

SHANK3 gene were found in the patients with autism spectrum disorders [Durand et al., 2007]. On the other hand, a duplication of a distal part of 22q is less frequent. Barajas-Barajas et al. [2004] summarized clinical findings of distal trisomy 22, that is, severe mental and growth retardation, failure to thrive, congenital hypotonia, hydrocephalus, microcephaly, epicanthic folds, low-set ears, broad prominent nasal bridge, cleft palate, long philtrum, micrognathia, finger-like thumbs and cryptorchidism. Feenstra et al. [2006] reported three patients with cryptic duplication of a distal segment of 22q.

We encountered two unrelated patients with a submicroscopic duplication of 22q13. Here we describe their clinical manifestations and propose their disorder as a recognizable syndrome.

MATERIALS AND METHODS

Patient 1

The patient, a 4-year-old girl, was the first child of nonconsanguineous healthy parents. Family history

was unremarkable. She was born at 37 weeks gestation weighing 2,600 g (mean), 46 cm in length (-0.5 SD) and OFC of 32 cm ($+1$ SD). At age 4 months, she was referred to us because of generalized hypotonia and developmental delay. She started to walk unaided at 3½ years. Her mental development was moderately delayed. She used several meaningful words and could understand simple sentences. Her development quotient (DQ) was 40 estimated by the standard method. Craniofacial abnormalities noted included round face, prominent forehead, hypertelorism, arched eyebrows, downslanting palpebral fissures, broad and flat nasal bridge, shallow philtrum, low-set deformed ears and high-arched palate (Fig. 1a). She also had mild hypopigmentation of the skin and hair. Routine laboratory investigations were normal. Her G-banded karyotype was 46,XX. Her height, weight and OFC at age 4 years were 87 cm (-3.2 SD), 11.6 kg (-2.1 SD), and 46.0 cm (-2.6 SD), respectively. Brain MRI showed no significant abnormalities. EEG revealed sporadic spikes in the bilateral frontal areas. No epileptic seizures have been observed.

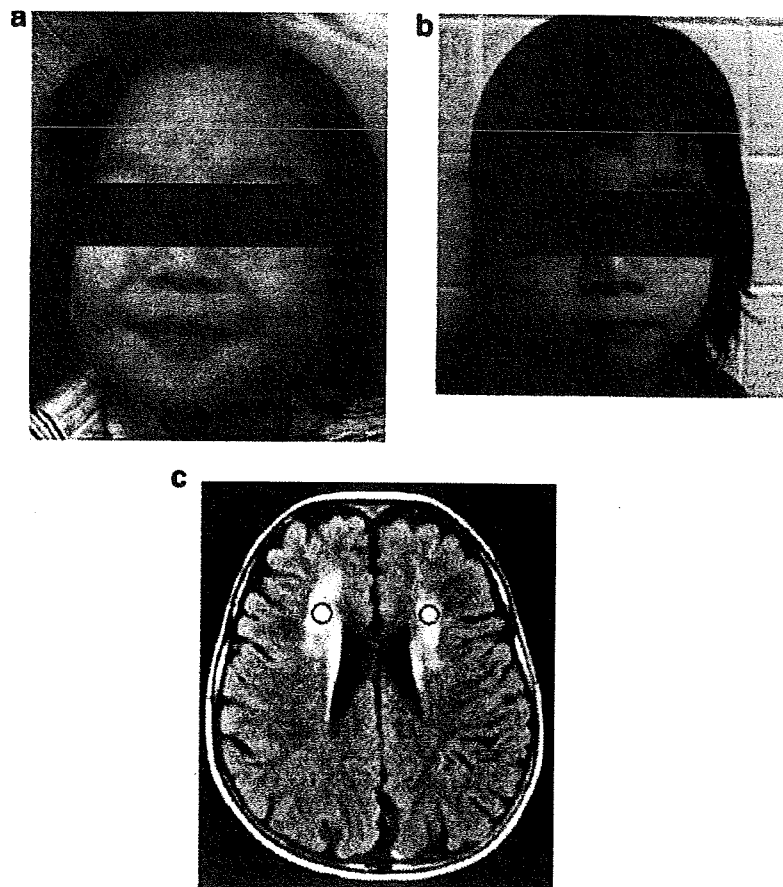


FIG. 1. Frontal view of Patient 1 at age 4 years (a) and Patient 2 at 6 years (b), and brain MRI (FLAIRE image) of Patient 2 showing prominent white matter lesions (indicated by circles) (c). [Color figure can be viewed in the online issue, which is available at www.interscience.wiley.com.]

Her character was affective and friendly, but not autistic.

Patient 2

The patient, a 6-year-old girl, was the second child of nonconsanguineous healthy parents. Her brother had severe developmental delays with a characteristic facial appearance. She was born at 40 weeks gestation. Her birth weight was 2,640 g (-0.9 SD), body length 45 cm (-1.6 SD), and OFC 32.8 cm (-0.4 SD). She was referred to us because of feeding difficulty. She was noted to have the following craniofacial abnormalities: round face, prominent forehead, hypertelorism, epicanthal folds, arch-shaped eyebrows, downslanting palpebral fissures, broad and flat nasal bridge, low-set deformed ears and high-arched palate (Fig. 1b). Her developmental milestones were delayed with estimated DQ of 46. She started to walk unaided at age 2 $\frac{4}{12}$ years. At age 6 years, she could understand simple sentences and speak several meaningful words. Initial standard G-banded karyotyping did not detect any abnormality and revealed 46,XX. Her height at age 6 years was 99.5 cm (-3.1 SD). Brain MRI showed abnormal signal intensity in the frontal white matter. The lesion was hypointense in T1-weighted image and hyperintense in T2-weighted image, whereas fluid-attenuated inversion recovery (FLAIR) image clearly demonstrated the white matter lesions (Fig. 1c). Screening for metabolic disorders was normal. Partial GH deficiency was found, and a replace therapy was started.

Analysis With Microarray Comparative Genomic Hybridization (CGH) and Fluorescence In Situ Hybridization (FISH)

The studies were approved by the Ethics Committee in Osaka Medical Center and Research Institute for Maternal and Child Health.

Patient 1 was studied with CGH on high-density Whole-Genome Microarray containing 4,523 BAC/PAC clones covering the entire genome at intervals of approximately 0.7 Mb [Inazawa et al., 2004]. Detailed methods have been reported previously [Hayashi et al., 2005]. If copy-number changes are suspected, subsequent FISH analyses were performed using BAC clones within the region of interest as probes to confirm the changes on normal metaphase chromosomes. Consequently, a duplication of the genomic region at 22q13.31–q33 was found, and its size was approximately 6.0 Mb (Fig. 2). FISH analysis using the *SHANK3* probe revealed that the duplicated segment included *SHANK3* (Fig. 3a). The *ARSA* locus at 22q11.2 deletion syndrome (data not shown). FISH analyses of her parent's chromosomes were normal (data not shown). However, we could not

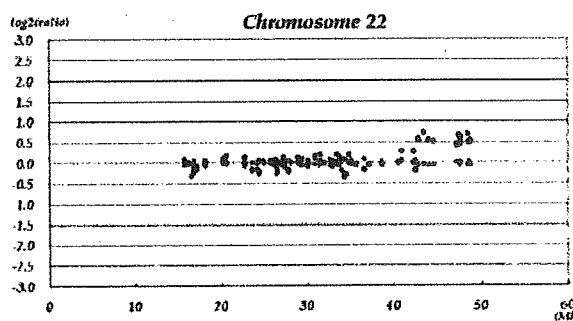


FIG. 2. Result of array CGH analysis of Patient 1. Each of the dots represents the \log_2 ratio of each BAC. Blue dots (arrow) represent results of the patient, whereas red dots represent average ratios from six independent healthy males. Copy number change in chromosome 22q13.31–13.33 is demonstrated. The duplication size was approximately 6.0 Mb. [Color figure can be viewed in the online issue, which is available at www.interscience.wiley.com.]

figure out orientation of the duplication because of its small size. Two color FISH with red and green signals showed one yellow signal. Because two patients with a distal 22q duplication derived from $\text{inv}(22)(p13q12)$ in a parent have been reported by Barajas-Barajas et al. [2004], most plausible karyotype of Patient 1 was 46,XX,ish dup(22)(qter → q13::p13 → qter)dn.

Patient 2 and her brother were screened with FISH for subtelomeric abnormality using a fosmid clone containing important domains of *SHANK3* as a probe (BACPAC resources Center, Oakland, CA; Fig. 3b). By the analysis, her karyotype was correctly interpreted as 46,XX,der(17)(22)(p13;q13). She inherited the derivative chromosome 17 from her father, who carries an apparently balanced cryptic reciprocal translocation involving the terminal regions of 17p and 22q. Duplicated segment including *SHANK3* was found at the short arm of chromosome 17 (Fig. 3b). The size of the 22q duplication was <2 Mb with further FISH analyses (Table I), and the deletion extent on chromosome 17 was <2.5 Mb from subtelomere, as the *LIS1* region was intact (data not shown). Her brother had a 46,XY,der(22)t(17;22)(p13;q13)pat karyotype.

DISCUSSION

Cryptic trisomy for distal 22q that contains the *SHANK3* gene was found in the present two patients. The trisomy in Patient 1 was de novo and that in Patient 2 was derived from paternal translocation, $t(17;22)(p13;q13)$. The clinical manifestations of her brother whose karyotype was 46,XY,der(22)t(17;22)(p13;q13) were compatible with the 22q13 deletion syndrome (PMS). Both Patients 1 and 2 had infantile hypotonia, moderate developmental delay, and growth deficiency without visceral anomalies. Craniofacial features common to them were round face, prominent forehead, hypertelorism, arch-shaped eyebrows, downslanting palpebral

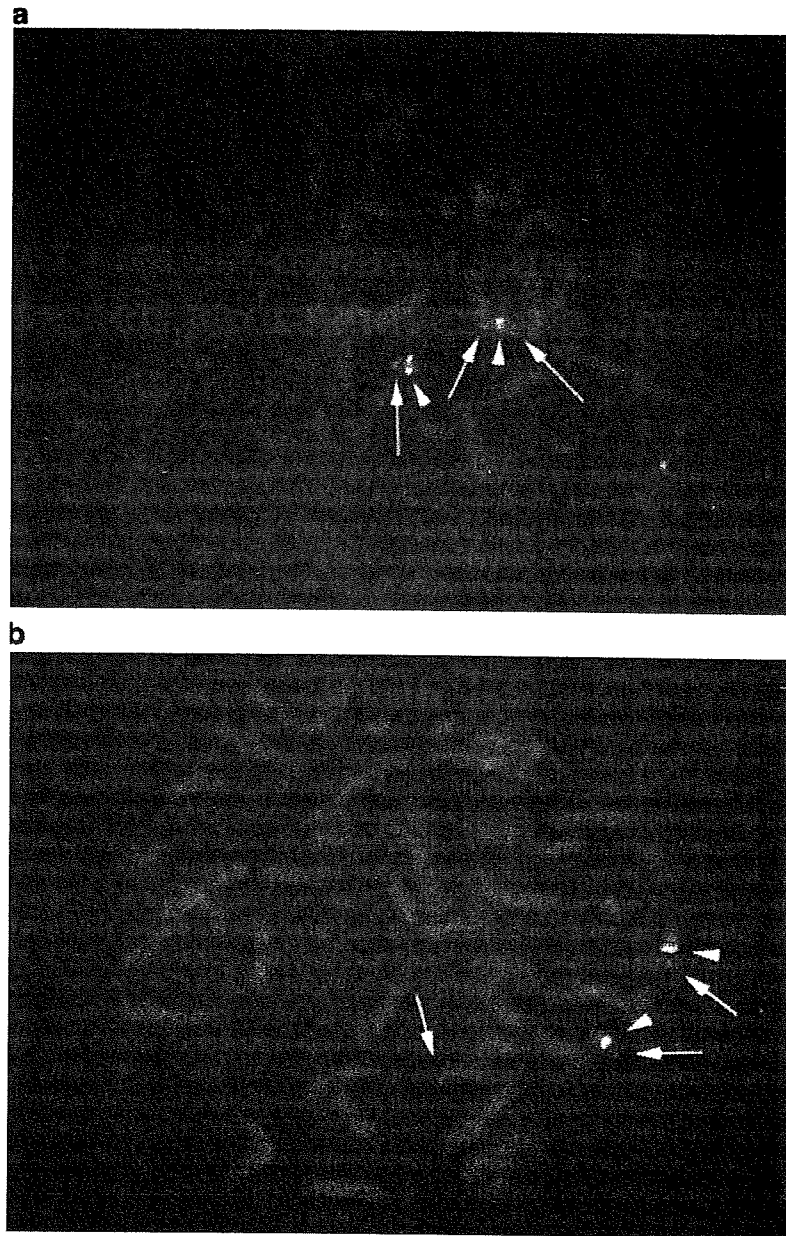


FIG. 3. FISH analysis of Patient 1 using a *SHANK3* probe (arrows) and 22q11 control probes (arrowheads) (a) showing a duplication of *SHANK3*. FISH of Patient 2 with the same probe showing another *SHANK3* signal on 17p in addition to two signals on chromosomes 22 (b). [Color figure can be viewed in the online issue, which is available at www.interscience.wiley.com.]

fissures, broad and flat nasal bridge, shallow philtrum and high-arched palate. The 22q duplicated region in our two patients seems similar to the deleted region in PMS, in which the deletion extent varied from 130 kb to 9 Mb encompassing *SHANK3*. This is not surprising, especially in Patient 2, because her duplication was derived from familial t(17;22)(p13;q13) and reflect PMS in her brother as mentioned above.

There have been three reported cases of cryptic, terminal 22q duplication [Feenstra et al., 2006]. One of them carrying a terminal 22q duplication due to a de novo unbalanced translocation, der(21)t(21;22)(p13;q13.2) had some similarities in craniofacial features to both of our patients. Growth failure and moderate developmental delay were also common. On the other hand, although one of the patients reported by Feenstra et al. [2006] also

TABLE I. Probes Used for FISH Study of Patient 2

Chromosome band	Probe	Physical distance from telomere	Result of FISH
22cen			
22q 11.2	<i>TUPLE1</i>		N
22q 13.2	<i>RP11-794G14</i>	8 Mb	N
22q 13.31	<i>RP11-766K21</i>	6 Mb	N
22q 13.32	<i>RP11-53E22</i>	2 Mb	N
22q 13.33	<i>SHANK3</i>	0.1 Mb	D
	<i>ARSA</i>	3 kb	D
22qter			D

N, normal; D, duplication.

manifested pulmonary valve stenosis and ectopic kidney, neither of our patients had such visceral anomalies. The other two patients reported by Feenstra et al. [2006] had a familial cryptic duplication of terminal 22q due to der(21)t(21;22)(p10;q13.3), and had very mild manifestations. A recent large-scale study of subtelomere FISH analysis found five patients with terminal 22q duplication that was associated with deletions of other chromosomes [Ravnan et al., 2006]. However, dysmorphic features were not described in their report. Barajas-Barajas et al. [2004] reported two patients with a distal 22q duplication derived from inv(22)(p13q12) in a parent. Distal trisomy 22q detected by conventional chromosome analysis has also been described in more than 15 patients [Barajas-Barajas et al., 2004]. Their clinical manifestations were severe mental and growth retardation, failure to thrive, congenital hypotonia, hydrocephalus, microcephaly, epicanthic folds, low-set ears, broad prominent nasal bridge, long philtrum, cleft palate, micrognathia, finger-like thumbs, cryptorchidism, sensorineural deafness, and occasional early-death. These severe phenotypes are distinct from the features of our patients with terminal 22q microduplication.

Patient 2 also had a deletion for 17p13.3-pter. *LIS1* region responsible for Miller-Dieker syndrome was conserved. Ravnan et al. [2006] reported four patients with terminal 17p deletion. The features observed among them were DiGeorge/Velocardiofacial syndrome, developmental delay and Williams syndrome. Patient 2 lacked features of DiGeorge/Velocardiofacial syndrome and Williams syndrome. We suppose that her abnormal features were attributable mainly to the duplication of distal 22q and to some extent to the terminal deletion of 17p.

SHANK3 is a multidomain protein localized in the postsynaptic density, interacts with various synaptic molecules, and is predominantly expressed in the spine during synaptogenesis [Sheng and Kim, 2000; Uchino et al., 2006]. Thus, terminal 22q duplication may cause the overexpression of *SHANK3*, resulting in interference of proper synaptic development, such as developmental deficiency and abnormal MRI signals observed in Patient 2. Durand et al. [2007] confirmed that haploinsufficiency of *SHANK3* gene is

associated with autism. They also identified a 22qter partial trisomy in a boy with Asperger syndrome. Our report may indicate that overexpression of *SHANK3* do not always cause autism.

In conclusion, we here propose a submicroscopic terminal 22q13-duplication as a clinically recognizable syndrome. This duplication may have remained undetected in many cases. Characteristic craniofacial abnormalities, and growth and developmental deficiencies with or without abnormal MRI are most prominent features suggestive of this syndrome. Therefore, such patients are recommended to undergo FISH analysis with subtelomeric probes, for example, *ARSA*, a control probe for the 22q11.2 deletion syndrome. It remains to be investigated whether neurological abnormalities in other patients with the syndrome are associated with *SHANK3* duplication.

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Direct measurement of protein dynamics inside cells using a rationally designed photoconvertible protein

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All biological reactions depend on the diffusion and re-localization of biomolecules. Our understanding of biological processes requires accurate measurement of biomolecule mobility in living cells. Currently, approaches for investigating the mobility of biomolecules are generally restricted to measuring either fast or slow diffusion kinetics. We describe the development and application of a photoconvertible fluorescent protein, Phamret, that can be highlighted by UV light stimulation inducing a change in fluorescence emission from cyan fluorescent protein (CFP) to photoactivated GFP (PA-GFP). Phamret can be monitored by single excitation-dual emission mode for visualization of molecular dynamics for a broad range of kinetics. We also devised a microscopy-based method to measure the diffusion coefficient from the fluorescence decay after photostimulation of Phamret, enabling analysis of diffusion kinetics ranging from less than $0.1 \mu\text{m}^2/\text{s}$ up to $\sim 100 \mu\text{m}^2/\text{s}$, and found significant changes in free protein movement during cell-cycle progression.

Application of GFP and related fluorescent proteins has revolutionized our ability to analyze a wide range of biological processes such as gene expression, protein localization and cell motility in living specimens. Advances in fluorescence microscopy techniques have also enabled higher-resolution imaging of the fluorescence signals from fluorescent protein fusion constructs, providing insights into the movement of biomolecules and their interactions with cellular components^{1,2}.

Among these methods, imaging fluorescence resonance energy transfer (FRET) between two fluorescent proteins provides spatio-temporal information of protein-protein interactions and protein conformational changes in living cells³. FRET is the radiation-less energy transfer from an excited donor to an acceptor fluorophore that occurs when both molecules are in close proximity within ~ 10 nm at an appropriate orientation of the dipole moment. This technology has been used to develop genetically encoded fluorescent indicators for various cellular events³.

Several microscopy techniques, including fluorescence correlation spectroscopy (FCS) and fluorescence recovery after photobleaching (FRAP), are used to investigate mobility of biomolecules

in living cells. FCS is used to determine the diffusion coefficient and the concentration of biomolecules in live cells by monitoring fluctuations in fluorescence intensity in a diffraction-limited spot of a laser beam⁴. FRAP is also used to investigate protein dynamics by photobleaching fluorescent molecules using a high-powered laser and then recording the movement of surrounding non-bleached fluorescent molecules into the photobleached area⁵. From the recovery curve, it is possible to estimate both the diffusion coefficient and immobile fraction of the tested proteins⁶.

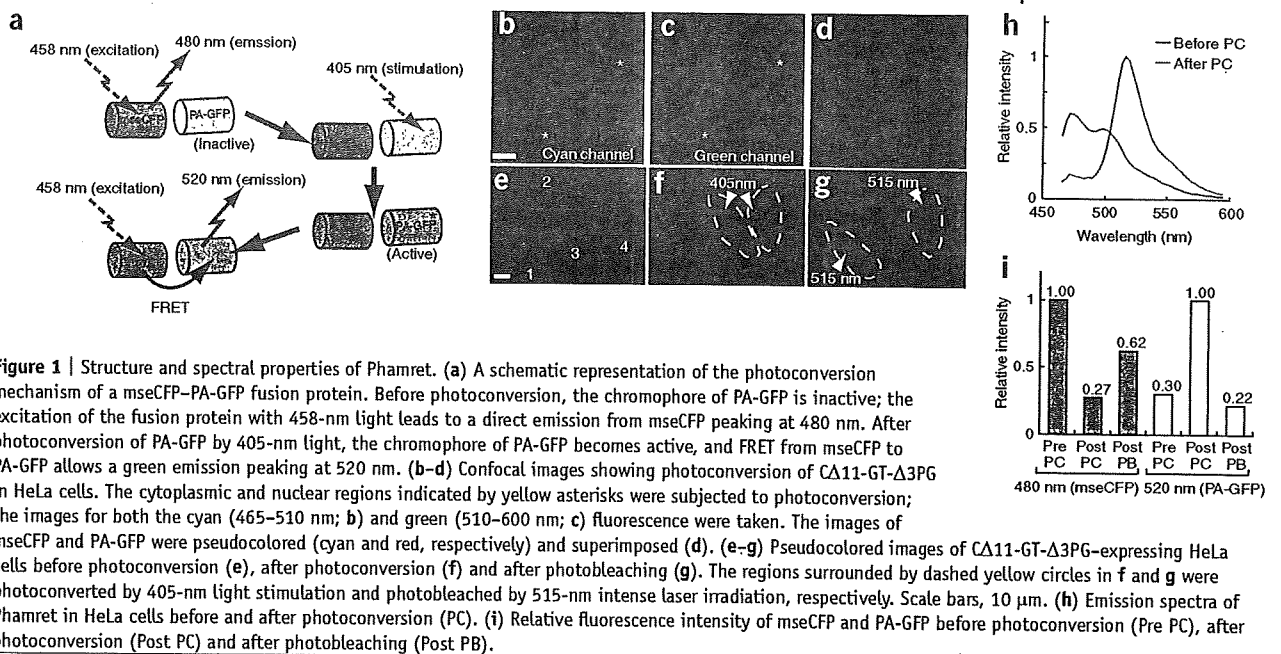
In recent years, various photosensitive fluorescent proteins have been developed by engineering existing fluorescent proteins or cloning new proteins from fluorescent organisms⁷. These photosensitive fluorescent proteins provide means to optically highlight selected proteins and to measure protein dynamics. Photosensitive fluorescent proteins can be classified into two types: photoactivatable and photoconvertible fluorescent proteins. Photoactivatable fluorescent proteins are those that are reversibly or irreversibly changed from a dark state to a bright state by photostimulation, such as PA-GFP⁸, photoactivatable mRFP1 (ref. 9), KFP1 (ref. 10) and Dronpa¹¹. In contrast, photoconvertible fluorescent proteins maintain a bright state but undergo an emission wavelength change from the pre- to post-photoconversion state by photostimulation. Examples of photoconvertible fluorescent proteins are Kaede¹², mEosFP¹³, PS-CFP¹⁴, KikGR¹⁵ and Dendra¹⁶. The ability to detect both pre- and post-photoconversion states is a preferred characteristic for live-cell imaging, but all presently available photoconvertible fluorescent proteins undergo a change in excitation wavelength in addition to the shift in emission wavelength. This therefore requires a complicated microscope setup and also makes it difficult to measure rapid molecular dynamics. Furthermore, photoconvertible fluorescent proteins except PS-CFP, mEosFP and Dendra function as oligomers, which hinders their use as protein tags.

To overcome these problems, we rationally designed a monomeric photoconvertible fluorescent protein, Phamret, that requires only one wavelength to excite both the pre- and post-photoconverted states, thus enabling quantitative observation of rapidly diffusible molecules. We also developed a microscopy method, FDAP, for measurement of rapid diffusion of molecules, up to $\sim 100 \mu\text{m}^2/\text{s}$ using Phamret or other photosensitive

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fluorescent proteins. The characteristic features of this method are (i) quick photostimulation time (0.25 ms); (ii) small light energy necessary for photostimulation ($<1 \text{ W/cm}^2$ in case of Phamret); (iii) fast acquisition of fluorescence decay (4,100 Hz) by reciprocal line scanning; and (iv) consideration of photobleaching during fluorescence decay measurement.

RESULTS

Design and evaluation of Phamret

To develop a photoconvertible fluorescent protein that can be excited by the same wavelength in both pre- and post-photoconversion states, we designed a fusion protein composed of a CFP variant (mseCFP) fused to a PA-GFP⁸ (Fig. 1a). We designed this fusion protein to emit cyan fluorescence (480 nm) in the pre-photoconverted state, which can be shifted to green fluorescence (520 nm) by UV light stimulation of PA-GFP into a FRET acceptor for the mseCFP donor (Fig. 1a). This approach requires a high FRET efficiency between mseCFP and activated PA-GFP; otherwise no or small changes in fluorescence emission can be observed after UV stimulation. To achieve a high FRET efficiency, we concatenated mseCFP containing a C-terminal 11-amino-acid truncation to PA-GFP with a 3-amino-acid truncation from the N terminus via a dipeptide (Gly-Thr) linker. The bacterially expressed chimeric protein (CA11-GT-Δ3PG) exhibited a fivefold increase in the emission ratio (520 nm/480 nm) upon brief photoactivation by 420-nm pulsed laser. When expressed in living mammalian cells, CA11-GT-Δ3PG was distributed uniformly in both the cytoplasm and the nuclei (Fig. 1b-d). Spectral imaging revealed that all fluorescent cells had an emission spectrum identical to that of mseCFP, whereas upon 405-nm laser stimulation, the fluorescence emission in the stimulated area quickly changed from cyan to green, indicative of complete maturation of both mseCFP and PA-GFP in CA11-GT-Δ3PG at 37 °C (Fig. 1e-g and Supplementary Fig. 1a-f online). Upon activation, green fluorescence increased

3.3-fold, and cyan fluorescence emission decreased 3.7-fold, resulting in an approximately 12.2-fold ratio change between the pre- and post-photoconverted states (Fig. 1h,i). To confirm that the photoconversion of CA11-GT-Δ3PG was indeed due to FRET from mseCFP to activated PA-GFP, we bleached the acceptor PA-GFP. The decrease in PA-GFP emission peak was accompanied by dequenching of the mseCFP signal (Fig. 1g-i and Supplementary Fig. 1g-i), demonstrating that the dominant mechanism of the fluorescence color change in CA11-GT-Δ3PG was caused by FRET between mseCFP and activated PA-GFP. Therefore, we named this fusion protein Phamret for photoactivation-mediated resonance energy transfer. The photoconversion of Phamret was achieved using a lower laser power density ($<1 \text{ W/cm}^2$) than that for photobleaching. Accordingly, the quantum yield for photoconversion of Phamret was 2.7×10^{-2} , which was five times greater than that for the efficient highlighter, KikGR¹⁵ (4.7×10^{-3}). pH titration of Phamret revealed that a high dynamic range (>10 -fold) was achieved in a neutral to alkaline environment ($> \text{pH } 7$), but it was strongly attenuated at acidic pH (Supplementary Fig. 2a online) and displayed a twofold dynamic range at pH 6.5. Phamret thus functions as a highlighter at physiological pH ranging from 6.5 to 8.0. Phamret was estimated to be a 53.4-kDa protein and is monomeric in living cells without displaying any unexpected binding to protein or proteolytic digestion (Supplementary Fig. 2b-d). Concordantly, Phamret in fusion with human β -actin and fibrillarin as well as targeting sequences for the Golgi bodies and the peroxisome showed an expected localization pattern (Fig. 2a-d) as reported previously¹⁷⁻²⁰. In addition, the fusion proteins did not substantially perturb cellular functions such as cell division. Furthermore, all the fusion proteins tested underwent pronounced photoconversion by 405-nm laser illumination (Fig. 2a-d). Although we successfully labeled most of the proteins tested with Phamret, labeling of α -tubulin was unsuccessful (data not shown). Optimization of the amino-acid linker sequence and length between Phamret



and the protein of interest may resolve this problem. The properties of Phamret in comparison with other photoconvertible fluorescent proteins developed so far are shown in **Table 1**.

Cellular application of Phamret

To demonstrate the applicability of Phamret to stably label the intracellular structures, we expressed Phamret in mitochondria and took time-lapse images after Phamret photoconversion in one region. During a 15-min recording, a long thread-like mitochondrion fused and divided frequently, dramatically changing the pattern of the mitochondria network (**Fig. 2e–h** and **Supplementary Video 1** online). In parallel with the changes in the mitochondria structure, the shifted fluorescence color in the photoconverted region spread out and entered a surrounding mitochondrion. In addition, the labeled region in the fused mitochondrion was exchanged until it came to equilibrium at the intermediate color, indicating conjugation of the mitochondrial matrix and diffusion of the material in the fused mitochondrion.

We also observed positioning of chromosomes during mitosis in living mammalian cells. We labeled chromosomes in HeLa cells by expressing a histone 2B–Phamret fusion protein (H2B–Phamret). Owing to the very low dissociation rate of H2B from chromatin²¹, the photoconverted marking remained detectable for many hours, allowing imaging of the dynamics of labeled chromosomes²². Just before mitosis, we photoconverted the nuclear halves and performed time-lapse imaging. In most cells (82%, $n = 14$), the global pattern of the mother cells was transmitted to the two daughter nuclei in G1 phase in a mirror-symmetric fashion (**Fig. 2i,j** and **Supplementary Video 2** online), indicating the heritability of chromosomal positions during cell division as previously shown by FRAP analysis using fluorescent protein tags in normal rat kidney cells²².

Visualization of rapid protein dynamics using Phamret

All photoconvertible fluorescent proteins described to date undergo a change in excitation wavelength in addition to the shift in

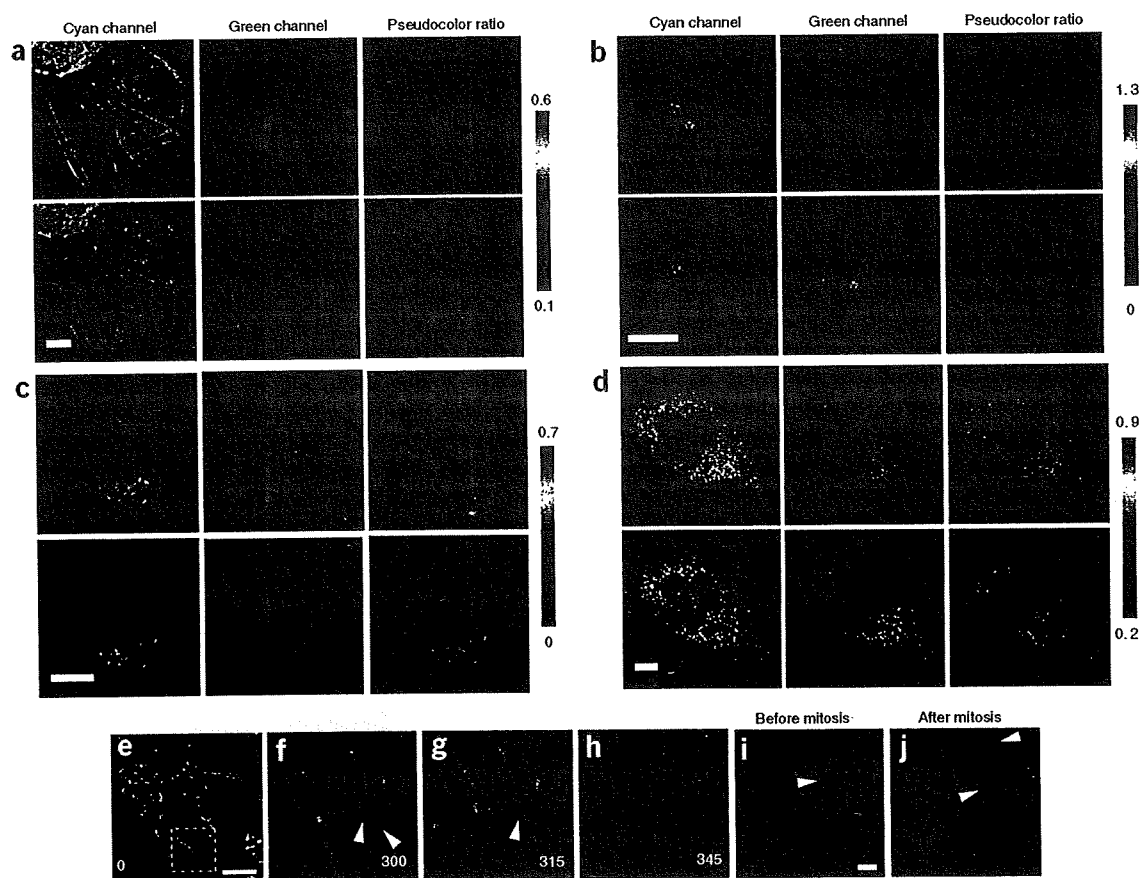


Figure 2 | Photoconversion of Phamret fusion protein in living cells. (a–d) Confocal fluorescence images of HeLa cells expressing Phamret fused to actin (a), fibrillarin (b), Golgi body localizing signal (c) and SKL tripeptide for peroxisome localization (d) before photoconversion (top) and after photoconversion (bottom) in the selected area, as shown in red (bottom right). The cyan channel, green channel and pseudocolored emission ratio (green to cyan) images are shown. Color bars represent green-to-cyan intensity ratio. (e–h) To track mitochondria, Phamret-expressing mitochondria in the selected area (as shown in red in e) were subjected to photoconversion (e). A yellow dashed box in e shows the region used for time-lapse imaging. Representative images taken at 300 s (f), 315 s (g) and 345 s (h) after photoconversion are shown. The yellow and white arrowheads in f indicate two mitochondria that were about to fuse. Arrowhead in g indicates the point of mitochondrial fusion, which was followed by spreading of Phamret protein in the fused mitochondrion (h). (i,j) Tracking of H2B–Phamret during mitosis. Half of the nucleus (arrowhead) being photoconverted just before mitosis (red; i). The daughter nuclei (arrowheads) show the preserved color pattern (j). Scale bars, 10 μm .

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Table 1 | Properties of known photoconvertible proteins

Protein	Fluorescence color		Observed wavelength ^a (nm)		Stimulation		Oligomeric status	Ref.
	Before photoconversion	After photoconversion	Excitation	Emission	Wavelength (nm)	Power density (W/cm ²)		
Phamret	Cyan		458	475	405	<1 ^b ($\Phi_{PC} = 2.7 \times 10^{-2}$) ^b	~15 ^b	Monomer
	Green		458	517				
PS-CFP	Cyan		435	468	405	5–10	~1,500	Monomer
	Green		490	511				
Kaede	Green		488	518	405	1.3	~2,000	Tetramer
	Red		543	580				
KikGR	Green		488	517	405	~1 ($\Phi_{PC} = 4.7 \times 10^{-3}$)	NS	Tetramer
	Red		543	593				
EosFP	Green		488	516	405	NS	NS	Tetramer
	Red		543	581				
d2EosFP	Green		488	516	405	500	NS	Dimer
	Red		543	581				
mEosFP	Green		488	516	405	NS	NS	Monomer
	Red		543	581				
Dendra	Green		488	505	488	1.5	~1,500–4,500	Monomer
	Red		543	575	405	0.6		
Cy11.5	Yellow		440	527	515 (bleaching)	>10 ^b	NS	Monomer
	Cyan		440	476				

^a Φ_{PC} quantum yield for photoconversion, NS, not stated.

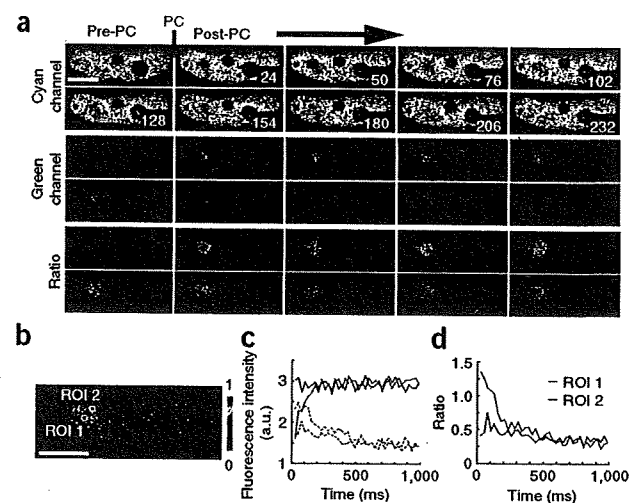
^bWavelength of excitation light for live imaging by microscopy and peak of emission spectrum. ^bMeasured in our laboratory. A laser power meter was used to measure total power of the light after the objective lens. Light power density was estimated by dividing the total power by the area of the illuminated region.

emission wavelength upon photoconversion, and thus require measurement in dual excitation–dual emission mode. Generally, two different excitation wavelengths are alternated to obtain images both before and after photoconversion. This is unfavorable for observing rapidly diffusing molecules because of the acquisition time lag between two images. Even if we excite simultaneously the two states of photoconvertible fluorescent proteins, it is impractical because two lasers must be aligned to the same confocal spot by bringing two laser beams to a perfect and stable overlap. The single excitation property of Phamret overcomes this problem, but it may be possible to measure the presently available dual-excitation photoconvertible fluorescent proteins in single-excitation mode also. To address this, we compared the photoconversion contrast of Phamret with the dual-excitation photoconvertible fluorescent proteins, tandem dimer Dendra (td-Dendra), which is comparable in size to Phamret¹⁶. We expressed both proteins in HeLa cells, photoconverted them by 405-nm laser irradiation and simultaneously measured the change in fluorescence intensity of both pre- and post-photoconversion states at the frame rate of 41 Hz using an

appropriate excitation wavelength for each. At the first frame image after photoconversion, Phamret showed a 1.3-fold decrease and 2.4-fold increase in cyan and green fluorescence, respectively, yielding a 3.1-fold change in the emission ratio (Supplementary Fig. 3a online). The slower decrease in green fluorescence may be due to the photobleaching of PA-GFP moiety in Phamret. In contrast, td-Dendra had a 1.4-fold decrease in green fluorescence and no change in red fluorescence just after photoconversion, resulting in smaller contrast than for Phamret (Supplementary Fig. 3b). These results indicate that when using the single excitation–dual emission mode for fast frame acquisition, Phamret promises a higher contrast than Dendra. To further evaluate this,

Figure 3 | Visualization of rapid protein dynamics using Phamret.

(a) Confocal images of donor CFP (top), acceptor PA-GFP (middle) and pseudocolored emission ratio (green/cyan; bottom) showing diffusion of photoconverted PP2Cy-Phamret. Images were taken every 26 ms. (b) A magnified view of the first image just after photoconversion. The white circles (diameter 1.10 μ m) represent ROIs used for intensity calculation. ROI 1 was set on the photoconverted circular region (diameter 1.38 μ m). ROI 2 was placed outside of the photoconverted region. Distance between the centers of two ROIs is 2.1 μ m. (c) Time course of cyan (solid line) and green (dashed line) fluorescence intensity of Phamret in ROI 1 (red) and ROI 2 (blue). (d) Time course of green to cyan emission ratio in ROI 1 and ROI 2. Scale bars, 10 μ m.



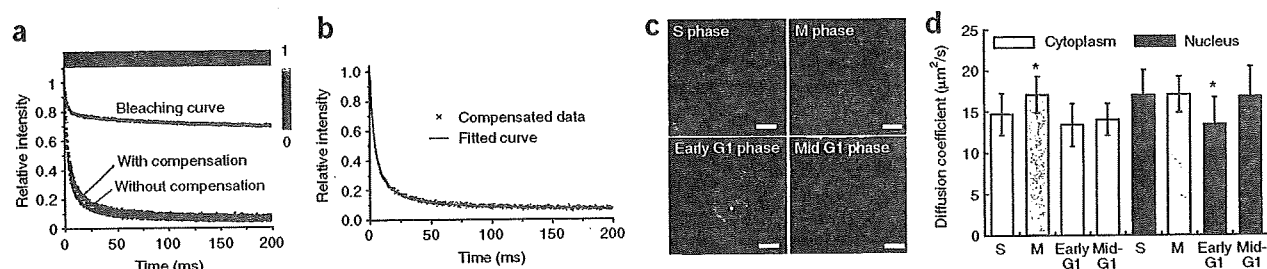


Figure 4 | Determination of diffusion coefficient of Phamret by FDAP. (a) Line-scanned images of photoconverted Phamret in solution were taken, and the kymographs of the images are shown in pseudocolor (top). Color bar indicates normalized fluorescence intensity. Average fluorescence decay curves in the solution were calculated (bottom). The blue curve represents the bleaching of photoconverted Phamret during image acquisition. (b) The compensated fluorescence decay curve determined by equation (3). (c) Fluorescence images of a cell at the indicated cell-cycle stages used for FDAP measurements. Scale bar, 10 μm . (d) Diffusion coefficient of Phamret in the cytoplasm and the nucleus at the indicated cell-cycle stages. In the case of M phase, the same data are shown (light gray bars) because the cytoplasm and nucleus cannot be distinguished due to the disappearance of the nuclear membrane. Asterisks (*) indicate the cell phase where the diffusion coefficient is significantly different from other phases in either the cytoplasm or nucleus, respectively. Error bars are s.d. ($n > 10$). Validity of the differences was statistically confirmed by one-way analysis of variance (ANOVA) and defined as significant at $P = 4.0 \times 10^{-6}$ and 4.1×10^{-4} , respectively. Differences between cytoplasm and nucleus in S and G1 phase were also confirmed by using two-sided t -test ($P = 0.005$ and 0.008) with significance level $\alpha = 0.05$.

we examined a PP2C γ -Phamret fusion protein in the nucleus of a HeLa cell. After photoconversion of PP2C γ -Phamret in a region of the nucleus, we acquired fluorescence images at 41 Hz that show how fast the photoconverted PP2C γ -Phamret diffuses (Fig. 3 and Supplementary Video 3 online).

Determination of biomolecule diffusion coefficients

To determine diffusion coefficients of proteins tagged with photosensitive fluorescent proteins, we devised a new microscopy technique that enables measurement of a wide range of diffusion coefficients. This technique, FDAP, is based on measurement of fluorescence decay after photostimulation of photosensitive fluorescent proteins by quick (0.25 ms) photo-irradiation using a focused laser followed by repeated reciprocal line scanning at 4,100 Hz. We used a laser confocal microscope equipped with a dual laser scanner to carry out photostimulation during fluorescence measurement. We used Phamret as the photosensitive fluorescent protein, and measured the diffusion coefficient in aqueous solution (Fig. 4a). When we used averaged fluorescence decay data derived from 10 measurements directly for fitting by Eq. 3, the estimated diffusion coefficient was $70.4 \pm 0.8 \mu\text{m}^2/\text{s}$. This value is much larger than $50.4 \mu\text{m}^2/\text{s}$ determined by FCS for the GFP tandem dimer²³. Because the FDAP experiment required about ten times more intense laser irradiation for excitation than that used in FRAP to acquire line images with a high-enough signal-to-noise ratio, we speculated that the difference in measured diffusion coefficients was due to photobleaching of PA-GFP moiety in Phamret during the fluorescence decay measurement (Supplementary Fig. 3a). To estimate the influence from photobleaching, we recorded a time course of fluorescence intensity using fully photoconverted Phamret in solution or in a cell in which we

neglected the fluorescence decay caused by the molecular diffusion. Although the fluorescence attenuation rate in FDAP was larger than that expected from simple bleaching immediately after starting the measurement, the total number of bleached molecules was comparable between FDAP and FRAP at the end of measurements (Supplementary Fig. 4a,b online). We used the measured decay curve (Fig. 4a) for data compensation and applied the compensated data for nonlinear curve fitting (Fig. 4b). The diffusion coefficient after correction was $49.5 \pm 0.6 \mu\text{m}^2/\text{s}$, which was almost equivalent to the previous FCS data²³. Recently, a method to measure faster diffusion using FRAP by attempting to account for the finite time of the photobleaching has been proposed²⁴. Therefore, we performed FRAP measurements to compare the results with those of FDAP (Supplementary Fig. 4c–f) and FCS analyses. All three methods gave comparable results for tandem fluorescent protein dimers (Table 2). However, the diffusion coefficient of a single fluorescent protein measured by FRAP was substantially different from those obtained by FDAP and FCS, indicating that FDAP may be more reliable than FRAP for analysis of fast-diffusing molecules with $>20 \mu\text{m}^2/\text{s}$ diffusion coefficient, provided that an accurate bleaching curve can be obtained for correction of the FDAP data (Table 2).

To validate the performance of FDAP, we compared the diffusion coefficient of Phamret in HeLa cells at different stages of the cell cycle (S/G2, M, early G1 and mid-G1) as well as in different compartments, cytoplasm and nucleus (Fig. 4c). We obtained a correction curve for this experiment using fully photoconverted Phamret in HeLa cells. Generally, the diffusion coefficient of Phamret in the nucleus was greater than that in cytoplasm except in early-G1 phase in which Phamret in both nucleus and cytoplasm showed a similar diffusion coefficient (Fig. 4d). Furthermore, we found that the diffusion coefficients in the nucleus during early-G1 phase ($13.4 \pm 3.3 \mu\text{m}^2/\text{s}$) were significantly smaller than those in other phases (17.0 ± 3.1 in S phase, 17.1 ± 2.2 in M phase, 16.8 ± 3.7 in mid-G1 phase; Fig. 4d). Although the cells in M phase are classified into neither cytoplasm nor nucleus because both compartments are mixed after disappearance of the nuclear membrane, the diffusion coefficient of Phamret in M phase tends to show the

Table 2 | Comparison of FDAP with other methods

Fluorescent protein	FDAP D ($\mu\text{m}^2/\text{s}$)	FRAP D ($\mu\text{m}^2/\text{s}$)	FCS D ($\mu\text{m}^2/\text{s}$)
Single	22.9 ± 3.7	34.0 ± 8.5	23.4 ± 2.5
Tandem dimer	14.1 ± 2.4	18.3 ± 6.4	16.4 ± 0.8

value for S and mid-G1 phase nucleus, suggesting that the cellular environment of the M-phase cell was more nuclear-like than cytoplasm-like.

DISCUSSION

The microscopy method we developed, FDAP, allowed reliable measurement of diffusion coefficients up to $\sim 100 \mu\text{m}^2/\text{s}$, the measurement of which has been quite difficult using FRAP. The reason why FRAP gave a different diffusion coefficient in the comparison of FDAP and FCS, may be due to the use of the first frame image after photobleaching to calculate the bleaching constant in FRAP²⁴. The first frame image after photobleaching contains irrelevant diffusion data obtained during the photobleaching and the first image acquisition. Thus, this may affect the calculation of the bleaching constant, especially for fast-diffusing molecules, resulting in an overestimation of the diffusion coefficient. According to reference 25, the total bleaching time should be at least 15 times smaller than the characteristic recovery time²⁵. The photostimulation time of 0.25 ms in our FDAP measurement is brief enough that the diffusion during photostimulation can be neglected. Moreover, the FRAP measurement has other drawbacks: the bleaching constant needs to be determined whenever the target molecules or intracellular environment are changed because the value of the bleaching constant depends on the diffusion constant of the target molecules. In the presence of a highly immobile fraction, the bleaching profile in the first image contains contributions of both the diffusing mobile fraction and the stationary immobile fraction, requiring complex assumptions²⁴. Our FDAP method is not affected by this issue.

Compared to FCS, FDAP has the advantage of retrieving additional information regarding the states of the immobile molecules. FDAP can be used to investigate any diffusion kinetics ranging from $< 0.1 \mu\text{m}^2/\text{s}$ to $\sim 100 \mu\text{m}^2/\text{s}$. Notably, when compared with FCS, measurement time for a fast diffusible protein ($> 10 \mu\text{m}^2/\text{s}$) by FDAP is much shorter (200 ms for FDAP versus $> 10 \text{ s}$ FCS²³), which is an advantage when analyzing molecules that quickly change diffusion coefficient upon stimulation.

In the post genomic era, many cascade maps for signal transduction pathways activated by biological events have been described. These maps are very useful for understanding the mechanisms of cellular activity at the molecular level. Information on protein and molecule movement rates within cells provides enhanced understanding of not only signal transduction but also various physiological phenomena at the molecular level. The ability to measure molecular mobility over a broad kinetic range with this single technique provides a useful complement to FRAP or FCS, thus benefiting studies on molecular dynamics in living cells.

METHODS

Imaging. For cell imaging we used an Olympus confocal inverted microscope FV1000 equipped with UPLSAPO 60 \times 1.35 numerical aperture (NA) oil objective and multi-Argon ion laser. We used a 405 nm laser diode for photostimulation. We acquired the cyan and green fluorescence signals by excitation at 458 nm and detected them at 465–510 nm and 510–600 nm wavelength range, respectively. For td-Dendra imaging, we simultaneously acquired the green (495–525 nm) and red fluorescence (560–650 nm) signals by excitation at 488 nm. We created the fluorescence ratio images using AquaCosmos software (Hamamatsu Photonics).

Determination of diffusion coefficient by FDAP. We estimated the activation characteristics of the laser using fixed cells expressing Phamret. First, we photoconverted Phamret in a fixed cell by the pulse irradiation with a 405-nm laser for 0.25 ms, and measured fluorescence intensity. Then we photoconverted the whole region of the same cell again until the fluorescence came to equilibrium, and again measured the fluorescence intensity. We divided the fluorescence intensity of once-photoconverted Phamret at the position (r) from the center of the activated region by the fluorescence intensity of fully photoconverted Phamret. We fitted the divided values at different positions to the Gaussian laser profile modified from the previously published one²⁶ so that the center of the activation profile became the peak value of fluorescence intensity as described by following equation:

$$C(r) = 1 - \exp\left(-K \exp\left(-\frac{2r^2}{w^2}\right)\right), \quad (1)$$

where $C(r)$ is the concentration of the photoconverted Phamret, K is the activation constant for the fixed cells, and w is the half-width of the laser beam at $1/e^2$ intensity.

Each FDAP experiment started with image scans, followed by a 405-nm laser irradiation for 0.25 ms on a point in the scanning area. We collected a series of line scanned images of the fluorescence emission in the region of 510–600 nm at 0.244 ms intervals ($\approx 4,100 \text{ Hz}$) for 200 ms using 488-nm laser as excitation light. We skipped the first line scanning image to avoid direct influence of the irradiated pulse of the 405 nm laser. We fixed the length of line scanning to 80 pixels, and each pixel width was 103 nm. We used the central 8 pixels (0.824 μm) in the scanned line as a region of interest for the fluorescence intensity measurement. We calculated the background signals as the average intensity in the region of interest, which we measured 50 ms before photoconversion. We calculated the average fluorescence in the region of interest (ROI) at time t after the photoconversion, $I_{\text{ROI}}(t)$, from each line image with the subtracted background signal. The fluorescence signal measured in a region of interest normalized to the change in total fluorescence was determined as

$$I_{\text{rel. image}}(t) = \frac{I_{\text{ROI}}(t)}{I_{\text{max}}}, \quad (2)$$

where I_{max} is the maximum intensity after the photoconversion.

Because the measured fluorescence decay contains contribution from photobleaching, the original fluorescence decay data must be compensated. To do this, we measured a time course of the photobleaching of completely photoconverted Phamret. We then divided the originally acquired decay curve by the photobleaching curve and used the recalculated data for the curve fitting. Using the values of K and w , we fitted the FDAP decay curves of $I_{\text{rel. image}}^*(t)$ to the decay function, $I_{\text{rel. calc}}(t)$ modified from that reported for FRAP²⁷:

$$\begin{aligned} I_{\text{rel. image}}^*(t) &= \alpha \times I_{\text{rel. calc}}(t) \\ &= \alpha \left(1 - \left((1 - \beta) \sum_{n=0}^{+\infty} \frac{(-K)^n}{n!} \left(1 + n \left(1 + \frac{2t}{\tau_D} \right) \right)^{-1} + \beta \frac{1 - e^{-K}}{K} \right) \right) \end{aligned} \quad (3)$$

where α is a parameter to conform $I_{\text{rel. calc.}}$ to $I_{\text{rel. image}}^*$ at $t = 0$ and β is the fraction of immobile molecules (ranging from 0 to 1).



τ_D is the characteristic diffusion time related to the diffusion coefficient, D , by $\tau_D = w^2/4D$. The series solution for the fluorescence decay was truncated after 40 terms¹⁸, assuring that the neglected terms made an insignificant contribution. All of the curve fittings were done by using a weighted least-squares algorithm implemented in Origin (OriginLab).

Additional methods. The methods for plasmid construction, cell culture and transfections, protein purification, gel filtration, spectroscopy, pH titration, measurement of photoconversion quantum yield and western blotting are available in **Supplementary Methods** online.

Note: Supplementary information is available on the Nature Methods website.

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AUTHOR CONTRIBUTIONS

T.M. performed experiments, analyzed data and prepared the manuscript; A.M. contributed to data analysis; T.N. contributed to the conceptual development and experimental design and performed experiments, analyzed data and prepared the manuscript.

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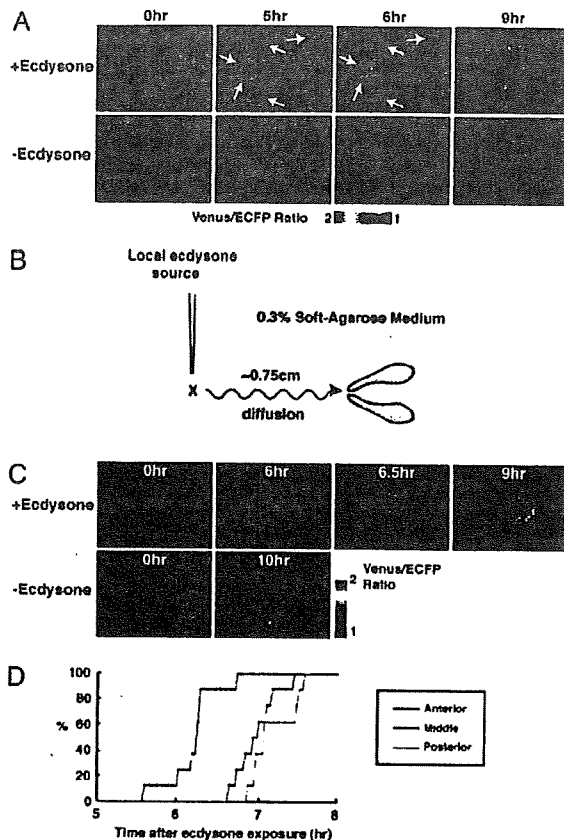


Fig. 3. *In vitro* response of salivary gland to ecdysone. (A) Random initiation of caspase activation induced by ecdysone exposure *in vitro*. Salivary glands at 8 h APF were carefully dissected and cultured *in vitro*, and 50 μ M ecdysone was added to cultured salivary glands to induce caspase activation. Arrows indicate cells with high caspase activity. The genotype was *N393/+; UAS-SCAT3/+*. (B–D) Local initiation and propagation of caspase activation by anterior-localized source of ecdysone. Salivary glands at 8 h APF were carefully dissected and cultured *in vitro* in 0.3% soft agarose-containing medium (2 ml). Then, 1 μ l of 50 mM ecdysone or ethanol (control) was added to the anterior part of the salivary gland. The time courses of caspase activation in anterior, middle, and posterior region are plotted in D ($n = 8$). The percentage of salivary glands that showed caspase activation in the indicated region was plotted. Caspase activation was determined by a 20% decrease from the basal ratio.

caspase activation was initiated locally in the anterior region and propagated to the posterior region of the salivary gland.

***In Vitro* Response to Ecdysone in Salivary Gland Cells.** Next, we examined whether this pattern of caspase activation occurred specifically *in vivo*. The salivary glands from pupae were isolated at 8 h APF and cultured *in vitro* in culture medium. The salivary glands could be maintained for at least 17 h under these culture conditions (data not shown). Strong caspase activation was observed 6 h after the addition of ecdysone to the salivary glands (Fig. 3A Upper). However, the caspase activation was initiated in a random pattern *in vitro* (arrows in Fig. 3A), unlike the *in vivo* pattern shown in Figs. 1 and 2. These results suggest that the ability to respond to ecdysone is equal among salivary cells.

We also examined the results of local application of ecdysone in 0.3% soft agarose-containing medium to achieve slow diffu-

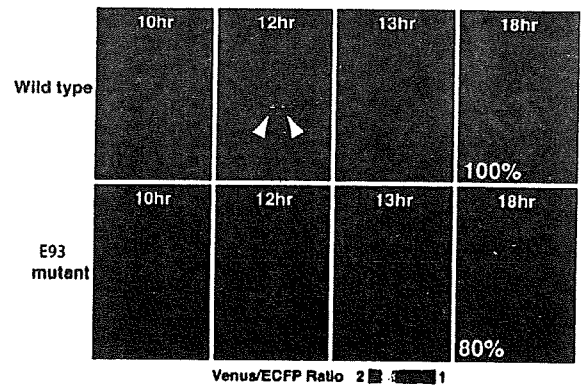


Fig. 4. Defect of caspase activation in *E93* mutants *in vivo*. *In vivo* live imaging was performed on pupae from 10 h APF. Arrowheads indicate the symmetrical initiation of caspase activation in the wild-type control. Numbers indicate the population of flies that showed these phenotypes. The indicated genotypes were: wild-type (*N393/+; UAS-SCAT3/+*) and *E93* mutant (*N393/+; UAS-SCAT3/+; E93¹/Df(3R)93F²*).

sion of ecdysone from anterior to posterior *in vitro* (Fig. 3B). Caspase activation was shown to be initiated in the anterior cells and propagated to the posterior cells in the salivary gland by diffusion of ecdysone from the anterior part (Fig. 3C Upper). Caspase activation was not observed at least within 10 h in control experiments (Fig. 3C Lower). We also plotted the time course of caspase activation in anterior, middle, and posterior regions (Fig. 3D), and the results indicated that caspase activation was initiated in anterior cells and propagated to middle and posterior cells. These results suggest that the spatiotemporal pattern of caspase activation in the salivary gland *in vivo* is the result of ecdysone diffusion and transport from the anterior side.

Defective Caspase Activation in *E93* Mutants. To investigate how the caspase activation pattern was formed and regulated *in vivo*, we used live-imaging analysis of mutants defective in ecdysone-induced genes. It has been reported that flies with mutations in *E93*, *E74A*, *β FTZ-F1*, or *BR-C* show inhibited programmed cell death in the salivary glands (6, 7, 17, 18). In *E93* mutants, late genes, including the *Drosophila* caspases *dronc* and *dark*, showed reduced expression (19), resulting in inhibition of salivary gland cell death. We first examined the *E93* gene mutation with SCAT3 live-imaging analysis (Fig. 4). In all of the *E93* mutants examined, head eversion occurred normally, suggesting that the prepupal pulse of ecdysone was normal. However, our live-imaging analysis showed that caspase activation in these mutants was strongly inhibited, at least within the first 18 h APF (80%; $n = 10$). These results suggested that the *E93* gene is an executor for caspase activation in salivary gland *in vivo*.

Defects in Spatial Regulation of Caspase Activation in *β FTZ-F1* Mutants. We next examined whether the spatial distribution of the ecdysone pulse *in vivo* could be involved in determining the spatial pattern of caspase activation in the salivary gland. Previous studies indicated that *β FTZ-F1* mutants show defective adult head eversion and leg elongation, suggesting that the prepupal pulse of ecdysone is abnormal in these mutants (18). Therefore, we investigated the spatial pattern of caspase activation in a *β FTZ-F1* mutant (Fig. 5). Almost all of the *β FTZ-F1* mutant pupae expressing SCAT3 showed defects in adult head eversion (90%; $n = 21$). The results of live-imaging analysis with SCAT3 *in vivo* indicated complete inhibition of caspase activation in 29% of the *β FTZ-F1* mutants, at least within the first 18 h APF (Fig. 5A case 1; $n = 21$). In the other mutants, caspase activation was significantly delayed: decreases in

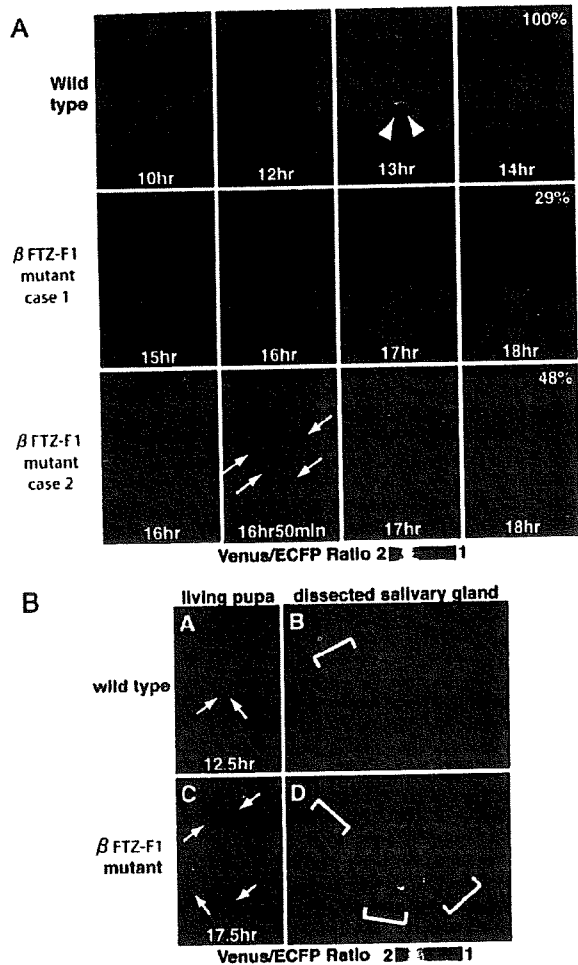


Fig. 5. Defects in adult head eversion and the spatial pattern of caspase activation in β FTZ-F1 mutants *in vivo*. (A) *In vivo* live imaging was performed from 10 h APF in wild-type controls and β FTZ-F1 mutants. Arrowheads indicate the symmetrical initiation of caspase activation in wild-type controls. Arrows indicate the random initiation of caspase activation in β FTZ-F1 mutants. Case 1 refers to pupae showing no caspase activation up to 18 h APF. Case 2 refers to the pupae that showed delayed and randomly initiated caspase activation. In case 2, the propagation of caspase activation characteristic of wild-type controls (Fig. 1A) was not observed. Numbers indicate the percentages of the population. (B) Defect in the spatial pattern of caspase activation in β FTZ-F1 mutants. The spatial pattern of caspase activation was compared between dissected salivary glands from wild-type controls and β FTZ-F1 mutants. Once the caspase activation was started as determined by *in vivo* imaging (A and C; arrows), the salivary gland from the observed pupa was dissected and fixed. Time indicates APF (in hours). The indicated genotypes in this figure are wild-type ($N393/+$; $UAS-SCAT3/+$) and β FTZ-F1 mutant ($N393/+$; $UAS-SCAT3/+$; β FTZ-F1¹⁷/ β FTZ-F1¹⁹).

the emission ratio were detected from 15 h 32 min \pm 1 h 30 min APF. Interestingly, in some of the β FTZ-F1 mutants, caspase activation was significantly delayed and occurred in a random pattern (Fig. 5A case 2, arrows; 48%; $n = 21$), in contrast to the anterior-to-posterior wave of activation seen in wild-type controls (Fig. 1). Moreover, the symmetry of caspase activation between the left and right salivary glands was almost completely abolished in these mutants. Some β FTZ-F1 mutants (19%; $n = 21$) showed an

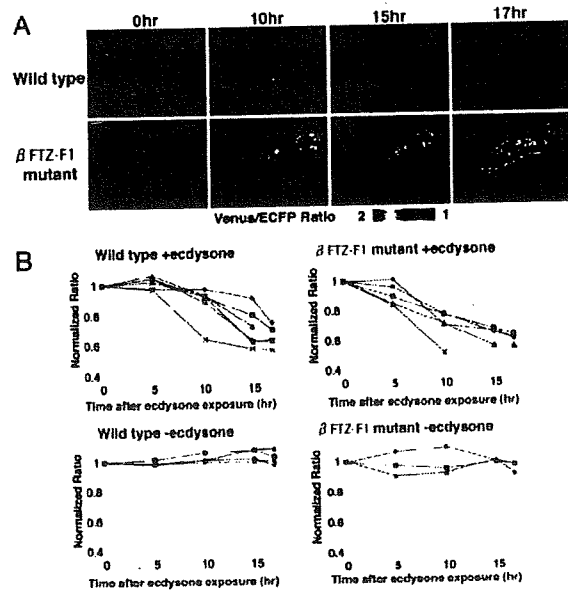


Fig. 6. Normal response to ecdysone in salivary glands isolated from β FTZ-F1 mutants *in vitro*. (A) Caspase activation in β FTZ-F1 mutants in response to ecdysone. The salivary glands were carefully dissected from wild-type controls or β FTZ-F1 mutants at 8 h APF. *In vitro* live imaging was performed in one of the pair by confocal microscopy with 50 μ M ecdysone in culture medium. (B) Time course of caspase activation in wild-type and β FTZ-F1 mutant salivary glands with or without ecdysone *in vitro*. In each experiment, the average ratio between the anterior, middle, and posterior region was calculated. Average ratio in individual salivary gland was plotted in B. To compare wild-type and mutant animals, the emission ratio was normalized by defining the ratio shown in 0 h as 1. Live imaging of at least three salivary glands in each experiment was performed for 17 h or until the cells were completely destroyed. Note that no caspase activation was observed without ecdysone for at least 17 h in wild-type and β FTZ-F1 mutant salivary glands (Lower). The indicated genotypes are: wild-type ($N393/+$; $UAS-SCAT3/+$) and β FTZ-F1 mutant ($N393/+$; $UAS-SCAT3/+$; β FTZ-F1¹⁷/ β FTZ-F1¹⁹).

anterior-to-posterior spatial pattern of caspase activation similar to that of wild-type controls; however, these mutants also showed defects in adult head eversion and a marked delay in the initiation of caspase activation (16 h 4 min \pm 1 h 12 min).

To examine the caspase activation pattern of the β FTZ-F1 mutants in detail, we examined caspase activities at the single-cell level, as shown in Fig. 2. In contrast to wild-type controls, the initial caspase activation occurred randomly in β FTZ-F1 mutants (Fig. 5BC). This random activation was confirmed in isolated salivary glands (Fig. 5BD). These results strongly suggested that β FTZ-F1 and the normal ecdysone pulse are involved not only in the temporal regulation but also in the spatial regulation of caspase activation *in vivo*.

Normal Response to Ecdysone of Salivary Glands Isolated from β FTZ-F1 Mutants *In Vitro*. To determine the association between β FTZ-F1 and the ecdysone response, we examined the response to ecdysone of salivary glands isolated from β FTZ-F1 mutants (Fig. 6). Salivary glands from wild-type controls and β FTZ-F1 mutants were maintained in culture for at least 17 h (Fig. 6B Lower; -ecdysone). The salivary glands from β FTZ-F1 mutants showed the same pattern of caspase activation as wild-type controls in live imaging *in vitro* (Fig. 6A), and the time courses of the *in vitro* response to ecdysone were similar in both wild-type controls and β FTZ-F1 mutants (Fig. 6B Upper). These results indicated that the β FTZ-F1 mutant salivary glands have the ability to respond normally to

ecdysone. The results of our *in vivo* and *in vitro* experiments suggest that the defects in spatiotemporal caspase activation in the β FTZ-F1 salivary gland *in vivo* are likely caused by the abnormal regulation of the ecdysone pulse generated in the ring gland. Thus, regulated synthesis and local exposure to ecdysone from the ring gland to the anteriormost part of the salivary gland are crucial to generate the unique caspase activation pattern in the salivary gland during metamorphosis.

Discussion

Our live-imaging experiments revealed three characteristics of caspase activation during salivary gland programmed cell death in wild-type controls *in vivo* (Figs. 1 and 2). First, the caspase activation was always initiated in only a few cells located in the anteriormost region of the salivary glands. Second, the caspase activation was propagated from the anterior cells to posterior cells of the salivary glands. Third, these spatial patterns of caspase activation were symmetrical along the median line. This anterior-to-posterior pattern could not be detected *in vitro* in cultured salivary glands (Fig. 3), suggesting that the sensitivity to ecdysone is equivalent among the gland cells. In contrast, local ecdysone stimulation from the anterior side induced anterior-to-posterior patterns of caspase activation *in vitro* likely to be observed *in vivo*. Therefore, we assume that a well organized system for ecdysone diffusion and transport from anterior side should form the spatiotemporal pattern of caspase activation in the salivary gland *in vivo*.

To determine the molecular mechanisms involved in caspase activation *in vivo*, we applied our live-imaging technique to mutants deficient in ecdysone-induced genes. *E93* is an ecdysone response gene that controls the expression of late genes, including the *Drosophila* caspase *dronc* (7, 20). An *E93* mutant showed strong inhibition of caspase activation, although the pupal-prepupal ecdysone pulse seemed to be normal (Fig. 4). These observations suggest that *E93* is an executor for caspase activation in the salivary gland programmed cell death through induction of late genes in the salivary gland.

Because the ecdysone pulse did not seem to be affected in the *E93* mutants, we hypothesized that the spatial pattern of caspase activation could be coordinated by the spatial distribution of the ecdysone pulse. Therefore, we examined caspase activation in β FTZ-F1 mutants, in which a defect in adult head eversion suggests that the prepupal pulse of ecdysone is abnormal. In this mutant, caspase activation was inhibited or delayed, and in some cases it occurred in a random pattern in the salivary gland cells. There was no significant spatial pattern in these mutants, in contrast to the organized pattern seen in wild-type controls. Moreover, in these mutants, the symmetry of the spatial pattern of caspase activation had disappeared almost completely. The partial influence of β FTZ-F1 on ecdysone response is likely because the alleles selected for this experiment were not nulls. However, the salivary glands from the β FTZ-F1 mutant showed normal induction of caspase activity in response to ecdysone *in vitro*, suggesting that β FTZ-F1 does not make a major contribution to cell death itself in the salivary gland. From these results, obtained by live imaging of β FTZ-F1 mutant salivary glands both *in vivo* and *in vitro*, we hypothesized that β FTZ-F1 regulates the ecdysone pulse in the ring gland where ecdysone is synthesized and secreted for salivary gland programmed cell death *in vivo*. The ring gland is located on the prothorax near the salivary glands, suggesting that the local activation of caspase may depend on the local interaction between the ring gland and salivary glands.

One possible mechanism for β FTZ-F1 to regulate the ecdysone pulse involves its coordination of ecdysteroidogenesis by controlling the expression of downstream genes. *E75A* is a downstream gene of β FTZ-F1 (21). The expression pattern of *E75A* is correlated with that of β FTZ-F1 at 10 h APF (22). It has been hypothesized that *E75A* acts as a feedforward factor in ecdysteroidogenesis by enhancing the expression of steroidogenic enzymes (23, 24). Taken to-

gether, these observations suggest that β FTZ-F1 may regulate ecdysteroidogenesis through regulation of *E75A* expression. Our current hypothesis is that a β FTZ-F1-*E75A* feedback loop in the ring gland results in the biosynthesis of precise levels of ecdysteroid, creating the spatiotemporal pattern of the ecdysone pulse and consequently of caspase activation in the salivary glands. At least in third-instar larvae, β FTZ-F1 is expressed in the ring gland (24). However, the detailed function of β FTZ-F1 in the ring gland remains to be elucidated. SCAT3-based live-imaging analysis will provide information regarding not only ecdysone-mediated biological events, including cell death, but also insight into the dynamics of ecdysone pulse.

Materials and Methods

Fly Stocks. The following fly strains were used in this work: *UAS-SCAT3* (25), *UAS-DRONC DN/TM3* (26), *N393/Binsinscy* (16), and *sca-Gal4/CyO* (27). To generate the *E93* and β FTZ-F1 mutants expressing SCAT3, *E93¹/TM6b*, *Df(3R)93F²/TM6b*, β FTZ-F1¹⁷/TM6b, and β FTZ-F1¹⁰/TM6b (27) were used. *Drosophila* crosses were carried out by standard procedures at 25°C.

Live Imaging of Caspase Activation in the Programmed Cell Death of Salivary Glands *in Vivo*. Live-imaging analysis of caspase activation *in vivo* with wide-field microscopy was performed as described in our previous reports with several modifications (15). Late third-instar larvae were selected from the appropriate crosses and monitored every 10–15 min for pupal formation. Each staged pupa was picked up and placed on a glass coverslip in a humid chamber to maintain viability. Animals were maintained at 23–26°C in a temperature-controlled room. Head eversion occurred \approx 11.5 h after puparium formation in wild-type controls (*N393/+*; *UAS-SCAT3/+*) in this culture system, consistent with a previous report (17). The optical system for *in vivo* live imaging was described in our previous report (15).

Detailed Spatiotemporal Pattern Analysis in Dissected Salivary Glands. After the beginning of caspase activation, as determined by *in vivo* imaging, the salivary glands from the observed pupa were dissected in ice-cold PBS within 15 min and fixed with 4% paraformaldehyde at 4°C for 5 min. The salivary glands were placed immediately on coverslips. FRET images in fixed salivary glands were collected by confocal microscopy as described in our previous report (25).

Live Imaging of Caspase Activation During Programmed Cell Death in the Salivary Gland *in Vitro*. Confocal imaging analysis of caspase activation was performed as described in our previous report with several modifications (25). Salivary glands dissected at 8 h APF were cultured on glass coverslips in Schneider's *Drosophila* medium (Gibco, Grand Island, NY). Cultured salivary glands were maintained at 23–26°C in a temperature-controlled room. To protect the gland cells from damage, we preserved the interconnections between each salivary gland. After 50 μ M ecdysone or ethanol (as a control) was added, confocal FRET images were acquired with the Aquacosmos/Ashura system (Hamamatsu Photonics, Hamamatsu, Japan) with a UPlanApo \times 10 0.40 NA objective (Olympus, Tokyo, Japan) as described in our previous report (25).

In the case of local stimulation by ecdysone (Fig. 3B), salivary glands were cultured in 0.3% soft agarose-containing medium to obtain slow diffusion of ecdysone *in vitro*. The distance between the anteriormost cells of the salivary gland and the point of ecdysone injection was \approx 0.75 cm. We measured the diffusion of Alexa Fluor 488-maleimide dye to monitor the time for diffusion from anterior to posterior salivary gland cells. It was estimated to be \approx 60 min under these conditions (data not shown). The imaging analysis was performed with a \times 4 0.16 N.A. objective (Olympus).

Mutant Imaging Analysis. The *E93* and *BFTZ-F1* mutants used in this work and their general defects in salivary gland cell death were described previously (6, 18, 19, 28). Controls (*N393/+*; *UAS-SCAT3/+*), *E93* [*N393/+*; *UAS-SCAT3/+*; *E93¹Df(3R)93F^{Δ2}*], and *BFTZ-F1* (*N393/+*; *UAS-SCAT3/+*; *BFTZ-F1¹/BFTZ-F1¹⁹*) mutants were used for SCAT3 imaging analysis *in vivo*.

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蛍光イメージング—最近の進歩：回折限界の壁を越える工夫—

永井健治*

はじめに

本特集は「空間」つまり形態学にその基礎を置いていた病理学に、生きた細胞を経時的に観察することで得られる「時間」軸の概念をプラスすることで、新たな病理学の方角性を見出そうという試みであるが、本稿では今一度「空間」に焦点を当て、従来不可能と言われていた回折限界の壁を越える「超解像」の最新知見を紹介する。

I. 共焦点顕微鏡の進歩

高い空間分解能での顕微鏡観察と言えば、まず共焦点蛍光顕微鏡を挙げないわけにはいかない。共焦点蛍光顕微鏡は、1957年にMIT (Massachusetts Institute of Technology) のMinskyが考案し、1980年代後半の実用化以降、多くの研究者に利用されている。通常の蛍光顕微鏡が励起光を試料全体に均一に照射(ケーラー照明)し、試料全体から射出する蛍光を同時に観察するのに対し、共焦点顕微鏡は、回折限界まで絞り込んだスポット光を試料の1点のみを照明(クリティカル照明)し、その点から射出する蛍光を、対物レンズで集めて結像させる。この結像位置にピンホールを配置すれば、ピンホールに結像した光はそこを通過し、光電子増倍管 photomultiplier tube (PMT) などの検出器で蛍光強度が測定される。ピンホールに結像しない光、つまり試料面以外からの蛍光は遮断され検出器まで届かない。したがって、本方法を用いることにより、試料内の焦点からの光だけが選択的に検出されるわけである。試料自体か、あるいは励起用のスポット光を二次元に走査することで試料全体の蛍光像を観察することができるが、その試料全体の像は焦点面の

情報しか含まないため、ボケ像を排除した光学切片像となる。

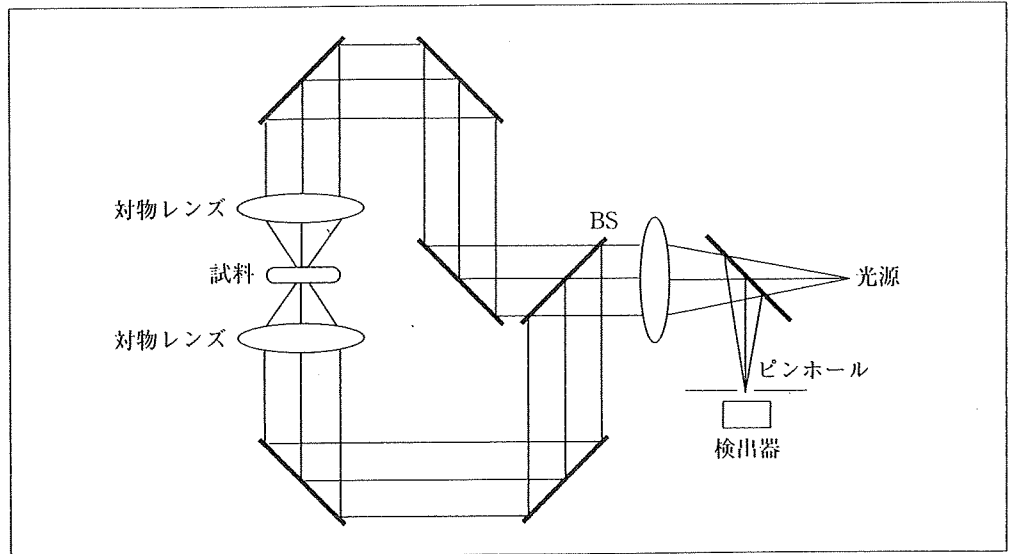
走査方法はガルバノミラーを用いた単点走査型が一般的であり、512×512の解像度で画像を1枚取得するのに1秒程度かかる。これではミリ秒スケールで起こる生理現象の観察はできない。そこで、空間分解能を犠牲にするぶん時間分解能を高める方式として、点ではなく線でレーザーを走査する共焦点顕微鏡が登場した。ZeissからリリースされているLSM 5 Liveである。点走査の場合x軸方向とy軸方向の2方向にレーザースポットを走査するが、LSM 5 Liveでは線状のレーザー光を1軸方向にのみ走査するため、512×512と同等の解像度の場合、最速120枚/秒の超高速画像取得が可能になった。

一方、線走査ではなく、点走査でも時間分解能を上げる方法がある。どうするのかというと、単点でなく多点で走査するのである。512×512の画像取得が1点走査で1秒かかるのであれば、1,000点を同時に走査すれば、1ミリ秒で画像取得ができるという理屈である。横河電機からリリースされているCSU (confocal scanner unit) は、ニポウディスクという“多数のピンホールが渦巻き状に配置された回転円板”を使用し、多点走査により共焦点画像を得ている。ガルバノミラーによる往復運動はウォブリングの発生のため、高速化には限界があるが、ニポウディスクは回転運動を利用しているため、高速化によるウォブリングの発生はない。例えば、CSU-X1は原理上2,000枚/秒という高速性を有しており、現時点では共焦点光学系の中かで最も高い時間分解能を有する。ただし、このように高速化すると、当然の帰結として、1枚の画像を取得する間に得られるシグナル(光子数)は減少し、したがって、S/N比の悪い画像にならざるをえない。もちろん、励起光強度を上げれば得られるシグナルは大きくなるが、蛍光分子の光褪色が無視できなくなってしまう。

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図1 4 π 共焦点顕微鏡の光学系

光源から射出したレーザー光はビームスプリッター(BS)によって光路を2分割され、それぞれ試料の上下に設置された同一焦点をもつ対物レンズを通して、試料内にコヒーレントに絞り込まれる。試料からの蛍光信号は2つの対物レンズによって捉えられ検出器へ向かう。本図では励起・蛍光光学系の双方が4 π 光学系になっているが、どちらか一方のみの構成も存在する。



そこで必要になるのが超高感度受光素子である。近年、オンチップシグナル増幅が可能なEM-CCD (electron multiplying charge coupled device) カメラやHARP (high-gain avalanche rushing amorphous photoconductor) カメラが登場し、超高速共焦点画像取得を可能にした。後者はNHKが高感度なハイビジョン撮影のために開発したものである。中野らはこのHARPカメラとCSUの組み合わせに、さらにデコンボリューション演算を加えることで100 nmの空間分解能を達成した¹⁾。この顕微鏡を用いてGolgi体の動態を観察した結果、「Golgi体では1つの槽が網目状の構造をとりながらその中で違う性質の膜の融合と分離を繰り返し、次第に全体の性質を変えながら内部の蛋白を移動させていく」という、新しいメカニズムが働いていることを世界で初めて明らかにしている。

II. 4 π 共焦点顕微鏡

共焦点顕微鏡の空間分解能をさらに上げる工夫として、4 π 共焦点顕微鏡がHellとStelzerによって提案された²⁾ (図1)。これは試料を対物レンズで挟み、4 π ステラジアン(steradian)の立体角で励起光の照明と蛍光の観察を行うというものである。原理上、2倍の開口数になるため点像分布関数も狭小化され、したがって空間分解能が上昇する。2光子顕微鏡との組み合わせにより100 nmを上回る空間分解能を達成しているが、試料内での焦点面の移動、試料の交換、あるいは対物レンズの交換などがあると、光路長および焦点位置の再調整が必要となる。これらの微妙な調整が難しく普及が遅れている。

III. STED (stimulated emission depletion) 顕微鏡

これも共焦点顕微鏡の応用で、Hellによって開発された。4 π 顕微鏡が開口数の増加による空間分解能の上昇を狙ったのに対し、STED顕微鏡は試料面の蛍光分子が励起されうる範囲を極力小さくすることで空間分解能の上昇を達成している。従来の考えでは、回折限界以下に励起レーザーの絞り込みを行うことはできない。そこで、Hellらは励起レーザーを取り囲むような、ドーナツ状のレーザー照射を行うことを考案した³⁾ (図2)。このドーナツ状の光(STEDビーム)は、誘導放出のための光であり、励起状態にある蛍光分子が発光する前に、強制的に基底状態へと戻す働きがある。したがって、蛍光発光する分子がより局所に絞り込まれ、空間分解能が向上する。Hellらはこの顕微鏡により45 nmの空間分解能を達成し、シナプス小胞が開口放出した後もシナプトタグミン分子がクラスターを形成し続けていることを見出した⁴⁾。この方法の利点はSTEDビームのためのレーザーが1本増えただけで原理的には通常の共焦点顕微鏡と変わらないことである。しかしながら、誘導放出させるためにGW/cm²という莫大なパワーのSTEDビームを照射する必要があり、蛍光分子のみならず、試料そのものへの光損傷が懸念されていた。

そこでHellらは光照射により蛍光状態が可逆的に変化する蛍光蛋白を利用すれば照射エネルギーを減少させることができるのではないかと考え、RESOLFT (reversible saturable optical fluorescence transitions) という方法を考案した⁵⁾。RESOLFTは莫大なエネルギー