has an extended chain conformation below 32°C and dehydrated PIPAAm has a collapsed chain conformation above 32°C.[15–27] This property of PIPAAm has been exploited in intelligent materials for drug delivery systems and chromatography technology.[16–23] The PIPAAm-grafted dish has been found to enable the recovery of cell monolayers easily without enzyme treatment because cells cannot adhere to a hydrophilic surface below 32°C.[24–26] Cell monolayers are the basic units used to construct three-dimensional tissues *in vitro*. Because a cell monolayer recovered without enzyme treatment maintains normal adhesive and junctional proteins, it can easily adhere to the other tissues or cell sheets to construct a three-dimensional artificial tissue.[27–29] Thus, the PIPAAm-grafted dish has the potential to enable the development of new techniques in tissue engineering.

Although the PIPAAm-grafted dish has made a new era in tissue engineering possible, its effects on connexin-43 (Cx43) expression and GJIC have not been studied well. These effects are important because Cx43 plays an important role in cell proliferation and cell differentiation.

In this study, GJIC and expression of Cx43 molecules were examined by scrape-loading dye transfer (SLDT) assay[30] and Western blotting, respectively, using NHDF cells cultured on PIPAAm-grafted dishes irradiated with various doses of electron beams in order to clarify the safety and appropriateness of this material for the culture of artificial cultured tissues.

MATERIALS AND METHODS

Materials

N-isopropylacrylamide monomer (NIPAAm) was purchased from Wako Pure Chemical Industries (Osaka, Japan). Isopropyl alcohol was obtained from Dojindo (Kumamoto, Japan), and Lucifer yellow dye was from Molecular Probes (Eugene, OR).

Cell culture

Normal human dermal fibroblasts (NHDF cells; Sanko Junyaku, Tokyo, Japan) were cultured in Dulbecco's modified Eagle's medium (GIBCO DMEM; Invitrogen, San Diego, CA), supplemented with 10% heat-inactivated fetal calf serum (FCS; Invitrogen) and antibiotics (penicillin [100 units/mL]-streptomycin [100 units/mL]) (Invitrogen) at 37°C. NHDF cells were maintained in a humidified atmosphere of 5% CO_2 and 95% air.

Preparation of PIPAAm-grafted culture dishes

One hundred microliters of 40% NIPAAm dissolved in isopropyl alcohol was added to 35-mm dishes and irradiated with various doses of electron beams (25, 100, 250, or 500 kGy), using an area electron beam-processing system (Nissin High Voltage, Kyoto, Japan). The PIPAAm-grafted dishes were then rinsed three times with ice-cold sterile water (2 ml) for 5 min, sealed, and dried under vacuum.

Cell morphology

NHDF cells were cultured on control and PIPAAm-grafted dishes. Confluent cells (after 4 days of culture) were fixed with formalin solution, stained with 3% Giemsa solution, and observed with an optical microscope.

Protein assay

The protein concentration of cells cultured on control and PIPAAm-grafted dishes was measured with a bicinchoninic acid (BCA) protein assay kit (Pierce Biotechnology, Rockford, IL). Ten-microliter cell samples were

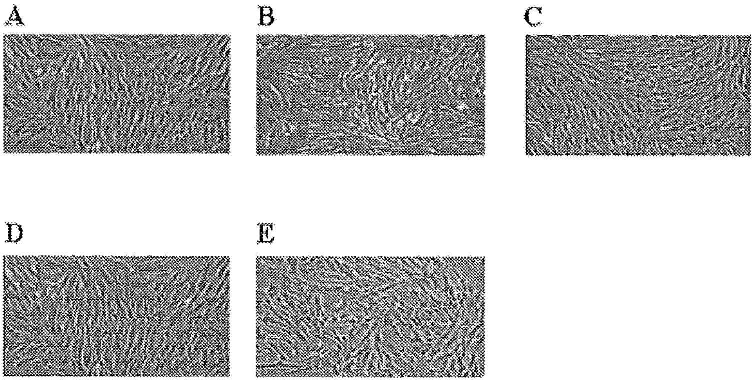

FIG. 1. Optical microscopy images of NHDF cells cultured on PIPAAm-grafted dishes. NHDF cells were cultured for 4 days on PIPAAm-grafted dishes prepared by irradiation with various doses of electron beams (0, 25, 100, 250, or 500 kGy). (**A**) Non-irradiated; (**B**) 25-kGy electron beam; (**C**) 100-kGy electron beam; (**D**) 250-kGy electron beam; (**E**) 500-kGy electron beam.

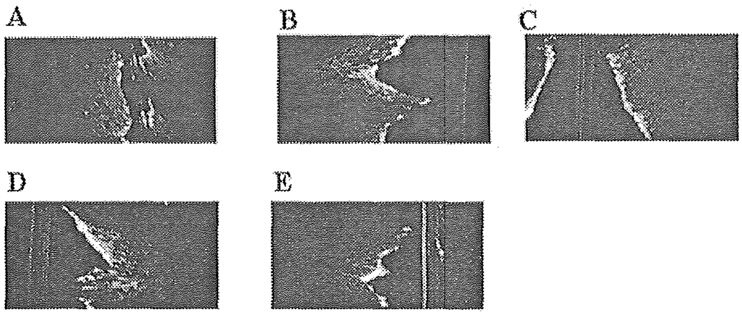

FIG. 2. Fluorescence of NHDF cells by SLDT assay. Transmission of Lucifer yellow into NHDF cells cultured on PIPAAm-grafted dishes irradiated with various doses of electron beams was detected 5 min after scrape-loading. (**A**) Nonirradiated; (**B**) 25-kGy electron beam; (**C**) 100-kGy electron beam; (**D**) 250-kGy electron beam; (**E**) 500-kGy electron beam.

added to 200 μL of the working solution and incubated at 37°C for 30 min in a 96-well plate. Absorbance was then measured at 562 nm in accordance with the manufacturer's protocols.

Scrape-loading dye transfer assay

NHDF cells were seeded on control and PIPAAm-grafted dishes at a density of 1×10^5 cells/mL and cultured for 4 days to form a confluent monolayer. Confluent NHDF cells were washed three times with phosphate-buffered saline containing Ca^{2+} and Mg^{2+} [PBS(+)], and the cell monolayer was scraped with a surgical blade. Fluorescent dye (Lucifer yellow; MW 457.2) at a concentration of 0.1% in PBS(+) was added.[30,31] Cells were exposed to the dye at 37°C for 5 min, and then the dye was discarded and the cells were washed four times with PBS(+). The distance that the dye had migrated was measured under a fluorescence microscope equipped with a type UFX-DXII CCD camera and super high-pressure mercury lamp power supply (Nikon, Tokyo, Japan). The dye migration was measured from the cut edge of the scrape to the edge of the dye front in the cells that were visually detectable.[30]

Western blotting

NHDF cells were cultured for 4 days. After being washed with ice-cold PBS(–) three times, the cells were lysed in 500 μL of lysis buffer (50 mM Tris-HCl [pH 6.8] containing 150 mM NaCl, 5 mM EDTA, 0.1 mM leupeptin, 1 mM phenylmethylsulfonyl fluoride, and 1% Nonidet P-40) for 30 min on ice with shaking. The cell lysates were centrifuged (10,000 rpm) at 4°C for 20 min, and the supernatants were collected. The protein concentrations of the lysates were determined by BCA assay.

Equivalent amounts of protein sample were applied to 12% sodium dodecyl sulfate (SDS)–polyacrylamide gels and then transferred to a nitrocellulose membrane at 120 V for 60 min. The membrane was blocked with Block Ace (Yukijirusi, Tokyo, Japan) overnight at 4°C. After being washed for 30 min in PBS with 0.05% Tween 20, the membrane was incubated for 2 h with anti-Cx43 polyclonal antibody [diluted 1:1000 in PBS(–) with 0.05% Tween 20; Zymed Laboratories, South San Francisco, CA], followed by incubation with horseradish peroxidase (HRP)-conjugated goat anti-rabbit IgG secondary antibody (diluted 1:5000; Zymed Laboratories). The image was visualized with an enhanced chemiluminescence (ECL) detection kit (Amersham Biosciences/GE Healthcare, Little Chalfont, UK).

Statistical analysis

Significant differences between groups were evaluated by Student *t* test. Mean differences were considered significant when $p < 0.05$.

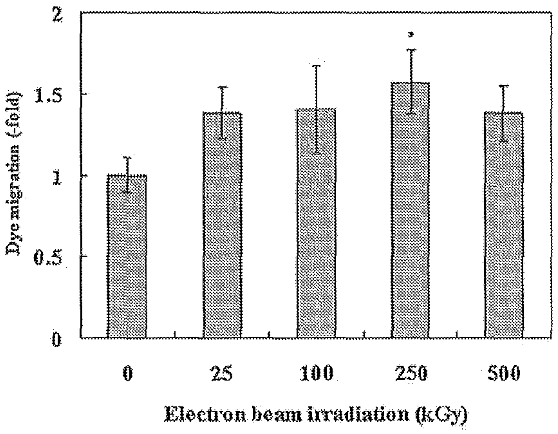

FIG. 3. Positive dye transfer in NHDF cells cultured on PIPAAm-grafted dishes. Transmission of Lucifer yellow was detected 5 min after scrape-loading in NHDF cells cultured on PIPAAm-grafted dishes irradiated with various electron beam doses (0, 25, 100, 250, or 500 kGy). Values represent means ± SD for three dishes. *Significant difference compared with control at $p < 0.05$ by *t* test.

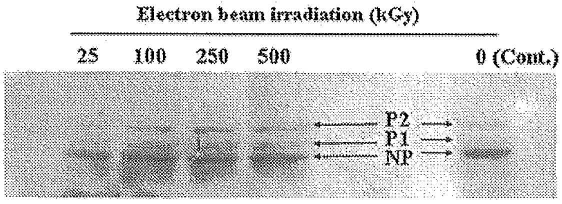

FIG. 4. Western blot of Cx43-NP, Cx43-P1, and Cx43-P2 expression; lysates of NHDF cells cultured on PIPAAm-grafted dishes irradiated with various doses of electron beams (0, 25, 100, 250, or 500 kGy) were applied to SDS–polyacrylamide gels. Fractionated proteins in the gels were transferred to nitrocellulose membrane and immunoblotted with anti-Cx43 polyclonal antibody as described in Material and Methods. Images of Cx43 on Western blot were captured with an Image scanner and analyzed with NIH Image software.

RESULTS

The appearance of NHDF cells grown on PIPAAm-grafted dishes irradiated with various doses of electron beams are shown in Fig. 1. No significant differences were observed by optical microscopy analysis between cells grown in dishes irradiated with various doses of electron beams. These results suggest that PIPAAm-grafted dishes are not toxic to NHDF cells.

The SLDT assay showed that dye migration in cells cultured on PIPAAm-grafted dishes irradiated with electron beams (25, 100, or 500 kGy) was enhanced by about 1.4-fold compared with that on control dishes. Interestingly, the dye migration in cells cultured on PIPAAm-grafted dishes irradiated with the 250-kGy electron beam was particularly enhanced, about 1.6 times higher than that on control dishes (Figs. 2 and 3). These results suggested that the GJIC of NHDF cells cultured on PIPAAm-grafted dishes was enhanced and that the GJIC on PIPAAm-grafted dishes irradiated with the 250-kGy electron beam was affected the most.

To further elucidate the effects of the PIPAAm grafting of culture dishes on GJIC, we analyzed the expression of Cx43, a transmembrane protein involved in GJIC. There are three forms of Cx43: Cx43-NP (nonphosphorylated Cx43), Cx43-P1 (monophosphorylated Cx43), and Cx43-P2 (another phosphorylated Cx43); Cx43-P2 is the most important and functional protein involved in GJIC. The results of Western blotting showed that the expression of Cx43-P1 and Cx43-P2 in NHDF cells cultured on PIPAAm-grafted dishes irradiated with 25, 100, 250, or 500 kGy of electron beams was considerably enhanced. Further, NHDF cells cultured on PIPAAm-grafted dishes irradiated with 100, 250, or 500 kGy of electron beams showed enhanced Cx43-NP expression (Figs. 4 and 5A). The Cx43-P2 expression of cells cultured on PIPAAm-grafted dishes irradiated with the 250-kGy electron beam dose showed the highest value, about 46% higher than that of control dishes. Cells cultured on PIPAAm-grafted dishes irradiated with electron beam doses of 25, 100, and 500 kGy were shown to have enhanced total Cx43 expression. Cells cultured on PIPAAm-grafted dishes irradiated with 100- and 250-kGy electron beam doses showed the highest total Cx43 expression, about 36.6% higher than that of control dish (Fig. 5B).

The Cx43-P2 expression of NHDF cells cultured on PIPAAm-grafted dishes irradiated with 25, 100, 250, and 500 kGy correlated well with GJIC ($R^2 = 0.9398$).

DISCUSSION

Thermoresponsive PIPAAm-grafted dishes irradiated with electron beams have been used to culture cell monolayers because the monolayers can be recovered without enzyme treatment, making PIPAAm a useful material for tissue engineering.

It has been reported that junctional proteins, cellular adherence proteins on the cell membrane, interact via

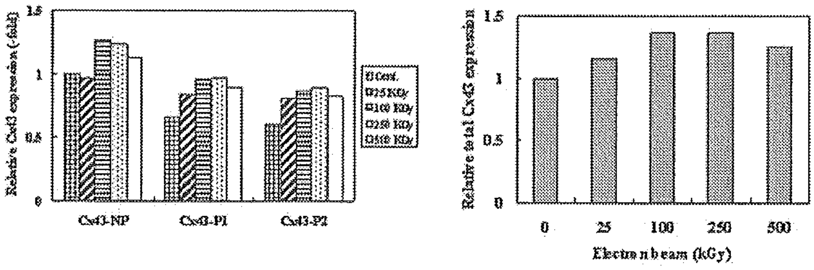

FIG. 5. Relative expression levels of Cx43-NP, Cx43-P1, and Cx43-P2 (**A**) and relative expression levels of total Cx43 (NP+P1+P2) (**B**) of NHDF cells cultured on PIPAAm-grafted dishes irradiated with various doses of electron beams (0, 25, 100, 250, or 500 kGy).

GJIC.[31] In this study, an SLDT assay demonstrated that dye migration in cultured NHDF cells was significantly enhanced in all PIPAAm-grafted dishes tested. Therefore, the chemical structure of the PIPAAm surface may stimulate junctional proteins on the cell membrane, and the stimulated junctional proteins may induce the enhancement of GJJIC.

Cx43 expression of NHDF cells cultured on PIPAAm-grafted dishes irradiated with a 250-kGy electron beam changed significantly. Structural differences in PIPAAm triggered by the 250-kGy electron beam induced Cx43 protein expression by NHDF cells, probably by affecting the gene expression of NHDF cells. Further, total Cx43 expression was shown to be enhanced in cells cultured on PIPAAm-grafted dishes irradiated with various doses of electron beams (25, 100, 250, or 500 kGy). Differences due to the electron beam dose should be studied further.

Although the mechanism involved was not determined, it has been reported that basic fibroblast growth factor (bFGF) and keratinocyte growth factor (KGF) enhance GJIC activity and the expression of Cx43.[32–35] If bFGF and KGF in FCS are adsorbed onto the PIPAAm surface, cells can efficiently access these growth factors from the PIPAAm surface, and GJIC may be enhanced. It is also reported that bFGF activates protein kinase A (PKA),[36] an important regulator of Cx43, promoting the phosphorylation of Cx43 and enhancing GJIC.[37] Therefore, bFGF adsorbed onto the PIPAAm surface may bind its receptor and induce the activation of PKA, resulting in an enhancement of GJIC on NHDF cells caused by the increase in Cx43-P2 band protein.

In the process of posttranslational change, Cx43-P2 becomes insoluble in Triton X-100.[38] Thus, not all Cx43-P2 may be included in the lysate, and some Cx43-P2 may have been included in the pellet. More Cx43-P2 may have existed than was detected in the present results obtained by Western blotting.

In this study, it was shown that the use of PIPAAm-grafted dishes irradiated with various doses of electron beams enhanced GJIC and Cx43 expression in cultured NHDF cells. This suggests that PIPAAm-grafted dishes may promote efficient tissue regeneration, because GJIC plays an important role in increasing tissue strength.[39]

ACKNOWLEDGMENTS

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In vitro study on the osteogenesis of normal human osteoblasts cultured on the discs of various kinds of calcium phosphate ceramics

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Keywords: Calcium phosphate ceramics, osteogenesis, cytotoxicity,

Abstract. We estimated effects of various CP ceramics on the properties of normal human osteoblasts (NHOst) as well as a viability of V79 fibroblasts. In the present study, five kinds of CP ceramics, namely, hydroxyapatite (HAp) flouroapatite (FAp), α-tricalcium phosphate (α-TCP), β-tricalcium phosphate (β-TCP) and tetracalcium phosphate (TTCP), were tested. Cytotoxicity test was carried out using V79 fibroblasts by colony assay system. The amounts differentiation level of NHOst was estimated from alkaline phosphatase (ALP) activity and osteocalcin.

From the results of colony assay, FAp and α-TCP showed strong cytotoxicities on V79 cells. The results from the proliferation studies of NHOst with CP ceramics were consistent with the results of colony assay. In addition, the ALP activities of NHOst with CP ceramics after 1week culture were significantly suppressed in comparison with that of NHOst alone. The osteocalcin amounts produced from NHOst cultured on β-TCP was the highest among five kinds of CP ceramics.

Introduction

Calcium phosphate (CP) ceramics have been studied to utilize as the scaffolds for repairing bone defects. For instance, hydroxyapatite ($Ca_{10}(PO_4)_6(OH)_2$, HAp) or β-tricalcium phosphate (β-$Ca_3(PO_4)_2$, β-TCP), can be biologically bonded to natural bones and their porous materials are effective for restoration of bone defects [1]. Fluoroapatite ($Ca_{10}(PO_4)_6F_2$, FAp) has been reported to have a potential of novel bone repairing materials with high stability *in vivo*, since solubility of FAp is lower than that of HAp [2]. In addition, CP cement is also promising for bone repair and it is well known that α-tricalcium phosphate (α-$Ca_3(PO_4)_2$, α-TCP) or tetracalcium phosphate ($Ca_4(PO_4)_2O$, TTCP) are starting materials for the harden reaction of the bone cement [3].

To develop biomaterials for utilizing for bone tissue, various properties, e.g. biological, physical or chemical property, should be satisfied. Among them, biological safety and osteogenesis properties, e.g. proliferation and differentiation of the osteoblasts, should be important factors to provided to the biomaterials. However, understandings of the biological interaction between osteoblasts and various CP ceramics are few, since the interaction has not been studied under the same experimental condition in detail. Therefore, we estimated effects of various CP ceramics on the properties of normal human osteoblasts (NHOst) as well as a viability of V79 fibroblasts in this study.

Materials and Methods

Materials

Cytotoxicity and osteogenesis of NHOst on five kinds of CP ceramics, namely, HAp, FAp, α-TCP, β-TCP and TTCP (Wako chem. Co. Ltd., Tokyo, Japan), were evaluated. 0.25g of CP powders was put into stainless mold and uniaxially pressed at 30MPa for 1 min to form pellets. The dimensions of the obtained CP pellet were 1mm in thickness and 12mm in diameter. CP pellets were sterilized by the autoclave 121°C for 20 min.

Cytotoxicty test on CP ceramics

Cytotoxicity test was carried out using Chinese hamster V79 lung fibroblasts by the colony assay system. V79 cells were maintained in Eagle's minimum essential medium (Nissui Pharmaceutical Co. Ltd.,) with 10% fetal calf serum (FCS, Intergen company) and incubated at 37 °C in a humidified atmosphere with 5% CO_2.

The method of cell seeding was shown below; At first, each CP pellets were placed in each culture wells of 24 well culture plates (Corning Co. Ltd.) and 300μl of culture medium was added into each well. Next, 50 cells/300μl of culture medium was added into each well and incubated for 4 h at 37°C. Finally, 400μl of culture medium was added and incubated at 37 °C in a humidified atmosphere with 5 % CO_2 for 7days.

In order to investigate the cell adhesive property on the CP ceramics, the culture medium was changed after cultivations for 4 h and incubated for 7days. The removed culture medium was transferred to another well of the plate and incubated for 7days as well.

Cytotoxicity of extracts from CP ceramics was also investigated in this study. Suspensions of CP ceramics in the culture medium (100mg/mL) were stirred at 37°C for 3days in 150rpm. The suspensions were centrifuged and the supernatants were collected to use as test extracts. The cytotoxicity test was carried out culturing 50 V79 cells in 1ml of the extracts and incubated at 37 °C for 7days.

After 7days, the cells were fixed in methanol and the number of the V79 colonies was counted after staining cells with 5%-Giemsa solution. In addition, the pH of the medium after 7-days culture was measured to estimate effect of the pH of the medium on the cytotoxicity test.

Osteogenesis evaluation of NHOst cultured on CP ceramics

NHOst were purchased from BioWhittaker Inc.(Walkersville,MD). The NHOst were maintained in alpha minimum essential medium (αMEM, Gibco, Grand Island, NY) containing 10%-FCS. incubators at 37 °C in a humidified atmosphere with 5% CO_2. All assays were performed using αMEM containing 10%-FCS supplemented with 10mM beta-glycerophosphate. Similar to the method of the cytotoxicity test, each CP pellets were placed in 24-well culture plates (Corning Co. Ltd.) and 300μl of culture medium was added into each well, followed by addition of 1ml of cell suspension (4×10^4 cells/ml) into each well.

Proliferation of NHOst cells cultured on various kinds of CP ceramics was estimated by Tetracolor One assay (Seikagaku Co., Ltd. Tokyo, Japan), which incorporates an oxidation reduction indicator based on detection of metabolic activity. After 7-days incubation, 2%-TetraColor One/αMEM solution was added to each well, followed by 2h incubation. The absorbance of the supernatant at 450nm was estimated using μQuant spectrophotometer (Bio-tek Instrument, Inc., Winooski, VT). After estimating the proliferation, the cells were washed by phosphate–buffered saline (PBS(-)), followed by addition of 1ml of 0.1M glycine buffer (pH=10.5) containing 10mM $MgCl_2$, 0.1mM $ZnCl_2$ and 4mM p-nitrophenylphosphate sodium salt. After incubating at room temperature for 5min, the absorbance of 405 nm of glycine buffer was detected using μQuant spectrophotometer to evaluated alkaline phosphatase (ALP) activity of the test cells. The amount of Osteocalcin produced by NHOst was evaluated using Gla-type Osteocalcin EIT kit (Takara. Co., Ltd.). The structural change of CP before and after autoclave sterilization or culture were investigated by powder X-ray diffraction (XRD) analysis and scanning electron microscopy(SEM). XRD analysis was carried out (Rigaku Co., Ltd. / RINT 2000) with the CuK_α radiation at 40kV, 50mA. SEM observations were performed (JEOL / JSM-5800LV) with an accelerating voltage of 25kV.

Results

Cytotoxicity of various CP ceramics

The results of the cytotoxicity test of CPs are summarized in table 1. Notably, the colonies were hardly formed on FAp and α-TCP pellets and the ratios of the colony formation against V79-alone culture were 22.6% and 0.0%, respectively. In addition, the ratios of the colony formation on the HAp, β-TCP and TTCP pellets were 58.1%, 57.3% and 78.4%, respectively. From these results, it is suggested that V79 cells were viable and adhered on the pellet after for 4h after seeding despite of the type of CP ceramics, irrespective of the type of CP ceramics. On the other hand, the cytotoxicity test of extracts from CPs revealed that the tendency of their cytotoxicity was almost the same as that of the respective CP pellets themselves (table1).

Proliferation and differentiation of NHOst cultured on CP ceramics

The effects of various kinds of CP ceramics on the osteogenesis of NHOst are represented in table2. The effects of the CPs on proliferation were consistent with those on the colony formation. Similar to the cytotoxicity test, the proliferation of NHOst was inhibited on FAp and α-TCP pellets. ALP activities of NHOst on CP ceramics after 7-days culture were significantly suppressed in comparison with that of NHOst alone. On the other hand, the osteocalcin amounts produced from NHOst were influenced by the type of CP ceramics. NHOst on β-TCP showed the highest Osteocalcin production among five kinds of CP ceramics.

4. Discussion

The fact that less formation of colonies was observed on FAp and α-TCP pellets suggests that they are strongly cytotoxic. It is suggested that the differences in the colony formation on various CP pellets are ascribed to difference in extract properties from the CP related with the composition or crystal structure (table1). In addition, proliferation of NHOst also was inhibited on FAp and α-TCP. The pH values of culture medium after incubation for 7 days are shown in table1. As shown in the table, the pH of culture medium after incubation with FAp pellets is almost the same as that of HAp, while the pH of the α-TCP medium is much lower than other CP ceramics. In order to considering the reason of the low pH of the culture medium with α-TCP pellet, a surface structural change of α-TCP before and after incubation was analyzed by SEM. SEM images of α-TCP after extraction treatment are shown in Fig.1.

Table1. Cytotoxicity test of various CP ceramics.

Samples	Composition	Formation of colony		pH of medium after culturing	Ca concentration$^{1)}$ /ppm
		On pellets /%	Extraction / %		
V79 alone	-	100.0±4.5	100.0±13.9	7.12	-
HAp	$Ca_{10}(PO_4)_6(OH)_2$	58.1±12.8	84.6±15.1	7.24	0.19
FAp	$Ca_{10}(PO_4)_6F_2$	22.6±20.9**	26.9±8.6*	7.20	0.17
α-TCP	α-$Ca_3(PO_4)_2$	0.0*	7.6±5.1*	6.76	72.62
β-TCP	β-$Ca_3(PO_4)_2$	57.3±6.9	81.1±19.3	7.40	1.27
TTCP	$Ca_4(PO_4)_2O$	78.2±5.0	93.7±6.8	7.65	0.58

*$p<0.01$ against V79 alone, **$p<0.05$ against V79 alone, 1)The Ca ions concentration was extracted Ca ions from CP-ceramics in PBS(-), which were measured by inductivity coupled plasma-atomic emission spectroscopy.

Table2. Osteogenesis of NHOst cultured on various kinds of CP ceramics.

Samples	Proliferation / %	Differentiation level	
		ALP activity / %	Osteocalcin / %
NHOst alone	100±7.9	100±4.4	100±46.2
HAp	63.2±3.5	20.4±1.8*	81.1±31.0
FAp	42.9±19.5	1.24±0.3*	47.2±20.7
α-TCP	18.3*±2.5	17.9±3.8*	110.7±18.8
β-TCP	56.0±4.7	6.3±3.2*	177.1±78.4**
TTCP	82.3±27.3	17.5±4.6*	114.8±4.0

*$p<0.01$ against NHOst alone, **$p<0.01$ against HAp

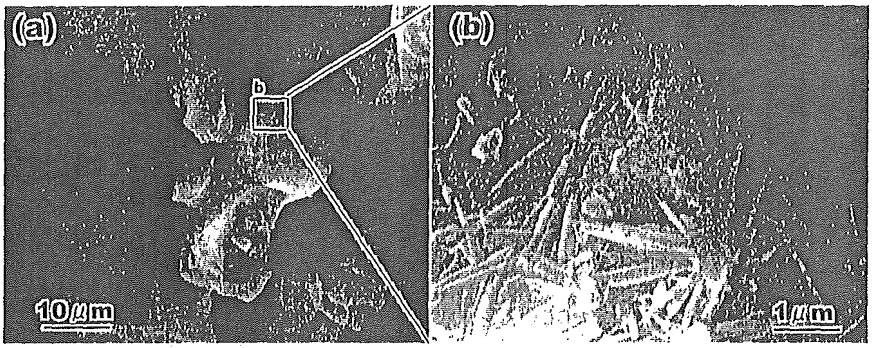

Fig.1. SEM images of α-TCP after extract treatment. (a) whole image and (b) enlarged image of the area enclosed by a rectangle in (a)

Before the extraction, a particle size of α-TCP was about 10μm and its surface was smooth. However, as shown in Fig.1, whisker-like precipitates of 1-2μm in length and 2-300nm in width are observed at the surface of α-TCP after the extraction, although there is no change in its particle size. It is well known that slightly water-soluble calcium phosphates convert to HAp in aqueous solution with high pH value. Since the solubility of α-TCP is higher than that of other calcium phosphates, the α-TCP converts to HAp rapidly as following the reaction.

$$10Ca_3(PO_4)_2+6H_2O \rightarrow 3Ca_{10}(PO_4)_6(OH)_2+2H_3PO_4$$

According to the report of this conversion [4], HAp produced by the above reaction has whisker-like morphology. Therefore, the whisker-like precipitates can be regarded as HAp, so that it is considered that the above conversion occurs at the surface of the α-TCP during incubation. In this case, phosphoric acid is produced as a byproduct in the conversion reaction and the phosphoric acid caused the decrease in the pH of solution. Morita and co-workers [5] have reported that low pH itself could be clastogenic to mammalian cells and the pH of 50% V79 cell survival was 6.5 for 24h incubation. Therefore, it is suggested that the cytotoxicity of α-TCP was mainly due to the pH decreasing resulting from an increase of the phosphoric acid ion produced by the hydrolysis conversion from α-TCP to HAp.

On the other hand, FAp has the same crystal structure of HAp but the hydroxyl ions in HAp substituted by fluorine ions. Since difference of the colony formation on various CP ceramics would be due to eluted substances from CP as described above, the cytotoxicity of FAp would be due to eluted fluoride ions from FAp.

Effects of CP ceramics on osteogenesis function of NHOst are shown in table2. As shown in the table, ALP activities of NHOst were significantly suppressed on CP ceramics irrespective of their type and the amount of osteocalcin on β-TCP was the highest among five kinds of CP ceramics. Since it is well known that osteocalcin express in maturated stage of differentiation level of NHOst, these results suggest that maturation of NHOst proceeds on β-TCP. . The differences of maturation of NHOst on various kinds of CP ceramics may be related with the amount of extracted Ca^{2+} and/or PO_4^{3-} ions.

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Cytotoxicity of Various Calcium Phosphate Ceramics

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Keywords: Calcium phosphate ceramics, Cytotoxicity,

Abstract. The cytotoxicity of five calcium phosphate ceramics, hydroxyapatite (HAp), flouroapatite (FAp), α-tricalcium phosphate (α-TCP), β-tricalcium phosphate (β-TCP) and tetracalcium phosphate (TTCP), was investigated. Based on the guidelines of biological test for medical devices in Japan, a cytotoxicity test of these calcium phosphates was carried out using Chinese hamster V79 lung fibroblasts. The cytotoxic study revealed that FAp and α-TCP showed high cytotoxicities. From various analyses, it was considered that the cytotoxicity of the FAp was due to fluorine ions extracted in a culture medium and the cytotoxicity of α-TCP resulted from a decrease in pH of the medium by the phosphoric acid, which produced by hydrolysis of the α-TCP.

Introduction

From the view point of biological affinity to bone, calcium phosphate (CP) ceramics have been studied to utilize for many purposes in a medical field. For instance, hydroxyapatite ($Ca_{10}(PO_4)_6(OH)_2$, HAp) and β-tricalcium phosphate (β-$Ca_3(PO_4)_2$, ß-TCP), are known to be biologically bonded to natural bones and their porous materials have been studied for effective restoration of bone defects.[1,2] Fluoroapatite ($Ca_{10}(PO_4)_6F_2$, FAp) has been reported to have a potential of novel bone repairing materials with high stability *in vivo*, since solubility of FAp is lower than that of HAp.[3,4] In addition, CP cement is also promising for bone repair and it is well known that α-tricalcium phosphate (α-$Ca_3(PO_4)_2$, α-TCP) and tetracalcium phosphate ($Ca_4(PO_4)_2O$, TTCP) are starting materials for the harden reaction of the bone cement.[5,6]

To develop biomaterials for utilizing for bone tissue, various properties, e.g. biological, physical and chemical property, should be satisfied. Among them, biological safety is important for the biomaterials. Since only a few studies which discuss the cytotoxicity of calcium phosphate ceramics have been reported, the cytotoxicity of CP ceramics is worthy to be investigated in order to design bioceramics with good biological safety for medical application. Therefore, the cytotoxicities of five calcium phosphate ceramics, hydroxyapatite (HAp), flouroapatite (FAp), α-tricalcium phosphate (α-TCP), β-tricalcium phosphate (β-TCP) and tetracalcium phosphate (TTCP) were investigated.

Materials and Methods

Materials

Five kinds of CP ceramics, HAp, FAp, α-TCP, β-TCP and TTCP were purchased from Wako chem. Co. Ltd. CP powders (0.25 g) was put into stainless mold and uniaxially pressed at 30MPa for 1 min to form a pellet. The dimensions of the obtained CP pellet were 1mm in thickness and 12mm in diameter. CP pellets were sterilized by an autoclave at 121°C for 20 min.

Cytotoxicty test on CP ceramics

Cytotoxicity test was carried out using Chinese hamster V79 lung fibroblasts by a colony assay system. V79 cells were maintained in Eagle's minimum essential medium (Nissui Pharmaceutical Co. Ltd.) with 10% fetal calf serum (FCS, Intergen Co. Ltd.) and incubated at 37 °C in a humidified atmosphere with 5% CO_2.

The method of cell seeding in the cytotoxicity test of CP ceramics was shown below; each CP pellets were placed in each culture wells of 24 well culture plates (Corning Co. Ltd.) and 300μl of culture medium was added into each well. Then, 50 cells/300μl of the cell suspension in the culture medium were added into each well and incubated at 37°C for 4 h. Finally, 400μl of the culture medium was added into each well and the plates were incubated at 37 °C in a humidified atmosphere with 5 % CO_2 for 7days. In order to investigate a cell adhesive property on the CP ceramics, the culture medium was changed after 4 h and further incubated for 7days. The removed culture medium was transferred to another well of a new plate and incubated for 7days as well.

Cytotoxicity of extracts from CP ceramics was also investigated in this study. Suspensions of CP ceramics in the culture medium (100mg/mL) were stirred at 37°C for 3days under the rotation condition at 150rpm. The suspensions were centrifuged and the supernatants were collected as test extracts. In addition, media with various pH values were prepared using HCl solution to investigate an effect of pH on cell survival. Fifty V79 cells in 1ml of the extracts or the medium with different pH value were incubated at 37 °C for 7days.

After 7-day incubation, the cells were fixed in methanol and the number of the V79 colonies was counted after staining cells with 5%-Giemsa solution to estimate the cytotoxicity of the test sample. In addition, the pH of the medium after 7-days culture was measured to estimate the effect of the pH of the medium on the cytotoxicity test.

Characterization of CP ceramics

The structural changes of CP before and after an autoclave-sterilization or an incubation at 37°C culture were investigated by powder X-ray diffraction (XRD) analysis and scanning electron microscopy (SEM). XRD analysis was carried out (Rigaku Co., Ltd. / RINT 2000) with the CuK_α radiation at 40kV, 50mA. SEM observations were performed (JEOL / JSM-5800LV) with an accelerating voltage of 25kV.

Results and Discussion

Cytotoxicity of various CP ceramics

From XRD analysis, no structural changes of CPs were observed after an autoclave sterilization. After staining CP pellets, it was observed that cell colonies were formed on various CP ceramics pellets (Fig.1(a)). The results of the cytotoxicity test of CPs are shown in Fig.1(b). The cell colonies were hardly formed on FAp and α-TCP pellets and the ratios of the colonies formed on these pellets against V79-alone culture were 22.6% and 0.0%, respectively. In addition, the ratios of the colonies on the HAp, β-TCP and TTCP pellets were 58.1%, 57.3% and 78.4%, respectively. As no colonies were observed after 7-day culture of the removed medium in cell adhesion studies of CP ceramics, these results suggested that V79 cells can adhere and be viable on these pellets, irrespective of the type of CP ceramics. Figure 2 shows the formation of colonies cultured in extract from CP ceramics. The cytotoxicity test of extracts from CPs revealed that the tendency of their cytotoxicities was similar to that of the cytotoxicities on the respective CP pellets themselves (Fig.1(b)).

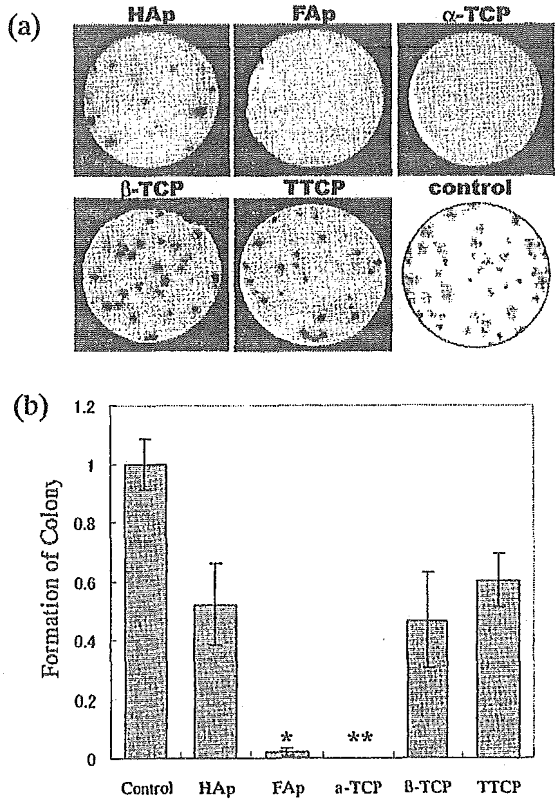

Fig.1. The appearance of colonies on various CP pellets (a) and their colony formation ratios (b). (*$p<0.05$ against for V79 alone, **$p<0.01$ against for V79 alone)

The fact that less formation of colonies was observed on FAp and α-TCP pellets suggests that they are highly cytotoxic. In addition to results shown in Fig.2, it is suggested that the differences in the colony formation ratio on various CP pellets are ascribed to difference in extract properties from the CP, which may be related with the composition or crystal structure. As shown in Table 1, the pH of culture medium after incubation with FAp pellets is almost the same as that of HAp, while the pH of the α-TCP-incubated medium is much lower than that of the other CP ceramics-incubated media.
In order to consider the reason of the low pH of the a-TCP-incubated medium, a surface structural change of α-TCP before and after incubation was analyzed by SEM. SEM images of α-TCP before and after extraction treatment are shown in Fig.3. Before extraction, a particle size of α-TCP was about 10μm and its surface was smooth (Fig.3(a) and (b)). However, whisker-like precipitates of 1-2μm in length and 2-300nm in width were observed at the surface of α-TCP after the extraction, although there was no change in its particle size (Fig.3(c) and (d)). It is well known

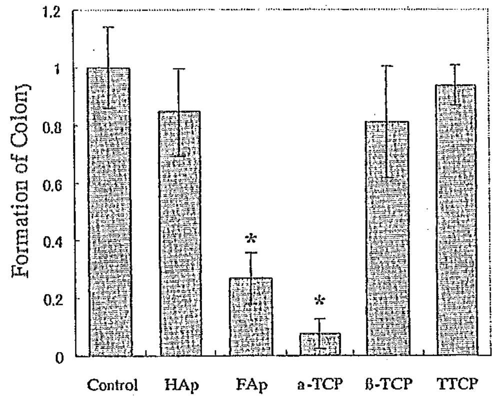

Fig.2. Formation of colony cultured in extract from various CP ceramics. (*p<0.01 against for V79 alone)

Table 1. The pH and Ca concentration of culture medium after incubation.

Samples	pH of medium after culturing	Ca concentration /ppm
V79 alone	7.12	-
HAp	7.24	0.19
FAp	7.20	0.17
α-TCP	6.76	72.62
β-TCP	7.40	1.27
TTCP	7.65	0.58

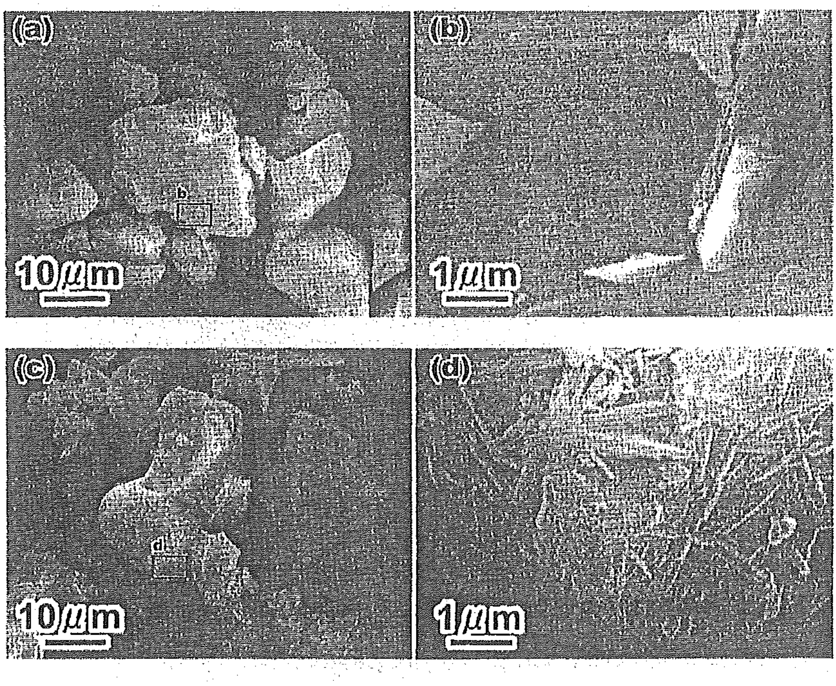

Fig.3. SEM images of α-TCP before (a), (b) and after extract treatment (c), (d).
(a) and (c) are whole image of before and after extract treatment, respectively. (b) and (d) are enlarged image of the area enclosed by a rectangle in (a) and (c), respectively.

that calcium phosphates convert to HAp in aqueous solution with high pH value. Since the solubility of α-TCP is higher than that of other calcium phosphates, α-TCP rapidly converts to HAp as follows;

$$10Ca_3(PO_4)_2+6H_2O \rightarrow 3Ca_{10}(PO_4)_6(OH)_2+2H_3PO_4$$

According to the report of this conversion [7], HAp produced by the above reaction has whisker-like morphology. Therefore, the whisker-like precipitates in Fig.3 (d) can be regarded as HAp, so that it is considered that the above conversion occurs at the surface of the α-TCP during incubation.

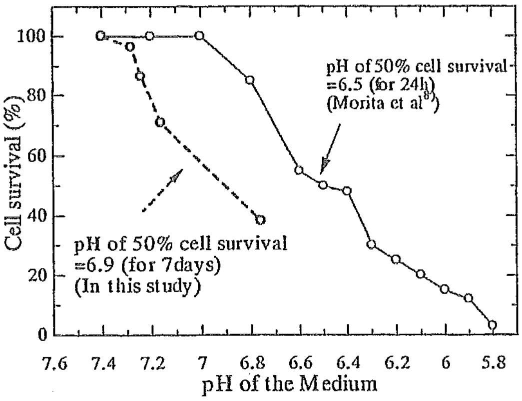

Fig.4. V79 cell survival in the medium with various pH values.

In this case, phosphoric acid is produced as a byproduct in the conversion reaction and the phosphoric acid causes the decrease in pH of the solution. As shown in Fig.4, Morita and co-workers[8] have reported that low pH itself could be clastogenic to mammalian cells and the pH of 50% V79 cell survival was 6.5 for 24h incubation. In the present colony assay system, the pH of 50% V79 cell survival was 6.9 for 7-days incubation. In addition, we confirmed that phosphoric acid showed no or weak cytotoxicities under our present experimental conditions. Therefore, it is suggested that the cytotoxicity of α-TCP is mainly due to the pH decrease resulting from an increase of the phosphoric acid ion by the hydrolysis conversion from α-TCP to HAp.

On the other hand, FAp has the same crystal structure of HAp but the hydroxyl ions in HAp substituted by fluorine ions. Since it is probable that difference of the colony formation on various CP ceramics are due to eluted substances from CP as described above, the cytotoxicity of FAp would be due to eluted fluoride ions from FAp. In conclusion, this study has revealed that FAp and α-TCP have a cytotoxicity, while TTCP has lower cytotoxicity than other calcium phosphates. To develop biomaterials made from calcium phosphate, further studies are necessary to clarify their cytotoxic mechanisms.

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Novel Calcium Phosphate Ceramics : The Remarkable Promoting Action on the Differentiation of the Normal Human Osteoblasts

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Keywords: Hydroxyapatite, Niobium ion, Osteoblast, Alkaline phosphatase activity

Abstract.

To promote the activity of normal human osteoblasts (NHOst), the novel HAp ceramics containing Nb ions (NbHAp) were synthesized by wet chemical process, which reacting aqueous solution containing a mixture of $Ca(NO_3)_2$, $(NH_4)_2HPO_4$, and the Nb aqueous solution. X-ray diffraction patterns indicated that NbHAp had a monolithic apatitic structure, although crystallite decreased as Nb content increased. From inductively coupled plasma analysis, maximum amount of Nb ions in the sample was almost 8.2atom% of P ions. The NbHAps were presented as aggregates and composed of fine crystal of $<1\mu m$ in diameter. Nb ions in NbHAp were uniformly distributed in the aggregates. Furthermore, high-resolution XPS spectra of Nb $3d_{5/2}$ indicated that Nb ions in the HAp were presented as Nb^{5+}. These results suggested that Nb ions were at PO_4 site in crystal structure of HAp. When NHOst were cultured with the NbHAp, their ALP activity were twice as much as that of NHOst cultured with HAp without Nb ions.

Introduction

Tissue engineering takes advantages of the combined use of cultured living cells and scaffolds to deliver vital cells to the damaged site of the patient. Some tissue engineering approaches have been devised to repair large bone defect. In developing of the scaffold for bone tissue, the interaction between osteoblasts cells and scaffolds are much important. To achieve the restoration the bone tissue at early stage, the scaffold is required to have the ability of promoting proliferation and mineralization.

It is well known that hydroxyapatite ($Ca_{10}(PO_4)_6(OH)_2$, HAp) ceramics can be biologically bonded to natural bones and have been studied to utilize as the scaffolds. In addition, the structure is very tolerant of ionic substitutions and Ca^{2+} ions, PO_4^{3-} ions and OH^- ions can be replaced by various cationic or anionic ions, partly or completely[1]. For example, K^+, Mg^{2+} and Sb^{3+}, can substituted for Ca ions and CO_3^{2-} and VO_4^{3-} can substituted for PO_4^{3-} ions, completely or partially. Thus various kinds of ion substitutions can be made to synthesize novel modified-HAps.

Recently, our co-workers reported that niobium (Nb) ions have the significant effect which promotes the proliferation and differentiation of normal human osteoblastic cells (NHOst)[2]. In the present study, therefore, we attempted to synthesize the novel HAp ceramics containing Nb ions (NbHAp) to promote the activity of NHOst and investigated the interaction between NbHAp and NHOst.

Materials and Methods

Synthesis of Nb containing HAp

The NbHAp was synthesized by wet chemical process, which reacting aqueous solution containing a mixture of $Ca(NO_3)_2$, $(NH_4)_2HPO_4$, and the Nb aqueous solution. The reagent grade $Ca(NO_3)_2$, $(NH_4)_2HPO_4$ and $NbCl_5$ (Wako Pure Chemical Industries, Ltd) were used without purification. The metal ion chemical reagent was completely dissolved in an exact amount of distilled water. The Nb aqueous solution was prepared by the mixing of distilled water and $NbCl_5$ solution, which dissolved in 5vol%-hydroxyaceton and 5vol%-2-aminoethanol[3].

0.2M-$(NH_4)_2HPO_4$ and 0.01M $NbCl_5$ solutions were mixed and stirred with a magnetic ba The Nb/(Nb+P) molar ratio of the mixing solution was set to 0.0000, 0.0167 and 0.1667. The p of the mixing solution was adjusted to 10 using 1N-NaOH. 0.2M-$Ca(NO_3)_2$ was slowly droppe in the mixing solution (20ml/min) The ionic content of those starting solutions are shown in tabl 1. The pH was monitored and the reaction was terminated at pH 10.0. After the reaction, th suspension was stirred for 24h at room temperature. The precipitates were centrifuged at 3000rp for 5min and washed with distilled water. The obtained apatites were annealed at 800°C for 2 (heating rate: 5°C/min). In this study, those precipitates obtained by reaction of $Ca(NO_3)_2$ solutio and the mixing solution with different Nb/(Nb+P) molar ratio of 0.000, 0.0167 and 0.1667 ar named HAp , NbHAp-I and NbHAp-II, respectively.

Characterization of NbHAp

The NbHAps were characterized by X-ray diffraction analysis (XRD, Rigaku, Rint2000). Ca, P and Nb ions concentrations in apatites are measured by inductively coupled plasma (ICP, Hewlett-Packard, HP4500). Microstructural evaluation was performed by scanning electron microscopy (SEM) and energy dispersive X-ray spectroscopy (EDS) (JEOL, LV5800). The chemical state of Nb ions in HAp was investigated by X-ray photon spectroscopy (XPS, Shimadzu, ESCA-3200).

Osteogenesis evaluation of NHOst cultured with NbHAp

NHOst were purchased from BioWhittaker Inc.(Walkersville,MD). The NHOst were maintained in alpha minimum essential medium (αMEM, Gibco, Grand Island, NY) containing 10%-FCS in incubators at 37°C in a humidified atmosphere with 5% CO_2. All assays were performed using αMEM containing 10%-FCS supplemented with 10mM beta-glycerophosphate. NHOst cells (4×10^4 cells/well/ml) were co-cultured with 5mg of the apatites for 7days to evaluated the effects of the apatites on NHOst.

Proliferation of NHOst cells cultured with the apatites was estimated by Tetracolor One assay (Seikagaku Co., Ltd. Tokyo, Japan), which incorporates an oxidation reduction indicator based on detection of metabolic activity. After 7-days incubation, 2%-TetraColor One/αMEM solution was added to each well, followed by 2h incubation. The absorbance of the supernatant at 450nm was estimated using μQuant spectrophotometer (Bio-tek Instrument, Inc., Winooski, VT). After estimating the proliferation, the cells were washed by phosphate-buffered saline (PBS(-)), followed by addition of 1ml of 0.1M glycine buffer (pH=10.5) containing 10mM $MgCl_2$, 0.1mM $ZnCl_2$ and 4mM p-nitrophenylphosphate sodium salt. After incubating at room temperature for 5min, the absorbance at 405 nm was detected using the μQuant spectrophotometer to evaluated alkaline phosphatase (ALP) activity of the test cells.

Results and Discussion

XRD patterns of NbHAps prepared by wet chemical process are shown in Fig.1(a). Irrespective of Nb/(Nb+P) molar ratio in starting solution, the precipitates were identified as monolithic HAp.

Table1. The ionic content of starting solution and the composition of the obtained precipitates.

Samples	Ionic content of Starting Solution*, Ca	PO4	Nb	Theoretical Ca/(Nb+P)**	Nb/(Nb+P)** Theoretical	Measured***	Color of Precipitates
HAp	60.0	36.0	0.0	1.67	0.0000	-	White
NbHAp-I	60.0	35.4	0.6	1.67	0.0167	0.015	Pale yellow
NbHAp-II	60.0	30.0	6.0	1.67	0.1667	0.082	Buff yellow

*mmol, **Molar ratio, ***The precipitates were dissolved with HCl and the ionic concentration of HCl solutions were measured by ICP.

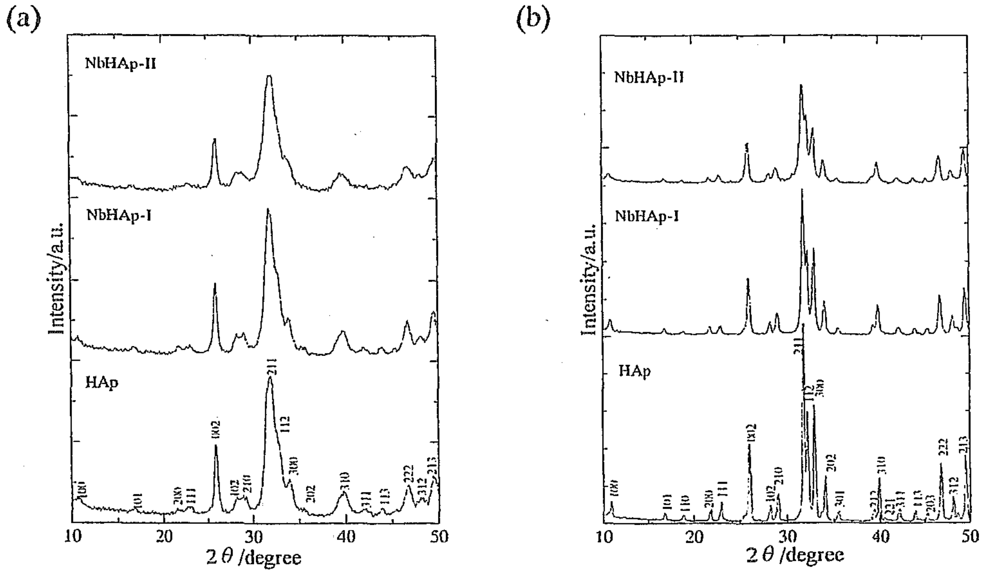

Fig.1. XRD patterns of HAp and NbHAp-I and NbHAp-II before (a) and after (b) annealing(800°C, 2h).

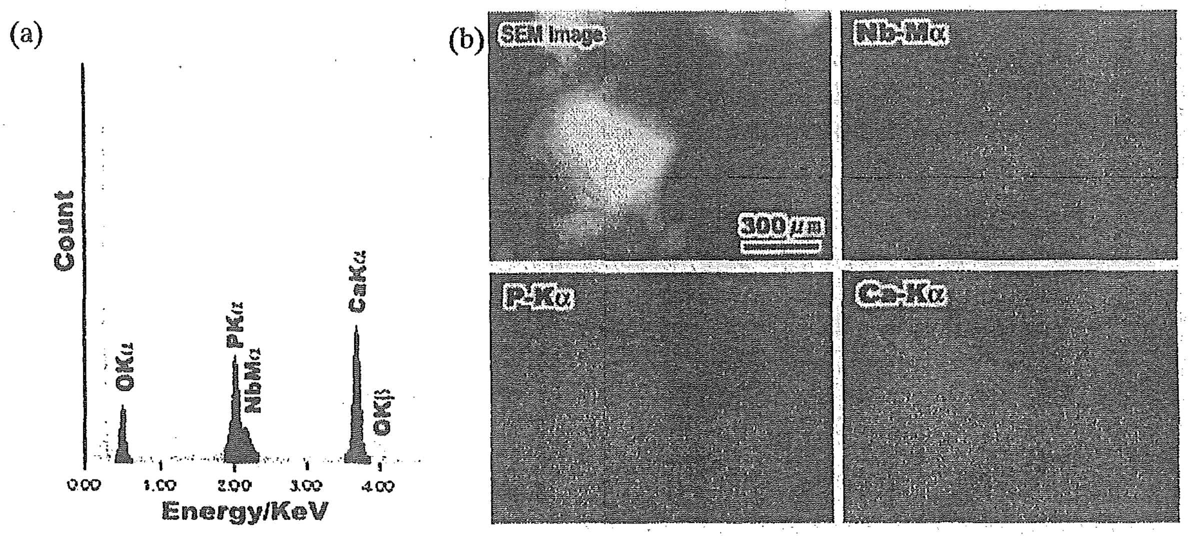

Fig.2. SEM-EDX analysis of NbHAp-II. ((a) An EDX spectrum and (b) SEM image and element mapping images of Nb, Ca and P).

As shown in Table1, the Nb/(Nb+P) molar ratio of NbHAp-I and NbHAp-II were 0.015 and 0.082, respectively. SEM observation revealed that the precipitates were present as aggregates composed of primary particles of less than 1μm in diameter.

XRD patterns of NbHAps annealed at 800°C are shown in Fig.1(b). The crystalline of the precipitates become high by the annealing and XRD patterns of all annealed NbHAps could be identified as monolithic apatitic structure. It is noted that the crystallite of the NbHAp decreased as Nb content increased. Figure 2(a) shows an EDX spectra of the whole region of SEM image in Fig.2(b). The EDX spectrum from Nb M_α was separated from P K_α line and could be observed at 2.17KeV, although the intensity of the spectra was weak. The mapping image of Nb, Ca and P ions are shown in Fig.2(b). As shown in Fig.2(b), Nb ions were present at the same site of Ca and P ions. Based on these observations, Nb ions are suggested to be uniformly distributed in the aggregates. High-resolution XPS spectrum of Nb $3d_{5/2}$ of NbHAp-II annealed at 800°C is shown in Fig.3. The peak of XPS spectra due to $3d_{5/2}$ of Nb ions from annealed NbHAp-II is at 208.3eV. Since XPS peak of $3d_{5/2}$ due to Nb^{2+} from NbO and Nb^{5+} from Nb_2O_5 appears at 203.5eV and 207.2eV, respectively, the Nb ions in NbHAp can be identified as Nb^{5+}.

These results suggest that the NbHAp has apatitic structure containing Nb ions and the Nb ions are homogenously distributed in the grain. Generally, Nb^{5+} ions in the solution is not present as Nb^{5+} but as niobiumate acid, $H_xNb_6O_{19}{}^{(8-x)-}$ ions (X=0,1,2)[4]. The PO_4 in HAp can be replaced by anionic atomic group, e.g. $CO_3{}^{2-}$, $VO_4{}^{3-}$ and $AsO_4{}^{3-}$. Therefore, it is probable that Nb ions are substituted in PO_4 site in HAp. However, measured Nb/(Nb+P) molar ratio in NbHAp-II was 0.082, despite their theoretical Nb/(Nb+P) ratio of 0.1667, suggesting that the value of the measured ratio might be the maximum amount of Nb ions in PO_4, practically.

Since Nb ions are expected to have an effect to promote the proliferation and ALP activity of osteoblastic cells, the NbHAps have a potential to promote the ALP activity of osteoblastic cells.

Figure 4 shows ALP activity of NHOst cultured with annealed NbHAps. As shown in Fig.4, NHOst cultured with the NbHAp expressed the ALP activities twice as much as that of NHOst cultured with HAp without Nb ions. It is well known that ALP is often expressed when fracture of bone is repaired *in vivo*. Furthermore, from the recent study, it has revealed that the ALP contributed to mineralization in bone formation[5]. Therefore, this enhancement in ALP activity of NHOst by NbHAp suggests that the NbHAp can promote the mineralization of bone formation.

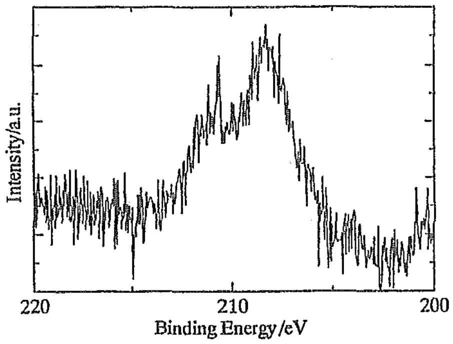

Fig.3. High-resolution XPS spectrum of Nb $3d_{5/2}$ of NbHAp-II annealed at 800°C.

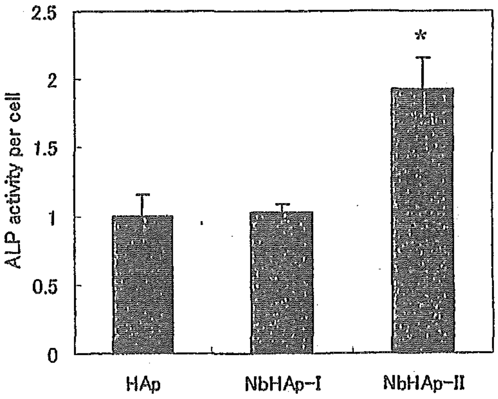

Fig.4. ALP activity of NHOst cultured with annealed NbHAp
*$p<0.05$ against HAp (without Nb ions)

Conclusion

We have succeeded to synthesize novel HAp containing Nb ions. The NbHAp would be a solid solution, which Nb ions were in PO_4 site in HAp and could enhance the ALP activity in NHOst.

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Enhancement of Differentiation and Homeostasis of Human Osteoblasts by Interaction with Hydroxyapatite in Microsphere Form

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Key words: osteoblasts, differentiation, homeostasis, hydroxyapatite, biocompatibility

Abstract. The aseptic loosening of artificial joints with associated periprosthetic bone resorption may be partly due to the suppression of osteoblast function to form new bone by wear debris derived from the joint. To assess the effect of wear debris on osteoblasts, we cultured normal human osteoblasts (NHOst) in contact with several kinds of microspheres as models of wear debris. The NHOst in contact with polystyrene, polyethylene, and alumina microspheres showed a lower differentiation level than NHOst alone as estimated from the amounts of deposited calcium. On the other hand, hydroxyapatite particles enhanced the differentiation of NHOst. In addition, sintered hydroxyapatite enhanced expression of osteocalcin mRNA and gap junctional communication of NHOst. This study suggests that polystyrene, polyethylene, and alumina microspheres have the potential to disorder not only the differentiation but also the homeostasis of NHOst in contact with them. However, hydroxyapatite enhanced the differentiation as well as the homeostasis of NHOst, even in microsphere form, suggesting its good biocompatibility as biomaterials for bone tissues.

Introduction

Biomaterials implanted into the harsh environment of the body cannot maintain their original shape, or even their desired function, resulting in undesirable side effects. One good example is the aseptic loosening of artificial joints observed in many patients who underwent a total joint replacement 5 to 25 years ago. Many researchers have reported that aseptic loosening with associated periprosthetic bone resorption is partly due to the activation of macrophages and osteoclasts by wear debris from the artificial joint [1-3], but few researches have focused on the interaction between wear debris and osteoblasts, especially normal human osteoblasts [4]. In this study, normal human osteoblasts were cultured in contact with various kinds of microspheres made from polymers or ceramics used as model wear debris, and the effects of the microspheres' characteristics and interaction conditions were discussed in regard to the proliferation, differentiation and homeostasis maintenance of the osteoblasts.

Materials and Methods

Microspheres. Monodispersed polystyrene (PS) microspheres with different diameters (0.1, 0.5, 1, 5, and 10 μm) were kindly supplied by Japan Synthetic Rubber Co., Ltd. (Tokyo, JAPAN). Low-density polyethylene (PE) microspheres were kindly provided by Sumitomo Seika chemicals Co., Ltd. (Tokyo, JAPAN). Alumina (Al_2O_3) microspheres were obtained from the Association of Powder Process Industry and Engineering. Sintered and un-sintered hydroxyapatite (HAp) microspheres (7.2 μm in diameter) were prepared and supplied by Ube Material Industries, Ltd. (Chiba, Japan). Determined by Multisizer II (Coulter Electronics Inc., Hialeah, FL), the average diameters of PE and alumina microspheres were found to be 6.4 and 5.1 μm, respectively. Sterile microspheres and microsphere-coated plates were prepared by the method previously reported [5]. The obtained microspheres and microsphere-coated plates (20 μg/well) were subjected to the assays.

Cellular Assays. Normal human osteoblasts (NHOst) were purchased from BioWhitteker Inc. (Walkersville, MD). The cells were maintained using alpha minimum essential medium (Gibco) containing 20% fetal calf serum (FCS) in incubators (37°C, 5%-CO_2-95%-air, saturated humidity).

All assays were carried out using the medium supplemented with 10mM β-glycerophosphate. NHOst ($2x10^4$ cells/well/500 μl medium) were cultured on the microsphere-coated plates for estimating the effect of the microspheres from the bottom of the cells. To estimate the effect of microspheres on cells adhered to the culture plates, the NHOst were cultured with microsphere-containing medium (20 μg/500 μl medium) after they had adhered to the collagen-coated plates. The cell number ratio of NHOst cultured with microspheres was evaluated using the alamar Blue™ assay (BioSource International, Inc., Camarillo, CA), which incorporates an oxidation-reduction indicator based on the detection of metabolic activity, according to manufacturer's instruction.

The level of alkaline phosphatase (ALP) activity of the NHOst and the amounts of calcium deposited during a 7-day incubation were evaluated to estimate differentiation level of NHOst as previously reported [6]. In addition, RT-PCR was performed to detect the expression of osteocalcin mRNA in the NHOst (primers for human osteocalcin [7]; forward 5'CATGAGAGCCCTCACA3' and reverse 5'AGAGCGACACCCTAGAC3'; product size 307-bp).

Gap junctional intercellular communication (GJIC), which is a function that plays an important role in maintaining cell and tissue homeostasis by exchanging low molecular weight molecules [8], among NHOst co-cultured with microspheres were evaluated using FRAP assay as previously reported [9].

All data were expressed as the mean value ± the standard deviation (SD) or the standard error of means (SEM) of the obtained data as indicated in all figures and tables. The Fisher-Tukey criterion was used to control for multiple comparisons and to compute the least significant difference between means.

Results and Discussion

Figure 1 shows the effect of the diameter of pre-coated polystyrene microspheres on proliferation, the ALP activity of co-cultured NHOst cells, and the amounts of deposited calcium on the NHOst. To compare the effect of the microspheres on the ALP activities and the calcium amounts for each NHOst, the obtained data were standardized based on the cell number ratio co-cultured with the microspheres. As shown in figure, suppression on ALP activity of NHOst and the amounts of deposited calcium were observed when 0.1 μm and 5 μm microspheres were co-cultured. When the microspheres were added after cell adhesion, they did not show a significant inhibitory effect on the functions of NHOst (data not shown). By pre-coating of the microspheres on the bottom of the test plates, the area they occupied became larger as their diameter became smaller. This increase in the microsphere occupied area would affect many functions of the test cells, resulting in the inhibitory effect of the 0.1μm microspheres on the function of NHOst when the same quantity of microspheres was coated. On the other hand, the suppression of ALP activity of NHOst and calcium deposition by pre-coated 5 μm PS microspheres suggests that not only the area they occupied but also their size may cause the unique inhibitory activity of the 5 μm PS microspheres. It is well known that the size of a microsphere plays an important role in phagocytosis [10], although it is unclear that there is the same size dependence on phagocytosis by the NHOst as by macrophages. In addition, our previous study suggested that even fibroblasts were likely to phagocyte microspheres of a specific

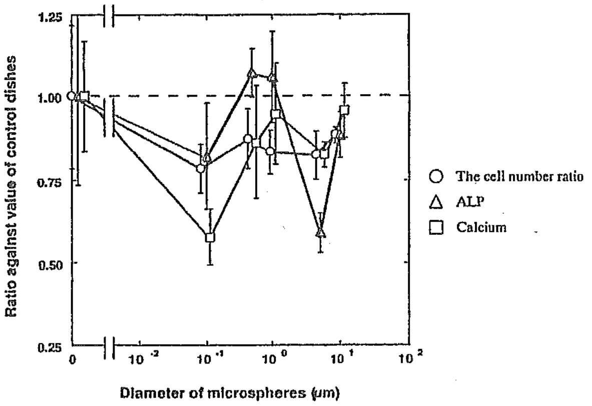

Figure 1. Effects of diameter of pre-coated PS on various functions of NHOst. Data are shown as the means±SD