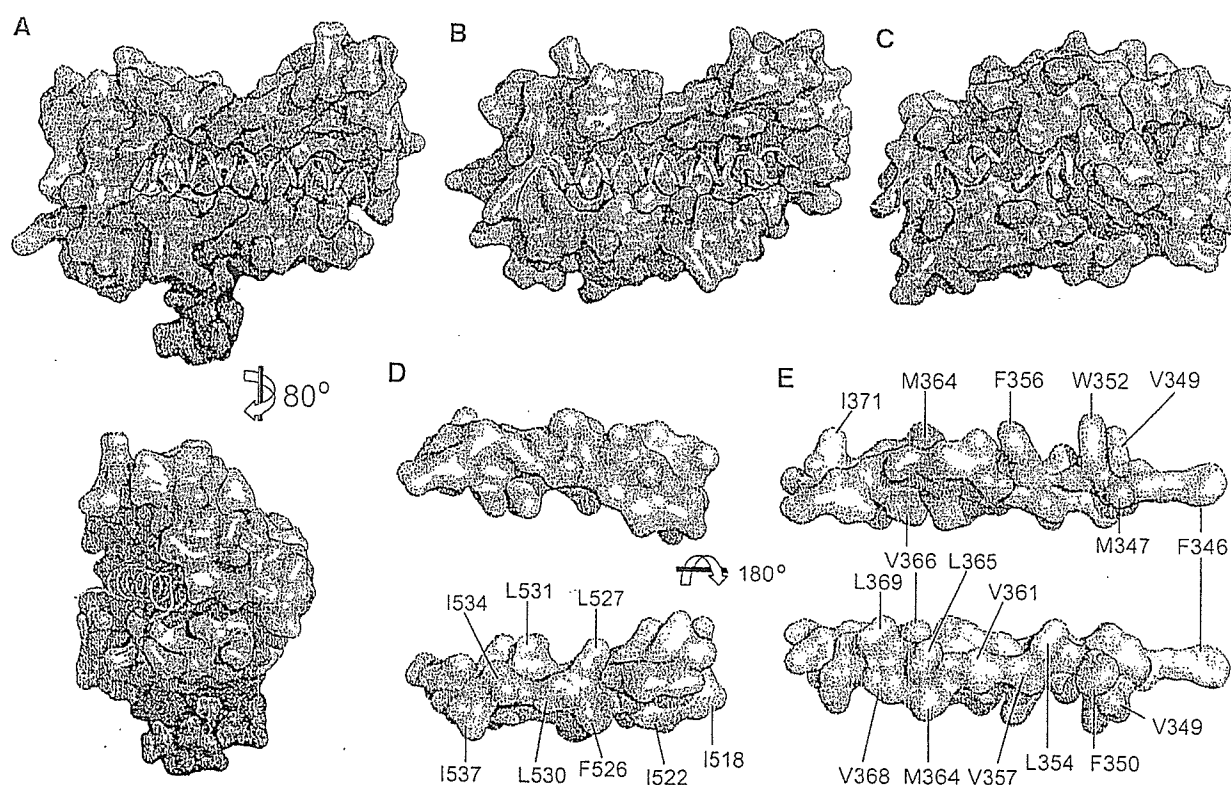


$Y^{3+}$ -bound form of CHP2 preserved the ability to interact with the full-length NHE1 (Supplementary Figure 1). Therefore, we consider our solved structure compatible with the  $Ca^{2+}$ -bound form of CHP2. The overall structure of CHP2 is also similar in folding topology to the structures of other EF-hand-containing proteins, including CNB (Kissinger *et al*, 1995),  $K^+$ -channel interacting protein (KChIP1) (Zhou *et al*, 2004; Supplementary Figure 2), AtCBL2 (Nagae *et al*, 2003), NCS-1 (Bourne *et al*, 2001), neurocalcin (Vijay-Kumar and Kumar, 1999), and CIB (Gentry *et al*, 2005). A common structural feature of these proteins is that they all have four EF-hands in pairs such that EF1 and EF2 form the N-lobe and EF3 and EF4 form the C-lobe. However, some local differences were observed between CHP2 and CNB or between CHP2 and KChIP1. For example, the orientation of EF-hand  $\alpha$ -helices is different among these molecules because of the swiveling motion between the N- and C-lobes of each molecule, although each pair of EF hands is relatively fixed via hydrogen bonds. This may explain the incomplete superposition between overall structures of CHP2 and CNB (root mean square deviation, r.m.s.d. 1.7 Å), in contrast to the relatively good superposition between the N-lobes or between the C-lobes themselves (r.m.s.d. 1.3 or 1.0 Å, respectively). Although CHP2 and CNB have about 36% identity in their amino-acid sequences (Figure 1C), CHP2 coordinates two  $Ca^{2+}$  ions in EF3 and EF4, unlike CNB capable of coordinating four  $Ca^{2+}$  ions in its four EF-hands (Kissinger *et al*, 1995). Lack of  $Ca^{2+}$ -coordination in EF1 and EF2 would be derived from significant deviation from the canonical EF-hand sequence and resulting atypical structure, as described previously in detail (Naoe *et al*, 2005).

The most remarkable difference between CHP2 and other calcium binding proteins is that the N- and C-lobes of CHP2 are linked by a long flexible region, which protrudes by a length of about 14 Å for the determined region (Figure 3A). This domain, referred to as the CHP-unique region, was not found in other  $Ca^{2+}$ -binding proteins. Five residues, Thr100 to Lys104, were not assigned in the structure due to the absence of their electron density map. Particularly, the region from aa 93–108 did not make any contact with other regions of CHP2. In addition, we found that the side chain oxygen atoms of Asp95 in this region coordinate  $Y^{3+}$  in the neighboring molecule in the crystal and thus participate in stabilization of this region. This observation explains why CHP2/NHE1-peptide was crystallized only in the presence of  $Y^{3+}$ . These findings suggest that the CHP-unique region is very flexible in aqueous solution. This is consistent with the finding that this region was not seen in the structure of NHE-free CHP1 (Naoe *et al*, 2005), which was solved in different crystal packing.

#### Interaction between CHP2 and its binding domain in NHE1

Structure determination of the complex revealed the orientation of CHP2 toward the cytoplasmic region of NHE1. The N- and C-terminal halves of the cytoplasmic  $\alpha$ -helix of NHE1 are inserted into the hydrophobic cleft in such a way that they face the C- and N-lobes of CHP2, respectively (Figure 3A). This cleft constitutes the region that traps the cytoplasmic  $\alpha$ -helix of NHE1 and maintains the stability of the complex by means of hydrophobic interactions. The contact area between CHP2- and NHE1 peptide is 1466 Å<sup>2</sup>, which accounts for 13.0

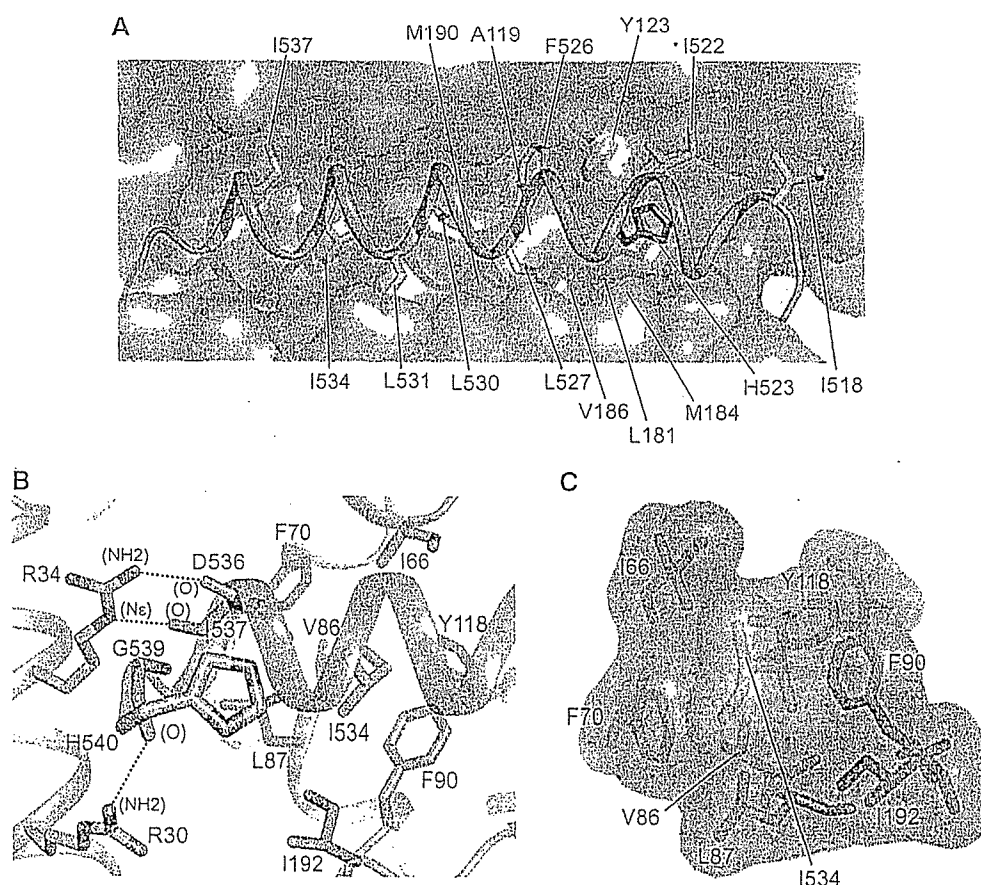


**Figure 3** Target specificity of hydrophobic cleft. (A–C) Surface features of CHP2, CNB, and KChIP1 are presented together with  $\alpha$ -helices of target peptides, respectively. In CHP2, front (upper) and side (lower) views are shown. The N- and C-lobes are colored light blue and light green, while the CHP-unique region is colored red. (D, E) Surface view of NHE1 (left) and CNA (right) peptides, respectively. The upper panels indicate the side facing outside the cleft and the lower panels represent the side facing the cleft. Hydrophobic residues are colored yellow.

and 59.8% of the total surface areas, respectively, implying that a large area is used for interaction between the two molecules. The NHE1 peptide (Arg516–His540) solved in this structure contains different hydrophobic residues, all of which face toward the hydrophobic cleft of CHP2 (Figure 3D). Ile518, Ile522, Phe526, Leu527, and Leu530 are accommodated into the cavity formed by hydrophobic residues provided mainly from the C-lobe of CHP2, whereas Leu531, Ile534, and Ile537 are inserted into the cavity formed mainly by the N-lobe of CHP2 (Figure 4A and B). All hydrophobic side chains of the NHE1 peptide, with the exception of Ile518, make van der Waals contacts with side chain atoms from many hydrophobic residues of CHP2. For example, side chain atoms of Ile534 make van der Waals contacts with those of Leu57, Ile66, Phe70, Val86, Leu87, Phe90, Tyr118, and Ile192 of CHP2 (Figure 4C), while side chain atoms of Leu527 make interactions with those of Ala119, Leu181, Val186, Met184, and Met190 (Figure 4A). In addition to hydrophobic interactions, hydrogen bonds strengthen the association between CHP2 and NHE1 peptide. In the N-lobe of CHP2, the guanidinium group of Arg30 makes hydrogen bonds with the main chain carbonyl oxygen of Gly539, while the guanidinium group of Arg34 makes hydrogen bonds with the main chain carbonyl oxygens of Asp536 and Ile537 (Figure 4B). These hydrogen bonds are very important for the C-terminal end of the NHE1 helix to fix to the edge of the hydrophobic cleft of CHP2. The conserved Gly539 residue of NHE1 would

allow the following cytoplasmic stretch to leave the cleft by inducing clear bending of the NHE1 peptide (Figures 3A and 4B). Several other hydrogen bonds are also formed. The hydrogen bond between the imidazole group (N $\delta$ ) of His523 in NHE1 and the side chain oxygen of Tyr123 in CHP2 is particularly interesting because it is the only polar interaction in the hydrophobic surface of the cleft (Supplementary Figure 3). These polar interactions are important to determine the specificity and orientation of CHP2 toward the cytoplasmic  $\alpha$ -helix of NHE1.

Although CNB and KChIP1 have similar hydrophobic clefts (Figure 3B and C), their size and shape are clearly different from those of CHP2. Interestingly, target peptides show sequence features that just fit to their clefts. While NHE1 peptide shows a uniform distribution of hydrophobic residues all facing toward the cleft of CHP2 (Figure 3D), CNA contains more hydrophobic residues that face toward both the CNB crevice and the outside (Figure 3E). In addition, CNA peptide contains four aromatic residues (Phe346, Phe350, Trp352, and Phe356) in the N-terminus, which are accommodated in corresponding hydrophobic cavities in the C-lobe of CNB, whereas NHE1-peptide contains only one aromatic residue (Phe526) located in the central part of CHP2. These observations suggest that highly selective fitting of each peptide to its corresponding crevices may be caused by differences in the distribution of hydrophobic residues of the target peptides and in the shape of the cleft formed by  $\alpha$ -helices of EF-hands.



**Figure 4** Closeup view showing the interaction between CHP2 and NHE1-peptide. (A) The NHE1-peptide backbone is shown in *magenta*, while hydrophobic side chains are shown in *yellow*. The hydrophobic pocket surrounding Leu527 is marked in *red*. His523 of NHE1 and Tyr123 of CHP2 are marked in *blue*. (B) Closeup view showing interaction between the N-lobe of CHP2 and the C-terminus of NHE1-peptide. (C) Ile534 is accommodated into the hydrophobic pocket produced by residues mainly in the N-lobe of CHP2.

### Effect of mutations on interaction between NHE1 and CHP2 in cells

The present structure indicated that the correct CHP-binding domain of NHE1 consists of the region from aa 516–540, extended by 10 residues toward the C-terminus of the region (aa 510–530), as predicted previously (Pang *et al*, 2001). This prompted us to mutate residues in this extended region of NHE1 interacting with the N-lobe of CHP2. We mutated the Ile534 and Ile537 residues of NHE1 into charged residues (Lys or Asp) and stably expressed these mutants in exchanger-deficient PS120 cells. These mutants were expressed in the plasma membrane (as indicated by the existence of surface-expressed mature NHE1 in Supplementary Figure 4). We examined the interactions of these mutants with CHP2 by assessing whether stably transfected green fluorescent protein (GFP)-tagged CHP2 was localized to the plasma membrane. As shown in Figure 5A, most of the CHP2 was localized to the plasma membrane of cells expressing the wild-type NHE1 but not in nontransfected PS120 cells (not shown; see Pang *et al*, 2001), indicating a strong interaction. Of note, in most cells expressing the wild-type NHE1 almost no GFP-fluorescence was detected in the intracellular space (Figure 5A), despite the accumulation of immature NHE1 in the intracellular membranes under forced expression (data not shown), suggesting that CHP2 interacts predominantly with mature NHE1 in the plasma membrane. This was further confirmed by the finding that almost no immature NHE1 co-immunoprecipitated with CHP2 (Supplementary Figures 1 and 4). In contrast to the wild-type NHE1, the plasma membrane localization of CHP2 was almost completely abolished when transfected into cells expressing the NHE1 mutants, I534K, I534D and I537K (Figure 5, and also D for summarized data), indicating that these mutations drastically reduced the affinity for interaction with CHP2.

Furthermore, as expected, the plasma membrane localization of CHP2 was also markedly reduced in cells expressing the wild-type NHE1 when Leu87 or Tyr118 of CHP2 was changed to Lys (Figure 5C and D), indicating that these mutants are not able to replace completely endogenous CHP1 bound to NHE1. As the expression of GFP-tagged CHP2 was approximately 10-fold higher than that of endogenous CHP1 (data not shown), these results suggest that these mutations would reduce the affinity for interaction with NHE1 at least one-order of magnitude. Similar analysis was performed with mutation of the Arg residues (Arg30 and Arg34) in the N-terminal  $\alpha$ -helix of CHP2. The plasma membrane localization of CHP2 was abolished when these two residues were simultaneously changed to Glu (Figure 5C and D), while it was still partially preserved when either Arg residue alone was changed to Glu. Similar results were also obtained for the NHE1/CHP2 interaction in a co-immunoprecipitation experiment (Supplementary Figure 4). Thus, the hydrophobic and polar interactions involving these residues would be important in determining the strong and highly specific association between NHE1 and CHP2. Furthermore, in addition to the C-lobe, the N-lobe of CHP2 plays a crucial role in the tight interaction with NHE1, suggesting that our crystal structure reflects the interaction between native NHE1 and CHP2 molecules expressed in cells. On the other hand, structure determination indicated the existence of a unique protruding region in CHP2. In contrast to mutations of residues involving formation of the cleft, a mutant with deletion

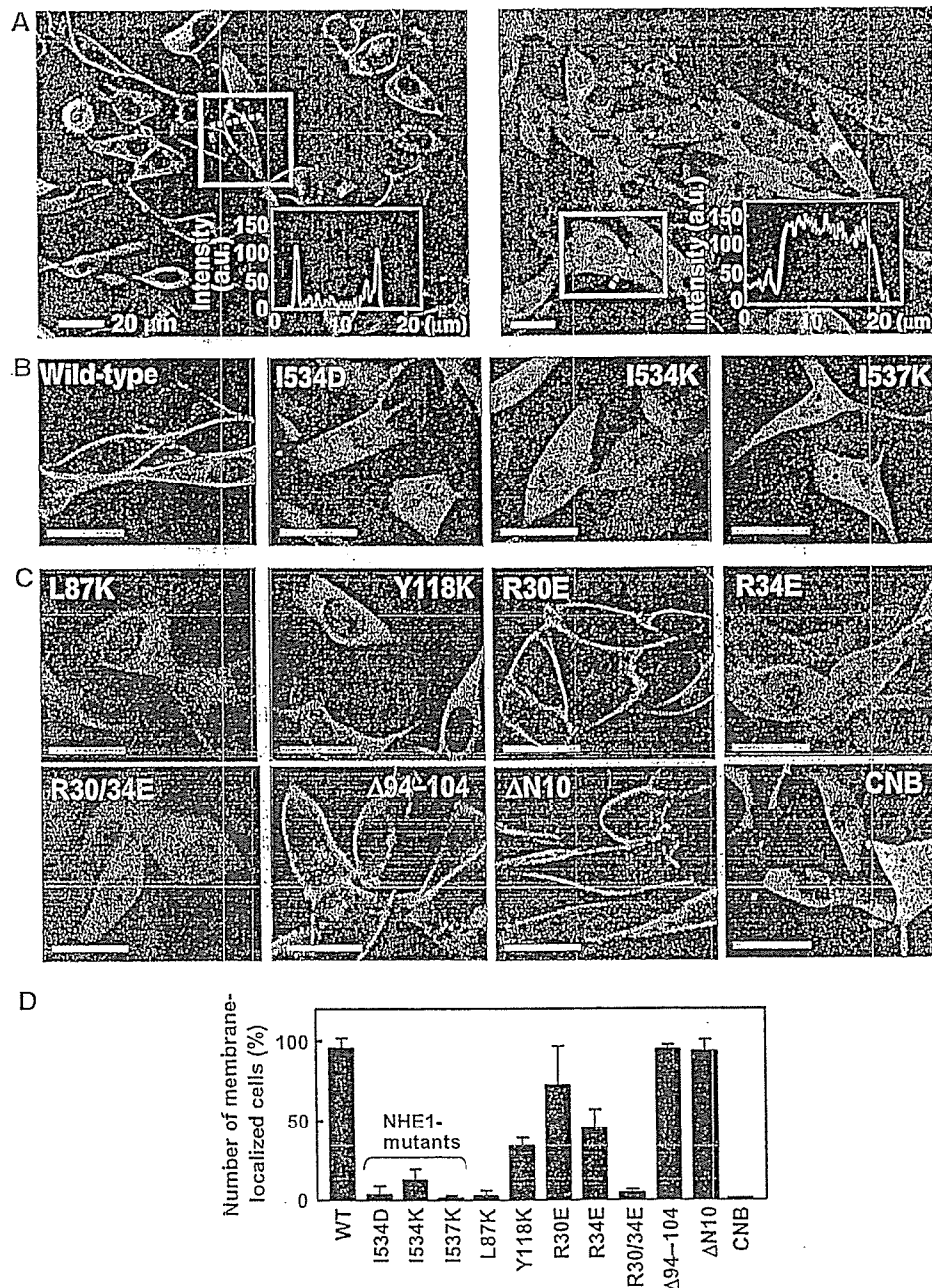
of this CHP-unique region ( $\Delta$ 94–104) was mostly localized to the plasma membrane of cells expressing wild-type NHE1 (Figure 5C), indicating that deletion did not disrupt the interaction of CHP2/NHE1. Hence, as also predicted from structure, the CHP-unique region was not involved in the interaction between CHP2/NHE1. The 10 N-terminal residues of CHP2 were also found not to be involved in the interaction, as indicated by the plasma membrane localization of  $\Delta$ N10 (Figure 5C).

### Functional consequence of mutations

We measured the NHE activity in cells expressing mutant exchangers. Figure 6A demonstrates the  $pH_i$ -dependence of EIPA-sensitive  $^{22}\text{Na}^+$ -uptake activity. While the wild-type NHE1 exhibited high  $^{22}\text{Na}^+$ -uptake activity, with  $pK \sim 6.5$  for  $pH_i$  (Hill coefficient,  $\sim 1.7$ ), the activity of mutant exchangers, I534D, I534K and I537K, which lack CHP-binding was very low (see Supplementary Table I for kinetic parameters). The inhibitory effect of the mutations was characterized by changes in two parameters: (i) a drastic reduction of maximal  $^{22}\text{Na}^+$ -uptake activity ( $V_{\max}$ ) at acidic  $pH_i$ , and (ii) a large acidic shift of the  $pH_i$ -dependence of uptake ( $> 0.6$  pH units) (see Figure 6A, inset for normalized activity). We then compared the  $pH_i$ -dependence of  $^{22}\text{Na}^+$ -uptake in cells co-expressing NHE1 with GFP-tagged CHP2 or its deletion mutant  $\Delta$ 94–104, which preserves interaction with CHP. Interestingly, expression of  $\Delta$ 94–104 significantly shifted the  $pH_i$ -dependence of uptake towards acidic  $pH_i$  ( $\sim 0.2$  pH unit) without any change in  $V_{\max}$ , while it preserved the cooperative  $pH_i$  dependence, with a Hill coefficient  $\sim 1.5$  (Figure 6B, see also inset for the sigmoidal internal  $H^+$  dependence), suggesting that the CHP-unique region is involved in regulation of pH-sensing of NHE1. In general, the sigmoidal  $H^+$ -dependence has been interpreted as exhibiting involvement of at least two  $H^+$ -binding sites:  $H^+$ -transport and  $H^+$ -regulatory sites in NHE (Wakabayashi *et al*, 1997). To examine the effect of deletion of a CHP-specific region on the  $H^+$ -regulatory site, we measured the reverse reaction of NHE1, that is,  $^{22}\text{Na}^+$  efflux coupled to  $H^+$ -influx. If we assume that NHE1 catalyzes a counter-transport reaction only involving the transport site, intracellular acidification should result in inhibition of  $^{22}\text{Na}^+$  efflux due to cytosolic  $\text{Na}^+/\text{H}^+$  competition. In contrast to this thermodynamically expected inhibition, modest acidification from 7.5 to 7.2 dramatically stimulated the rate of EIPA-inhibitable  $^{22}\text{Na}^+$  efflux in cells co-expressing the wild-type NHE1 and CHP2 (Figure 6D), suggesting that protonation of  $H^+$ -regulatory sites activated NHE1 (Figure 6C), as reported in detail, previously (Aronson *et al*, 1982; Wakabayashi *et al*, 2003a). Consistent with the acidic shift of  $pH_i$ -dependence of  $^{22}\text{Na}^+$  uptake, we observed that deletion of a CHP-unique region significantly reduced the rate of  $^{22}\text{Na}^+$  efflux (Figure 6D). EIPA-sensitive fraction of  $^{22}\text{Na}^+$  efflux at  $pH_i$  7.2 during the initial 3 min was reduced to  $\sim 30\%$  upon expression of  $\Delta$ 94–104, suggesting that the affinity of the  $H^+$ -regulatory site for  $H^+$  decreased upon deletion of this region.

### Discussion

In the present study, we solved the first crystal structure of the CHP2/NHE1-peptide complex at 2.7 Å. This structure provides detailed information regarding the interaction between

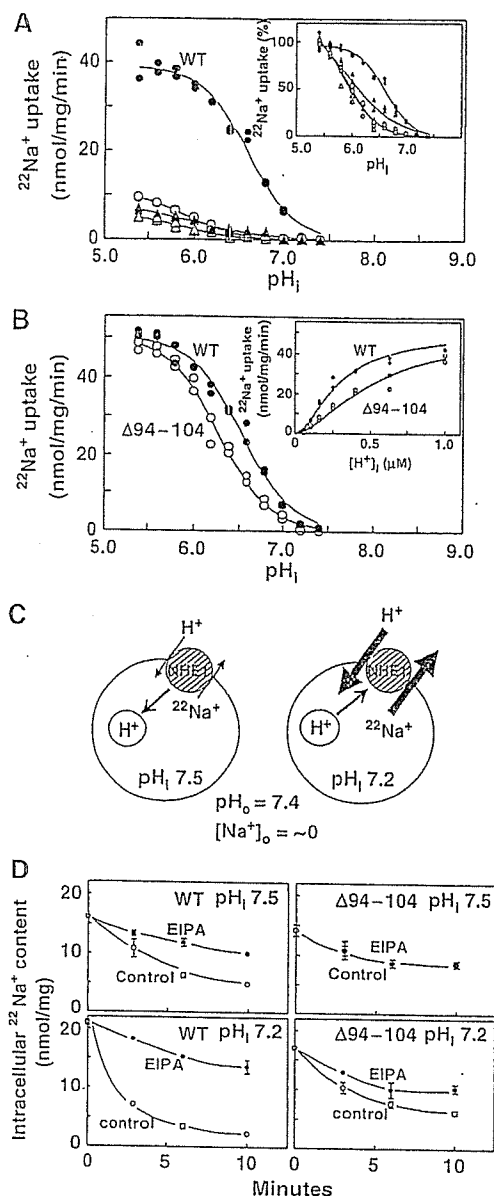


**Figure 5** Effects of mutations on the interaction between NHE1 and CHP2 in cells. (A) Low magnification confocal images of cells coexpressing GFP-tagged CHP2 and the wild-type (left) or I537K (right) mutant exchangers. Inset shows the intensity profile of GFP fluorescence along the dotted line in a marked cell. In most cells expressing the wild-type NHE1 but not I537K, strong fluorescent signals were detected at the cell edge. (B) Subcellular localization of CHP2 expressed in cells. GFP-tagged CHP2 was coexpressed in cells stably expressing the wild-type or mutant NHE1 variants and GFP-fluorescence was observed by confocal microscopy. (C) Subcellular localization of mutant CHP2. GFP-tagged CHP2 mutants were expressed in cells stably expressing the wild-type NHE1. Eleven residues from Glu94 to Lys104 of CHP2 were deleted in  $\Delta 94-104$ , while the 10 N-terminal residues from Met1 to Val10 were deleted in  $\Delta N10$ . For one control experiment, GFP-tagged human CNB was expressed in NHE1-transfectants. (D) Summary data for membrane localization of GFP-tagged CHP2. Intensity profile analysis was performed on confocal images as shown in (A). The number of cells with strong fluorescence signal at the cell edge (at least three times more than the average of fluorescence in the internal cell region) was counted. Data are expressed as the mean  $\pm$  s.d. from 6–8 images (total cell number analyzed, 99–341).

NHE1 and CHP: (i) the interaction with NHE1 occurs in a hydrophobic cleft encompassing the N- and C-lobes of CHP2, (ii) this interaction occurs by extensive Van der Waals contact between hydrophobic residues, as well as by some specific hydrogen bonds, (iii) the interacting region of NHE1 forms an  $\alpha$ -helix which bends at a conserved Gly539 and (iv) two domains of CHP2 are connected by a large flexible CHP-unique region. These features strengthened our previous

functional study (Pang *et al*, 2001, 2002, 2004) from structural aspects and at the same time provided new information to be addressed regarding the function of NHE1.

**A unique feature of interaction between CHP and NHE**  
Structure comparison among  $\text{Ca}^{2+}$ -binding proteins provided valuable information regarding the target specificity of CHP1/2 proteins. Although the crystal structure of CNB/CNA com-



**Figure 6** Effect of mutations on the exchange activity. (A), pH<sub>i</sub>-dependence of EIPA-sensitive <sup>22</sup>Na<sup>+</sup>-uptake in cells expressing wild-type NHE1 (●) or CHP binding-defective mutants, I534D (○), I534K (▲) and I537K (△). pH<sub>i</sub> was clamped at various values with K<sup>+</sup>/nigericin. Data were fitted to Hill equations with the kinetic parameters shown in Supplementary Table I and plotted after normalization by the maximal activity at pH<sub>i</sub> = 5.4 (inset). (B) pH<sub>i</sub>-dependence of EIPA-sensitive <sup>22</sup>Na<sup>+</sup>-uptake in cells co-expressing wild-type NHE1 and GFP-tagged CHP2 (●) or deletion mutant Δ94-104 of CHP2 (○). Data were fitted to Hill equations with the kinetic parameters shown in Supplementary Table I. The <sup>22</sup>Na<sup>+</sup>-uptake activity was also plotted against intracellular H<sup>+</sup> concentration up to 1 μM (inset). (C) Schematic drawing of <sup>22</sup>Na<sup>+</sup>-efflux protocol. The efflux experiment was done in <sup>22</sup>Na<sup>+</sup>-loaded, pH<sub>i</sub>-clamped cells at extracellular pH 7.4. At lower pH<sub>i</sub>, <sup>22</sup>Na<sup>+</sup> efflux would be accelerated by H<sup>+</sup> binding to the regulatory site, while at high pH<sub>i</sub> it would be inhibited by H<sup>+</sup>-release from the regulatory site. (D) Time courses of <sup>22</sup>Na<sup>+</sup> efflux. Cells were loaded with <sup>22</sup>Na<sup>+</sup> and at the same time pH<sub>i</sub>-clamped at pH<sub>i</sub> 7.5 or 7.2. After removal of the radioactive solution, cells were exposed to the nonradioactive solutions with or without 0.1 mM EIPA. Data are expressed as the mean ± s.d. of three determinations. Error bars are sometimes smaller than symbol sizes.

plex (Kissinger *et al*, 1995) revealed a similar mode of interaction through its hydrophobic groove, comparison between the hydrophobic clefts of CHP2 and CNB showed

several different structural features (Figure 3A and B). In addition, there is a marked difference in the distribution of hydrophobic residues between NHE1- and CNB peptides (Figure 3D and E). Such local structural differences between CHP2 and CNB, together with differences between target peptide sequences, may explain the selectivity of CHP1/2 toward the NHE members and of CNB toward CNA, and led us to predict that NHE1 may not be a target for CNB. In fact, we observed that GFP-tagged CNB was not localized to the plasma membrane when co-expressed with NHE1 (Figure 5C). On the other hand, since the C-lobe of KChIP1 is occupied by the α10 helix of itself (Figure 3C), KChIP1 associates with its target K<sup>+</sup>-channel molecule only through the N-lobe (Zhou *et al*, 2004). Crystal structures have been also solved for several other Ca<sup>2+</sup>-binding proteins belonging to the NCS family: recoverin (Flaherty *et al*, 1993), NCS-1 (Bourne *et al*, 2001), neurocalcin (Vijay-Kumar and Kumar, 1999), AtCBL2 (Nagae *et al*, 2003), and CIB (Gentry *et al*, 2005). Although all these proteins have hydrophobic crevices that would interact with the target molecules, the sizes and shapes of these crevices are clearly different. In contrast to calmodulin, which is able to interact with a variety of proteins with broad specificity, target molecules for CNB and NCS family proteins appear to be limited. Structural differences in the hydrophobic cleft together with highly specific polar interactions would enable the diverse array of Ca<sup>2+</sup>-binding proteins belonging to these families to associate selectively and tightly with the target molecules.

Of note, the N-lobe of CHP2 associates tightly with the C-lobe within a large area (Figure 3A). The contact area between the two domains is 1066 Å<sup>2</sup>, accounting for 16.6 and 15.2% of the total surface areas of the N- and C-lobes, respectively. Such interaction between the two lobes would result in the formation of a rigid cleft structure independent of the target peptide. In fact, the structure of the hydrophobic cleft of CHP2 is very similar to that of target-free CHP1 (Naoy *et al*, 2005). In addition, the N-lobe of CHP2 does not contain the methionine residue that was suggested to produce plasticity allowing fine-tuning toward various target molecules in calmodulin (Osawa *et al*, 1998). Therefore, NHE1-peptide would enter the preformed cleft, rather than the interaction being caused by a conformational change in the cleft. This target-independent rigid structure would allow the CHP-unique region to exert specific physiological functions, beyond a role as a connecting linker. This is in contrast to calmodulin the flexible linker region between the two domains of which is known to act as a hinge when it recognizes various target molecules (Zhang *et al*, 1995).

CHP1/2 is myristoylated and has two Ca<sup>2+</sup> ions. However, these properties are different from those of other CNB and NCS family proteins. Mutation of CHP1 that prevents myristoylation has no apparent effect on plasma membrane expression or the exchange activity of NHE1. Therefore, myristoylation of CHP1/2 would not be required for the plasma membrane translocation of NHE1 or for the exchange activity (Pang *et al*, 2001, 2004), in contrast to KChIP1 (An *et al*, 2000). In addition, unlike recoverin, which undergoes the Ca<sup>2+</sup>-myristoyl switch (Ames *et al*, 1997), the myristoyl moiety of CHP1/2 would always be exposed outside the core structure upon interaction with NHE1 and probably embedded in the plasma membrane. Thus, the physiological function of myristoylation is still unknown. On the other hand,



unlike many other  $\text{Ca}^{2+}$ -binding proteins, only EF3 and EF4 of CHP1/2 are able to coordinate  $\text{Ca}^{2+}$  ions. Removal of  $\text{Ca}^{2+}$  with a  $\text{Ca}^{2+}$ -chelator significantly reduced the interaction between NHE1 and CHP2 (Supplementary Figure 1) and a double mutation of EF3 and EF4 of CHP1 abolished the interaction with NHE1 (Pang *et al*, 2004). Furthermore, the  $\text{Ca}^{2+}$  affinity of CHP1 increases markedly (40-fold) upon interaction with NHE1 (Pang *et al*, 2004). These findings suggest that  $\text{Ca}^{2+}$ -binding sites and the hydrophobic cleft are structurally coupled, that is, the  $\text{Ca}^{2+}$ -bound conformation of EF-hands is required for the formation of the appropriate structure of the hydrophobic cleft for the interaction with NHE1. By analogy with calmodulin (Zhang *et al*, 1995), we consider that  $\text{Ca}^{2+}$  binding opens the hydrophobic pockets of EF-hands so that the residues of the C-lobe can fit into the hydrophobic cleft. However, such  $\text{Ca}^{2+}$ -induced conformational changes of CHP1/2 bound to NHE1 would not occur physiologically in cells, since the  $\text{Ca}^{2+}$  affinity for such a complex would be extremely high, that is,  $K_d$  for  $\text{Ca}^{2+}$  ( $2\sim 3\text{ nM}$ ) is much less than the physiological cytosolic  $\text{Ca}^{2+}$  concentration ( $0.1\text{--}1\text{ }\mu\text{M}$ ) (Supplementary Figure 1 and see also Pang *et al*, 2004). Hence, we suggest that  $\text{Ca}^{2+}$  bound to EF-hands plays a structural role in stabilizing the hydrophobic cleft of CHP1/2. In the case of NHE1,  $\text{Ca}^{2+}$ -induced activation would take place on another  $\text{Ca}^{2+}$ -binding protein CaM, which binds to the middle of the cytoplasmic domain of NHE1 (Bertrand *et al*, 1994; Wakabayashi *et al*, 1994).

#### Implications for roles of CHP in NHE function

We demonstrated that Ile534 and Ile537 in NHE1 are critical residues for interaction with CHP2 (Figure 5). Mutations of these residues resulted in a disruption of NHE1 function, as characterized by a drastic reduction of the maximal exchange activity and a large acidic shift of the  $\text{pH}_i$ -dependence of exchange (Figure 6). This is consistent with our previous findings obtained by simultaneous mutation of four hydrophobic residues (Phe526, Leu527, Leu530 and Leu531) of NHE1, substituted with Gln or Arg (Pang *et al*, 2001, 2004). On the other hand, deletion of the CHP-unique region ( $\Delta 94\text{--}104$ ) significantly reduced the physiological exchange activity by inducing an acidic shift of the  $\text{pH}_i$ -dependence of  $^{22}\text{Na}^+$ -uptake (Figure 6B) and inhibited the rate of  $^{22}\text{Na}^+$  efflux (Figure 6D), while preserving the maximal activity at acidic  $\text{pH}_i$  (Figure 6B), suggesting that this region functions as an important segment controlling  $\text{pH}_i$  by interacting with NHE1. Based on these findings, we propose that CHP1/2 plays two important roles in the function of NHE1. First, CHP functions as an obligatory subunit, which activates almost non-functional NHE1 by tightly associating with its cytoplasmic domain via the hydrophobic cleft. This activation is characterized by increases in both  $V_{\text{max}}$  and the  $\text{H}^+$ -affinity. Secondly, CHP would participate in the delicate  $\text{pH}_i$  regulation of NHE1 through the CHP-unique region, which is involved in modulation of the  $\text{H}^+$ -affinity, but not  $V_{\text{max}}$ .

We predict that CHP may stabilize the structure of the juxtamembrane domain by inducing a stable  $\alpha$ -helix, thereby preserving NHE1 in the functional conformation. Indeed, circular dichroism measurements indicated that the CHP-free, CHP-binding peptide has no secondary structure in aqueous solution (data not shown), although we do not exclude the possibility that this region is folded within the

entire structure. On the other hand, the dominant-negative effect of  $\Delta 94\text{--}104$  raises the interesting possibility that it may regulate the  $\text{pH}_i$ -sensing by interacting with some regions of NHE1. We observed that NHE1 and CHP2 crosslinked with each other through IL5 of NHE1 and the CHP-unique region (Supplementary Figure 5), suggesting that these regions in the two proteins are located in accessible positions beneath the membranes. Since, similar to  $\Delta 94\text{--}104$  of CHP2, mutation of Arg440 in IL5 results in a large acidic shift of the  $\text{pH}_i$ -dependence of  $^{22}\text{Na}^+$ -uptake and efflux (Wakabayashi *et al*, 2003a, b), we consider that IL5 would be one of targets for the CHP-unique region. Although we do not have direct evidence, IL4 may be another target region because mutation of Arg327 in IL4 has also been reported to lead to a similar functional defect of NHE1 (Lacroix *et al*, 2004). Activation of  $^{22}\text{Na}^+$  efflux by cytosolic acidification predicted the existence of an additional  $\text{H}^+$ -regulatory site(s) (Figure 6C and D; Aronson *et al*, 1982; Wakabayashi *et al*, 2003a). This phenomenon does not appear to be fully explained by the recent allosteric model, in which only  $\text{H}^+$ -transport sites are assumed to participate in the cooperative  $\text{H}^+$ -activation of NHE1 (Lacroix *et al*, 2004). We speculate that multiple charged residues in loops of NHE1, as well as in CHP1/2, may serve as 'pH-sensor' sites, which accept protons, although further investigation will be required to support this concept. The recently reported crystal structure of the bacterial  $\text{Na}^+/\text{H}^+$  antiporter, NhaA, predicted that modification of charged residues provided by cytoplasmic loops may activate NhaA by exposing the cation transport site via reorientation of transmembrane helices (Hunte *et al*, 2005).

Finally, it should be noted that the relatively long juxtamembrane domain (aa 503–595) of NHE1 is essential for the physiological exchange activity (Ikeda *et al*, 1997; Wakabayashi *et al*, 1997), although we focused on the CHP-binding domain in the present study. Similar to the CHP-binding region, it is likely that the region covering aa 503–595 forms a stable structure by interacting with several accessory factors. Indeed, this region appears to be structurally unstable when expressed in *Escherichia coli* or in mammalian cells as a single polypeptide, as evidenced by its rapid degradation (unpublished observation), despite the fact that the whole cytoplasmic domain can be easily expressed in these cells. In addition, a previous study (Aharonovitz *et al*, 2000) indicated that positively charged clusters (aa 509–516 and aa 552–560 in human NHE1) interact with polyphosphoinositides ( $\text{PIP}_2$ ). These regions were also reported to interact with ezrin, although interaction with ezrin is independent of the exchange activity (Denker *et al*, 2000; Baumgartner *et al*, 2004). Furthermore, we recently reported that a region (aa 560–580) of NHE1 may be involved in dimeric interactions (Hisamitsu *et al*, 2004). Such homotypic interactions may provide another way for stabilization of the structure, as deletion of aa 560–580 resulted in a marked reduction of exchange activity by inducing the acidic shift of  $\text{pH}_i$ -dependence (Hisamitsu *et al*, 2004). These findings raise the possibility that multiple homotypic and heterotypic interactions may induce stabilization of the juxtamembrane region and thereby form a substructure regulating the exchange activity. Clearly, CHP is an obligatory member in such regulatory machinery of NHE1.

In summary, we first determined the crystal structure of CHP2 complexed with its binding region in NHE1 and

clarified the mechanism by which CHP tightly and specifically associates with plasma membrane members of the NHE family. Structure-based mutagenesis revealed the physiological importance of CHP in  $\text{pH}_i$  regulation by NHE1. Most  $\text{Ca}^{2+}$ -binding proteins have long been recognized to function as  $\text{Ca}^{2+}$ -sensors or  $\text{Ca}^{2+}$ -buffers. In contrast to this general understanding, CHP does not appear to be a  $\text{Ca}^{2+}$ -sensor, but rather acts as a critical regulator of pH-sensing activity in the exchangers, presumably mediated by the CHP-unique region. The results of the present study cast new light on a unique function of CHP that was not reported in other canonical EF-hand  $\text{Ca}^{2+}$ -binding proteins.

## Materials and methods

### Protein expression and purification

The complex of human full-length CHP2 (aa 1–196) with its binding region (aa 503–545) in NHE1 was expressed and purified essentially as described previously (Pang *et al*, 2004; Ben Ammar *et al*, 2005).

### Crystallization and data collection

Crystals of the complex CHP2/NHE1-peptide were grown using the sitting-drop vapor diffusion technique at 20°C. To obtain the best crystal quality, 1.5  $\mu\text{l}$  of the protein complex solution containing 20 mM yttrium chloride was mixed with 1  $\mu\text{l}$  of the reservoir solution containing 200 mM ammonium acetate, 100 mM Bis-Tris, pH 5.5, and 25% (w/v) PEG 3350 as described previously (Ben Ammar *et al*, 2005). Crystals were not obtained without adding yttrium chloride to the crystallization solution, suggesting that yttrium ion(s) were involved in crystal packing. Therefore, taking advantage of the yttrium ion(s) in the crystal, we collected multiple wavelength data sets around the absorption edge of the yttrium atom at SPring-8 beamline BL44B2. A high-resolution single-wavelength data set ( $\lambda = 1.1 \text{ \AA}$ ) was collected at beamline BL41XU at SPring-8. The statistics of the data collection are summarized in Table 1.

### Structural determination and refinement

The structure of the CHP2/NHE1-peptide complex was determined by MAD phasing. The program SOLVE (Terwilliger and Berendzen, 1999) was used to determine two yttrium positions and the initial phases with a figure of merit of 0.43 at 3.1  $\text{\AA}$  resolution. The program RESOLVE (Terwilliger, 2000) improved the phases and produced the initial polyalanine model, which covered 65% of the residues of the CHP2/NHE1-peptide complex. The model was built with TURBO-FRODO and refined against the high resolution data set to 2.7  $\text{\AA}$  using CNS (Brunger *et al*, 1998), and subsequent rounds of model building and refinement produced the final structural model. The residues in the final model lie in 87.2% in the most favorable and 12.8% in the additionally allowed regions of the Ramachandran plot. Refinement statistics are summarized in Table 1. Figures 2–4 were generated using PyMOL graphing software (<http://www.pymol.org>).

### Construction of mammalian expression plasmids

The plasmid carrying the cDNA encoding NHE1 containing unique restriction sites cloned into the mammalian expression vector pECE

was described previously (Wakabayashi *et al*, 1992). Construction of plasmids for various NHE1 or CHP2 mutants tagged with GFP or hemagglutinin (HA) epitope YPYDVPDYAS was carried out by a PCR-based strategy as described previously (Wakabayashi *et al*, 2000). PCR fragments were digested and cloned into the appropriate restriction sites of vectors pECE or pGFP-N1 (Clontech, Palo Alto, CA) for NHE1 or CHP2, respectively.

### Cell culture and plasmid transfection

The exchanger-deficient cell line PS120 (Pouyssegur *et al*, 1984) and corresponding transfectants were maintained in Dulbecco's modified Eagle's medium containing 25 mM  $\text{NaHCO}_3$  and supplemented with 5% (v/v) fetal calf serum. All cDNA constructs were transfected into PS120 cells with Lipofectamine 2000 (Invitrogen), and stable clones for NHE1 and its mutant constructs were selected by repetitive  $\text{H}^+$ -killing selection procedures as described previously (Wakabayashi *et al*, 1992). GFP-tagged CHP2 variants were stably expressed in cells expressing various mutant NHE1 proteins and fluorescence images were taken under a confocal fluorescence microscope (BioRad).

### Measurement of $^{22}\text{Na}^+$ -uptake and $^{22}\text{Na}^+$ -efflux activities

$^{22}\text{Na}^+$ -uptake activity was measured by the  $\text{K}^+$ /nigericin  $\text{pH}_i$  clamp method as described previously (Ikeda *et al*, 1997). Data were simulated by fitting the values to the sigmoidal dose-response equation, rate of EIPA-sensitive  $^{22}\text{Na}^+$ -uptake =  $V_{\text{max}}/(1 + 10^{(\log(\text{pK} - \text{pH}_i)/n)})$  (pK,  $\text{pH}_i$  giving half maximal  $^{22}\text{Na}^+$  uptake;  $n$ , Hill coefficient), using the simulation program included in Graphpad Prism (Microsoft Corp., Redmond, WA).  $^{22}\text{Na}^+$  efflux was measured as described previously (Wakabayashi *et al*, 2003a). Briefly, serum-depleted cells in 24-well dishes were loaded with  $^{22}\text{Na}^+$  by preincubating them for 30 min at 37°C in chloride/KCl medium containing 1 mM  $^{22}\text{NaCl}$  (37 kBq/ml) and at the same time  $\text{pH}_i$ -clamped at 7.5 or 7.2 in presence of 5  $\mu\text{M}$  nigericin. The radioactive solution was removed and  $^{22}\text{Na}^+$  efflux was initiated by adding the nonradioactive medium. At the times indicated in figures, cells were rapidly washed four times with ice-cold PBS and the remaining  $^{22}\text{Na}$ -radioactivity in the cells was counted.

### Coordinates

Coordinates and structure factor amplitudes have been deposited in the Protein Data Bank with accession code 2BEC.

### Supplementary data

Supplementary data are available at *The EMBO Journal* Online.

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## Enhanced Magnification Angiography Using 20- $\mu\text{m}$ -Focus Tungsten Tube

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A microfocus X-ray tube is useful for performing magnification radiography, and its X-ray generator (L9631, Hamamatsu Photonics) consists of a personal computer for controlling the tube voltage and current, and a main unit with a high-voltage circuit and a fixed-anode X-ray tube. The maximum tube voltage, current, and electric power were 110 kV, 800  $\mu\text{A}$ , and 50 W, respectively. The focal-spot size was proportional to the electric power of the tube, and the size was approximately 20  $\mu\text{m}$  with a power of 20 W. Using a 3-mm-thick aluminum filter, the X-ray intensity was 7.75  $\mu\text{Gy/s}$  at 1.0 m from the source with a tube voltage of 60 kV and a current of 100  $\mu\text{A}$ . Because the peak photon energy was approximately 38 keV using the filter with a tube voltage of 60 kV, the bremsstrahlung X-rays were absorbed effectively by iodine-based contrast media at an iodine K-edge of 33.2 keV. Enhanced angiography was performed by fourfold magnification imaging with a computed radiography system using iodine-based microspheres 15  $\mu\text{m}$  in diameter. In the angiography of nonliving animals, we observed fine blood vessels of approximately 100  $\mu\text{m}$  with high contrast. [DOI: 10.1143/JJAP.45.8005]

KEYWORDS: high-contrast angiography, magnification digital radiography, microfocus X-ray tube, energy-selective imaging

### 1. Introduction

To perform high-speed medical radiography, several various flash X-ray generators using cold-cathode tubes have been developed.<sup>1–4)</sup> In particular, quasi-monochromatic flash X-ray generators<sup>5–10)</sup> have been designed to perform preliminary experiments for producing clean K-series X-rays, and higher-harmonic hard X-rays have been observed in a weakly ionized linear plasma of copper and nickel. However, in monochromatic flash radiography, difficulties in increasing X-ray duration and in performing X-ray computed tomography (CT) have been encountered.

Synchrotrons are capable of producing high-dose-rate monochromatic parallel X-ray beams using silicon crystals, and the beams have been applied to phase-contrast radiography<sup>11,12)</sup> and enhanced K-edge angiography.<sup>13,14)</sup> In angiography, monochromatic X-rays with photon energies ranging from 33.3 to 35 keV have been employed because the rays are absorbed effectively by iodine-based contrast media with an iodine K-edge of 33.2 keV.

Without using synchrotrons, phase-contrast radiography<sup>15)</sup> for edge enhancement can be performed using a microfocus X-ray tube, and the enhancement has been achieved in mammography<sup>16)</sup> with a computed radiography (CR) system<sup>17)</sup> using a 100- $\mu\text{m}$ -focus tube. Subsequently, we developed a cerium X-ray generator<sup>18,19)</sup> to perform enhanced K-edge angiography using cone beams, and succeeded in observing fine blood vessels and coronary arteries with high contrast using cerium K $\alpha$ -rays of 34.6 keV.

Although the magnification radiography is used to improve the spatial resolution in angiography utilizing a digital imaging system, it is difficult to design a small focus cerium tube for angiography. Therefore, narrow-photon-

energy bremsstrahlung X-rays<sup>20–22)</sup> with a peak energy of approximately 35 keV from a tungsten tube are used to perform high-contrast angiography.

In this research, we employed a microfocus tungsten tube, and performed enhanced magnification angiography by controlling bremsstrahlung X-ray spectra using an aluminum filter.

### 2. Principle of Enhanced Magnification Angiography

Figure 1 shows the mass attenuation coefficients of iodine at the selected energies; the coefficient curve is discontinuous at the iodine K-absorption edge of 33.2 keV. The effective bremsstrahlung X-rays for K-edge angiography are shown above the K-edge. Using a 3.0-mm-thick aluminum filter for absorbing soft X-rays, the peak photon energy of the bremsstrahlung rays increases to approximately 38 keV. In angiography, iodine contrast media in blood vessels easily absorb the rays, and soft bremsstrahlung rays are absorbed effectively by objects (muscles). Therefore, blood vessels are observed with high contrast. Subsequently, spatial resolution is improved by fourfold magnification imaging using a microfocus X-ray tube in conjunction with a CR system (Regius 150, Konica Minolta) at a sampling pitch of 87.5  $\mu\text{m}$ .

### 3. Experimental Methods

The microfocus X-ray generator (L9631, Hamamatsu Photonics) consists of a personal computer and a system unit. The unit includes all the hardware in the X-ray generator, such as, a high-voltage circuit and a fixed anode X-ray tube. Tube voltage, current, and exposure time can be controlled by the computer. The maximum tube voltage, current, and electric power were 110 kV, 800  $\mu\text{A}$ , and 50 W,

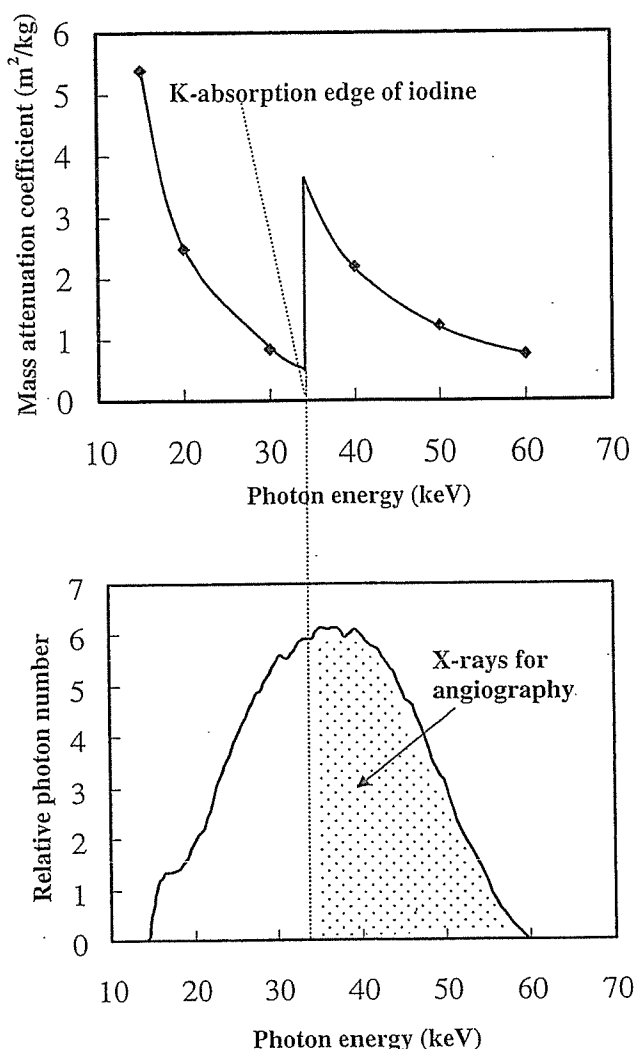


Fig. 1. Mass attenuation coefficients of iodine and bremsstrahlung X-rays for enhanced K-edge angiography.

respectively. The focal-spot size was proportional to the electric power of the tube, and its size was approximately 20  $\mu\text{m}$  in diameter with a power of 20 W. In this experiment, the tube voltage applied ranged from 45 to 70 kV, and the tube current was regulated to within 170  $\mu\text{A}$ . The exposure time is controlled to obtain optimum X-ray intensity for angiography, and narrow-photon-energy bremsstrahlung X-rays are produced using the aluminum filter.

## 4. Results

### 4.1 X-ray intensity

X-ray intensity was measured using a Victoreen 660 ionization chamber, with a volume of 400  $\text{cm}^3$ , at 1.0 m from the X-ray source using the filter (Fig. 2). At a constant tube current of 100  $\mu\text{A}$ , X-ray intensity increased when tube voltage was increased. At a tube voltage of 60 kV, the X-ray intensity with the filter was 7.75  $\mu\text{Gy/s}$ .

### 4.2 X-ray spectra

To measure X-ray spectra using the filter, we employed a cadmium telluride detector (CDTE2020X, Hamamatsu Photonics) (Fig. 3). When tube voltage was increased, bremsstrahlung X-ray intensity increased, and both max-

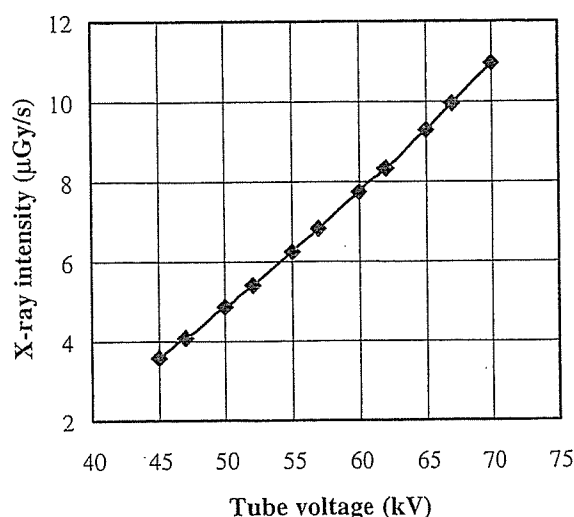


Fig. 2. X-ray intensity ( $\mu\text{Gy/s}$ ) as a function of tube voltage (kV) with tube current of 100  $\mu\text{A}$ .

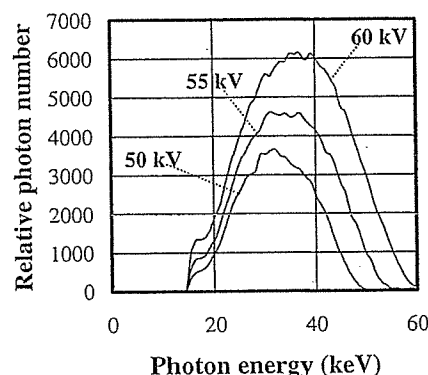


Fig. 3. Bremsstrahlung X-ray spectra measured using cadmium telluride detector with changes in tube voltage.

imum photon energy and spectrum peak energy increased.

To perform K-edge angiography, bremsstrahlung X-rays of approximately 35 keV are used; the high-energy bremsstrahlung X-rays decrease image contrast. When this filter was used, because bremsstrahlung X-rays with energies higher than 60 keV were not absorbed easily, the tube voltage for angiography was determined to be 60 kV by considering the filtering effect of radiographic objects.

### 4.3 Enhanced magnification angiography

The enhanced angiography was performed by fourfold magnification imaging using the CR system and the filter at a tube voltage of 60 kV, and the distance between the X-ray source and the imaging plate was 1.0 m (Fig. 4). First, the spatial resolutions of cohesion and magnification radiographies were realized using a lead test chart at an exposure time of 30 s. In the magnification radiography, 50- $\mu\text{m}$ -thick lines (10 line pairs) were clearly visible (Fig. 5). Figure 6 shows radiograms of tungsten wires in a 25-mm-diameter rod made of poly(methyl methacrylate) (PMMA) at an exposure time of 30 s. Although image contrast decreased slightly with decreasing wire diameter owing to the blurring of the image caused by the sampling pitch of 87.5  $\mu\text{m}$ , a 20- $\mu\text{m}$ -diameter-wire could be observed.

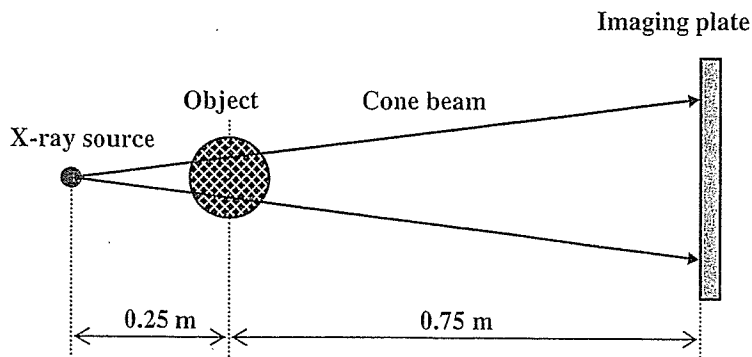


Fig. 4. Fourfold magnification imaging using imaging plate in conjunction with microfocus tube.

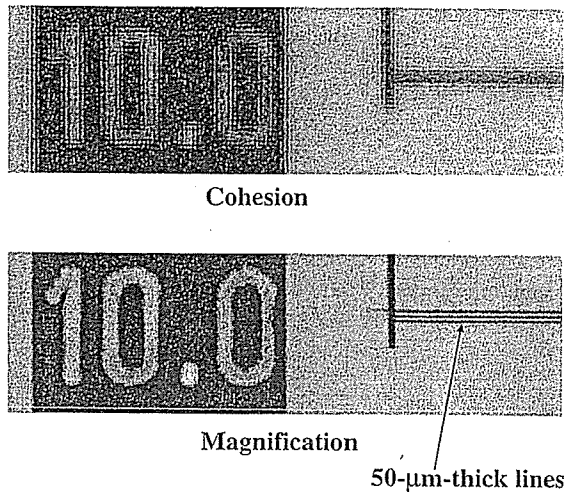


Fig. 5. Radiogram of test chart for measuring spatial resolution.

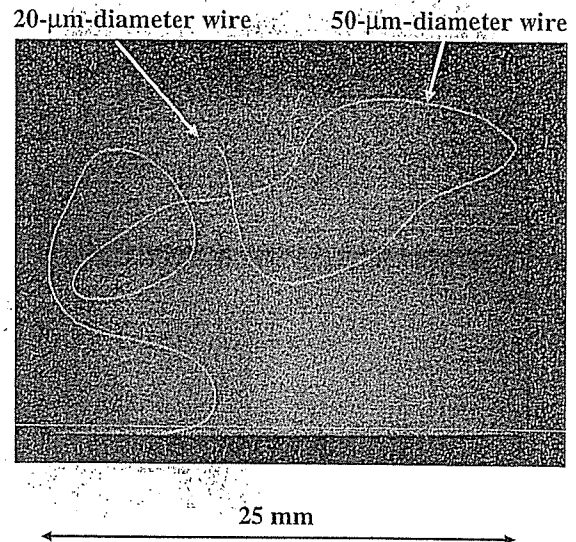


Fig. 6. Radiograms of tungsten wires in PMMA rod.

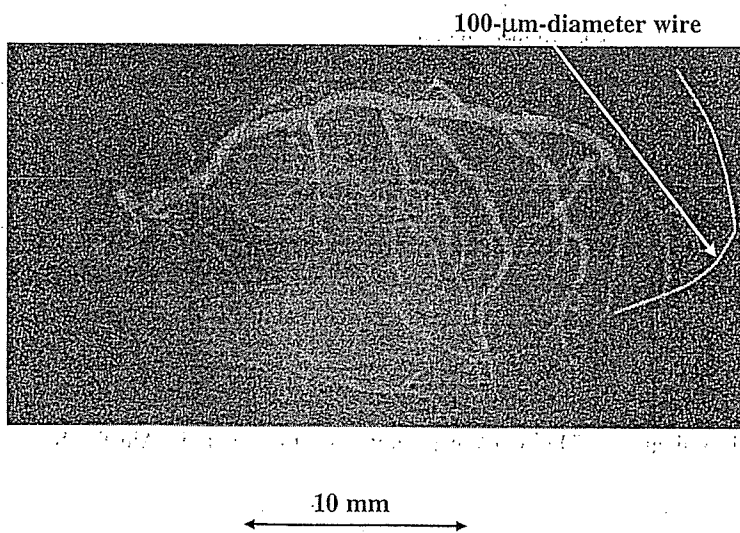


Fig. 7. Angiogram of extracted rabbit heart using iodine microspheres.

Figures 7 and 8 show angiograms of a 19-mm-thick rabbit heart specimen and a 41-mm-thick thigh specimen, respectively. The exposure time was 30 s, and these images were obtained using iodine microspheres of 15 μm diameter. The microspheres are very useful for making the phantoms of nonliving animals used for angiography. The iodine plastic

spheres contained 37% iodine by weight, and the coronary arteries and fine blood vessels were visible.

Figure 9 shows angiograms of a dog heart specimen of 65 mm thickness using iodine spheres with an exposure time of 60 s. Although the image contrast decreased slightly with increasing thickness of the PMMA plate facing the X-ray

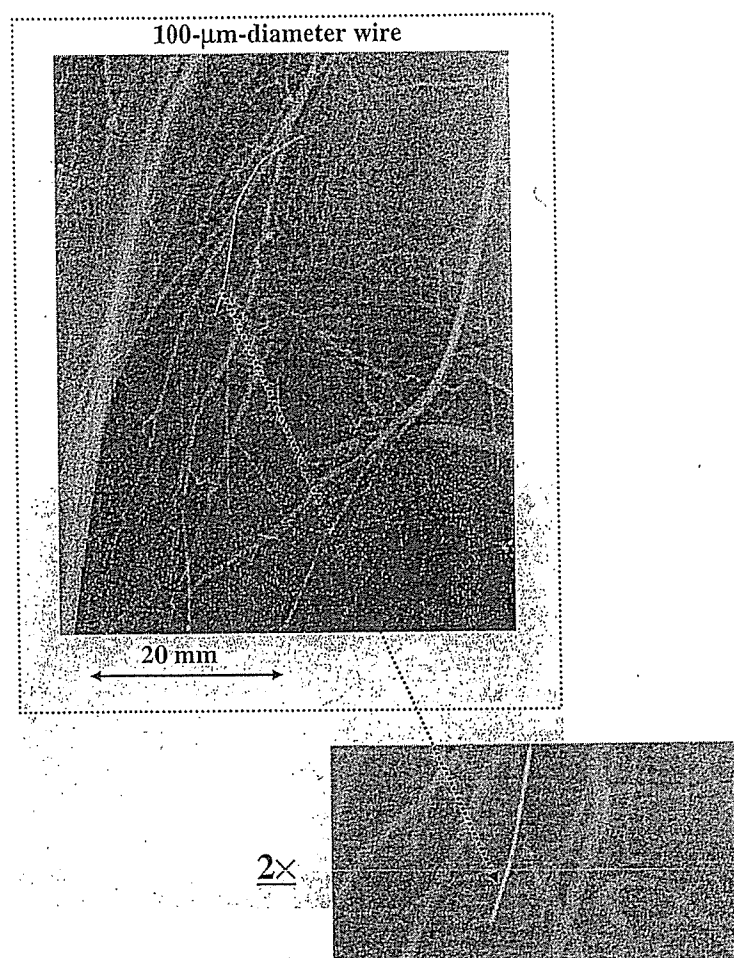


Fig. 8. Angiograms of rabbit thigh.

source, the coronary arteries of approximately 100  $\mu\text{m}$  diameter were observed using a 100-mm-thick plate.

## 5. Conclusions

We employed a microfocus X-ray generator with a tungsten target tube to perform enhanced magnification angiography using narrow-photon-energy bremsstrahlung X-rays at a peak photon energy of approximately 38 keV, which can be absorbed easily by iodine-based contrast media. Although bremsstrahlung X-ray intensity substantially increased with increasing tube voltage, the optimal tube voltage for increasing image contrast was determined to be 60 kV.

Because the sampling pitch of the CR system is 87.5  $\mu\text{m}$ , we obtained spatial resolutions of approximately 50  $\mu\text{m}$  using fourfold magnification imaging achieved with a 20- $\mu\text{m}$ -focus tube. To observe fine blood vessels of less than 100  $\mu\text{m}$  diameter, the spatial resolution of the CR system should be improved to 43.8  $\mu\text{m}$  (Regius 190, Konica Minolta), and iodine density should be increased.

In this research, we controlled bremsstrahlung X-rays to the optimum spectral distribution for realizing enhanced angiography using iodine-based contrast media. On the other hand, gadolinium-based contrast media with a K-edge energy of 50.2 keV have been employed to perform angiography in MRI, and the gadolinium density used has been increasing. In view of this situation, tungsten K $\alpha$  rays (58.9 keV) are useful for enhancing K-edge angiography,

because the K $\alpha$  rays are absorbed effectively by gadolinium media. As compared with angiography using iodine media, the absorbed dose can be decreased considerably using gadolinium media.

At a tube voltage of 60 kV and a current of 170  $\mu\text{A}$ , the photon number was approximately  $2 \times 10^7$  photons/( $\text{cm}^2 \cdot \text{s}$ ) at 1.0 m from the source, and photon count rate can be increased easily using a rotating anode microfocus tube developed by Hitachi Medical Corporation. Recently the maximum electric power of the microfocus X-ray tube has been increasing, and a kilowatt-range tube is realizable. Therefore, real-time magnification radiography will become possible using a flat panel detector with a pixel size of less than 100  $\mu\text{m}$ .

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using 100-mm-thick PMMA plate

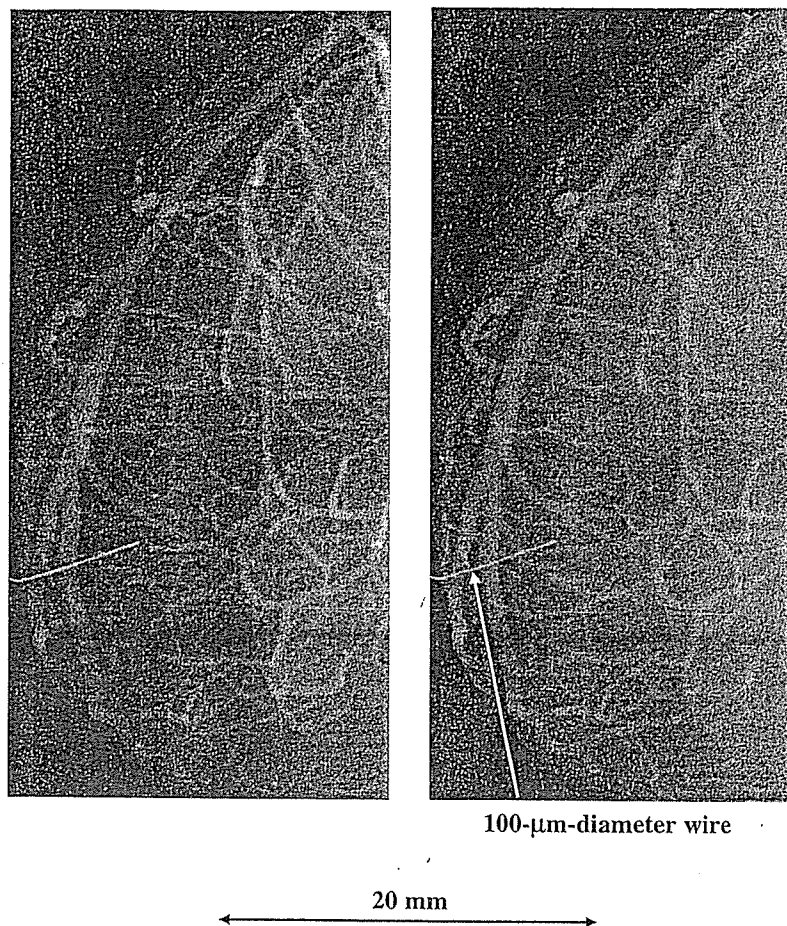


Fig. 9. Angiograms of extracted dog heart.

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## Efficient Preparation of Cationized Gelatin for Gene Transduction

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We previously reported gene therapy using cationized gelatin microspheres of  $\phi$ 20-32  $\mu$ m, prepared from pig skin, as a transducing agent, but although the gelatin offered various advantages, its yield was extremely low (only 0.1%). In this study, we markedly improved the yield of  $\phi$ 20-32  $\mu$ m cationized gelatin microspheres and prepared a newly less than  $\phi$ 20  $\mu$ m cationized gelatin. Conventionally, cationized gelatin is prepared by cationization, particulation by agitation, and cross-linking. The yield is determined by the particulation step, for which we had used a three-necked distillation flask of 500 mL and an agitation speed of 420 rpm. The yield was significantly increased from  $0.13 \pm 0.02\%$  to  $8.80 \pm 1.90\%$  by using a smaller flask of 300 mL and an agitation speed of 25000 rpm ( $p < 0.01$ ). We could also prepare cationized gelatin of less than  $\phi$ 20  $\mu$ m, which had not been possible previously. We confirmed that efficient gene introduction into peritoneal macrophages could be achieved with the new cationized gelatin.

Key words: gelatine microsphere, macrophage, yield

### INTRODUCTION

Efficient gene transduction methods are necessary for gene therapy [1], and currently available methods can be divided into viral vector techniques and non-viral approaches, such as lipofection or electroporation. Viral vectors such as adenovirus or retrovirus offer high transduction efficiency, but there are questions regarding safety [2]. On the other hand, the efficiency of transduction with non-viral vectors is generally poor [3]. In recent years, nucleofection has been developed for highly efficient gene transduction, but it can be applied to only certain cells, and it causes damage in some cases [4].

We showed that intramuscular injection of FGF-4 gene-gelatin complex induced significantly greater angiogenesis than injection of the bare FGF-4 gene [5]. Furthermore, we showed that adrenomedullin (AM) gene-gelatin complex effectively transduced the AM gene into endothelial progenitor cells (EPCs), and the transduced EPCs had a therapeutic effect in pulmonary hypertension [6]. In those studies, we used cationized gelatin microspheres of  $\phi$ 20-32  $\mu$ m, derived from pig skin. However, the yield of gelatin was only about 0.1%. Cascone *et al.* reported that the preparation of nanoparticulate gelatin required an agitation speed of cationized gelatin and olive oil of more than 10,000 rpm [7], so in this study, we examined whether the use of a higher agitation speed during preparation of the gelatin particles would increase the yield and reduce the particle size in our procedure. We also confirmed the efficacy of the gelatin particles thus obtained for gene transduction.

### MATERIALS

Gelatin of pig skin origin (PI 9) was purchased from Nitta Gelatin Corp, Japan. 1-Ethyl-3-(3-dimethylaminopropyl) carbodiimide (EDC),  $\beta$ -alanine, acetone, glycine, hydrochloric acid, ethylenediamine, olive oil, glutaraldehyde solution (GA), potassium dihydrogenphosphate, disodium hydrogenphosphate and sodium hydrogen carbonate were purchased from Wako Pure Chemical Industry, Japan. Liquid nitrogen was purchased from Tomoe Corporation, Japan.

Rat peritoneal macrophages were collected by intra-peritoneal injection of thioglycolate culture medium as previously described [8]. DNA encoding GFP with the cytomegalovirus enhancer-chicken  $\beta$ -actin hybrid promoter was constructed [5].

### METHODS

Conventional preparation of gelatin microspheres involves three steps: (1) cationized gelatin production, (2) microsphere production and (3) cross-linking of cationized gelatin microspheres. In order to increase the yield of cationized gelatin microspheres, we aimed to improve the second step, i.e., microsphere production.

#### Cationized gelatin production

PI 9 (10 g) was completely dissolved in 0.1 M phosphate buffer (PBS, 450 mL) containing potassium dihydrogenphosphate and disodium hydrogenphosphate. Ethylenediamine (31.1 mL) and hydrochloric acid were added, and the pH was adjusted to 5.0. EDC (5.35 g) was added to this solution, which was made up to 500 mL with PBS and left for 18 hours. The solution was

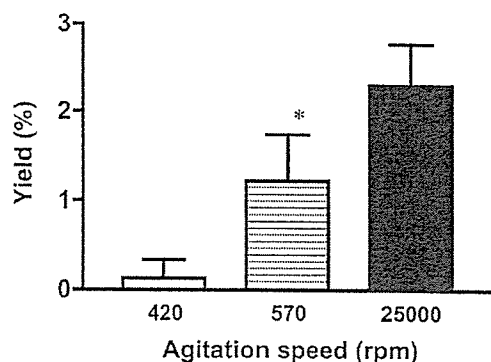


Fig. 1 Yield of  $\phi$ 20-32  $\mu$ m cationized gelatin using a 500 mL three-necked distillation flask.

The open bar shows the control (420 rpm) group, horizontal lined bar, the 570 rpm group and closed bar, the 25,000 rpm group. Data are presented as mean  $\pm$  SEM. The yield in the 570 rpm group was significantly higher than that in the control group (\* $p$  < 0.001 vs 420 rpm).

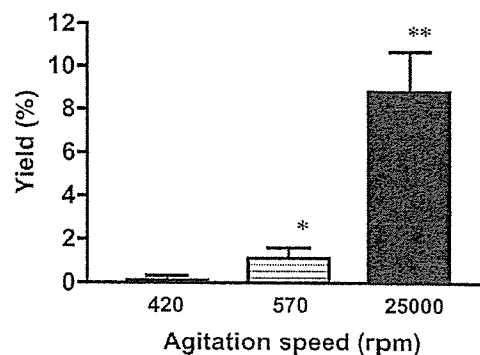


Fig. 2 Yield of  $\phi$ 20-32  $\mu$ m cationized gelatin using a 300 mL three-necked distillation flask.

The open bar shows the 420 rpm group, horizontal lined bar, the 570 rpm group and closed bar, the 25,000 rpm group. Data are presented as mean  $\pm$  SEM. The yield in the 570 rpm group was significantly higher than that in the 420 rpm group (\* $p$  < 0.001 vs 420 rpm). The yield in the 25,000 rpm group was significantly higher than that in the other groups (\*\* $p$  < 0.0001 vs other groups).

then dialyzed for 2 days with 16 changes of water. After the dialysis, this solution was freeze-dried for 4 to 7 days to afford cationized gelatin. The conversion rate of carboxyl groups to amino groups was measured by the TNBS method to characterize the product [13].

#### Microsphere production

In the conventional procedure, cationized gelatin aqueous solution and olive oil were placed in a three-necked distillation flask of 500 mL at 40°C, and centrifuged at 420 rpm for 10 minutes. This solution was stirred for 30 minutes at 0°C. Acetone was added, and the mixture was centrifuged. After centrifugation, the oil layer was removed, and acetone was added. This solution was centrifuged again, homogenized and sieved with  $\phi$ 20  $\mu$ m,  $\phi$ 32  $\mu$ m and  $\phi$ 90  $\mu$ m sieves (Test sieves, #JIS Z 8801, Tokyo Screen Co., Ltd., Japan). The microspheres were dried in a refrigerator overnight, and the yield of each fraction was determined.

In this experiment, we examined the effect of increasing the agitation speed to 570 rpm and 25000 rpm, and the effect of using a smaller three-necked distillation flask (300 mL) to obtain smoother mixing.

#### Cross-linking of cationized gelatin microspheres

Acetone and hydrochloric acid (7:3) were added to cationized gelatin microspheres, the crosslinking agent GA was added, and the reaction was allowed to proceed for 24 hours. After the reaction, centrifugation was performed and the supernatant was removed. Glycine solution (100 mM) was added to remove GA for one hour. After centrifugation, the supernatant was removed and cross-linked microspheres were cooled with liquid nitrogen, freeze-dried, and weighed.

#### Gene introduction with the newly developed cationized gelatin microspheres

Gene gelatin complex was prepared by mixing 2 mg

of cationized gelatin and 50  $\mu$ g/100  $\mu$ l gene (GFP or luciferase). The complex was incubated with rat peritoneal macrophages for 14 days. Effective gene introduction was demonstrated by cellular expression of GFP or luciferase.

## RESULTS

#### Effect of agitation conditions on yield of cationized gelatin

In the conventional method (500 mL/420 rpm), the yield of the  $\phi$ 20-32  $\mu$ m cationized gelatin was  $0.13 \pm 0.02\%$ , but when the agitation speed was increased to 570 rpm, the yield rose to  $1.22 \pm 0.52\%$  (\* $p$  < 0.001 vs 420 rpm). The yield was further increased to  $2.30 \pm 0.47\%$  by increasing the agitation speed to 25000 rpm from 570 rpm, but this further increase was not statistically significant ( $p=0.136$ )(Fig. 1). Next we used a smaller (300 mL) three-necked distillation flask with agitation at 420 rpm, 570 rpm and 25,000 rpm. When the agitation speed was increased to 570 rpm, the yield rose to  $1.12 \pm 0.49\%$  from  $0.11 \pm 0.01\%$  (\* $p$  < 0.001 vs 420 rpm). The yield was markedly increased to  $8.80 \pm 1.90\%$  by increasing the agitation speed to 25,000 rpm from 570 rpm (\*\* $p$  < 0.0001 vs 420 or 570 rpm) (Fig. 2).

The yields of different-sized microsphere fractions are summarized in Table 1. The use of the highest agitation speed and the smaller flask allowed us to obtain cationized gelatin microspheres of less than  $\phi$ 20  $\mu$ m, which we had not been able to prepare with the conventional method, in addition to increasing the total yield of the cationized gelatin microspheres.

#### Gene introduction with the new cationized gelatin

We examined the efficiency of the new, smaller-sized cationized microspheres for gene introduction into rat peritoneal macrophages. As shown in Figure 3A, after coincubation of the macrophages and GFP

Table 1 Yields of different-sized cationized gelatines (%).

Flask size (mL) / Agitation speed (rpm)	> $\phi$ 20 $\mu$ m	$\phi$ 20-32 $\mu$ m	$\phi$ 32-90 $\mu$ m	$\phi$ 90 $\mu$ m >
500/420	0	0.13 $\pm$ 0.02	15.1 $\pm$ 3.21	14.0 $\pm$ 5.30
500/570	0	1.22 $\pm$ 0.52*	13.2 $\pm$ 3.52	14.1 $\pm$ 6.13
500/25000	0	2.30 $\pm$ 0.47	17.2 $\pm$ 4.10	7.23 $\pm$ 1.60
300/420	0	0.11 $\pm$ 0.01	19.1 $\pm$ 5.32	17.4 $\pm$ 7.12
300/570	0	1.12 $\pm$ 0.49**	22.1 $\pm$ 7.62	11.3 $\pm$ 2.52
300/25000	2.12 $\pm$ 0.21	8.80 $\pm$ 1.90***	32.2 $\pm$ 11.0	9.10 $\pm$ 2.10

Data are presented as mean  $\pm$  SEM. \*p < 0.001 vs 500/420, \*\*p < 0.001 vs 300/420

\*\*\*p < 0.0001 vs 300/420 or 300/570

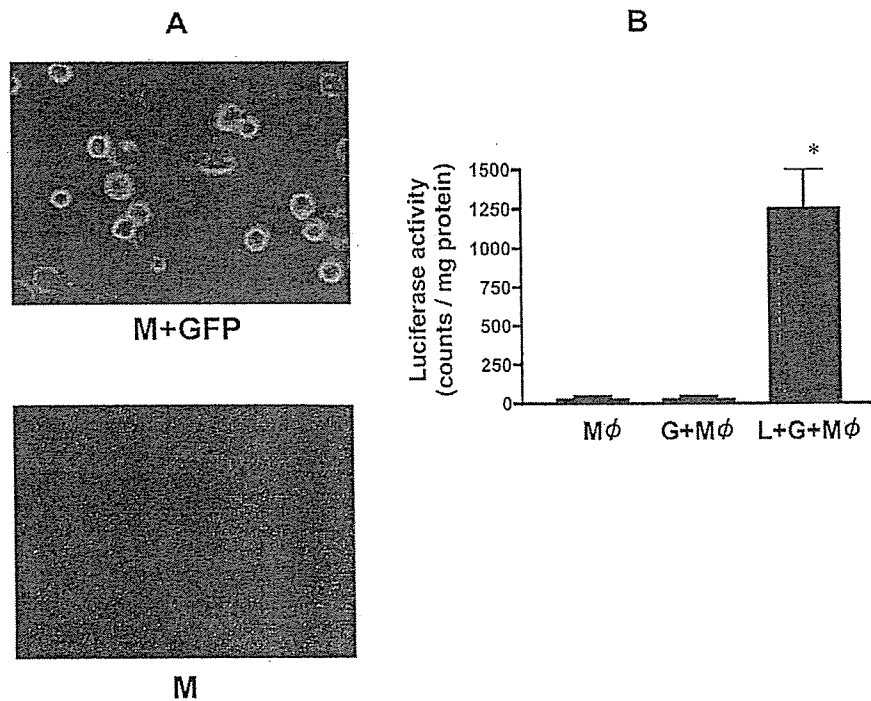


Fig. 3 Gene introduction into rat peritoneal macrophages with cationized gelatin.

A. Upper column: Peritoneal macrophages were coincubated with GFP gene-cationized gelatin complex (M + GFP) for 14 days. GFP was expressed in the cytoplasm of the macrophages. Lower column: Peritoneal macrophages were coincubated with cationized gelatin complex (M) for 14 days. GFP was not expressed in the macrophages.

B. Luciferase activity. Peritoneal macrophages were coincubated with luciferase gene-cationized gelatin complex (L + G + M $\phi$ , closed bar) or with cationized gelatin (G + M $\phi$ , horizontal lined bar) or with no additive (M $\phi$ , open bar) for 14 days. Data are presented as mean  $\pm$  SEM. The luciferase activity of L+G+M $\phi$  was significantly higher than that of M $\phi$  or G+M $\phi$  (\*p < 0.01).

gene-cationized gelatin complex, the cells expressed GFP. Coincubation of the macrophages and cationized gelatin alone did not result in expression of GFP. As shown in Figure 3B, after coincubation of the macrophages and luciferase gene-cationized gelatin complex, the cells expressed luciferase activity of  $1251 \pm 257$  (counts/mg protein) on day 14, while the activity in the control group, in which macrophages were cultured alone, was only  $5 \pm 2$  (counts/mg protein) (\*p < 0.01). The luciferase activity was  $8 \pm 2$  (count/mg protein) in the macrophage + cationized gelatin group.

## DISCUSSION

In this study, we showed that the yield of cationized gelatin microspheres of  $\phi$  20-32  $\mu$ m increased with increasing agitation speed and with the use of a smaller three-necked flask for the agitation of cationized gelatin with olive oil. In addition, cationized gelatin microspheres smaller than  $\phi$  20  $\mu$ m could be prepared for the first time with the highest agitation speed and the smaller flask.

In the conventional method, 30% of cationized

gelatin finally formed microspheres, but almost all were larger than  $\phi 32 \mu\text{m}$  [9]. Gene introduction with cationized gelatin microspheres involves cellular phagocytic activity, which is inefficient for particles as large as  $\phi 30 \mu\text{m}$  [6]. By using a speed as high as 25,000 rpm and a smaller flask (300 mL), we were able to increase the yield of cationized gelatin microspheres of  $\phi 20\text{--}32 \mu\text{m}$  to 8.80%. Furthermore, we could manufacture cationized gelatin microspheres smaller than  $\phi 20 \mu\text{m}$ , which could not be obtained by the conventional method, in a yield of 2.12%.

Gedanken *et al.* succeeded in the production of nanoparticles from various chemicals by using ultrasonic irradiation [10]. However, when we used an ultrasonic homogenizer for agitating cationized gelatin and olive oil, the yield decreased to 1.30%.

We previously showed that our gelatin microsphere-gene complexes were introduced into cells by phagocytosis. Since the efficiency of cellular phagocytotic activity is greater for smaller particles, the development of smaller-sized cationized gelatin microspheres is expected to increase the efficiency of gene introduction via phagocytosis. Further, Kaul *et al.* showed that gene introduction into fibroblasts, which exhibit endocytosis but not phagocytosis, was possible by using nanoparticles of polyethylene glycol [11]. Therefore, if our method can be extended to obtain cationized gelatin microspheres in the nano size range, the variety of cells to which they would be applicable may be considerably extended. It is still the case that a gene introduction method with adequate safety and efficiency for clinical application is not yet available [12]. The ingredient, gelatin, used in this study is already in clinical use, and is considered to be safe. Cationized gelatin microspheres cannot be used to introduce genes into all types of cells, and the efficiency of gene introduction is lower than that of viral vectors. However, the use of cationized gelatin microspheres to introduce a gene into endothelial progenitor cells did have an apparent and prolonged therapeutic effect [5, 6]. The smaller cationized gelatin microspheres developed in this study may provide increased efficiency of gene introduction into various cells.

In conclusion, we have improved the preparation of cationized gelatin microspheres for gene transduction, obtaining a greater yield, as well as smaller microspheres, which may have clinical potential.

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## Intravenous injection of phagocytes transfected ex vivo with FGF4 DNA/biodegradable gelatin complex promotes angiogenesis in a rat myocardial ischemia/reperfusion injury model

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**Abstract** Conventional gene therapies still present difficulties due to poor tissue-targeting, invasiveness of delivery, method, or the use of viral vectors. To establish the feasibility of using non-virally ex vivo transfected phagocytes to promote angiogenesis in ischemic myocardium, gene-transfection into isolated phagocytes was performed by culture with positively charged gelatin impregnated with plasmid DNA. A high rate of gene transfection was achieved in rat macrophages and human monocytes, but not in mouse fibroblasts. The efficiency was  $68 \pm 11\%$  in rat macrophages and  $78 \pm 8\%$  in human monocytes. Intravenously injected phagocytes accumulated predominantly in ischemic tissue ( $13 \pm 8\%$ ) and spleen ( $84 \pm 6\%$ ), but negligibly in other organs in rodents. The efficiency of accumulation in the target ischemic tissue reached more than 86% on direct local tissue injection. In a rat model of myocardial ischemia-reperfusion, intravenous injection of fibroblast growth factor 4 (FGF4)-gene-transfected macrophages significantly increased regional blood flow in the ischemic myocardium ( $78 \pm 7.1\%$  in terms of flow ratio of ischemic/non-ischemic myocardium) compared with intravenous administration of saline ( $36 \pm 11\%$ ) or non-transfected macrophages ( $42 \pm 12\%$ ), or intramuscular administration of naked DNA encoding FGF4 ( $75 \pm 18\%$ ). Enhanced angiogenesis in the ischemic tissue we confirmed histologically. Similarly, intravenous injection of FGF4-gene-transfected monocytes enhanced regional blood flow in an ischemic hindlimb model in mice ( $93 \pm 22\%$ ), being superior to the three other treatments described above ( $38 \pm 12$ ,  $39 \pm 15$ , and  $55 \pm 12\%$ , respectively).

Phagocytes transfected ex vivo with FGF4 DNA/gelatin promoted angiogenesis. This approach might have potential for non-viral angiogenic gene therapy.

**Key words** angiogenesis – cells – gene therapy – growth substances – ischemia

### Abbreviations and acronyms

ANOVA = analysis of variance  
FGF4 = fibroblast growth factor-4  
GFP = green fluorescent protein  
pI = isoelectric point

### Introduction

Conventional gene therapies still require improvement with regard to transfection efficiency and safety [1, 2], as well as tissue targeting [3], despite recent advances. Achievement of a high transfection rate often requires a viral vector, but the safety of the viruses has not yet been



established [4–6]. Conventional non-viral vectors seem to be inferior to viral ones in transfection efficiency, except for nucleofection [7, 8]. Conventional gene therapy using a viral vector can induce inflammation in the gene-transduced tissue [9]. Moreover, *in vivo* gene-delivery to the localized target tissue usually necessitates invasive approaches. For example, direct gene-transfection to cardiomyocytes requires surgical operation [10] or cardiac catheterization [11, 12]. On the other hand, *ex vivo* gene-transfection is less invasive, but tissue-targeting by intravenous injection is difficult to achieve [3].

Macrophages accumulate in ischemic tissue based on the mechanism of immune response (chemotaxis) [13]. This suggests that intravenous transplantation of macrophages may target the ischemic tissue *in vivo*. Tabata *et al.* previously reported that gelatin particles are phagocytized by macrophages [14, 15]. The isoelectric point (pI) of gelatin can be changed by modification of its residues, and positively charged gelatin can be impregnated with negatively charged substances [16] such as nucleic acid [17]. Thus, gelatin may be suitable as a vector for transfecting phagocytes *ex vivo*.

We describe here a study aimed at examining the feasibility of a new concept for less invasive, cell-based gene therapy, by means of *ex vivo* gene transfection into isolated phagocytes (macrophages and monocytes) using a non-viral vector, gelatin, followed by intravenous injection of the transfected phagocytes. The present method has significant advantages over conventional cell-based gene delivery [18, 19], in that the intravenously injected cells (phagocytes) not only produce protein from the transfected gene, but have a tissue-targeting ability.

## Methods

This study was performed in accordance with the Guideline of Tokai University School of Medicine on Animal Use, which conforms to the NIH Guide for the Care and Use of Laboratory Animals (DHEW publication No. (NIH) 86-23, Revised 1985, Offices of Science and Health Reports, DRR/NIH, Bethesda, MD 20205).

### Animals

A total of 121 Fisher rats (male, 10 weeks old, Clea Japan Inc., Tokyo) and 61 nude SCID mice (male, 6 weeks old, Shizuoka Animal Center, Shizuoka, Japan) were used. Rats were anesthetized by inhalation of diethyl ether for harvesting macrophages and with isoflurane (1.5–3%) for thoracotomy, after which they were mechanically ventilated with a mixture of oxygen and nitrous oxide. Mice were anesthetized by intraperitoneal injection of sodium pentobarbital (40 mg/kg).

A model of myocardial ischemia-reperfusion injury

was prepared in 41 rats. The remaining 80 rats were used for collecting activated macrophages. The heart was exposed via thoracotomy, and the proximal left anterior descending coronary artery was ligated [20] for 180 min, followed by reperfusion. A model of hindlimb ischemia was prepared in 61 mice. The left femoral artery was ligated and resected [21].

### Cells

Macrophages were obtained from 80 rats. Thioglycolate (4%, 8 ml) was injected into the peritoneal cavity, and after 4 days, peritoneal macrophages were collected [22]. Monocytes were obtained from peripheral blood of healthy volunteers. Leukocyte-rich plasma was obtained by dextran 500 sedimentation and layered onto Nycoprep 1.068 (Nycomed, Birmingham, UK). The monocyte-containing layer was aspirated, washed twice and allowed to adhere to the dish for 90 minutes. Fibroblasts (NIH 3T3, Invitrogen Corporation, Carlsbad, CA) were also used. The cells were resuspended in RPMI 1640 medium (Sigma) containing 5% heat-inactivated fetal calf serum and cultured for 7–14 days. The cell viability and type were determined by trypan blue exclusion and by immunostaining using anti-macrophage antibody up to 14 days.

### Genes and vector

Complementary DNA (cDNA) of green fluorescent protein (GFP), Renilla luciferase or human hst1/FGF4 (FGF4) [17] was inserted into the expression vector pRC/CMV (Invitrogen Corporation, Carlsbad, CA) and the constructs were designated as pRC/CMV-GFP, pRC/CMV-luciferase and pRC/CMV-HST1-10, respectively. Preparation and purification of the plasmid from cultures of pRC/CMV-GFP-, pRC/CMV-luciferase-, or pRC/CMV-HST1-10-transformed *Escherichia coli* were performed by equilibrium centrifugation in cesium chloride-ethidium bromide gradients.

Gelatin was prepared from porcine skin [14]. After swelling in water the gelatin particles used in this study were spheroids with a diameter of approximately 5–30  $\mu$ m, water content of 95%, and pI of 11. Gelatin (2 mg) was incubated with 50  $\mu$ g of the plasmid for 7 days at 4 °C to make a gelatin-DNA complex [14].

### Experimental protocols

**Ex vivo gene transfection** Macrophages, monocytes, and fibroblasts ( $1 \times 10^6$ ) were cultured with the gelatin-DNA complex (2 mg of gelatin plus 50  $\mu$ g of DNA) for 14 days on a culture dish (100 mm in diameter). Gene ex-

pression of GFP was evaluated by fluorescence microscopy and fluorescence-activated cell sorting. Luciferase activity in the cell lysate was evaluated with a photon counter system after cell lysis [23].

*Organ distribution of phagocytes injected intravenously and directly into ischemic muscle* To examine tissue-targeting by intravenous injection of transfected phagocytes, the distribution of the cells into organs was evaluated by immunohistochemistry. In the rat model of myocardial ischemia-reperfusion injury, the GFP-gene-transfected macrophages ( $1.0 \times 10^6$  each) were injected into the superficial dorsal vein of the penis at the initiation of reperfusion ( $n=7$  and  $5$ , respectively). In the mouse model of hindlimb ischemia, the GFP-gene-transfected monocytes ( $1.0 \times 10^6$ ) were injected into the caudal vein 14 days after induction of ischemia ( $n=5$ ). To examine the tissue-targeting by direct local injection of transfected phagocytes, the distribution of the cells into organs was also evaluated. In the rat model of myocardial ischemia-reperfusion injury ( $n=7$ ) and the mouse model of hindlimb ischemia ( $n=5$ ), the same numbers of transfected macrophages and monocytes were directly injected into ischemic myocardium and ischemic skeletal muscle, respectively. Tissue samples were obtained 24 hours after cell administration. Each tissue was homogenized and cytospin was performed. Immunohistochemical analysis was done with anti-GFP antibody (CLONTECH, USA. GFP-monoclonal antibody). GFP positive macrophages were counted in each tissue and expressed as a percentage of total GFP-positive cells.

*Amelioration of ischemia by intravenous injection of angiogenic gene-transfected phagocytes* The angiogenic effect of intravenously injected FGF4-gene-transfected phagocytes on the ischemia models was evaluated. In the rat model of myocardial ischemia-reperfusion injury, FGF4-gene-transfected macrophages ( $n=5$ ), non-transfected macrophages ( $1.0 \times 10^6$  each) ( $n=5$ ), or saline ( $n=5$ ) were injected into the superficial dorsal vein of the penis, or naked FGF4-DNA ( $50 \mu\text{g}$ ) was injected directly into the ischemic myocardium ( $n=5$ ), at the initiation of reperfusion. Fourteen days after the cell administration, blood flows in the ischemic and non-ischemic regions in the heart were evaluated with a non-contact laser Doppler flowmeter (FLO-N1, Omegawave Corporation). Then, tissue samples were obtained and histological analysis was performed. In a mouse model of hindlimb ischemia, just after induction of ischemia, FGF4-gene-transfected monocytes ( $n=15$ ), non-transfected monocytes ( $n=8$ ) ( $1.0 \times 10^6$  each), or saline ( $n=10$ ) were injected into the caudal vein, or naked FGF4-DNA ( $50 \mu\text{g}$ ) was injected directly into the ischemic muscle ( $n=12$ ). Fourteen days after induction of ischemia, blood flows in the limbs were evaluated with

the noncontact laser Doppler flowmeter (FLO-N1, Omegawave Corporation).

### Histology

Ten micrometer sections were cut from formalin-fixed, paraffin-embedded tissue. Two sections were used for H.E. staining and azan staining, and eight sections were used for immunohistochemical staining. Immunohistochemical staining was performed by an indirect immunoperoxidase method. Anti-GFP antibody, anti-Mac1 antibody (BMA Biomedicals Ag, Switzerland), and anti-CD31 antibody (Serotec, UK) were used as primary antibodies. Mac1-antigen is specific to macrophages/monocytes. Anti-Ig, peroxidase-linked species-specific F(ab')<sub>2</sub> fragments (Amersham Pharmacia Biotech UK Ltd., UK), were used as a secondary antibody. Double staining was performed with alkaline staining and peroxidase staining. The vessel density stained with von Willebrand factor-antibody was calculated by morphometric assessment in one 16 randomly selected fields of each heart and expressed as number/mm<sup>2</sup>.

### Statistical analysis

Data are presented as mean values  $\pm$  SD. Differences were assessed by using ANOVA (analysis of variance) with the Scheffe's multiple comparisons test. A value of  $P < 0.05$  was considered statistically significant.

## Results

### Ex vivo gene transfection

We studied whether genes could be transfected into isolated rat macrophages, human monocytes, and mouse fibroblasts ex vivo by using gelatin. Transfection of the GFP gene into isolated rat macrophages (Figs. 1A and B) and human monocytes (Figs. 1C and D), but not into mouse fibroblasts (data not shown), was achieved by culture with gelatin-DNA complex for 14 days. The gene transfection efficiency into rat macrophages was  $68 \pm 11\%$  (30 experiments, Fig. 2A) and that into human monocytes was  $78 \pm 8\%$  (30 experiments) as determined with a fluorescence activated cell sorter. Sequential analysis after luciferase-gene transfection into rat macrophages revealed high expression after 14 days of culture (Fig. 2B).