

ている鉄輸送タンパクであり、細胞表面に発現している TF 受容体と結合することにより、細胞内に鉄を送り込むが、腫瘍細胞の多くでこの TF 受容体が高発現している。Colon 26 マウス大腸がん細胞を移植したマウスを用いた生体内分布実験では、血中ホウ素濃度は BSH をそれぞれ封入した TF-PEG リポソームおよび TF-PEG リポソームの両方とも経時的に低下した。一方、腫瘍内ホウ素濃度は PEG リポソームでは 48 時間後は 35 ppm に到達し、その後時間の経過とともに低下していき、72 時間後には 20 ppm となったのに対し、TF-PEG リポソームの場合 72 時間後においてもおよそ 35 ppm と高い蓄積性を示した。また、ホウ素濃度の T/N 比は、48 時間後ホウ素濃度の T/N 比は 2.5、72 時間後では 6.0 と非常に高い値が得られた。さらに、ホウ素濃度 20 mg/kg 投与した担がんマウスに対し、72 時間後に中性子照射を行ったところ、中性子照射 100 日後では PEG リポソームを投与したマウスの生存率は 20% であったのに対し、TF-PEG リポソームを投与したマウスの生存率は 70% と TF を結合したことによる能動的ターゲティング効果が顕著に見出された。

また、増永・小野らはこの TF-PEG リポソーム技術を応用して、 $\text{Na}_2\text{B}_{10}\text{H}_{10}$ (GB) を封入した TF-PEG リポソームの SCC VII マウス扁平上皮がん細胞に対する BNCT 効果を検討した²⁴⁾。彼らは、増殖期にある細胞 (P-cell) だけでなく静止状態の細胞 (Q-cell) に対する BNCT 効果を *in vitro* で検討したところ、TF-PEG リポソームの方が PEG リポソームよりも効果的であり、Q-cell にも有効性が見出された。さらに、SCC VII 細胞を移植したマウスを用いて decahydrodecaborate (GB) および BSH を封入した TF-PEG リポソームの生体内ホウ素分布を調べたところ、腫瘍内ホウ素濃度は投与後 (投与ホウ素濃度: 35 mg/kg) 24 時間で蓄積量が最大となり、BSH 封入 TF-PEG リポソームでは 21.1 ppm であったのに対し、GB 封入 TF-PEG リポソームでは 35.6 ppm と GB 封入リポソームの方が腫瘍集積性が高いことがわかった。しかしながら、T/B 比はいずれの場合もおおよそ 0.5 と、血中の方がホウ素濃度が高い結果となった。

6.2. ホウ素脂質型リポソーム

このように、多面体構造のホウ素クラスターイオンを封入したリポソームを用いて、高い治療効果が達成できる可能性が示されてきた。しかしながら、使用されているホウ素封入リポソームは非常に高いイオン濃度であり高浸透圧的な溶液であることから、これ以上の高濃度化は困難であると同時に、このような条件下でのリポソーム膜安定性の問題が生じている。一方、リポソームの脂質二分子膜は、分子間相互作用により自己集合化し

ているため密度が高く、この二分子膜へホウ素分子を導入できれば、非常に高濃度でホウ素をデリバリーできると考えられる。さらに、リポソーム膜内にホウ素を導入させることで、リポソーム内に抗がん剤などさまざまな薬剤が封入できることから、BNCT と化学療法の複合治療が可能となる。

リポソーム膜内にホウ素を導入したホウ素リポソームの最初の報告は、Hawthorne らによって開発された一本鎖ホウ素イオンクラスター脂質 1 (Fig. 6) を用いたものであった²⁵⁾。この化合物は炭素鎖 16 の脂溶性部位と水溶性の *nido* 型カルボラン部位からなる両親媒性分子である。彼らは、DSPC、コレステロール、*nido* 型カルボラン脂質 1 からリポソームを調製した。EMT6 細胞を移植したマウスを用いて生体内ホウ素分布を調べたところ、投与ホウ素濃度 6 mg/kg では腫瘍内ホウ素濃度が投与後 6 時間で 22 ppm、その後 16~30 時間はおおよそ 34 ppm で一定であった。48 時間後には 25 ppm に低下したものの

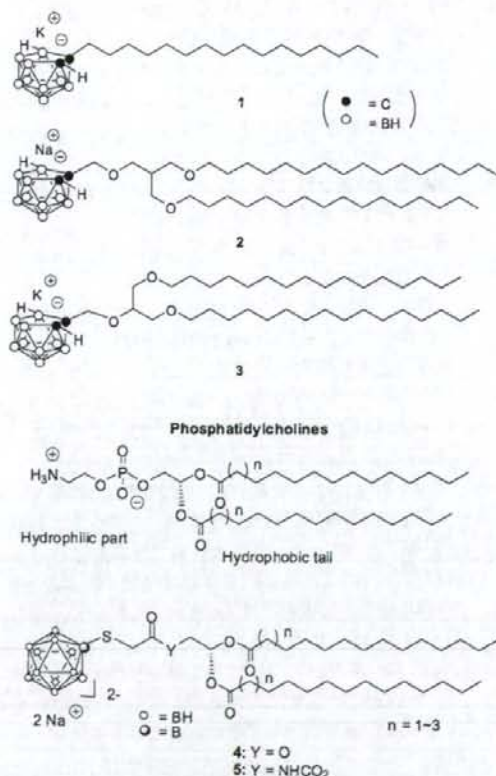


Fig. 6 Structures of *nido*-carborane lipids 1-3 and closo-dodecaborate lipids 4 and 5.

の T/N 比は 8.4 であった。

一方、我々はリポソーム膜へ効率良くかつ安定に生成するために、二分子膜を形成しているリン脂質のように脂溶性部位が二本鎖であれば良いと考えた。そこで、二本鎖ホウ素イオンクラスター脂質 2 を設計した²⁹⁾。電子顕微鏡で確認したところ、合成したイオン性ホウ素クラスター脂質 2 から 150~200 nm の大きさのベシクルが形成していることが分かった。これは世界で初めてのホウ素脂質ベシクルである。

このように安定なベシクルを形成することが分かったので、このホウ素イオンクラスター脂質 2 と DSPC、コレステロールを用いて、能動的ターゲティングを指向した TF 結合型ホウ素クラスターリポソームを合成し、担癌マウスを用いた体内分布ならびに中性子捕捉治療を行った²⁹⁾。ホウ素クラスターリポソームおよびトランスフェリン修飾型ホウ素クラスターリポソームを用いてマウス内での各臓器における分布を経時的に測定したところ、血液中の濃度変化はトランスフェリン修飾型ホウ素クラスターリポソームおよび非修飾型ホウ素クラスターリポソームともに速やかに低下した。一方、肝臓・腎臓・脾臓ではトランスフェリン修飾型ホウ素クラスターリポソームの方がより高濃度で蓄積していることがわかった。肺では両者とも血中濃度の低下に伴って低下することがわかった。興味深いことに、腫瘍ではトランスフェリン非修飾型ホウ素クラスターリポソームが時間に伴って濃度が減少しているのに対し、トランスフェリン修飾型ホウ素クラスターリポソームでは時間経過と関係なく蓄積しており、72 時間後でもトランスフェリン非修飾型ホウ素クラスターリポソームのおよそ 3 倍の濃度であることがわかった。

次に、担癌マウスを用いて中性子捕捉治療効果について検討した。左足に Colon 26 細胞を移植した BALB/c マウス (生後 6 週間, 16~18 g) にトランスフェリン修飾型ホウ素クラスターリポソームを ^{10}B 濃度で 7.2 mg/kg, 14.4 mg/kg それぞれ静脈投与し、72 時間後各臓器を分離しホウ素濃度をプロンプト法により測定した。7.2 mg/kg 投与したマウスでは、72 時間後、筋肉・心臓・脳ではホウ素蓄積はほとんど見られなかった。肺・血液ではおよそ 10 ppm、脾臓・肝臓では非常に高いホウ素蓄積が見られた。腫瘍内ホウ素蓄積量を見ても 7.2 mg/kg 投与した場合は 22 ppm, 14.4 mg/kg 投与の場合では 40 ppm であった。

さらに、トランスフェリン修飾型ホウ素クラスターリポソームを ^{10}B 濃度で 7.2 mg/kg 投与した担癌マウスを 72 時間後、京都大学原子炉において中性子照射した。照射後の生存曲線を Fig. 7(b) に示したが、ホウ素クラスターリポソームを投与していないマウスでは、中性子照

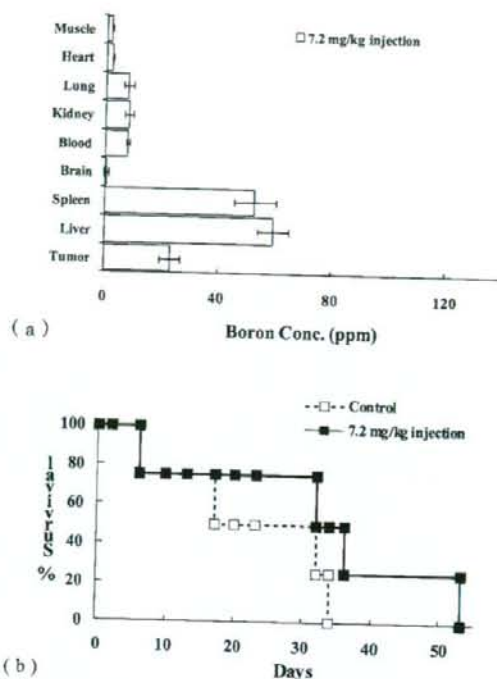


Fig. 7 (a) Boron concentration in various tissues at 72h after administration. (b) Survival curve of tumor-bearing mice after neutron irradiation. The mice were injected with 7.2 mg ^{10}B /kg of the Tf(+)-PEG-CL-liposome and incubated for 72 h before irradiation. Control indicates survival rates of tumor-bearing mice after neutron irradiation without administration of Tf(+)-PEG-CL liposomes.

射後の平均寿命が 22 日であったのに対し、ホウ素クラスターリポソームを ^{10}B 濃度で 7.2 mg/kg 投与したマウスでは、平均寿命 32 日とおよそ 1.5 倍延命効果が見られた。

これらの結果は、米国 NCI (National Cancer Institute) の Nanotech News for Cancer Therapy で紹介された²⁸⁾。最近、Hawthorne からも同様な二本鎖ホウ素イオンクラスター脂質 3 (Fig. 6) を開発している²⁹⁾。

このように、二本鎖ホウ素イオンクラスター脂質は安定なホウ素リポソームを形成し、腫瘍へも効率よく集積することが分かった。しかしながら、ホウ素濃度で 14.4 mg/kg 投与した場合に急性毒性が一部のマウスに見られたことから、我々はより低毒性なホウ素脂質の開発を目指し次世代ホウ素イオンクラスター脂質 4 および 5 (Fig. 6) を設計した³⁰⁾。この脂質は、脂溶性部位に生体リン脂質 (Phosphatidylcholines) と同じ立体構造を有して

おり、リンカー部位にエステル基（脂質 4）またはカルバメート基（脂質 5）を有し、BSH と S を介して結合している。これらのホウ素脂質から調整したリポソームは、正常マウスに対しホウ素濃度で 20 mg/kg では急性毒性は見られなかった。現在、NEDO「次世代 DDS 型悪性腫瘍治療システム」開発事業（平成 17～19 年度、プロジェクトリーダー：松村明教授・筑波大学）にて実用化に向けて研究を進めている。

6.3. 今後の展望

BNCT のためのホウ素キャリアーの開発には、いわゆるナノモルレベルで薬理効果が要求される抗がん剤のようなドラッグデザインではなく、ミリモルレベルで投与できるのに十分な低毒性であり、なおかつ腫瘍細胞に集積することが必要とされる。そのために、ここ数十年で低毒性小分子ホウ素化合物の開発だけでなく、本稿でも紹介したようにリポソームを用いたホウ素デリバリーシステムの開発が盛んに研究されてきた。BNCT において 1950 年代に開発された BSH、BPA という 2 剤以外には、まだ臨床応用されたホウ素薬剤は残念ながら登場していない。現在、核燃料の問題から BNCT に適応できる小型加速器の開発が精力的に行われている。熱中性子源が原子炉から加速器に移行できれば都市部病院併設型加速器による BNCT が可能となることから、将来放射線療法の一般的治療法の一つになるであろう。そのためにも治療効果の高いホウ素デリバリーシステムの開発が期待される。

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4 Synthesis of *closo*-Dodecaboryl Lipids 5 and their Liposomal Formation for Boron 6 Neutron Capture Therapy

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8 Yusuke Miyajima · Hyun Seung Ban

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13 **Abstract** High accumulation and selective delivery of
14 boron into tumor tissues are the most important require-
15 ments to achieve efficient neutron capture therapy of
16 cancers. We focused on liposomal boron delivery system
17 to achieve a large amount of boron delivery to tumor. We
18 succeeded in the synthesis of the double-tailed boron
19 cluster lipids **4a–c** and **5a–c**, which has a $B_{12}H_{11}S$ -moiety
20 as a hydrophilic function, by *S*-alkylation of $B_{12}H_{11}SH$
21 with bromoacetyl and chloroacetocarbamate derivatives of
22 diacylglycerols. Size distribution of liposomes prepared
23 from the boron cluster lipid **4b**, dimyristoylphosphatidyl-
24 choline, polyethyleneglycol-conjugated distearoylphospha-
25 tidylethanolamine, and cholesterol was determined as
26 100 nm in diameter by an electrophoretic light scattering
27 spectrophotometer. Calcein-encapsulation experiments
28 revealed that these boronated liposomes are stable at 37 °C
29 in fetal bovine serum solution for 24 h.

30 **Keywords** *closo*-dodecaborate · boron ion cluster lipid ·
31 boron neutron capture therapy · liposome ·
32 mercaptoundecahydrododecaborate · BSH

33 Introduction

34 Boron neutron capture therapy (BNCT) was first proposed as
35 a binary approach to cancer treatment in 1936 [1]. This
36 therapy is based on the capture reaction of thermal neutrons
37 using no radioactive ^{10}B , which produces an α -particle and a

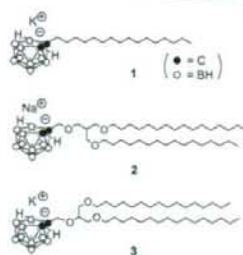
lithium-7 nuclei ion with approximately 2.4 MeV. These 38
high-linear energy transfer particles dissipate their kinetic 39
energy before traveling one cell diameter (5–9 μm) in 40
biological tissues ensuring their potential for precise cell 41
killing [2–4]. Their destructive effect is highly observed in 42
boron-loaded tissues. Therefore, the successful treatment of 43
cancer by BNCT demands the selective and marked 44
accumulation of ^{10}B in malignant tumor tissues. The amount 45
of ^{10}B required to obtain fatal tumor cell damage has been 46
calculated to be more than 30 $\mu g/g$ of tumor tissue, owing to 47
the low contact probability between thermal neutrons and 48
 ^{10}B [5]. Therefore, the marked accumulation and selective 49
delivery of boron into tumor tissues are the most important 50
requirement to achieve an effective BNCT of cancers. 51
Although mercaptoundecahydrododecaborate (BSH) [6, 7] 52
and L-4-dihydroxyboronylphenylalanine [8, 9] have been 53
utilized for BNCT, new boron-10 carriers that deliver an 54
adequate concentration of ^{10}B atoms to tumors should be 55
developed to achieve a potent and extensive cancer therapy 56

[10]. Recent promising approaches that meet these require- 57
ments entail the use of small boron molecules [11–16], such 58
as porphyrins [17–22], nucleosides [23–28], and amino acids 59
[29–39], and boron-conjugated biological complexes, such 60
as monoclonal antibodies [40–46], epidermal growth factors 61
[47–50], and carborane oligomers [51–55]. 62

Recently, Maruyama and co-workers have developed 63
transferrin-loaded (Tf) Polyethyleneglycol (PEG) liposomes 64
as a new type of target-sensitive liposome [56–60]. PEG 65
units have a heightened effect of prolonged residence time 66
in the circulation and escaping ability from reticulo- 67
endothelial-system (RES) uptake, resulting in an enhanced 68
extravasation of liposomes into solid tumor tissues. 69
Furthermore, this liposome is internalized into tumor cells 70
by receptor-mediated endocytosis and taken up into 71
endosome-like intracellular vesicles. They applied this 72

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Q1 Fig. 1 The *nido*-carborane as a hydrophilic moiety into the amphiphile 1



“BSH-activation” method, which enabled us to conduct 114
 S-alkylation of BSH under mild conditions. Our design of 115
 the boron lipids is based on biomimetic composition of 116
 phosphatidylcholines combined with the *closo*-type boron 117
 anion cluster to meet a sufficiently low toxic requirement 118
 [73, 74]. In this paper, we describe full accounts of the 119
 synthesis of *closo*-dodecaborate containing boron lipids 120
4a-c and **5a-c** and their liposomal property (Scheme 1). 121

Results and Discussion 122

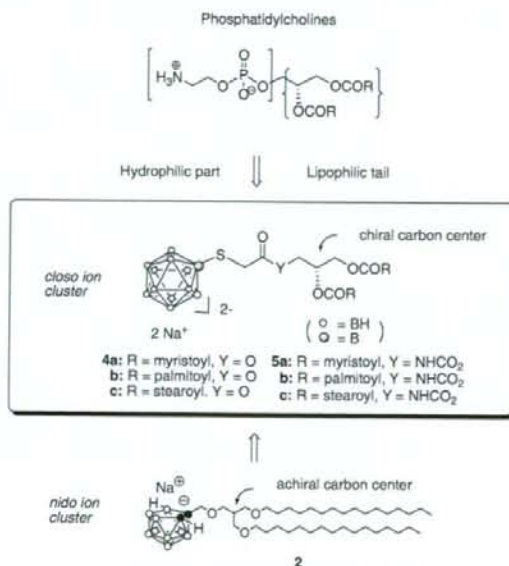
Synthesis of closo-Dodecaborate Containing Boron Lipids 123
4a-c and **5a-c** Synthesis of the hydrophobic tail functions 124
 of **4** is shown in Scheme 2. Reaction of the chiral alcohol **6** 125
 with 1.2 equiv of bromoacetyl bromide gave the ester **7**, 126
 quantitatively, and the deprotection of **7** was carried out 127
 using catalytic amounts of *p*-TsOH in MeOH to give the 128
 corresponding diol **8** in 38% yield. The ester formation of 129
 the diol **8** with various carboxylic acids was promoted by 130
 dicyclohexylcarbodiimide in the presence of catalytic 131
 amounts of *N,N*-dimethylaminopyridine in CH₂Cl₂ to 132
 afford the precursors **9a-c** in 61–75% yields. 133

Synthesis of the hydrophobic tail functions of **5** is shown 134
 in Scheme 3. We first examined the reaction of **6** with 135
 chloroacetyl isocyanate followed by deprotection of the 136
 acetal group; however, the chloroacetyl carbamate moiety 137
 decomposed under the acidic condition of *p*-TsOH in 138

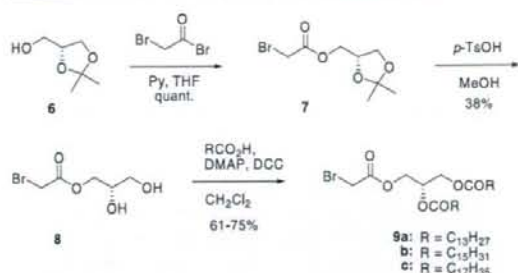
73 “active targeting” system to the selective boron delivery for
 74 BNCT. In this system, boron compounds are encapsulated
 75 in liposomes and delivered to tumor tissues [61].

76 As an alternative boron delivery system, a system
 77 involving the accumulation of boron in the liposomal
 78 bilayer is highly potent because drugs can be encapsulated
 79 into the vacant inner cell of a liposome. Furthermore,
 80 functionalization of liposomes is possible by combination
 81 of lipid contents. Therefore, boron and drugs may be
 82 simultaneously delivered to tumor tissues for BNCT and
 83 chemotherapy of cancers. Hawthorne and co-workers first
 84 introduced *nido*-carborane as a hydrophilic moiety into the
 85 amphiphile **1** (Fig. 1) and examined liposomal boron
 86 delivery in mice using **1** and distearoylphosphatidylcholine
 87 (DSPC) [62, 63]. We recently developed the *nido*-carborane
 88 lipid **2**, which has a double-tailed moiety conjugated with
 89 *nido*-carborane as a hydrophilic function [64]. This lipid
 90 has a symmetric carbon in the lipophilic alkyl chain. We
 91 investigated active targeting of the boronated liposomes to
 92 solid tumors by functionalization of transferrin on the
 93 surface of their liposomes and achieved a boron concentra-
 94 tion of 22 μg ¹⁰B/g tumor by the injection of the liposomes
 95 at 7.2 mg ¹⁰B/kg body weight with longer survival rates of
 96 tumor-bearing mice after BNCT [65]. However, the injec-
 97 tion of higher boron concentrations resulted in mortality of
 98 mice. We thought that this high toxicity may be due to a
 99 structure of “*nido*-type” carborane cage, although the
 100 cytotoxic mechanism of *nido*-carborane has not been
 101 studied in detail. Hawthorne and co-workers also recently
 102 reported synthesis of the *nido*-carborane lipid **3** and its
 103 unilamellar liposomes. They pointed out the high toxicity
 104 of the lipid **3** liposomes [66].

105 To overcome this problem, we focused on mercapto-
 106 undecahydrododecaborate (B₁₂H₁₁SH²⁻, BSH) as an alter-
 107 native hydrophilic function of boron lipids. BSH is a
 108 water-soluble divalent “*closo*-type” anion cluster and
 109 significantly lowered toxicity and thus has been utilized
 110 for clinical treatment of BNCT. However, few synthetic
 111 examples of BSH derivatives as boron carriers have been
 112 reported so far due to difficulty of their functionalizations
 113 [67–71]. Gabel and co-workers [72] reported a novel



Scheme 1 Scheme showing *closo*-dodecaborate containing boron lipids **4a-c** and **5a-c** and their liposomal property Q2



Q2 Scheme 2 Synthesis of the hydrophobic tail functions of 4

139 MeOH. Therefore, **6** was protected with benzylbromide
 140 using NaH, and the resulting dioxolane **10** was converted
 141 into the diol **11** using aqueous AcOH in 83% yield. The
 142 ester formation of **11** with various carboxylic acids was
 143 carried out in a similar manner to give **12a-c**, quantitative-
 144 ly. Deprotection of the benzyl group of **12a-c** by
 145 hydrogenation gave the corresponding alcohols **13a-c**
 146 (89->99% yields), which reacted with chloroacetyl isocya-
 147 nate in CH_2Cl_2 to give **14a-c** in 74-98% yields.

148 Introduction of BSH into the hydrophobic tail functions
 149 **9** and **12** was examined using the "activated BSH (**17**),"
 150 which was developed by Gabel and co-workers [72]. As
 151 shown in Scheme 4, BSH was treated with 2-iodopropioni-
 152 trile (2 equiv.) to give the monocation **16**, which underwent
 153 the dealkylation in the presence of base such as tetrameth-
 154 ylammmonium hydroxide to afford **17** in 80% yield.

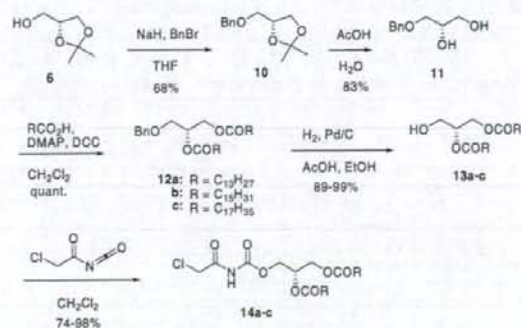
155 Finally, *S*-alkylation of **17** with **9a-c** proceeded in
 156 acetonitrile at 70 °C for 12-24 h, giving the corresponding
 157 *S*-dialkylated products **16a-c**, which were immediately
 158 treated with tetramethylammmonium hydroxide (1 equiv.) in
 159 acetone to give **4a-c** in 76-91% yields, as tetramethylam-
 160 monium salts. In a similar manner, the **5a-c** were obtained
 161 from **12a-c** in 54-83% yields. Ion-exchange reactions
 162 proceeded readily to afford their sodium salts (Scheme 5).

Q4

163 *Size Distributions of the Boronated Liposomes* We
 164 examined formation of the liposomes using the boron
 165 cluster lipid **4b**. Liposomes were prepared from cholesterol,
 166 dimyristoylphosphatidylcholine (DMPC), polyethyleneglycol-
 167 conjugated distearoylphosphatidylethanolamine (PEG-DSPE),
 168 and the boron cluster lipid **4b** (1:1-*X*:0.1:*X*=0-1, molar
 169 ratio) by the reverse-phase evaporation (REV) method [75].
 170 The liposomes obtained were subjected to extrusion 10 times
 171 through a polycarbonate membrane of a 100 nm pore size,
 172 using an extruder devise thermostated at 60 °C. Purification
 173 was accomplished by ultracentrifuging at 200,000 g for
 174 60 min at 4 °C, and the pellets obtained were resuspended in
 175 phosphate-buffered saline (PBS) buffer. Liposome size was
 176 measured with an electrophoretic light scattering spectropho-
 177 tometer. The size distribution of the liposomes composed of

178 **4b** before and after extrusion is shown in Fig. 2. Interestingly,
 179 increase of the contents of **4b** in liposome resulted in the
 180 wider size distribution, and two major maximum distributions
 181 were observed in the liposome with 100% boron lipid **4b**
 182 (Fig. 2d). The sizes of maximum distribution of the liposomes
 183 against **4b** contents were 103 (*X*=0.25), 105 (*X*=0.5),
 184 102 (*X*=0.75), and 108 nm (*X*=1) with 0.121, 0.092, 0.106,
 185 and 0.089 of polydispersity index values, respectively.

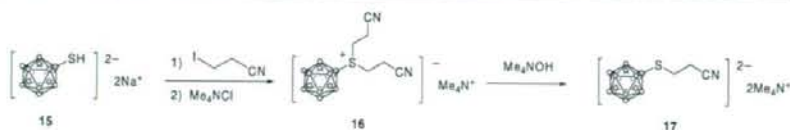
186 We next investigated the time-dependent stability of the
 187 boronated liposomes of **4b** in a fetal bovine serum (FBS).
 188 Fluorescent probes, such as calcein, are self-quenching at
 189 high concentrations, and the leakage of these fluorophores
 190 into the external medium results in the relief of self-
 191 quenching and an increase in the fluorescence. Therefore,
 192 the release of aqueous contents of liposomes can be
 193 monitored by an increase of fluorescent intensity [76]. We
 194 prepared the boronated liposomes at various concentrations
 195 of the boron cluster lipid **4b** using calcein (100 mM), and
 196 a liposome solution (the volume ratio, FBS/liposome
 197 solution=9:1) was added to FBS and incubated at 37 °C
 198 with stirring. The fluorescence of the FBS solutions was
 199 measured at 0-24 h. The results of the liposomes of **4b** with
 200 various ratios (*X*=0.25, 0.5, and 0.75) are shown in Fig. 3.
 201 No increase in the fluorescence intensity of the FBS
 202 solutions was observed within 24 h; therefore, the
 203 boronated liposomes were stable in the FBS solution at
 204 37 °C at least for 24 h. However, the increase of the
 205 fluorescence intensity was observed in the case of the
 206 liposome prepared from DSPC, cholesterol, PEG-DSPE,
 207 and the *nido*-carborane lipid **2** (*X*=0.5, Fig. 3d). These
 208 results indicate that the current boron lipids are more
 209 suitable for stable liposomal formation than the previous
 210 *nido*-carborane lipid **2** presumably due to the similar
 211 structure of lipophilic double tail moiety to the natural
 212 phospholipids. As the boron lipid **4b** has a similar chirality
 213 to phosphatidylcholines in the lipophilic double tail moiety,
 214 both lipids would tend to pack together densely and thus
 215 form stable liposomes.



Scheme 3 Synthesis of the hydrophobic tail functions of 5

Q2

Q2 **Scheme 4** BSH treatment with 2-iodopropionitrile giving monocation **16** and dealkylation giving **17**



217 **Conclusion**

218 We succeeded in the synthesis of the double-tailed boron
 219 cluster lipids **4** and **5**, which have a B₁₂H₁₁S-moiety as a
 220 hydrophilic function. A key for the current synthesis is
 221 S-alkylation of the activated BSH with bromoacetyl and
 222 chloroacetocarbamate derivatives of diacylglycerols. The
 223 liposomes prepared from the boron cluster lipid **4b** were
 224 stable in FBS, although the liposome prepared from the
 225 *nido*-carborane lipid **2** was not stable at 50% concentration
 226 (*X*=0.5), presumably due to the similar structure of
 227 lipophilic double tail moiety to the natural phospholipids.
 228 *In vivo* biodistribution and BNCT studies of the boronated
 229 liposomes of **4** and **5** are in progress in our laboratory.

230 **Experimental**

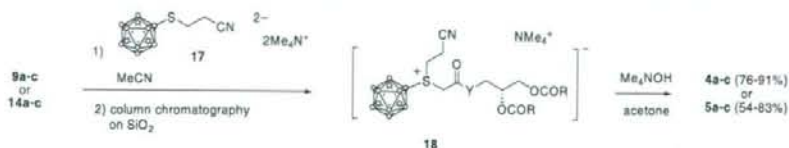
231 *General* ¹H NMR, ¹³C NMR, and ¹¹B NMR spectra were
 232 measured on a JEOL JNM-AL 300 (300 MHz) and Varian
 233 Unity-Inova 400 (400 MHz) spectrometers. Chemical shifts
 234 of ¹H NMR were expressed in parts per million downfield
 235 from CHCl₃ as an internal standard (δ =7.26) in CDCl₃.
 236 Chemical shifts of ¹³C NMR were expressed in parts per
 237 million downfield from CDCl₃ as an internal standard (δ =
 238 77.0) in CDCl₃. Analytical thin layer chromatography
 239 (TLC) was performed on glass plates (Merck Kieselgel 60
 240 F₂₅₄, layer thickness 0.2 mm). Column chromatography was
 241 performed on silica gel (Merck Kieselgel 70–230 mesh). All
 242 reactions were carried out under argon atmosphere using
 243 standard Schlenk techniques. Most chemicals and solvents
 244 were of analytical grade and used without further purification.
 245 Infrared (IR) spectra were recorded on a Shimadzu
 246 FT-IR 8200A spectrometer. Mass spectrometry data were
 247 collected by Shimadzu LCMS-2010 EV spectrometer.
 248 [B₁₂H₁₁SCH₂CH₂CN]²⁻·2(Me₄N⁺) was prepared from
 249 Na₂B₁₂H₁₂ according to the literature procedure [72].

250 *Synthesis of (S)-2,2-dimethyl-1,3-dioxolan-4-yl)methyl 2-*
 251 *bromoacetate (7)* To a stirred solution of (R)-(-)-2,

2-dimethyl-1,3-dioxolane-4-methanol **6** (1.2 ml, 10.0 mmol)
 and pyridine (0.97 ml, 1.2 equiv) in 50 ml of THF, which
 was cooled to 0 °C, was added a bromoacetyl bromide
 (1.0 ml, 1.2 equiv) at 0 °C. The reaction temperature was
 maintained at 0 °C for 30 min, after which the reaction
 mixture was warmed slowly to room temperature. After
 being stirred for an additional 4 h, the solid was removed
 by filtration through celite, the filtrate was concentrated
 under reduced pressure, and the product was purified by
 flash column chromatography eluting EtOAc/hexane
 (1:1). Yield: 2.5 g (10.0 mmol, >99%) of colorless oil.
 [α]_D²⁸ = +2.7 (c 1.0, CHCl₃); IR (KBr pellet, cm⁻¹)
 ν (C=O) 1743, ν (C–H) 2,889, 2,939, 2,960, 2,988;
¹H NMR (ppm, CDCl₃) δ 1.38 (s, 3H, CH₃), 1.45 (s, 3H,
 CH₃), 3.78 (dd, 2H, ²J_{C–H}=8.4 Hz, ³J_{C–C–H}=6.0 Hz,
 OCH₂CH), 3.89 (s, 2H, CH₂Br), 4.10 (dd, 2H, ²J_{C–H}=
 8.4 Hz, ³J_{C–C–H}=6.4 Hz, OCH₂CH), 4.19 (dd, 2H, ²J_{C–H}=
 11.4 Hz, ³J_{C–C–H}=6.4 Hz, CHCH₂OC(=O)CH₂Br), 4.26 (dd,
 2H, ²J_{C–H}=11.4 Hz, ³J_{C–C–H}=4.8 Hz, CHCH₂OC(=O)
 CH₂Br), 4.33–4.38 (m, 1H, CH); ¹³C NMR (ppm, CDCl₃)
 δ 25.3, 26.6, 32.2, 66.0, 73.2, 99.9, 167.0; Anal. Calcd
 for C₈H₁₃O₄Br: C, 37.96; H, 5.18. Found: C, 38.58;
 H, 5.19.

Synthesis of (S)-2,3-Dihydroxypropyl 2-Bromoacetate (8) To
 a stirred solution of compound **7** (2.53 g, 10.0 mmol) in
 20 ml of methanol was added a catalytic TsOH (0.17 g,
 0.1 equiv). The reaction mixture was stirred for 30 min at
 room temperature. The resulting solution was concentrated
 to dryness, and the residue was dissolved in CH₂Cl₂. After
 drying (Na₂SO₄) and filtration through celite, the filtrate was
 concentrate under reduced pressure, and the product was
 purified by flash column chromatography eluting EtOAc/
 hexane (2:1). Yield: 0.81 g (3.8 mmol, 38%) of pale yellow
 oil. [α]_D²⁸ = +0.75 (c 1.0, CHCl₃); IR (KBr pellet, cm⁻¹)
 ν (C=O) 1734, ν (C–H) 2,887, 2,958, ν (O–H) 3,335; ¹H
 NMR (ppm, CDCl₃) δ 3.65 (dd, 2H, ²J_{C–H}=11.2 Hz,
³J_{C–C–H}=6.0 Hz, HOCH₂CH), 3.75 (dd, 2H, ²J_{C–H}=
 12.2 Hz, ³J_{C–C–H}=4.0 Hz, HOCH₂CH), 3.88 (s, 2H, CH₂Br),
 3.97–4.03 (m, 1H, CH), 4.25 (dd, 2H, ²J_{C–H}=11.4 Hz,

Q2 **Scheme 5** Synthesis of **9a–c** or **14a–c** with purification by column chromatography on SiO₂



Synthesis of closo-Dodecaboryl Lipids for BNCT

Q5

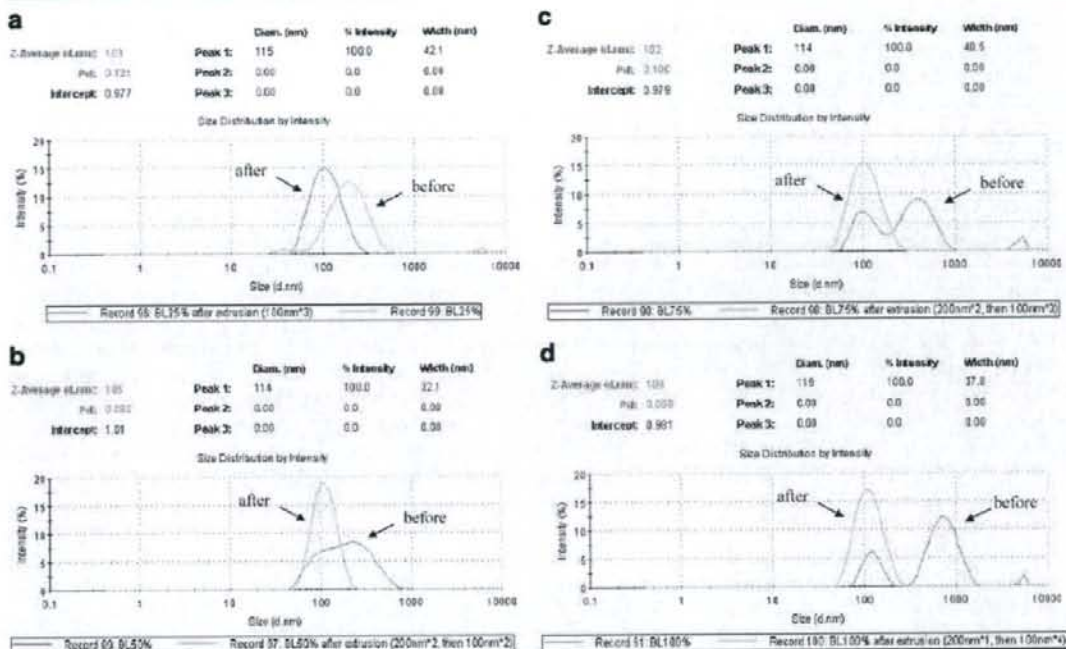


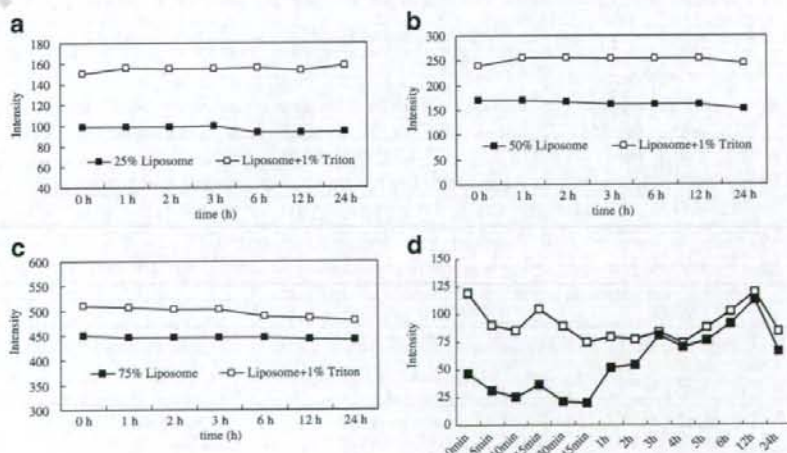
Fig. 2 Size distributions of the boronated liposomes before and after extrusion. The liposomes were prepared from cholesterol, DMPC, PEG-DSPE, and **4b**, (1:1-X:0.1:X, molar ratio). a X=0.25, b X=0.5, c X=0.75, d X=1.0

291 $^3J_{C-C-H}=6.4$ Hz, $CHCH_2OC(=O)CH_2Br$, 4.31 (dd, 2H,
 292 $^3J_{C-H}=11.6$ Hz, $^3J_{C-C-H}=4.4$ Hz, $CHCH_2OC(=O)CH_2Br$;
 293 ^{13}C NMR (ppm, $CDCl_3$) δ 25.8, 63.1, 66.6, 69.7, 167.7;
 294 Anal. Calcd for $C_5H_9O_4Br$: C, 28.19; H, 4.26. Found: C,
 295 28.15; H, 4.24.

296 *General Procedure for Synthesis of 1,2-O-diacyl-3-O-*
 297 *bromoacetyl-sn-glycerols 9* To a stirred solution of 3-O-

298 bromoacetyl-*sn*-glycerol **8** (0.64 g, 3.0 mmol), DMAP 298
 (0.07 g, 0.2 equiv) in 50 ml of dry CH_2Cl_2 at 0 °C were 299
 added DCC (1.36 g, 2.2 equiv) and the carboxylic acid (2.2 300
 equiv), and the resulting suspension was stirred for 12 h. 301
 The solid was removed by filtration through celite, the 302
 filtrate was concentrated under reduced pressure, and the 303
 product was purified by column chromatography using the 304
 solvent indicated as the eluent. 305

Fig. 3 Fluorescence intensities of calcein-encapsulated liposomes composed of the closo-dodecaborate lipid **4b** with various ratios (a X=0.25, b=0.5, c=0.75) and the nido-carborane lipid **2** (d X=0.5) in fetal bovine serum (FBS). The white plots show the fluorescence intensity of the FBS solution, and the black plots show that of the solution after destruction of liposomes by the addition of Triton X-100. The difference in fluorescence intensity between the black and white plots indicates calcein release from liposomes



306 3-*O*-bromoacetyl-1,2-*O*-dimyristoyl-*sn*-3-glycerol (**9a**)
307 obtained as a white powder in 61% (1.15 g, 1.8 mmol) yield
308 by column chromatography eluting with EtOAc/ hexane
309 (1:20). Mp.: 30–31 °C; $[\alpha]_D^{25} = +0.65$ (c 1.0, CHCl₃);
310 IR (KBr pellet, cm⁻¹) ν (C=O) 1746, ν (C–H) 2,855, 2,924,
311 2,957; ¹H NMR (ppm, CDCl₃) δ 0.88 (t, 6H, ³J_{C–H}=
312 6.4 Hz, CH₃), 1.26 (s, 40H, CH₂), 1.59–1.63 [m, 4H,
313 CH₂CH₂C(=O)], 2.32 [td, 4H, ²J_{C–H}=8.0 Hz, ³J_{C–H}=
314 4.0 Hz, CH₂C(=O)], 3.84 (s, 2H, CH₂Br), 4.17 (dd, 2H,
315 ²J_{C–H}=11.8 Hz, ³J_{C–H}=6.0 Hz, OCH₂CH), 4.26 (dd, 2H,
316 ²J_{C–H}=12.0 Hz, ³J_{C–H}=6.0 Hz, BrCH₂C(=O)OCH₂CH),
317 4.31 (dd, 2H, ²J_{C–H}=12.0 Hz, ³J_{C–H}=4.4 Hz, OCH₂CH),
318 4.41 (dd, 2H, ²J_{C–H}=11.8 Hz, ³J_{C–H}=4.4 Hz,
319 BrCH₂C(=O)OCH₂CH), 5.27–5.34 (m, 1H, CH);
320 ¹³C NMR (ppm, CDCl₃) δ 14.1, 22.7, 24.8, 25.2, 29.0,
321 29.1, 29.2, 29.4, 29.5, 29.6, 29.7, 31.9, 33.9, 34.0,
322 61.8, 63.9, 71.2, 166.8, 172.9, 173.2; Anal. Calcd for
323 C₃₃H₆₁O₆Br: C, 62.54; H, 9.70. Found: C, 62.58; H, 9.70.

324 3-*O*-bromoacetyl-1,2-*O*-dipalmitoyl-*sn*-3-glycerol (**9b**)
325 obtained as a white powder in 73% (1.51 g, 2.2 mmol) yield
326 by column chromatography eluting with EtOAc/ hexane
327 (1:20). Mp.: 39–40 °C; $[\alpha]_D^{25} = +0.45$ (c 1.0, CHCl₃);
328 IR (KBr pellet, cm⁻¹) ν (C=O) 1,744, ν (C–H) 2,851, 2,918,
329 2,957; ¹H NMR (ppm, CDCl₃) δ 0.88 (t, 6H, ³J_{C–H}=
330 6.8 Hz, CH₃), 1.26 (s, 48H, CH₂), 1.61–1.63 [m, 4H,
331 CH₂CH₂C(=O)], 2.32 [td, 4H, ²J_{C–H}=7.6 Hz, ³J_{C–H}=
332 4.0 Hz, CH₂C(=O)], 3.84 (s, 2H, CH₂Br), 4.17 (dd, 2H,
333 ²J_{C–H}=12.0 Hz, ³J_{C–H}=6.0 Hz, OCH₂CH), 4.26 (dd, 2H,
334 ²J_{C–H}=12.0 Hz, ³J_{C–H}=6.0 Hz, BrCH₂C(=O)OCH₂CH),
335 4.31 (dd, 2H, ²J_{C–H}=12.0 Hz, ³J_{C–H}=4.4 Hz, OCH₂CH),
336 4.41 (dd, 2H, ²J_{C–H}=11.8 Hz, ³J_{C–H}=4.4 Hz,
337 BrCH₂C(=O)OCH₂CH), 5.27–5.32 (m, 1H, CH);
338 ¹³C NMR (ppm, CDCl₃) δ 14.1, 22.7, 24.8, 25.2,
339 29.0, 29.1, 29.2, 29.4, 29.5, 29.6, 29.7, 31.9, 33.9, 34.0,
340 34.1, 61.8, 63.9, 71.2, 166.8, 172.9, 173.2; Anal. Calcd
341 for C₃₇H₆₉O₆Br: C, 64.42; H, 10.08. Found: C, 64.28;
342 H, 10.06.

343 3-*O*-bromoacetyl-1,2-*O*-distearoyl-*sn*-3-glycerol (**9c**)
344 obtained as a white powder in 75% (1.68 g, 2.3 mmol) yield
345 by column chromatography eluting with EtOAc/ hexane
346 (1:20). Mp.: 44–46 °C; $[\alpha]_D^{25} = +0.55$ (c 1.0, CHCl₃);
347 IR (KBr pellet, cm⁻¹) ν (C=O) 1,744, ν (C–H) 2,851, 2,918,
348 2,957; ¹H NMR (ppm, CDCl₃) δ 0.88 (t, 6H, ³J_{C–H}=
349 6.8 Hz, CH₃), 1.26 (s, 56H, CH₂), 1.58–1.65 [m, 4H,
350 CH₂CH₂C(=O)], 2.32 [td, 4H, ²J_{C–H}=7.6 Hz, ³J_{C–H}=
351 4.0 Hz, CH₂C(=O)], 3.84 (s, 2H, CH₂Br), 4.17 (dd, 2H,
352 ²J_{C–H}=11.8 Hz, ³J_{C–H}=6.0 Hz, OCH₂CH), 4.26 (dd, 2H,
353 ²J_{C–H}=12.0 Hz, ³J_{C–H}=6.0 Hz, BrCH₂C(=O)OCH₂CH),
354 4.31 (dd, 2H, ²J_{C–H}=12.0 Hz, ³J_{C–H}=4.4 Hz, OCH₂CH),
355 4.41 (dd, 2H, ²J_{C–H}=12.0 Hz, ³J_{C–H}=4.0 Hz,
356 BrCH₂C(=O)OCH₂CH), 5.27–5.32 (m, 1H, CH); ¹³C
357 NMR (ppm, CDCl₃) δ 14.1, 22.7, 24.8, 25.2, 29.0,
358 29.1, 29.2, 29.3, 29.4, 29.5, 29.6, 29.7, 31.9, 33.9,

34.0, 34.1, 61.8, 63.9, 68.5, 166.8, 172.8, 173.2; Anal. Calcd
for C₄₁H₇₇O₆Br: C, 66.01; H, 10.40. Found: C, 66.22;
H, 10.40.

Synthesis of (R)-4-((Benzyloxy)Methyl)-2,2-Dimethyl-1,3-Dioxolane (10)
NaH (0.26 g, 11 mmol) was washed with hexane and dissolved in THF (20 ml). To this solution was added (*R*)-(-)-2,2-dimethyl-1,3-dioxolane-4-methanol **6** (1.2 ml, 10.0 mmol) at 0 °C and the reaction mixture was stirred for 30 min. Benzyl bromide (1.43 ml, 12 mmol) was then added at 0 °C, and the reaction mixture was warmed slowly to room temperature. After being stirred for an additional 2 h, the saturated NH₄Cl solution was added, then the product was extracted with Et₂O (100 ml×3). The combined organic layer was dried over anhydrous Na₂SO₄ and concentrated under reduced pressure. Purification by column chromatography on SiO₂ with EtOAc/hexane (1:10) gave **10** as colorless oil (2.12 g, 9.5 mmol, 95%). $[\alpha]_D^{25} = -19.8$ (c 1.0, CHCl₃); IR (KBr pellet, cm⁻¹) ν (C–aryl) 698, 739, 1,053, 1,097, 1,371, 1,381, 1,454, ν (C–H) 2,866, 2,936, 2,988, 3,032; ¹H NMR (ppm, CDCl₃) δ 1.36 (s, 3H, CH₃), 1.42 (s, 3H, CH₃), 3.47 (dd, 2H, ²J_{C–H}=9.8 Hz, ³J_{C–H}=5.6 Hz, CHCH₂O), 3.55 (dd, 2H, ²J_{C–H}=9.8 Hz, ³J_{C–H}=5.6 Hz, CHCH₂O), 3.74 (dd, 2H, ²J_{C–H}=9.8 Hz, ³J_{C–H}=6.4 Hz, OCH₂CH), 4.05 (dd, 2H, ²J_{C–H}=8.0 Hz, ³J_{C–H}=6.4 Hz, OCH₂CH), 4.27–4.33 (m, 1H, CH), 4.57 (d, 2H, ²J_{C–H}=6 Hz, CH₂Ph), 7.25–7.34 (m, 5H, CH₂Ph); ¹³C NMR (ppm, CDCl₃) δ 25.3, 26.7, 66.8, 71.0, 73.4, 74.7, 127.6, 127.7, 127.9, 128.3, 128.4, 137.9; Anal. Calcd for C₁₃H₁₈O₃: C, 70.24; H, 8.16. Found: C, 71.04; H, 8.18.

Synthesis of (S)-3-(Benzyloxy)Propane-1,2-Diol (11)
(Martin SF, et al. *J Org Chem*. 1994;59:4805–20) To a solution of acetic acid (14 ml) and water (6 ml) was added **10** (2.0 ml, 9.0 mmol), and the reaction mixture was stirred at 65 °C for 1 h. The reaction mixture was neutralized with saturated aqueous NaHCO₃ solution (ca. 20 ml) and extracted with dichloromethane (20 ml×2). The organic layer was dried over anhydrous MgSO₄ and concentrated. Purification by column chromatography on SiO₂ with EtOAc/hexane (1:1) gave **11**, quantitatively (1.64 g, 9 mmol) as pale yellow oil. IR (KBr pellet, cm⁻¹) ν (C–aryl) 700, 739, 1,036, 1,043, 1,074, 1,454, 1,497, ν (C–H) 2,870, 2,924, ν (O–H) 3,364; ¹H NMR (ppm, CDCl₃) δ 3.53 (dd, 2H, ²J_{C–H}=9.8 Hz, ³J_{C–H}=6.0 Hz, CHCH₂O), 3.57 (dd, 2H, ²J_{C–H}=9.8 Hz, ³J_{C–H}=4.4 Hz, CHCH₂O), 3.60–3.72 (m, 2H, HOCH₂CH), 3.86–3.92 (m, 1H, CH), 4.55 (s, 2H, CH₂Ph), 7.30–7.38 (m, 5H, CH₂Ph); ¹³C NMR (ppm, CDCl₃) δ 63.9, 70.7, 71.6, 73.5, 127.7, 127.8, 128.4, 137.7; Anal. Calcd for C₁₀H₁₄O₃: C, 65.91; H, 7.74. Found: C, 65.25; H, 7.75.

- 410 *General Procedure for Synthesis of 1,2-O-Diacyl-3-O-* 463
 411 *Benzyl-sn-Glycerol (12)* (Martin-SF, et al. *J Org Chem.* 464
 412 *1994;59:4805-20*) To a solution of **11** (1.82 g, 10 mmol) 465
 413 and DMAP (1.22 g, 10 mmol) in dichloromethane (50 ml)
 414 was added dicyclohexylcarbodiimide (6.19 g, 30 mmol),
 415 and the mixture was stirred for 30 min. A carboxylic acid
 416 was then added and the resulting suspension was stirred for
 417 12 h. The solid was removed by filtration through celite,
 418 and the filtrate was concentrated under reduced pressure.
 419 Purification by column chromatography on SiO₂ with
 420 EtOAc/hexane (1:10) gave **12**.
- 421 1,2-O-Dimyristoyl-3-O-benzyl-sn-glycerol (**12a**)
 422 obtained as a white powder in quantitative yield. Mp.:
 423 32–33 °C; IR (KBr pellet, cm⁻¹) ν (C=O) 1,736, ν (C–H)
 424 2,853, 2,920, 2,955; ¹H NMR (ppm, CDCl₃) δ 0.88 (t, *J* =
 425 6.8 Hz, 6H, CH₃), 1.25 (s, 40H, CH₂), 1.56–1.63 (m, 4H,
 426 CH₂), 2.30 [td, 4H, ²*J*_{C–H} = 16.8 Hz, ³*J*_{C–H} = 7.6 Hz,
 427 CH₂C(=O)], 3.56–3.62 (m, 2H, CHCH₂OBn), 4.19 [dd, 2H,
 428 ²*J*_{C–H} = 11.2 Hz, ³*J*_{C–H} = 8.0 Hz, CHCH₂C(=O)], 4.34 [dd,
 429 2H, ²*J*_{C–H} = 12.0 Hz, ³*J*_{C–H} = 4.0 Hz, CHCH₂C(=O)],
 430 4.54 (d, 2H, ⁸*J*_{C–H} = 5.6 Hz, CH₂Ph), 5.22–5.27 (m, 1H,
 431 CH), 7.29–7.35 (m, 5H, C₆H₅); ¹³C NMR (ppm, CDCl₃)
 432 δ 14.1, 14.2, 22.7, 24.9, 29.1, 29.3, 29.5, 29.7, 29.8, 32.0,
 433 34.1, 34.4, 62.6, 68.3, 69.9, 73.3, 127.7, 128.5, 137.7, 173.2,
 434 173.5; Anal. Calcd for C₃₈H₆₅O₅: C, 75.83; H, 10.88.
 435 Found: C, 75.70; H, 10.92.
- 436 1,2-O-Dipalmitoyl-3-O-benzyl-sn-glycerol (**12b**) obtained
 437 as a white powder in 91% yield. Mp.: 40–41 °C; IR (KBr
 438 pellet, cm⁻¹) ν (C=O) 1,736, ν (C–H) 2,851, 2,918, 2,955;
 439 ¹H NMR (ppm, CDCl₃) δ 0.88 (t, *J* = 6.8 Hz, 6H, CH₃),
 440 1.25 (s, 48H, CH₂), 1.56–1.63 (m, 4H, CH₂), 2.30 (td, 4H,
 441 ²*J*_{C–H} = 16.8 Hz, ³*J*_{C–H} = 7.6 Hz, CH₂C(=O)), 3.56–3.62
 442 (m, 2H, CHCH₂OBn), 4.19 (dd, 2H, ²*J*_{C–H} = 11.2 Hz,
 443 ³*J*_{C–H} = 8.0 Hz, CHCH₂C(=O)), 4.34 (dd, 2H, ²*J*_{C–H} =
 444 12.0 Hz, ³*J*_{C–H} = 4.0 Hz, CHCH₂C(=O)), 4.54 (d, 2H,
 445 ⁸*J*_{C–H} = 5.6 Hz, CH₂Ph), 5.22–5.27 (m, 1H, CH), 7.28–
 446 7.36 (m, 5H, C₆H₅); ¹³C NMR (ppm, CDCl₃) δ 14.2, 22.7,
 447 24.9, 25.0, 29.0, 29.1, 29.3, 29.4, 29.5, 29.6, 29.7, 31.9,
 448 34.1, 34.3, 62.6, 68.2, 70.0, 73.3, 127.6, 127.7, 128.4, 137.7,
 449 173.1, 173.4; Anal. Calcd for C₄₂H₇₃O₅: C, 76.66; H, 11.18.
 450 Found: C, 77.48; H, 11.13.
- 451 1,2-O-Distearoyl-3-O-benzyl-sn-glycerol (**12c**) obtained as
 452 a white powder in quantitative yield. Mp.: 49–50 °C; IR (KBr
 453 pellet, cm⁻¹) ν (C=O) 1,734, ν (C–H) 2,851, 2,918, 2,957;
 454 ¹H NMR (ppm, CDCl₃) δ 0.88 (t, *J* = 6.8 Hz, 6H, CH₃),
 455 1.25 (s, 56H, CH₂), 1.56–1.63 (m, 4H, CH₂), 2.30 [td, 4H,
 456 ²*J*_{C–H} = 16.8 Hz, ³*J*_{C–H} = 7.6 Hz, CH₂C(=O)], 3.56–
 457 3.62 (m, 2H, CHCH₂OBn), 4.19 [dd, 2H, ²*J*_{C–H} = 11.2 Hz,
 458 ³*J*_{C–H} = 8.0 Hz, CHCH₂C(=O)], 4.34 [dd, 2H, ²*J*_{C–H} =
 459 12.0 Hz, ³*J*_{C–H} = 4.0 Hz, CHCH₂C(=O)], 4.54 (d, 2H,
 460 ⁸*J*_{C–H} = 5.6 Hz, CH₂Ph), 5.22–5.27 (m, 1H, CH), 7.29–
 461 7.35 (m, 5H, C₆H₅); ¹³C NMR (ppm, CDCl₃) δ 14.1, 22.7,
 462 24.9, 25.0, 29.0, 29.1, 29.3, 29.4, 29.5, 29.6, 29.7, 31.9, 34.1,
 463 34.3, 62.3, 68.2, 70.0, 73.3, 127.6, 127.8, 128.4, 137.7,
 464 173.1, 173.4; Anal. Calcd for C₄₆H₈₁O₅: C, 77.37; H, 11.43.
 465 Found: C, 77.96; H, 11.43.
- Typical Procedure for Synthesis of 1,2-O-Dimyristoyl-sn-* 466
Glycerol (13a) (Martin-SF, et al. *J Org Chem.* 467 Q6
 468 *1994;59:4805-20*) A solution of 1,2-O-dimyristoyl-3-O-
 469 benzyl-sn-glycerol **12a** (6.0 g, 10.0 mmol), 5% Pd/C
 470 (600 mg), and glacial acetic acid (20 ml) in ethanol
 471 (100 ml) was stirred under hydrogen atmosphere at room
 472 temperature. The reaction progress was monitored by TLC.
 473 When the reaction was complete, the reaction mixture was
 474 diluted with CH₂Cl₂, and the catalysts were removed by
 475 celite filtration. The filtrate was evaporated under reduced
 476 pressure, and the crude product was purified by column
 477 chromatography on SiO₂ with the EtOAc/hexane (1:3) to
 478 give **13c**, quantitatively, as a white solid (5.1 g, 10.0 mmol).
 479 Mp.: 56–58 °C; IR (KBr pellet, cm⁻¹) ν (C=O) 1,707,
 480 1,717, 1,732. ν (C–H) 2,851, 2,918, 2,957, ν (O–H) 3,649;
 481 ¹H NMR (ppm, CDCl₃) δ 0.88 (t, *J* = 6.8 Hz, 6H, CH₃),
 482 1.26 (s, 40H, CH₂), 1.56–1.63 (m, 4H, CH₂), 2.05 (t, 1H,
 483 *J* = 6.4 Hz, CH₂OH), 2.32 [td, 2H, ²*J*_{C–H} = 7.6 Hz, ³*J*_{C–H} =
 484 7.6 Hz, CH₂CH₂C(=O)], 2.35 [td, 2H, ²*J*_{C–H} = 7.2 Hz,
 485 ³*J*_{C–H} = 7.6 Hz, CH₂CH₂C(=O)], 3.72–3.74 (m, 2H,
 486 CHCH₂OH), 4.24 [dd, 2H, ²*J*_{C–H} = 12.0 Hz, ³*J*_{C–H} =
 487 5.6 Hz, CHCH₂C(=O)], 4.32 [dd, 2H, ²*J*_{C–H} = 12.0 Hz,
 488 ³*J*_{C–H} = 4.4 Hz, CHCH₂C(=O)], 5.06–5.11 (m, 1H, CH);
 489 ¹³C NMR (ppm, CDCl₃) δ 14.1, 22.7, 24.8, 24.9, 29.0,
 490 29.1, 29.2, 29.3, 29.5, 29.6, 29.7, 31.9, 34.1, 34.3, 61.5,
 491 62.0, 72.1, 173.4, 173.8; Anal. Calcd for C₃₁H₅₉O₅: C,
 492 72.75; H, 11.62. Found: C, 72.42; H, 11.64.
- 1,2-O-Dipalmitoyl-sn-glycerol (**13b**) was synthesized
 493 from **12b** (6.6 g, 10.0 mmol) using the procedure described
 494 for **13a** to give **13b** (5.3 g, 93%) as a white solid. Mp.: 62–
 495 64 °C; IR (KBr pellet, cm⁻¹) ν (C=O) 1,697, 1,717, 1,734,
 496 ν (C–H) 2,851, 2,918, 2,957, ν (O–H) 3,649; ¹H NMR (ppm,
 497 CDCl₃) δ 0.88 (t, *J* = 6.8 Hz, 6H, CH₃), 1.25 (s, 48H, CH₂),
 498 1.58–1.66 (m, 4H, CH₂), 2.08 (t, 1H, *J* = 6.4 Hz, CH₂OH),
 499 2.32, [td, 2H, ²*J*_{C–H} = 7.6 Hz, ³*J*_{C–H} = 7.6 Hz, CH₂CH₂C
 500 (=O)], 2.35 [td, 2H, ²*J*_{C–H} = 7.2 Hz, ³*J*_{C–H} = 7.6 Hz,
 501 CH₂CH₂C(=O)], 3.71–3.74 (m, 2H, CHCH₂OH), 4.24
 502 [dd, 2H, ²*J*_{C–H} = 12.0 Hz, ³*J*_{C–H} = 5.6 Hz, CHCH₂C
 503 (=O)], 4.32 [dd, 2H, ²*J*_{C–H} = 12.0 Hz, ³*J*_{C–H} = 4.4 Hz,
 504 CHCH₂C(=O)], 5.06–5.11 (m, 1H, CH); ¹³C NMR (ppm,
 505 CDCl₃) δ 14.1, 22.7, 24.8, 24.9, 29.0, 29.1, 29.2, 29.3,
 506 29.4, 29.5, 29.6, 29.7, 31.9, 34.1, 34.3, 61.6, 61.9, 72.1,
 507 173.4, 173.8; Anal. Calcd for C₃₅H₆₇O₅: C, 74.02; H,
 508 11.89. Found: C, 74.17; H, 11.90.
- 1,2-O-Distearoyl-sn-glycerol (**13c**) was synthesized from
 510 **12c** (7.2 g, 10.0 mmol) using the procedure described for
 511 **13a** to give **13c** (5.6 g, 89%) as a white solid. Mp.: 71–
 512 72 °C; IR (KBr pellet, cm⁻¹) ν (C=O) 1,697, 1,717, 1,734,
 513 ν (C–H) 2,851, 2,918, 2,957, ν (O–H) 3,649; ¹H NMR (ppm,
 514

515 CDCl₃) δ 0.88 (t, *J*=6.8 Hz, 6H, CH₃), 1.26 (s, 40H, CH₂),
516 1.56–1.63 (m, 4H, CH₂), 2.04 (t, 1H, *J*=6.4 Hz, CH₂OH),
517 2.33, [dd, 4H, ²*J*_{C-H}=16.6 Hz, ³*J*_{C-C-H}=8.0 Hz, CH₂CH₂C
518 (=O)], 3.72–3.75 (m, 2H, CHCH₂OH), 4.24 [dd, 2H, ²*J*_{C-H}=
519 12.0 Hz, ³*J*_{C-C-H}=5.6 Hz, CHCH₂C(=O)], 4.32 [dd, 2H,
520 ²*J*_{C-H}=12.0 Hz, ³*J*_{C-C-H}=4.4 Hz, CHCH₂C(=O)], 5.06–
521 5.11 (m, 1H, CH); ¹³C NMR (ppm, CDCl₃) δ 14.1, 22.7,
522 24.8, 24.9, 29.0, 29.1, 29.2, 29.3, 29.4, 29.5, 29.6, 29.7,
523 31.9, 34.1, 34.3, 61.6, 61.9, 72.1, 173.4, 173.8; Anal. Calcd
524 for C₃₉H₇₅O₅: C, 75.07; H, 12.11. Found: C, 75.01; H,
525 12.08.

526 *Typical Procedure for Synthesis of 3-O-chloroacetylcarbamoyl-*
527 *1,2-O-dimyristoyl-sn-glycerols (14a)* To a solution of **13a**
528 (5.1 g, 10.0 mmol) in CH₂Cl₂ (50 ml) was added
529 chloroacetyl isocyanate (Speziale AJ, et al. *J Org Chem*
530 **1963**, **28**, 1805–11) (1.4 g, 12.0 mmol) at 0 °C, and the
531 mixture was stirred for 6 h at 40 °C. After the reaction
532 mixture was concentrated under reduced pressure, the
533 product was purified by column chromatography on SiO₂
534 with CH₂Cl₂/CH₃OH (50:1) to give **14a** (4.7 g, 74%) as a
535 white solid: Mp.: 55–57 °C; [α]_D²⁸ = +2.1 (c1.0, CHCl₃);
536 IR (KBr pellet, cm⁻¹) ν(C=O) 1,732, 1,786, ν(C–H)
537 2,851, 2,920, 2,955, ν(N–H) 3,280; ¹H NMR (ppm,
538 CDCl₃) δ 0.88 (t, *J*=6.4 Hz, 6H, CH₃), 1.25 (s, 40H,
539 CH₂), 1.57–1.61 (m, 4H, CH₂), 2.32 [td, 4H, ²*J*_{C-H}=
540 11.2 Hz, ³*J*_{C-C-H}=7.6 Hz, 4H, CH₂C(=O)], 4.28 (dd,
541 ²*J*_{C-H}=11.2 Hz, ³*J*_{C-C-H}=7.6 Hz, 2H, CH₂), 4.29 (dd,
542 ²*J*_{C-H}=11.2 Hz, ³*J*_{C-C-H}=4.4 Hz, 2H, CH₂), 4.48 (s, 2H,
543 CH₂Cl), 5.22–5.26 (m, 1H, CH), 7.92 (s, 1H, NH); ¹³C
544 NMR (ppm, CDCl₃) δ 14.1, 22.6, 24.8, 29.0, 29.1, 29.2,
545 29.3, 29.4, 29.6, 29.7, 31.9, 33.9, 34.1, 43.5, 61.6, 64.4,
546 68.0, 150.7, 166.5, 172.9, 173.2; Anal. Calcd for
547 C₃₄H₆₂N₁O₇Cl: C, 64.58; H, 9.88; N, 2.22. Found: C,
548 64.26; H, 9.98; N, 2.27.

549 *3-O-Chloroacetylcarbamoyl-1,2-O-dipalmitoyl-sn-glycerol*
550 (**14b**) was synthesized from **13b** (5.7 g, 10.0 mmol) using
551 the procedure described for **14a** to give **14b** (5.9 g, 86%) as
552 a white solid: Mp.: 64–65 °C; [α]_D²⁸ = +1.45 (c1.0,
553 CHCl₃); IR (KBr pellet, cm⁻¹) ν(C=O) 1,736, 1,786,
554 ν(C–H) 2,851, 2,918, 2,950, ν(N–H) 3,358; ¹H NMR
555 (ppm, CDCl₃) δ 0.88 (t, *J*=6.4 Hz, 6H, CH₃), 1.28 (s, 48H,
556 CH₂), 1.57–1.61 (m, 4H, CH₂), 2.33 [td, 4H, ²*J*_{C-H}=
557 11.2 Hz, ³*J*_{C-C-H}=8.0 Hz, 4H, CH₂C(=O)], 4.30 (dd,
558 ²*J*_{C-H}=12.0 Hz, ³*J*_{C-C-H}=4.8 Hz, 2H, CH₂), 4.32 (dd,
559 ²*J*_{C-H}=12.0 Hz, ³*J*_{C-C-H}=4.4 Hz, 2H, CH₂), 4.49 (s, 2H,
560 CH₂Cl), 5.25–5.29 (m, 1H, CH), 7.93 (s, 1H, NH); ¹³C
561 NMR (ppm, CDCl₃) δ 14.0, 22.6, 24.8, 29.0, 29.1, 29.2,
562 29.3, 29.4, 29.5, 29.6, 29.7, 31.9, 33.9, 34.1, 41.9, 43.6,
563 61.7, 64.4, 68.4, 150.9, 166.8, 169.1, 172.8, 173.2; Anal.
564 Calcd for C₃₈H₆₉N₁O₇Cl: C, 66.40; H, 10.12; N, 2.04.
565 Found: C, 66.44; H, 10.07; N, 2.04.

3-*O*-Chloroacetylcarbamoyl-1,2-*O*-distearoyl-*sn*-glycerol
(**14c**) was synthesized from **13c** (6.3 g, 10.0 mmol) using
the procedure described for **14a** to give **14c** (7.4 g, >99%)
as a white solid: Mp.: 71–73 °C; [α]_D²⁸ = +1.35 (c1.0,
CHCl₃); IR (KBr pellet, cm⁻¹) ν(C=O) 1,734, 1,767, 1,786,
ν(C–H) 2,851, 2,918, 2,950, ν(N–H) 3364; ¹H NMR (ppm,
CDCl₃) δ 0.88 (t, *J*=6.0 Hz, 6H, CH₃), 1.25 (s, 56H, CH₂),
1.57–1.61 (m, 4H, CH₂), 2.33 [td, 4H, ²*J*_{C-H}=11.6 Hz,
³*J*_{C-C-H}=7.2 Hz, 4H, CH₂C(=O)], 4.28 (dd, ²*J*_{C-H}=
12.0 Hz, ³*J*_{C-C-H}=4.4 Hz, 2H, CH₂), 4.29 (dd, ²*J*_{C-H}=
12.0 Hz, ³*J*_{C-C-H}=4.4 Hz, 2H, CH₂), 4.48 (s, 2H, CH₂Cl),
5.25–5.29 (m, 1H, CH), 7.95 (s, 1H, NH); ¹³C NMR (ppm,
CDCl₃) δ 14.1, 22.7, 24.8, 29.0, 29.1, 29.3, 29.4, 29.5,
29.6, 29.7, 29.9, 31.9, 34.0, 34.3, 41.9, 43.5, 61.7, 64.5,
68.4, 150.7, 166.5, 172.9, 173.2; Anal. Calcd for
C₄₂H₇₈N₁O₇Cl: C, 67.75; H, 10.56; N, 1.88. Found: C,
68.86; H, 10.66; N, 1.86.

General Procedure for Synthesis of 4 and 5 To a solution
of B₁₂H₁₁SCH₂CH₂CN·2TMA **17** (300 mg, 0.8 mmol) in
CH₃CN (70 ml) was added 3-*O*-bromoacetyl-1,2-*O*-diacyl-
sn-glycerol **9** or 3-*O*-chloroacetylcarbamoyl-1,2-*O*-diacyl-
sn-glycerol **14** (1.2 equiv) at room temperature, and the
resulting suspension was stirred for 1 day at 70 °C. The
reaction mixture was concentrated under reduced pressure
and purified by column chromatography on SiO₂ with
EtOAc/acetone (5:1) as the eluent to give the compounds
18, which were immediately dissolved in a minimum
volume of acetone at room temperature, and an equimolar
amount of tetramethylammonium hydroxide (25% solution
in methanol) was added. The precipitate was filtered, and
the white solids obtained were washed with dry acetone
several times and dried under vacuum to give pure
products.

1,2-*O*-dimyristoyl-*sn*-glycerol-3-*O*-acetyl-SB₁₂H₁₁·2TMA
(**4a**) was obtained from **9a** (0.63 g, 1.0 mmol) as a white
powder (0.67 g, 76% yield): MS(ESI, negative) *m/z*=363.3
([M-2TMA]/2); Mp. 228–230 °C; [α]_D²⁸ = +8.7 (c0.50,
CH₃CN); IR (KBr pellet, cm⁻¹) ν(C=O) 1734, ν(B–H)
2496, ν(C–H) 2853, 2922, 2957; ¹H NMR (ppm, CD₃CN) δ
0.88 (t, 6H, ³*J*_{C-C-H}=6.8 Hz, CH₃), 1.27 (s, 40H, CH₂),
1.52–1.62 [m, 4H, CH₂CH₂C(=O)], 2.27 (dd, 2H, ²*J*_{C-H}=
6.4 Hz, ³*J*_{C-C-H}=2.8 Hz, OCH₂CH), 2.31 (dd, 2H, ²*J*_{C-H}=
7.6 Hz, ³*J*_{C-C-H}=2.8 Hz, OCH₂CH), 3.09 (s, 24H, NCH₃),
3.16 (s, 2H, CH₂S), 4.13 (dd, 2H, ²*J*_{C-H}=10.6 Hz, ³*J*_{C-C-H}=
6.4 Hz, SCH₂C(=O)OCH₂CH), 4.29 (dd, 2H, ²*J*_{C-H}=
12.0 Hz, ³*J*_{C-C-H}=3.6 Hz, SCH₂C(=O)OCH₂CH), 5.18–
5.22 (m, 1H, CH); ¹³C NMR (ppm, CD₃CN) δ 14.1, 23.1,
25.4, 29.5, 29.7, 29.8, 30.0, 30.1, 32.4, 34.4, 35.4, 55.9,
56.0, 56.1, 62.6, 62.8, 69.7, 173.4, 173.5, 173.7; Anal. Calcd
for C₄₁H₉₆B₁₂N₂O₆S: C, 56.28; H, 11.06; N, 3.20; S, 3.66.
Found: C, 56.21; H, 11.04; N, 3.26; S, 3.76.

- 617 1,2-*O*-dipalmitoyl-*sn*-glycero-3-*O*-acetyl-SB₁₂H₁₁-2TMA
 618 (**4b**) was obtained from **9b** (0.69 g, 1.0 mmol) as a white
 619 powder (0.75 g, 81% yield): MS(ESI, negative) *m/z*=391.4
 620 ([M-2TMA]²⁻); Mp. 219–221 °C; [α]_D²⁵ = +14.4 (c 0.50,
 621 CH₃CN); IR (KBr pellet, cm⁻¹) ν(C=O) 1,736, ν(B-H)
 622 2,494, ν(C-H) 2,851, 2,920, 2,957; ¹H NMR (ppm, CD₃CN)
 623 δ 0.88 (t, 6H, ³J_{C-C-H}=6.8 Hz, CH₃), 1.27 (s, 48H, CH₂),
 624 1.49–1.61 [m, 4H, CH₂CH₂C(=O)], 2.27 (dd, 4H, ²J_{C-H}=
 625 7.4 Hz, ³J_{C-C-H}=2.8 Hz, OCH₂CH), 2.30 (dd, 2H, ²J_{C-H}=
 626 7.4 Hz, ³J_{C-C-H}=2.8 Hz, OCH₂CH), 3.10 (s, 24H, NCH₃),
 627 3.17 (s, 2H, CH₂S), 4.13 [dd, 2H, ²J_{C-H}=11.6 Hz, ³J_{C-C-H}=
 628 6.8 Hz, SCH₂C(=O)OCH₂CH], 4.29 [dd, 2H, ²J_{C-H}=
 629 12.2 Hz, ³J_{C-C-H}=3.6 Hz, SCH₂C(=O)OCH₂CH], 5.17–
 630 5.22 (m, 1H, CH); ¹³C NMR (ppm, CD₃CN) δ 14.1, 23.1,
 631 25.4, 29.4, 29.5, 29.7, 29.8, 30.0, 30.1, 32.4, 34.5, 35.4,
 632 55.9, 56.0, 56.1, 62.6, 62.8, 69.7, 173.4, 173.5, 173.7; Anal.
 633 Calcd for C₄₅H₁₀₄B₁₂N₂O₆S₁: C, 58.05; H, 11.26; N, 3.01;
 634 S, 3.44. Found: C, 58.48; H, 11.28; N, 3.00; S, 3.44.
- 635 1,2-*O*-distearoyl-*sn*-glycero-3-*O*-acetyl-SB₁₂H₁₁-2TMA
 636 (**4c**) was obtained from **9c** (0.75 g, 1.0 mmol) as a white
 637 powder (0.90 g, 91% yield): MS(ESI, negative) *m/z*=419.4
 638 ([M-2TMA]²⁻); Mp. 215–217 °C; [α]_D²⁵ = +34.4 (c 0.50,
 639 CH₃CN); IR (KBr pellet, cm⁻¹) ν(C=O) 1736, ν(B-H)
 640 2,496, ν(C-H) 2,851, 2,918, 2,957; ¹H NMR (ppm,
 641 CD₃CN) δ 0.88 (t, 6H, ³J_{C-C-H}=6.8 Hz, CH₃), 1.27
 642 (s, 56H, CH₂), 1.52–1.61 [m, 4H, CH₂CH₂C(=O)], 2.27
 643 (dd, 2H, ²J_{C-H}=5.2 Hz, ³J_{C-C-H}=2.4 Hz, OCH₂CH), 2.31
 644 (dd, 2H, ²J_{C-H}=7.6 Hz, ³J_{C-C-H}=2.8 Hz, OCH₂CH), 3.09
 645 (s, 24H, NCH₃), 3.16 (s, 2H, CH₂S), 4.13 [dd, 2H, ²J_{C-H}=
 646 11.6 Hz, ³J_{C-C-H}=6.4 Hz, SCH₂C(=O)OCH₂CH], 4.29 [dd,
 647 2H, ²J_{C-H}=12.2 Hz, ³J_{C-C-H}=3.6 Hz, SCH₂C(=O)
 648 OCH₂CH], 5.16–5.24 (m, 1H, CH); ¹³C NMR (ppm,
 649 CD₃CN) δ 13.2, 22.2, 28.6, 28.7, 28.8, 28.9, 29.0, 31.5,
 650 33.5, 33.6, 55.0, 55.1, 55.2, 61.6, 61.7, 61.9, 68.8, 172.5,
 651 172.6, 172.9; Anal. Calcd for C₄₉H₁₁₂B₁₂N₂O₆S₁: C,
 652 59.61; H, 11.44; N, 2.84; S, 3.25. Found: C, 59.58; H,
 653 11.61; N, 2.84; S, 3.20.
- 654 1,2-*O*-dimyristoyl-*sn*-glycero-3-*O*-acetylcarbamoyl-
 655 SB₁₂H₁₁-2TMA (**5a**) was obtained from **14a** (0.63 g,
 656 1.0 mmol) as a white powder (0.49 g, 54% yield): MS(ESI,
 657 negative): *m/z*=384.8 ([M-2TMA]²⁻); Mp. 229–231 °C;
 658 [α]_D²⁵ = +20.4 (c 0.50, CH₃CN); IR (KBr pellet, cm⁻¹)
 659 ν(C=O) 1739, 1774, ν(B-H) 2484, ν(N-H) 3450, ν(C-H)
 660 2851, 2922, 2957; ¹H NMR (ppm, CD₃CN) δ 0.87 (t, 6H,
 661 ³J_{C-C-H}=6.8 Hz, CH₃), 1.26 (s, 40H, CH₂), 1.53–1.58 [m,
 662 4H, CH₂CH₂C(=O)], 2.28 (dd, 2H, ²J_{C-H}=6.4 Hz, ³J_{C-C-H}=
 663 2.8 Hz, OCH₂CH), 2.31 (dd, 2H, ²J_{C-H}=7.6 Hz, ³J_{C-C-H}=
 664 2.8 Hz, OCH₂CH), 3.09 (s, 24H, NCH₃), 3.15 (s, 2H, CH₂S),
 665 4.14 [dd, 2H, ²J_{C-H}=10.6 Hz, ³J_{C-C-H}=6.4 Hz, SCH₂C(=O)
 666 OCH₂CH], 4.29 [dd, 2H, ²J_{C-H}=12.0 Hz, ³J_{C-C-H}=3.6 Hz,
 667 SCH₂C(=O)OCH₂CH], 5.18–5.22 (m, 1H, CH), 9.67 (s, 1H,
 668 NH); ¹³C NMR (ppm, CD₃CN) δ 14.1, 23.1, 25.4, 29.5, 29.7,
 29.8, 30.0, 30.1, 32.4, 34.4, 35.4, 55.9, 56.0, 56.1, 62.6, 62.8,
 69.7, 173.4, 173.5, 173.7; Anal. Calcd for C₄₂H₉₆B₁₂N₃O₇S₁:
 C, 55.01; H, 10.55; N, 4.58; S, 3.50. Found: C, 54.85; H,
 10.60; N, 4.58; S, 3.69.
- 1,2-*O*-dipalmitoyl-*sn*-glycero-3-*O*-acetylcarbamoyl-
 SB₁₂H₁₁-2TMA (**5b**) was obtained from **14b** (0.69 g,
 1.0 mmol) as a white powder (0.59 g, 61% yield): MS
 (ESI, negative): *m/z*=412.9 ([M-2TMA]²⁻); Mp. 185–187 °C;
 [α]_D²⁵ = +12.7 (c 0.50, CH₃CN); IR (KBr pellet, cm⁻¹)
 ν(C=O) 1739, 1772, ν(B-H) 2,488, ν(N-H) 3,435, ν(C-H)
 2,851, 2,918, 2,957; ¹H NMR (ppm, CD₃CN) δ 0.87 (t, 6H,
³J_{C-C-H}=6.8 Hz, CH₃), 1.27 (s, 48H, CH₂), 1.49–1.61 [m,
 4H, CH₂CH₂C(=O)], 2.27 (dd, 4H, ²J_{C-H}=7.4 Hz, ³J_{C-C-H}=
 2.8 Hz, OCH₂CH), 2.30 (dd, 2H, ²J_{C-H}=7.4 Hz, ³J_{C-C-H}=
 2.8 Hz, OCH₂CH), 3.08 (s, 24H, NCH₃), 3.15 (s, 2H,
 CH₂S), 4.13 [dd, 2H, ²J_{C-H}=11.6 Hz, ³J_{C-C-H}=6.8 Hz,
 SCH₂C(=O)OCH₂CH], 4.28 [dd, 2H, ²J_{C-H}=12.2 Hz,
³J_{C-C-H}=3.6 Hz, SCH₂C(=O)OCH₂CH], 5.17–5.22 (m, 1H,
 CH), 9.69 (s, 1H, NH); ¹³C NMR (ppm, CD₃CN) δ 14.1,
 23.1, 25.4, 29.4, 29.5, 29.7, 29.8, 30.0, 30.1, 32.4, 34.5,
 35.4, 55.9, 56.0, 56.1, 62.6, 62.8, 69.7, 173.4, 173.5, 173.7;
 Anal. Calcd for C₄₆H₁₀₄B₁₂N₃O₇S₁: C, 56.77; H, 10.77; N,
 4.32; S, 3.30. Found: C, 56.76; H, 11.04; N, 4.39; S, 3.28.
- 1,2-*O*-distearoyl-*sn*-glycero-3-*O*-acetylcarbamoyl-
 SB₁₂H₁₁-2TMA (**5c**) was obtained from **14c** (0.74 g,
 1.0 mmol) as a white powder (0.86 g, 83% yield): MS(ESI,
 negative) *m/z*=440.9 ([M-2TMA]²⁻); Mp. 181–183 °C;
 [α]_D²⁵ = +125.4 (c 0.50, CH₃CN); IR (KBr pellet, cm⁻¹)
 ν(C=O) 1,740, 1,774, ν(B-H) 2,490, ν(C-H) 2,851, 2,918,
 2,957, ν(N-H) 3,425; ¹H NMR (ppm, CD₃CN) δ 0.88 (t, 6H,
³J_{C-C-H}=6.8 Hz, CH₃), 1.27 (s, 56H, CH₂), 1.52–1.61 [m,
 4H, CH₂CH₂C(=O)], 2.27 (dd, 2H, ²J_{C-H}=5.2 Hz, ³J_{C-C-H}=
 2.4 Hz, OCH₂CH), 2.31 (dd, 2H, ²J_{C-H}=7.6 Hz, ³J_{C-C-H}=
 2.8 Hz, OCH₂CH), 3.06 (s, 24H, NCH₃), 3.11 (s, 2H, CH₂S),
 4.13 [dd, 2H, ²J_{C-H}=11.6 Hz, ³J_{C-C-H}=6.4 Hz, SCH₂C(=O)
 OCH₂CH], 4.29 [dd, 2H, ²J_{C-H}=12.2 Hz, ³J_{C-C-H}=3.6 Hz,
 SCH₂C(=O)OCH₂CH], 5.20–5.25 (m, 1H, CH), 9.72 (brs,
 1H, NH); ¹³C NMR (ppm, CD₃CN) δ 14.1, 14.6, 23.1, 25.4,
 29.5, 29.7, 29.8, 29.9, 30.0, 30.1, 32.3, 34.4, 34.5, 38.9, 55.8,
 55.9, 56.0, 62.6, 63.8, 69.4, 160.5, 169.7, 172.2, 173.6; Anal.
 Calcd for C₅₀H₁₁₃B₁₂N₃O₇S₁: C, 58.29; H, 11.06; N, 4.08; S,
 3.11. Found: C, 58.68; H, 11.14; N, 4.20; S, 3.19.
- Preparation of Calcein-Encapsulated Boronated Liposomes*
 Boronated liposomes were prepared from cholesterol,
 dimyristoylphosphatidylcholine (DMPC), and boron
 cluster lipids (**4a–c** and **5a–c**) (1:1-*X*:*X*, *X*=0–1, molar
 ratio) by the REV method. The representative procedure for
 the preparation of 25% of **4c** containing liposomes is shown
 as follows: A mixture of DMPC (17.0 mg), cholesterol
 (19.3 mg), and **4c** (24.4 mg) were dissolved in 10 ml of
 chloroform/diisopropylether mixture (1:1, v/v) in a round-

- 721 bottom flask. An aqueous solution of calcein (100 mM,
722 5 ml) was added to the lipid solution to form an emulsion.
723 The volume ratio of the aqueous phase to the organic phase
724 was maintained at 1:2. The emulsion was sonicated for
725 1 min, and then the organic solvent was removed under
726 vacuum in a rotary evaporator at 37 °C with broken down
727 repeatedly to obtain a suspension of liposomes. The
728 liposomes obtained were subjected to extrusion ten times
729 through a polycarbonate membrane of 100-nm pore size,
730 using an extruder device (Lipex Biomembrane, Canada)
731 thermostated at 60 °C. Purification was accomplished by
732 ultracentrifuging at 200,000×g for 60 min at 4 °C (Hitachi
733 himac 65β, P50AT2 rotor), and the pellets obtained were
734 resuspended in PBS buffer. Liposome size was measured
735 with an electrophoretic light scattering spectrophotometer
736 (ELS-700, Otsuka Electronics, Tokyo).
- 737 *Stability of Boronated Liposomes in Fetal Bovine*
738 *Serum* The calcein-encapsulated boronated liposomes were
739 added to a fetal bovine serum (FBS) (volume ratio: FBS/
740 liposome solution=9:1), and the mixture was incubated at
741 37 °C with stirring. The fluorescence intensity of the FBS
742 solutions was measured at 0–24 h using an excitation
743 wavelength of 490 nm with emission-wave length of
744 520 nm. The fluorescence intensity was also measured at
745 each fraction after degradation of liposomes by the addition
746 of a 1% aqueous solution of Triton X-100 to the FBS
747 solution.
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753 neutron capture therapy with advanced drug delivery system.
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中性子捕捉がん治療のための次世代ホウ素デリバリーシステム

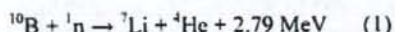
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1. はじめに

高齢化の進む我が国の死亡原因の第一位はがんであり、その年間死亡者数はおよそ 30 万人である。がん検診の普及、早期診断・早期治療、さらには初期治療としての手術・放射線・化学療法の進歩によって、ある程度治癒率の改善がみられるものの、化学療法では全身的な副作用との戦い、放射線治療では照射野内の正常組織損傷の問題が常に存在する。このような中で、化学療法と放射線療法の両方の原理を上手く利用したホウ素中性子捕捉療法 (BNCT: boron neutron capture therapy) が注目されている。

熱中性子は人体には無害であるが、ホウ素 10 と反応することにより、リチウムとヘリウム (α 線) を生じる。これらの粒子エネルギーは 2.79MeV とおよそ 1 つの細胞を破壊するのに十分なエネルギーである (式 1)。この核反応を利用しがんを殺傷するのが BNCT である。BNCT は、世界に先駆け日本で初めて臨床応用に成功を収めて以来、世界をリードしてきた分野であるが、原子炉からの熱・熱外中性子線を利用しているため、対応できる治療患者数および地域が限られている。現在、病院内設置可能な BNCT 用加速器の開発が日本をはじめ全世界で進められており、加速器から十分な熱中性子が得られるようになれば、都市型病院への併設が可能となることから BNCT は細胞選択的放射線療法として一般に普及することが期待される。



では、なぜホウ素分子なのか？中性子を原子核に照射した際に、中性子を捕捉する大きさ“中性子捕捉断面積”を主な元素について比較した (Table 1)。中性子捕捉断面積はバーン ($1 \text{ barn} = 10^{-24} \text{ cm}^2$) という単位で表される。 ^{135}Xe , ^{149}Sm , ^{151}Eu , ^{157}Gd などがきわめて大きい値を示している。 ^{10}B の中性子捕捉断面積は 3837 バーンとそれほど大きな値は示していないのに、中性子捕捉療法に有望であるのは主に次に挙げる 4 つの理由からである。(i) ^{10}B は非放射性で天然のホウ素に約 20% 含まれるため入手容易である。(ii) 上で述べたように核反応の際の α 線の飛程が 1 個の細胞内に限られる。(iii) ホウ素の広範な化学反応性と安定性により種々の生物活性分子や生体関連物質への導入が可能である。(iv) 重金属のような高い毒性を示さない。一方、生体中の元素も中性子を捕捉して放射線を生じるが、その中性子捕捉断面積は ^{10}B よりも数桁小さな値なので (Table. 1) 通常は無視できる。しかしながら水素と窒素は生体中に高濃度に存在するため、中性子の照射線量に大きく影響す

る。したがってこれらの影響を最小限にするためにも、腫瘍組織内の ^{10}B 濃度が $20\sim 35\mu\text{g/g}$ 、もしくは ^{10}B 原子が 10^9 個/細胞であれば、放射線量のおよそ85%が ^{10}B の中性子捕捉反応から生じると計算されている¹⁾。最終的には照射できる中性子線量の上限は、水素と窒素が中性子を捕捉して出す放射線に周囲の正常組織がどれほど耐えられるかに依存する。このためにも ^{10}B ががん細胞に選択的に集積することが必要であり、実際に臨床上の立場から腫瘍組織内 ^{10}B 濃度が $30\mu\text{g/g}$ 以上、 ^{10}B 濃度の腫瘍組織/血液および腫瘍組織/正常組織の比がいずれも5以上が望ましいとされている。

Table 1. Capture Cross Section Values of Various Nuclides for Thermal Neutrons

nuclide	cross section capture value ^a	nuclide	cross section capture value ^a
^6Li	942	H	0.332
^{10}B	3838	C	0.0037
^{113}Cd	20,000	N	1.75
^{135}Xe	2,720,000	O	<0.0002
^{149}Sm	41,500	P	0.19
^{151}Eu	59,002	S	0.52
^{157}Gd	240,000	Na	0.536
^{174}Hf	400	K	2.07

^a Cross section capture values in barns.

2. ホウ素デリバリーシステム

近年、ホウ素のがん組織への有効な送達法としてドラッグデリバリーシステムの利用が注目されている²⁾。リポソーム DDS を用いたホウ素デリバリーの方法として、大きく2つの戦略に分けられる (Figure 1)。一つは、ホウ素薬剤をリポソーム内に封入する方法である。この方法は、一般的なリポソームを用いた DDS を応用するものであり、BSH などのホウ素化合物を封入する^{3,5)}。もう一つの方法として、我々はホウ素をリポソーム膜に埋め込む方法を考えた。この方法では、リポソーム内にさらに抗がん剤などの薬剤を封入することができるため、化学療法との複合治療が期待できる。いずれの場合も、リポソーム膜を PEG 化することで EPR (enhanced permeability and retention) 効果を高めたり、さまざまな分子をリポソーム膜に結合させることにより、能動的にターゲティングできるような機能を持たせることが可能となってきた。

リポソーム膜内にホウ素を導入したホウ素リポソームの最初の報告は、Hawthorne らによって開発された一本鎖ホウ素イオンクラスター脂質 1 (Figure 2) を用いたものであった⁶⁾。この化合物は炭素鎖 16 の脂溶性部位と水溶性の nido 型カルボラン部位からなる両親媒性分子である。彼らは、DSPC、コレステロール、nido 型カルボラン脂質 1 からリポソームを調製した。EMT6 細胞を移植

したマウスを用いて生体内ホウ素分布を調べたところ、投与ホウ素濃度 6 mg/kg では腫瘍内ホウ素濃度が投与後 6 時間で 22 ppm、その後 16~30 時間はおよそ 34 ppm で一定であった。48 時間後には 25 ppm に低下したものの T/N 比は 8.4 であった。

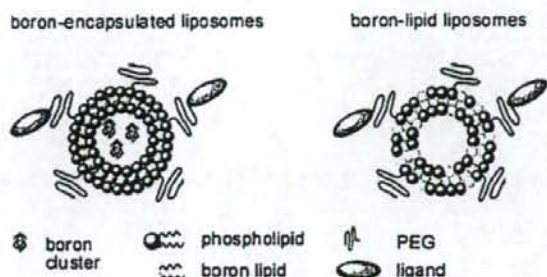


Figure 1. Boron-encapsulated liposomes and boron-lipid liposomes.

一方、我々はリポソーム膜へ効率良くかつ安定に生成するためには、二分子膜を形成しているリン脂質のように脂溶性部位が二本鎖であれば良いと考えた。そこで、二本鎖ホウ素イオンクラスター脂質 2 を設計した⁷⁾。電子顕微鏡で確認したところ、合成したイオン性ホウ素クラスター脂質 2 から 150~200 nm の大きさのベシクルが形成していることが分かった。これは世界で初めてのホウ素脂質ベシクルである。このホウ素イオンクラスター脂質 2 と DSPC、コレステロールを用いて、能動的ターゲティングを指向した TF 結合型ホウ素クラスターリポソームを合成し、坦癌マウスを用いた体内分布ならびに中性子捕捉治療を行った⁸⁾。左足に Colon 26 細胞を移植した BALB/c マウス（生後 6 週間、16~18 g）にトランスフェリン修飾型ホウ素クラスターリポソームをホウ素濃度で 7.2 mg/kg 投与したマウスでは、72 時間後、筋肉・心臓・脳ではホウ素蓄積はほとんど見られなかった。肺・血液ではおよそ 10 ppm、脾臓・肝臓では非常に高いホウ素蓄積が見られた。腫瘍内ホウ素蓄積量を見てみると 7.2 mg/kg 投与した場合には 22 ppm、14.4 mg/kg 投与の場合には 40 ppm であった。最近、Hawthorne らも同様な二本鎖ホウ素イオンクラスター脂質 3 を開発している⁹⁾。

このように、二本鎖ホウ素イオンクラスター脂質は安定なホウ素リポソームを形成し、腫瘍へも効率よく集積することが分かった。しかしながら、ホウ素濃度で 14.4 mg/kg 投与した場合に急性毒性が一部のマウスに見られたことから、我々はより低毒性なホウ素脂質の開発を目指し次世代ホウ素イオンクラスター脂質 4 および 5 を設計した¹⁰⁾。この脂質は、脂溶性部位に生体リン脂質 (Phosphatidylcholines) と同じ立体構造を有しており、リンカー部位にエステル基(脂質 4)またはカルバメート基(脂質 5)を有し、BSH と S を介して結合している。これらのホウ素脂質から調整したリポソームは、正常マウスに対しホウ素濃度で 20 mg/kg では急性毒性は見られなかった¹¹⁾。

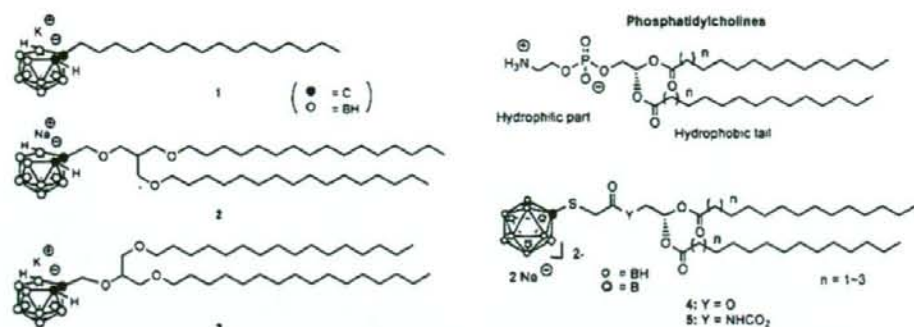


Figure 2. Structures of *nido*-carborane lipids 1-3 and closo-dodecaborate lipids 4 and 5

3. BNCT 効果

ホウ素脂質 4 ($n = 16$)、DSPC、DSPE-PEG2000、コレステロール（それぞれ 0.25:0.75:0.1:1.0）から調整したホウ素リポソームを用いて上記と同様に Colon 26 細胞を移植した BALB/c マウスに尾静脈より投与し (20 mgB/kg) ホウ素分布を調べたところ、投与 24 時間後に腫瘍内ホウ素濃度が 22 ppm であった (Figure 3)。そこで、投与 24 時間後に中性子照射を行い腫瘍の経時的变化を調べたところ、Figure 4 に示すようにホウ素リポソームを投与したマウスでは、中性子照射 1 週間後には腫瘍の委縮が見られ増殖抑制が見られた。

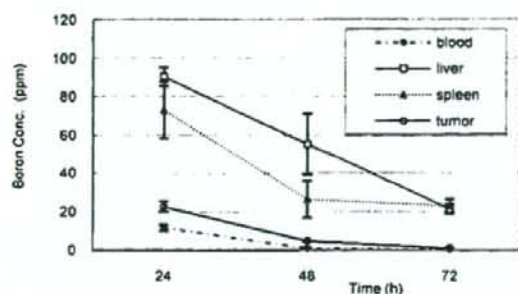


Figure 2. Time course of biodistribution of boron liposomes prepared from 4c in tumor-bearing mice.

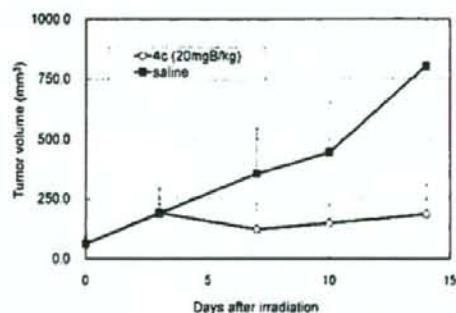


Figure 3. Tumor growth curve of mice bearing colon 26 tumors after injection of 20mg¹⁰B/kg of boronliposomes, thermal neutron irradiation with $0.9\text{-}1.4 \times 10^{12} \text{ n/cm}^2$.

4. おわりに

BNCTのためのホウ素キャリアーの開発には、いわゆるナノモルレベルで薬理効果が要求される抗がん剤のようなドラッグデザインではなく、ミリモルレベルで投与できるのに十分な低毒性であり、なおかつ腫瘍細胞に集積することが必要とされる。そのために、低毒性小分子ホウ素化合物の

開発だけでなく、リボソームを用いたホウ素デリバリーシステムの開発が十数年前から盛んに研究されてきた。BNCTにおいて1950年代に開発されたBSH、BPAという2剤以外には、まだ臨床応用されたホウ素薬剤は残念ながら登場してない。現在、核燃料の問題からBNCTに適応できる小型加速器の開発が精力的に行われている。熱中性子源が原子炉から加速器に移行できれば都市部病院併設型加速器によるBNCTが可能となることから、将来放射線療法の一般的治療法の一つになるであろう。そのためにも治療効果の高いホウ素デリバリーシステムの開発が期待される。

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