 4). At an irradiation intensity of 0.4 W/cm², LDH leakage was subsequently increased by addition of TiO₂ nanoparticles, and LDH activity was saturated in the

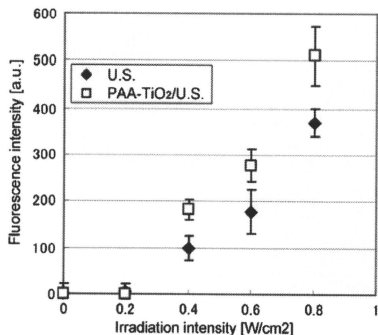


Figure 4. Measurement of OH radical generation by modified TiO₂ nanoparticles as a result of high frequency ultrasound irradiation. Generation of OH radicals was measured using ultrasonic irradiation with PAA-TiO₂ (open box) and without any particle (close diamond). Data are the mean of six independent experiments, and the error bar indicates the standard deviation.

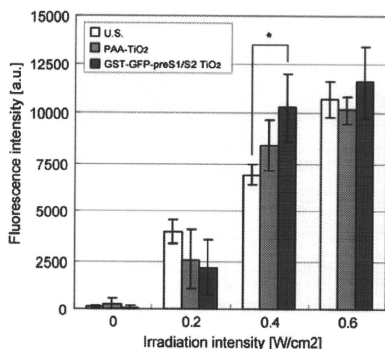


Figure 5. Membrane injury in HepG2 cells as a result of the combination of TiO₂ nanoparticles and ultrasound irradiation. LDH leaked from cells as a result of membrane injury was measured. Data are the mean of seven independent experiments, and the error bar indicates the standard error. *Significant difference between groups ($p < 0.05$, one-way ANOVA).

presence of GST-GFP-pre-S1/S2-modified TiO₂ nanoparticles. Based on these results, it was assumed that TiO₂ nanoparticles localized to HepG2 cells as a result of the pre-S1/S2 protein-enhanced OH radical generation, thereby injuring the cells.

The PAA-TiO₂ nanoparticles were approximately 100 nm in diameter, protein-modification increased particle diameter (Table 1). The increment in diameter was 20 nm, and it was assumed that the increased length was equivalent to the sum of the diameters of two protein molecules, as immobilized protein covered the TiO₂ nanoparticles in a single layer. Based on the theory of Flory, the diameter of GST-GFP-pre-S1/S2 was estimated to be 7 nm;²² therefore, the increased diameter of the nanoparticles was consistent with this theoretical estimate. The number of protein molecules immobilized on each TiO₂ nanoparticle was estimated to be 420

using the following parameters: average diameter of each TiO₂ nanoparticle, 100 nm; protein concentration of GST-GFP-pre-S1/S2, 64 mg/L; TiO₂ nanoparticle concentration, 3 g/L; specific gravity of TiO₂ nanoparticles, 4.5 g/cm³; and, the putative globule diameter of GST-GFP-pre-S1/S2 protein, 10 nm. The theoretical values for these parameters were as follows: number of protein molecules per nanoparticle, approximately 440; putative globule protein diameter, 10 nm; and, nanoparticle diameter, 100 nm. Applying these theoretical values to TiO₂ nanoparticles covered with a single layer of protein molecules, there was good agreement between the measured and theoretical number of protein molecules per nanoparticle. The theoretical estimates suggest that the surface of TiO₂ nanoparticles was completely covered with protein molecules.

The GST-GFP-pre-S1/S2 protein displayed on the surface of the TiO₂ nanoparticles was recognized by the anti-preS1 antibody (Fig. 2B), and allowed the nanoparticles to be localized to the HepG2 cells (Fig. 3D and J). Moreover, the protein-modified TiO₂ nanoparticles were capable of OH radical generation even though the particle surface was covered with protein (Fig. 4). Based on these results, it was concluded that the protein-modified TiO₂ nanoparticles have a dual function: targeting TiO₂ nanoparticles to specific cells and generating OH radicals that result in cell injury. The GST-GFP-pre-S1/S2-modified TiO₂ nanoparticles were localized in the vicinity of the cell membrane (Fig. 3D and J), while the free GST-GFP-pre-S1/S2 protein translocated to the cytosol (Fig. 3E and K). Although the fusion between hepatitis B virus and liver cells was complete after 6 h in a previous study,²⁰ only partial fusion occurred between the nanoparticles and HepG2 cells in this study. Therefore, it was assumed that the protein-modified nanoparticles cannot be cleared by endocytosis.

Ultrasound irradiation at intensity of 0.4 W/cm² and a frequency of 1 MHz to HepG2 cells that had incorporated TiO₂ nanoparticles resulted in cell damage (Fig. 5). The number of OH radicals generated in the presence of TiO₂ nanoparticles at 0.4 W/cm² was equivalent to that at 0.6 W/cm² in the absence of TiO₂ nanoparticles (Fig. 4). Therefore, it was assumed that cell damage could be induced by these OH radical concentrations, regardless of the experimental conditions. Because the high ultrasound irradiation intensity could be damage to the TiO₂ non-delivered cell, a comparable lower intensity should be required for target cell damaged irradiation. There are several possible ways to improve cell damage efficiency at lower ultrasound irradiation intensity as follows: enhance the immobilization efficiency of GST-GFP-pre-S1/S2 protein to the TiO₂ nanoparticles; improve, either directly or indirectly, the ultrasound irradiation method; and change the frequency of ultrasound irradiation. Furthermore, the combination of ultrasound and ultraviolet irradiation could be gain an advanced improvement of irradiation efficiency. In addition, the mechanism of cell injury that occurs as a result of the US/TiO₂ method warrants investigation, as it has not been studied.

As a conclusion, this is the first study demonstrating the use of TiO₂ nanoparticles to cause cell-specific damage. The protein-modification in the TiO₂ nanoparticles served the dual functions of specific cell-recognition and OH radical generation. Modification of TiO₂ nanoparticles with various targeting proteins, such antibodies or epidermal growth factor (EGF), will allow this method to be used to target specific cancer cells. Furthermore, the combination of ultrasound irradiation and TiO₂ nanoparticle will be an alternative targeted tissue specific cancer cell treatment methodology such like a PDT in the near future.

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