

Figure 8: Radiograms of tungsten wires coiled around rod made of polymethyl methacrylate.

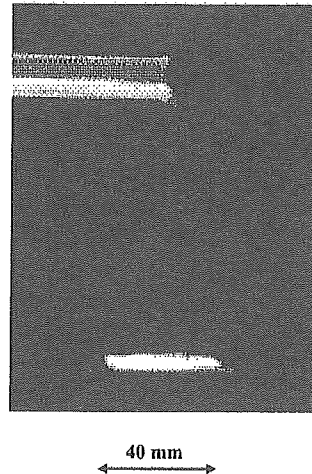


Figure 9: Radiogram of water falling into polypropylene beaker from glass test tube.

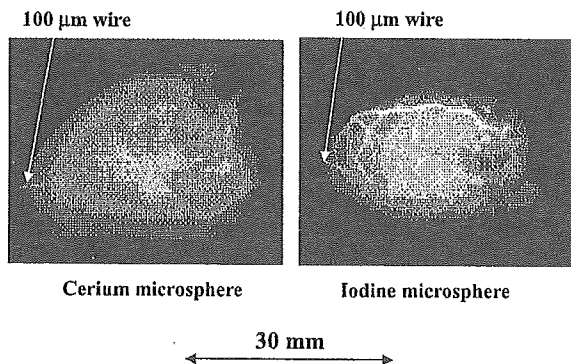


Figure 10: Angiograms of rabbit hearts using iodine and cerium microspheres.

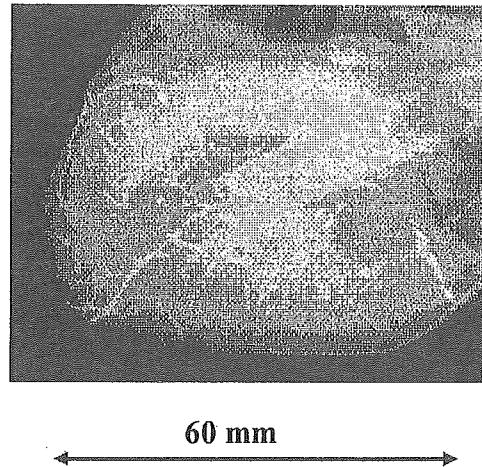


Fig. 11 Angiograms of extracted heart of dog.

## 6. DISCUSSION

Concerning the spectrum measurement, we obtained fairly clean cerium  $K\alpha$  and  $K\beta$  lines. Therefore, we are very interested in the measurement the characteristic rays from nickel, copper, molybdenum, silver, and tungsten targets; the target element should be selected corresponding to the radiographic objectives.

In this research, the generator produced instantaneous number of K photons was approximately  $5 \times 10^8$  photons/cm<sup>2</sup> per pulse at 1.0 m from the source. Subsequently, the intensity can be increased by increasing the electrostatic energy in condenser, and monochromatic  $K\alpha$  lines are produced using a barium oxide filter with a barium K-edge of 37.4 keV.

Using this flash x-ray generator, as high output voltages can be produced using cables, high-photon-energy K-series characteristic x rays can be produced by increasing the atomic number of the target element. With recent advances in angiography using MRI, if the density of gadolinium-based contrast media increases, enhanced K-edge angiography

utilizing monochromatic x-ray generators, which produce  $K\alpha$  rays from ytterbium, tantalum, and tungsten targets, will be a useful technique to decrease the absorbed dose during angiography.

## ACKNOWLEDGMENT

This work was supported by Grants-in-Aid for Scientific Research (13470154, 13877114, and 16591222) and Advanced Medical Scientific Research from MECSSST, Health and Labor Sciences Research Grants(RAMT-nano-001, RHGTEFB-genome-005 and RHGTEFB-saisei-003), Grants from Keiryō Research Foundation, The Promotion and Mutual Aid Corporation for Private Schools of Japan, Japan Science and Technology Agency (JST), and New Energy and Industrial Technology Development Organization (NEDO, Industrial Technology Research Grant Program in '03).

## REFERENCES

1. H. Mori, K. Hyodo, E. Tanaka, M. U. Mohammed, A. Yamakawa, Y. Shinozaki, H. Nakazawa, Y. Tanaka, T. Sekka, Y. Iwata, S. Honda, K. Umetani, H. Ueki, T. Yokoyama, K. Tanioka, M. Kubota, H. Hosaka, N. Ishizawa and M. Ando, "Small-vessel radiography in situ with monochromatic synchrotron radiation," *Radiology*, **201**, 173-177, 1996.
2. K. Hyodo, M. Ando, Y. Oku, S. Yamamoto, T. Takeda, Y. Itai, S. Ohtsuka, Y. Sugishita and J. Tada, "Development of a two-dimensional imaging system for clinical applications of intravenous coronary angiography using intense synchrotron radiation produced by a multipole wiggler," *J. Synchrotron Rad.*, **5**, 1123-1126, 1998.
3. A. Momose, T. Takeda, Y. Itai and K. Hirano, "Phase-contrast x-ray computed tomography for observing biological soft tissues," *Nature Medicine*, **2**, 473-475, 1996.
4. M. Ando, A. Maksimenko, H. Sugiyama, W. Pattanasiriwisawa, K. Hyodo and C. Uyama, "A simple x-ray dark- and bright- field imaging using achromatic Laue optics," *Jpn. J. Appl. Phys.*, **41**, L1016-L1018, 2002.
5. A. Ishisaka, H. Ohara and C. Honda, "A new method of analyzing edge effect in phase contrast imaging with incoherent x-rays," *Opt. Rev.*, **7**, 566-572, 2000.
6. E. Sato, E. Tanaka, H. Mori, T. Kawai, T. Ichimaru, S. Sato, K. Takayama and H. Ido, "Demonstration of enhanced K-edge angiography using a cerium target x-ray generator," *Med. Phys.*, **31**, 3017-3021, 2004.
7. R. Germer, "X-ray flash techniques," *J. Phys. E: Sci. Instrum.*, **12**, 336-350, 1979.
8. E. Sato, S. Kimura, S. Kawasaki, H. Isobe, K. Takahashi, Y. Tamakawa and T. Yanagisawa, "Repetitive flash x-ray generator utilizing a simple diode with a new type of energy-selective function," *Rev. Sci. Instrum.*, **61**, 2343-2348, 1990.
9. A. Shikoda, E. Sato, M. Sagae, T. Oizumi, Y. Tamakawa and T. Yanagisawa, "Repetitive flash x-ray generator having a high-durability diode driven by a two-cable-type line pulser," *Rev. Sci. Instrum.*, **65**, 850-856, 1994.
10. E. Sato, K. Takahashi, M. Sagae, S. Kimura, T. Oizumi, Y. Hayasi, Y. Tamakawa and T. Yanagisawa, "Sub-kilohertz flash x-ray generator utilizing a glass-enclosed cold-cathode triode," *Med. & Biol. Eng. & Comput.*, **32**, 289-294, 1994.
11. K. Takahashi, E. Sato, M. Sagae, T. Oizumi, Y. Tamakawa and T. Yanagisawa, "Fundamental study on a long-duration flash x-ray generator with a surface-discharge triode," *Jpn. J. Appl. Phys.*, **33**, 4146-4151, 1994.
12. E. Sato, M. Sagae, E. Tanaka, Y. Hayasi, R. Germer, H. Mori, T. Kawai, T. Ichimaru, S. Sato, K. Takayama and H. Ido: Quasi-monochromatic flash x-ray generator utilizing a disk-cathode molybdenum tube, *Jpn. J. Appl. Phys.*, **43**, 7324-7328, 2004.
13. E. Sato, R. Germer, Y. Hayasi, K. Murakami, Y. Koorikawa, E. Tanaka, H. Mori, T. Kawai, T. Ichimaru, F. Obata, K. Takahashi, S. Sato, K. Takayama and H. Ido, H.: Weakly ionized cerium plasma radiography, *SPIE*, **5210**, 12-21, 2003.
14. E. Sato, Y. Hayasi, R. Germer, E. Tanaka, H. Mori, T. Kawai, H. Obara, T. Ichimaru, K. Takayama and H. Ido, "Intense characteristic x-ray irradiation from weakly ionized linear plasma and applications," *Jpn. J. Med. Imag. Inform. Sci.*, **20**, 148-155, 2003.
15. E. Sato, Y. Hayasi, R. Germer, E. Tanaka, H. Mori, T. Kawai, H. Obara, T. Ichimaru, K. Takayama and H. Ido, "Irradiation of intense characteristic x-rays from weakly ionized linear molybdenum plasma," *Jpn. J. Med. Phys.*, **23**, 123-131, 2003.
16. E. Sato, Y. Hayasi, R. Germer, E. Tanaka, H. Mori, T. Kawai, T. Ichimaru, K. Takayama and H. Ido, "Quasi-monochromatic flash x-ray generator utilizing weakly ionized linear copper plasma," *Rev. Sci. Instrum.*, **74**, 5236-5240, 2003.
17. E. Sato, R. Germer, Y. Hayasi, Y. Koorikawa, K. Murakami, E. Tanaka, H. Mori, T. Kawai, T. Ichimaru, F. Obata, K. Takahashi, S. Sato, K. Takayama and H. Ido: Weakly ionized plasma flash x-ray generator and its distinctive characteristics. *SPIE*, **5196**, 383-392, 2003.

18. E. Sato, Y. Hayasi, R. Germer, E. Tanaka, H. Mori, T. Kawai, T. Ichimaru, S. Sato, K. Takayama and H. Ido, "Sharp characteristic x-ray irradiation from weakly ionized linear plasma," *J. Electron Spectrosc. Related Phenom.*, **137-140**, 713-720, 2004.

19. E. Sato, K. Sato and Y. Tamakawa, "Film-less computed radiography system for high-speed imaging," *Ann. Rep. Iwate Med. Univ. Sch. Lib. Arts and Sci.*, **35**, 13-23, 2000.

\*dresato@iwate-med.ac.jp; phone, phone +81-19-651-5111; fax +81-19-654-9282

## Weakly ionized linear plasma x-ray generator with molybdenum-target triode

Eiichi Sato<sup>a</sup>, Yasuomi Hayashi<sup>a</sup>, Rudolf Germer<sup>b</sup>, Etsuro Tanaka<sup>c</sup>, Hidezo Mori<sup>d</sup>, Toshiaki Kawai<sup>e</sup>,  
Toshio Ichimaru<sup>f</sup>, Shigehiro Sato<sup>g</sup>, Hidenori Ojima<sup>h</sup>, Kazuyoshi Takayama<sup>h</sup> and Hideaki Ido<sup>i</sup>

<sup>a</sup>Department of Physics, Iwate Medical University, 3-16-1 Honchodori, Morioka 020-0015, Japan

<sup>b</sup>ITP, FHTW FB1 and TU-Berlin, Blankenhainer Str. 9, D 12249 Berlin, Germany

<sup>c</sup>Department of Nutritional Science, Faculty of Applied Bio-science, Tokyo University of  
Agriculture, 1-1-1 Sakuragaoka, Setagaya-ku 156-8502, Japan

<sup>d</sup>Department of Cardiac Physiology, National Cardiovascular Center Research Institute, 5-7-1  
Fujishirodai, Suita, Osaka 565-8565 Japan

<sup>e</sup>Electron Tube Division #2, Hamamatsu Photonics K. K., 314-5 Shimokanzo, Toyooka Village,  
Iwata-gun 438-0193, Japan

<sup>f</sup>Department of Radiological Technology, School of Health Sciences, Hirosaki University, 66-1  
Honcho, Hirosaki 036-8564, Japan

<sup>g</sup>Department of Microbiology, School of Medicine, Iwate Medical University, 19-1 Uchimaru,  
Morioka 020-8505, Japan

<sup>h</sup>Shock Wave Research Center, Institute of Fluid Science, Tohoku University, 2-1-1 Katahira,  
Sendai 980-8577, Japan

<sup>i</sup>Department of Applied Physics and Informatics, Faculty of Engineering, Tohoku Gakuin University,  
1-13-1 Chuo, Tagajo 985-8537, Japan,

### ABSTRACT

In the plasma flash x-ray generator, a 200 nF condenser is charged up to 50 kV by a power supply, and flash x rays are produced by the discharging. The x-ray tube is a demountable triode with a trigger electrode, and the turbomolecular pump evacuates air from the tube with a pressure of approximately 1 mPa. Target evaporation leads to the formation of weakly ionized linear plasma, consisting of molybdenum ions and electrons, around the fine target, and intense characteristic x rays are produced. At a charging voltage of 50 kV, the maximum tube voltage was almost equal to the charging voltage of the main condenser, and the peak current was about 16 kA. When the charging voltage was increased, the linear plasma formed, and the K-series characteristic x-ray intensities increased. The K lines were quite sharp and intense. The x-ray pulse widths were approximately 600 ns, and the time-integrated x-ray intensity had a value of approximately 65  $\mu\text{C}/\text{kg}$  at 1.0 m from the x-ray source with a charging voltage of 50 kV.

**Keywords:** flash x-ray, weakly ionized linear plasma, molybdenum characteristic x rays, quasi-monochromatic x rays, x-ray resonance

### 1. INTRODUCTION

In conjunction with monochromators, synchrotrons produce monochromatic parallel beams, which are fairly similar to monochromatic parallel laser beams, and the beams have been applied to enhanced K-edge angiography,<sup>1,2</sup> phase imaging,<sup>3,4</sup> and crystallography. Therefore, the production of coherent hard x-ray lasers for various research projects, including biomedical applications, has long been wished for.

Recently, soft x-ray lasers<sup>5-7</sup> have been produced by a gas-discharge capillary, and the laser pulse energy substantially increased in proportion to the capillary length. These kinds of fast discharges can generate hot and dense plasma columns with aspect ratios approaching 1000:1. However, it is difficult to increase the laser photon energy to 10 keV or beyond. Because there are no x-ray resonators in the high-photon-energy region, new methods for increasing coherence will be desired in the future.

To apply flash x-ray generators to biomedicine, several different generators<sup>8-11</sup> have been developed, and plasma x-ray generators<sup>12-16</sup> are useful for producing clean characteristic x rays in the low-photon-energy region of less than 20 keV. By forming weakly ionized linear plasma using rod targets, we confirmed irradiation of intense K-series characteristic x rays from the axial direction of the linear plasmas of nickel, copper, and molybdenum, since the bremsstrahlung x rays are absorbed effectively by the linear plasma; monochromatic clean K $\alpha$  rays were produced using K-edge filters. Subsequently, since high-photon-energy bremsstrahlung x rays are not absorbed effectively by the linear plasma due to attenuation coefficients, high-photon-energy quasi-monochromatic x-ray generators<sup>17</sup> for producing characteristic x rays of molybdenum, silver, cerium, tantalum, and tungsten have been developed utilizing the angle dependence of bremsstrahlung x-ray intensity distribution.

In this paper, we describe a recent plasma flash x-ray generator utilizing a rod-target radiation tube, used to perform a preliminary experiment for generating intense and sharp quasi-monochromatic x rays under resonating conditions by forming a linear molybdenum plasma cloud around a fine target.

## 2. GENERATOR

### 2.1 High-voltage circuit

Figure 1 shows a block diagram of a high-intensity plasma flash x-ray generator. The generator consists of the following essential components: a high-voltage power supply, a high-voltage condenser with a capacity of approximately 200 nF, a turbomolecular pump, a krytron pulse generator as a trigger device, and a flash x-ray tube. In this generator, a low-impedance transmission line is employed in order to increase maximum tube current. The high-voltage main condenser is charged up to 50 kV by the power supply, and electric charges in the condenser are discharged to the tube after triggering the cathode electrode with the trigger device. The plasma flash x-rays are then produced.

### 2.2 X-ray tube

The x-ray tube is a demountable cold-cathode triode that is connected to the turbomolecular pump with a pressure of approximately 1 mPa (Fig. 2). This tube consists of the following major parts: a pipe-shaped graphite cathode with a bore diameter of 10.0 mm, a trigger electrode made from copper wire, a stainless-steel vacuum chamber, a nylon insulator, a polyethylene terephthalate (Mylar) x-ray window 0.25 mm in thickness, and a rod-shaped molybdenum target 3.0 mm in diameter. The distance between the target and cathode electrodes is approximately 20 mm, and the trigger electrode is set in the cathode electrode. As electron beams from the cathode electrode are roughly converged to the target by the electric field in the tube, evaporation leads to the formation of weakly ionized linear plasma, consisting of molybdenum ions and electrons, around the fine target.

### 2.3 Principle of characteristic x-ray irradiation

In weakly ionized linear plasma, bremsstrahlung spectra with photon energies of higher than the K-absorption edge are effectively absorbed and are converted into fluorescent x rays. The plasma then transmits the fluorescent rays easily, and bremsstrahlung rays with energies of lower than the K-edge are also absorbed by the plasma. In addition, because bremsstrahlung rays are not emitted in the direction opposite to electron acceleration, intense characteristic x rays are generated from the plasma-axial direction.

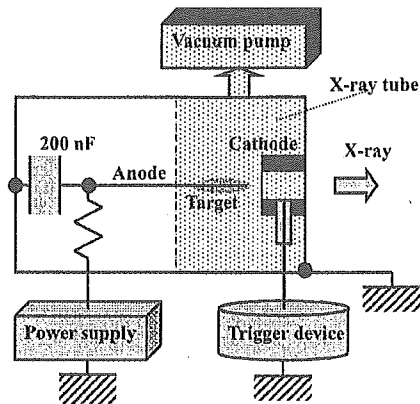


Figure 1: Block diagram of high-intensity plasma flash x-ray generator.

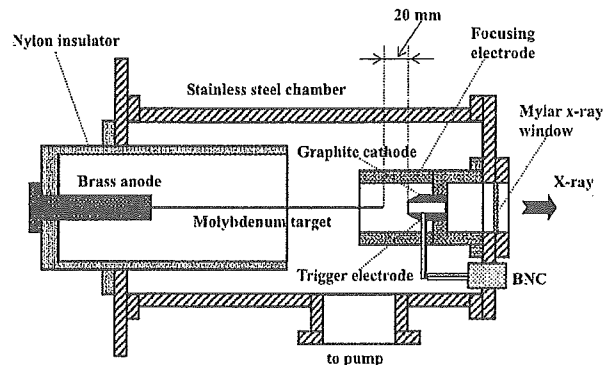


Figure 2: Schematic drawing of flash x-ray tube with rod target.

### 3. CHARACTERISTICS

#### 3.1 Tube voltage and current

Tube voltage and current were measured by a high-voltage divider with an input impedance of 1 G $\Omega$  and a current transformer, respectively. Figure 3 shows the time relation between the tube voltage and current. At the indicated charging voltages, they roughly displayed damped oscillations. When the charging voltage was increased, both the maximum tube voltage and current increased. At a charging voltage of 50 kV, the maximum tube voltage was almost equal to the charging voltage of the main condenser, and the maximum tube current was approximately 16 kA.

#### 3.2 X-ray output

X-ray output pulse was detected using a combination of a plastic scintillator and a photomultiplier (Fig. 4). The x-ray pulse height substantially increased with corresponding increases in the charging voltage. The x-ray pulse widths were about 600 ns, and the time-integrated x-ray intensity measured by a thermoluminescence dosimeter (Kyokko TLD Reader 1500 having MSO-S elements without energy compensation) had a value of approximately 65  $\mu\text{C}/\text{kg}$  at 1.0 m from the x-ray source with a charging voltage of 50 kV.

#### 3.3 X-ray source

In order to roughly observe images of the plasma x-ray source in the detector plane, we employed a pinhole camera with a hole diameter of 100  $\mu\text{m}$  and an x-ray film (Polaroid XR-7) (Fig. 5). When the charging voltage was increased, the plasma x-ray source grew, and both spot dimension and intensity increased. Because the x-ray intensity is the highest at the center of the spot, both the dimension and intensity decreased according to both increases in the thickness of a filter for absorbing x rays and decreases in the pinhole diameter.

#### 3.4 X-ray spectra

X-ray spectra from the plasma source were measured by a transmission-type spectrometer with a lithium fluoride curved crystal 0.5 mm in thickness. The spectra were taken by a computed radiography (CR) system<sup>18</sup> with a wide dynamic range, and relative x-ray intensity was calculated from Dicom digital data. Figure 6 shows measured spectra from the molybdenum target. In fact, we observed quite sharp lines of K-series characteristic x rays, and bremsstrahlung rays were detected slightly at a high charging voltage of approximately 50 kV. The characteristic x-ray intensity substantially increased with corresponding increases in the charging voltage. We found high-intensity lines with a photon energy of  $0.5E_{\alpha}$  corresponding to  $K\alpha$  lines with an average photon energy of  $E_{\alpha}$ . Although lines of  $0.5E_{\beta}$ , corresponding to  $K\beta$  lines with an average photon energy of  $E_{\beta}$ , were also detected, hardly any bremsstrahlung x rays were detected at all.

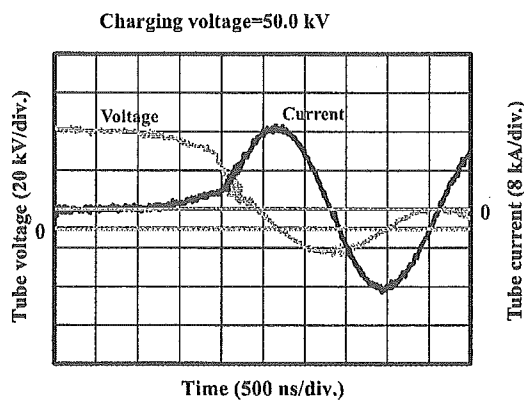
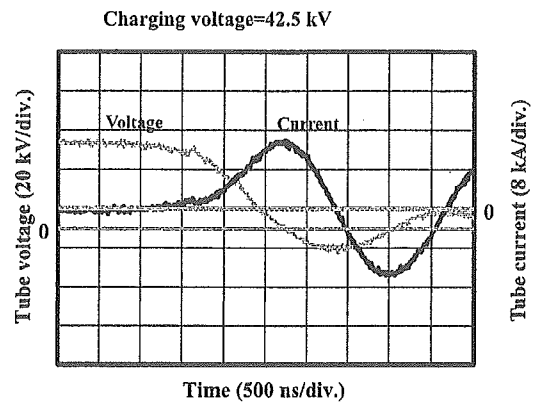
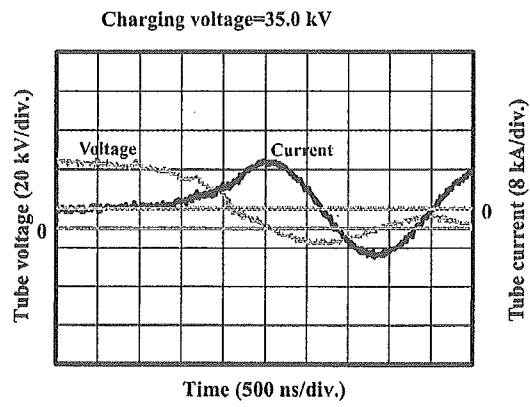


Figure 3: Tube voltages and currents with changing charging voltage.

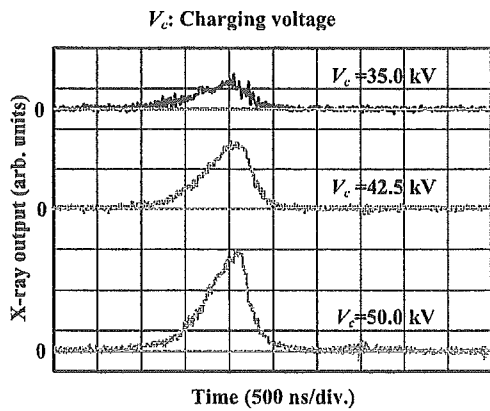


Figure 4: X-ray outputs at indicated conditions.

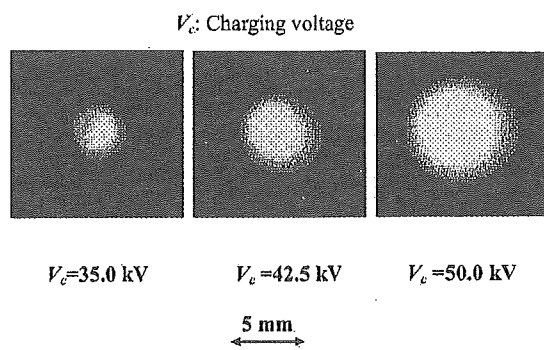


Figure 5: Images of plasma x-ray source.

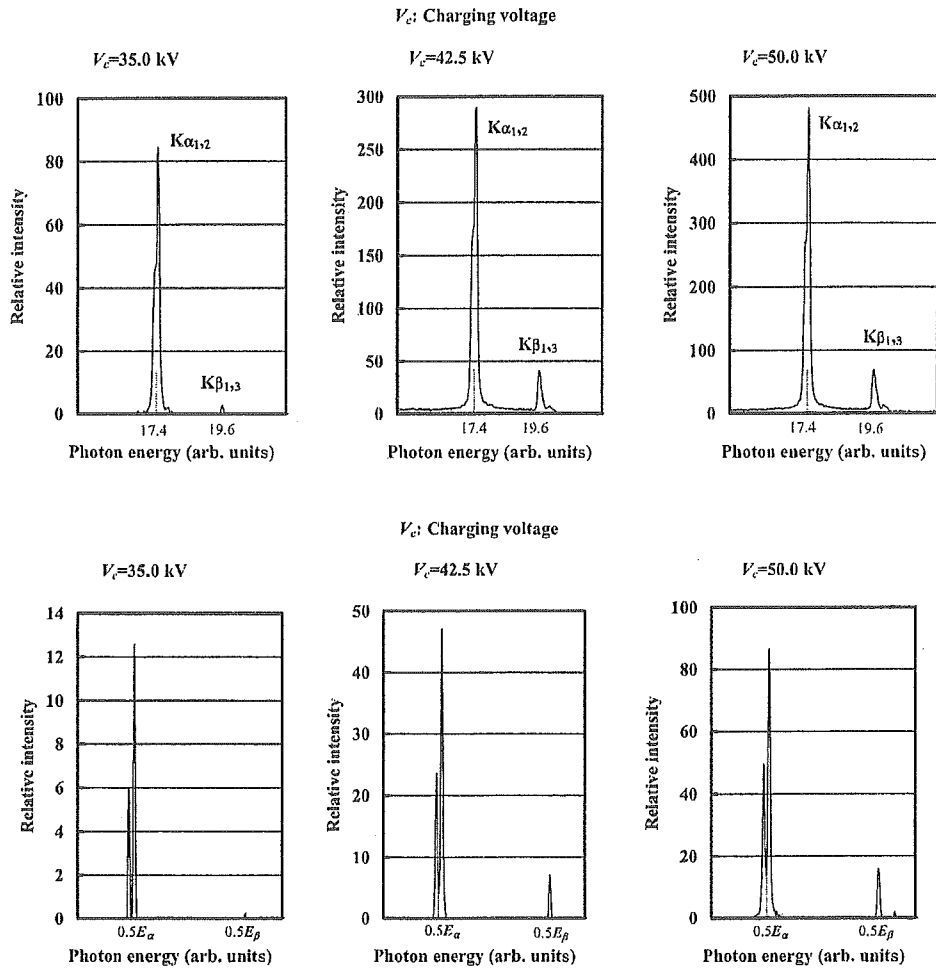


Figure 6: X-ray spectra from molybdenum plasma.

#### 4. RADIOGRAPHY

The plasma radiography was performed by the CR system (Konica Regius 150) without using a monochromatic filter, and the distance between the x-ray source and imaging plate was 1.2 m.

Firstly, rough measurements of image resolution were made using wires. Figure 7 shows radiograms of tungsten wires coiled around a pipe made of polymethyl methacrylate with a tube voltage of 50 kV. Although the image contrast decreased somewhat with decreases in the wire diameter, due to blurring of the image caused by the sampling pitch of 87.5  $\mu\text{m}$ , a 50- $\mu\text{m}$ -diameter wire could be observed.

The image of water falling into a polypropylene beaker from a plastic test tube is shown in Fig. 8. This image was taken with a charging voltage of 50 kV, with the slight addition of an iodine-based contrast medium. Because the x-ray duration was about 1  $\mu\text{s}$ , the stop-motion image of water could be obtained.

Figure 9 shows a radiogram of a vertebra with a charging voltage of 45 kV, and fine structures in the vertebra were observed. Figure 10 shows an angiogram of a rabbit heart with a charging voltage of 50 kV. In angiography, iodine-based microspheres of 15  $\mu\text{m}$  in diameter were used, and fine blood vessels of about 100  $\mu\text{m}$  were visible.



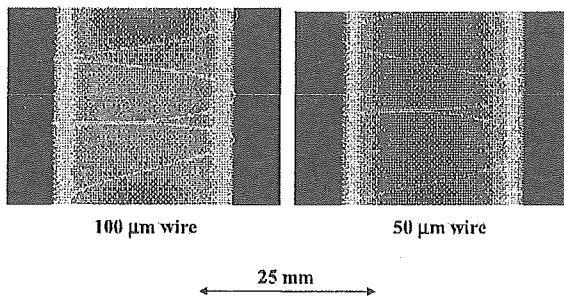


Figure 7: Radiograms of tungsten wires in PMMA rod.

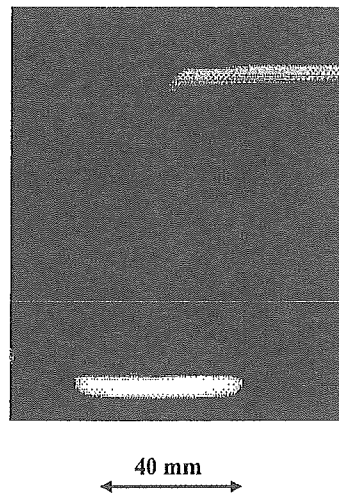


Figure 8: Radiogram of water falling into polypropylene beaker from glass test tube.

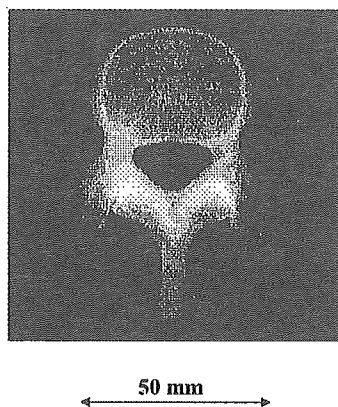


Figure 9: Radiogram of vertebra.

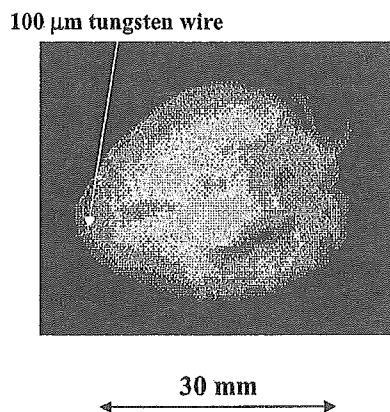


Figure 10: Angiograms of rabbit heart.

## 5. DISCUSSION

Regarding the spectrum measurement, although we obtained quite intense and sharp K-series lines by forming a linear plasma x-ray source, bremsstrahlung x rays were observed slightly at charging voltages of approximately 50 kV. In addition, we observed fairly intense and clean lines with photon energies of  $0.5E_{\alpha}$ . Because bremsstrahlung x rays were hardly observed, we thought that the  $0.5E_{\alpha}$  and  $0.5E_{\beta}$  lines were not characteristic x rays reflected by the high order diffraction and were produced by the hard x-ray resonance (oscillation) without using a resonator (Figs. 11 and 12). If we assume that x-ray intensities of the two lines and bremsstrahlung rays are signal and noise, respectively, the signal to noise ratio is higher than 1000:1, and this value is almost equal to those of soft x-ray lasers produced by the gas-discharge capillary.

In this research, we obtained sufficient x-ray intensity per pulse for CR radiography without using a monochromatic filter, and the generator produced number of characteristic photons was approximately  $1 \times 10^9$  photons/cm<sup>2</sup> at 1.0 m per pulse. In addition, since the photon energy of characteristic x rays can be controlled by changing target elements, various quasi-monochromatic high-speed radiographies, such as high-contrast micro angiography and dual-energy subtraction radiography, will be possible.

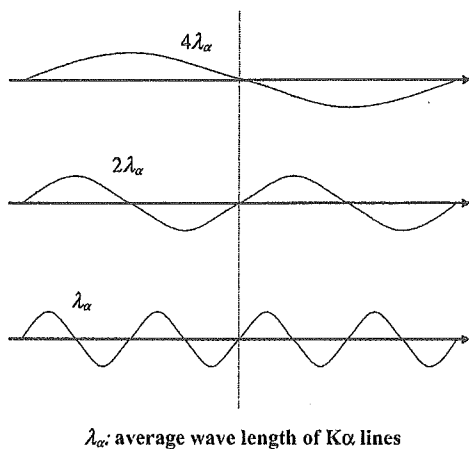


Figure 11: Assumption of hard x-ray resonance without using resonator.

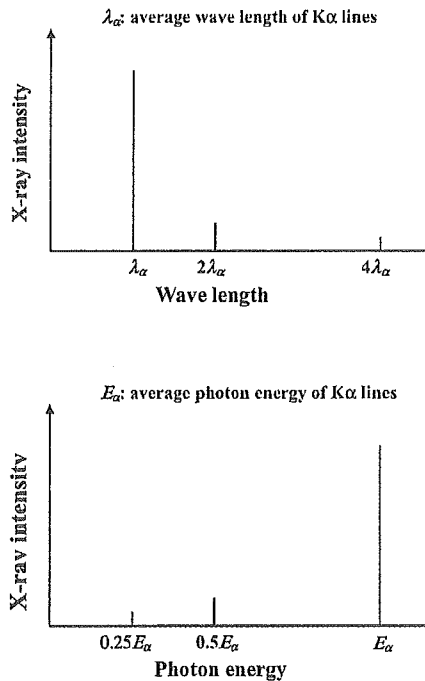


Figure 12: Estimated x-ray spectra under resonance.

#### ACKNOWLEDGMENT

This work was supported by Grants-in-Aid for Scientific Research (13470154, 13877114, and 16591222) and Advanced Medical Scientific Research from MECSST, Health and Labor Sciences Research Grants(RAMT-nano-001, RHGTEFB-genome-005 and RHGTEFB-saisei-003), Grants from Keiryō Research Foundation, The Promotion and Mutual Aid Corporation for Private Schools of Japan, Japan Science and Technology Agency (JST), and New Energy and Industrial Technology Development Organization (NEDO, Industrial Technology Research Grant Program in '03).

#### REFERENCES

1. H. Mori, K. Hyodo, E. Tanaka, M. U. Mohammed, A. Yamakawa, Y. Shinozaki, H. Nakazawa, Y. Tanaka, T. Sekka, Y. Iwata, S. Honda, K. Umetani, H. Ueki, T. Yokoyama, K. Tanioka, M. Kubota, H. Hosaka, N. Ishizawa and M. Ando, "Small-vessel radiography in situ with monochromatic synchrotron radiation," *Radiology*, **201**, 173-177, 1996.
2. K. Hyodo, M. Ando, Y. Oku, S. Yamamoto, T. Takeda, Y. Itai, S. Ohtsuka, Y. Sugishita and J. Tada, "Development of a two-dimensional imaging system for clinical applications of intravenous coronary angiography using intense synchrotron radiation produced by a multipole wiggler," *J. Synchrotron Rad.*, **5**, 1123-1126, 1998.
3. A. Momose, T. Takeda, Y. Itai and K. Hirano, "Phase-contrast x-ray computed tomography for observing biological soft tissues," *Nature Medicine*, **2**, 473-475, 1996.
4. M. Ando, A. Maksimenko, H. Sugiyama, W. Pattanasiriwisawa, K. Hyodo and C. Uyama, "A simple x-ray dark- and bright- field imaging using achromatic Laue optics," *Jpn. J. Appl. Phys.*, **41**, L1016-L1018, 2002.
5. J.J. Rocca, V. Shlyaptev, F.G. Tomasel, O.D. Cortazar, D. Hartshorn and J.L.A. Chilla, "Demonstration of a discharge pumped table-top soft x-ray laser," *Phys. Rev. Lett.*, **73**, 2192-2195, 1994.
6. J.J.G. Rocca, J.L.A. Chilla, S. Sakadzic, A. Rahman, J. Filevich, E. Jankowska, E.C. Hammarsten, B.M. Luther, H.C. Kapteyn, M. Murnane and V.N. Shlyapsev, "Advances in capillary discharge soft x-ray laser research," *SPIE*, **4505**, 1-6,

2001.

7. S. Le Pape, Ph. Zeitoun, J.J.G. Rocca, A. Carillon, P. Dhez, M. Francois, S. Hubert, M. Idir and D. Ros, "Characterisation of an x-ray laser beam," *SPIE*, **4505**, 23-34, 2001.

8. E. Sato, S. Kimura, S. Kawasaki, H. Isobe, K. Takahashi, Y. Tamakawa and T. Yanagisawa, "Repetitive flash x-ray generator utilizing a simple diode with a new type of energy-selective function," *Rev. Sci. Instrum.*, **61**, 2343-2348, 1990.

9. A. Shikoda, E. Sato, M. Sagae, T. Oizumi, Y. Tamakawa and T. Yanagisawa, "Repetitive flash x-ray generator having a high-durability diode driven by a two-cable-type line pulser," *Rev. Sci. Instrum.*, **65**, 850-856, 1994.

10. E. Sato, K. Takahashi, M. Sagae, S. Kimura, T. Oizumi, Y. Hayasi, Y. Tamakawa and T. Yanagisawa, "Sub-kilohertz flash x-ray generator utilizing a glass-enclosed cold-cathode triode," *Med. & Biol. Eng. & Comput.*, **32**, 289-294, 1994.

11. K. Takahashi, E. Sato, M. Sagae, T. Oizumi, Y. Tamakawa and T. Yanagisawa, "Fundamental study on a long-duration flash x-ray generator with a surface-discharge triode," *Jpn. J. Appl. Phys.*, **33**, 4146-4151, 1994.

12. E. Sato, Y. Hayasi, R. Germer, E. Tanaka, H. Mori, T. Kawai, H. Obara, T. Ichimaru, K. Takayama and H. Ido, "Intense characteristic x-ray irradiation from weakly ionized linear plasma and applications," *Jpn. J. Med. Imag. Inform. Sci.*, **20**, 148-155, 2003.

13. E. Sato, Y. Hayasi, R. Germer, E. Tanaka, H. Mori, T. Kawai, H. Obara, T. Ichimaru, K. Takayama and H. Ido, "Irradiation of intense characteristic x-rays from weakly ionized linear molybdenum plasma," *Jpn. J. Med. Phys.*, **23**, 123-131, 2003.

14. E. Sato, Y. Hayasi, R. Germer, E. Tanaka, H. Mori, T. Kawai, T. Ichimaru, K. Takayama and H. Ido, "Quasi-monochromatic flash x-ray generator utilizing weakly ionized linear copper plasma," *Rev. Sci. Instrum.*, **74**, 5236-5240, 2003.

15. E. Sato, R. Germer, Y. Hayasi, Y. Koorikawa, K. Murakami, E. Tanaka, H. Mori, T. Kawai, T. Ichimaru, F. Obata, K. Takahashi, S. Sato, K. Takayama and H. Ido: Weakly ionized plasma flash x-ray generator and its distinctive characteristics. *SPIE*, **5196**, 383-392, 2003.

16. E. Sato, Y. Hayasi, R. Germer, E. Tanaka, H. Mori, T. Kawai, T. Ichimaru, S. Sato, K. Takayama and H. Ido, "Sharp characteristic x-ray irradiation from weakly ionized linear plasma," *J. Electron Spectrosc. Related Phenom.*, **137-140**, 713-720, 2004.

17. E. Sato, M. Sagae, E. Tanaka, Y. Hayasi, R. Germer, H. Mori, T. Kawai, T. Ichimaru, S. Sato, K. Takayama and H. Ido: Quasi-monochromatic flash x-ray generator utilizing a disk-cathode molybdenum tube, *Jpn. J. Appl. Phys.*, **43**, 7324-7328, 2004.

18. E. Sato, K. Sato and Y. Tamakawa, "Film-less computed radiography system for high-speed imaging," *Ann. Rep. Iwate Med. Univ. Sch. Lib. Arts and Sci.*, **35**, 13-23, 2000.

\*dresato@iwate-med.ac.jp; phone, phone +81-19-651-5111; fax +81-19-654-9282

# Monochromatic flash x-ray generator utilizing copper-target diode

Eiichi Sato<sup>\*a</sup>, Michiaki Sagae<sup>a</sup>, Makoto Komatsu<sup>a</sup>, Rudolf Germer<sup>b</sup>, Etsuro Tanaka<sup>c</sup>, Hidezo Mori<sup>d</sup>,  
Toshiaki Kawai<sup>e</sup>, Toshio Ichimaru<sup>f</sup>, Shigehiro Sato<sup>g</sup>, Hidenori Ojima<sup>h</sup>,  
Kazuyoshi Takayama<sup>h</sup> and Hideaki Ido<sup>i</sup>

<sup>a</sup> Department of Physics, Iwate Medical University, 3-16-1 Honchodori, Morioka 020-0015, Japan

<sup>b</sup> ITP, FHTW FB1 and TU-Berlin, Blankenhainer Str. 9, D 12249 Berlin, Germany

<sup>c</sup> Department of Nutritional Science, Faculty of Applied Bio-science, Tokyo University of  
Agriculture, 1-1-1 Sakuragaoka, Setagaya-ku 156-8502, Japan

<sup>d</sup> Department of Cardiac Physiology, National Cardiovascular Center Research Institute, 5-7-1  
Fujishirodai, Suita, Osaka 565-8565 Japan

<sup>e</sup> Electron Tube Division #2, Hamamatsu Photonics K. K., 314-5 Shimokanzo, Toyooka Village,  
Iwata-gun 438-0193, Japan

<sup>f</sup> Department of Radiological Technology, School of Health Sciences, Hirosaki University, 66-1  
Honcho, Hirosaki 036-8564, Japan

<sup>g</sup> Department of Microbiology, School of Medicine, Iwate Medical University, 19-1 Uchimaru,  
Morioka 020-8505, Japan

<sup>h</sup> Shock Wave Research Center, Institute of Fluid Science, Tohoku University, 2-1-1 Katahira,  
Sendai 980-8577, Japan

<sup>i</sup> Department of Applied Physics and Informatics, Faculty of Engineering, Tohoku Gakuin University,  
1-13-1 Chuo, Tagajo 985-8537, Japan

## ABSTRACT

High-voltage condensers in a polarity-inversion two-stage Marx surge generator are charged from  $-50$  to  $-70$  kV using a power supply, and the electric charges in the condensers are discharged to an x-ray tube after closing the gap switches in the surge generator using a trigger device. The x-ray tube is a demountable diode, and the turbomolecular pump evacuates air from the tube with a pressure of approximately 1 mPa. Clean copper  $K\alpha$  lines are produced using a 10- $\mu\text{m}$ -thick nickel filter, since the tube utilizes a disk cathode and a rod target, and bremsstrahlung rays are not emitted in the opposite direction to that of electron acceleration. The peak tube voltage increased with increasing charging voltage. At a charging voltage of  $-70$  kV, the peak tube voltage and current were 140 kV and 0.8 kA, respectively. The pulse widths were approximately 30 ns, and the maximum dimension of the x-ray source was 3.0 mm in diameter. The number of generator-produced  $K\alpha$  photons was approximately  $2.5 \times 10^6$  photons/cm<sup>2</sup> at 0.5 m per pulse.

**Keywords:** flash x-ray, characteristic x rays, bremsstrahlung x-ray distribution, copper  $K\alpha$  lines, monochromatic radiography

## 1. INTRODUCTION

Flash radiography<sup>1</sup> is a major technique that uses high-voltage vacuum discharges to produce short x-ray pulses of less than 1  $\mu\text{s}$ . Basically, although there are several different types of generators, the generator with a multistage Marx surge generator in conjunction with a cold-cathode x-ray tube is popular.<sup>1,2</sup> To apply the generator to biomedicine, several different flash x-ray generators<sup>3-8</sup> have been developed, and monochromatic or quasi-monochromatic generators are useful to perform energy-selective imaging, for example, enhanced K-edge angiography<sup>9-11</sup> using iodine-based contrast media; the angiography is specially performed using a synchrotron in conjunction with a monochromator.

In order to produce clean characteristic x rays with photon energies of less than 20 keV, weakly ionized linear plasma x-ray generators<sup>12-15</sup> are very useful, and intense quasi-monochromatic x rays are produced from the plasma axial

direction. Without forming the linear plasma, because bremsstrahlung rays are not emitted in the opposite direction to that of electron acceleration, characteristic x rays can be produced by considering the angle dependence of bremsstrahlung x rays.<sup>16</sup> As compared with the plasma generator, the photon energy of the characteristic x rays can be increased by increasing the maximum output voltage, since a multistage Marx generator can be employed.

In this paper, we describe a compact flash x-ray generator utilizing a cold-cathode radiation tube, used to perform a preliminary experiment for generating clean copper  $K\alpha$  lines.

## 2. GENERATOR

### 2.1 High-voltage circuit

Figure 1 shows a block diagram of a compact monochromatic flash x-ray generator. This generator consists of the following components: a constant high-voltage power supply, a polarity-inversion two-stage surge Marx generator with a capacity during main discharge of 425 pF, a trigger device for the surge generator, a turbomolecular pump, and a flash x-ray tube. Since the electric circuit of the surge generator employs a polarity-inversion two-stage Marx line (Fig. 2), the surge generator produces twice the potential of the condenser charging voltage. When two condensers inside of the surge generator are charged from  $-50$  to  $-70$  kV, the ideal output voltage ranges from 100 to 140 kV.

### 2.2 X-ray tube

The x-ray tube is a demountable diode type, as illustrated in Fig. 3. This tube is connected to the turbomolecular pump with a pressure of approximately 1 mPa and consists of the following major devices: a rod-shaped copper target 3.0 mm in diameter, a disk cathode made of graphite, a polyethylene terephthalate (Mylar) x-ray window 0.25 mm in thickness, and a polymethyl methacrylate (PMMA) tube body. The target-cathode space was regulated to 1.25 mm from the outside of the x-ray tube by rotating the anode rod, and the transmission x rays are obtained through a 1.0-mm-thick graphite cathode and an x-ray window. Because bremsstrahlung rays are not emitted in the opposite direction to that of electron acceleration (Figs. 4 and 5), copper  $K\alpha$  rays can be produced using a 10- $\mu$ m-thick nickel K-edge filter.

## 3. CHARACTERISTICS

### 3.1 Tube voltage and current

Tube voltage and current were measured using a high-voltage divider with an input impedance of 10 k $\Omega$  and a current transformer, respectively (Fig. 6). The voltage and current displayed roughly damped oscillations because the discharge resistance in the tube varied rapidly from infinity to approximately 0  $\Omega$  during the discharge. Thus, at the first quarter cycle of the oscillations, when the voltage decreased, the current increased. The instantaneous voltage and current increased with increases in the charging voltage, and the voltage and current were approximately 140 kV and 0.8 kA, respectively, at a charging voltage of  $-70$  kV.

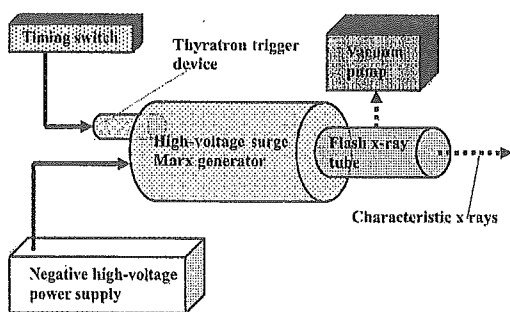


Figure 1: Block diagram of compact monochromatic flash x-ray generator.

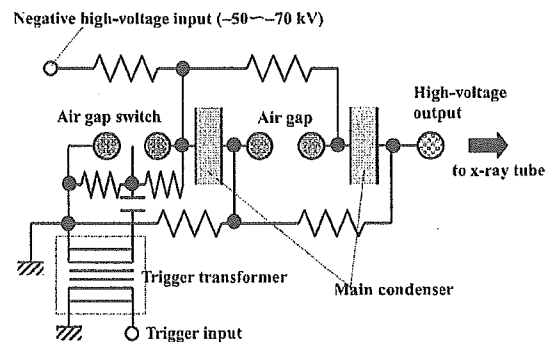


Figure 2: Circuit diagram of flash x-ray generator.

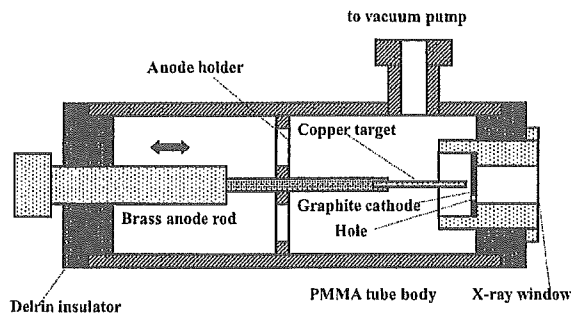


Figure 3: Schematic drawing of flash x-ray tube.

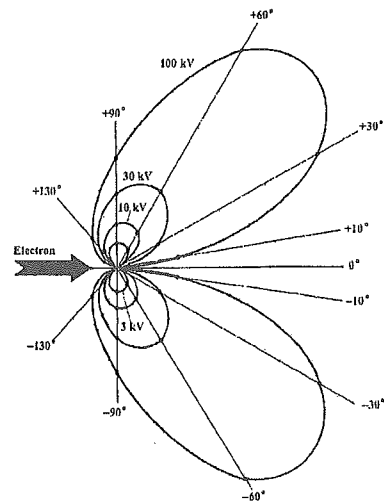


Figure 4: Bremsstrahlung x-ray intensity distribution vs angle.

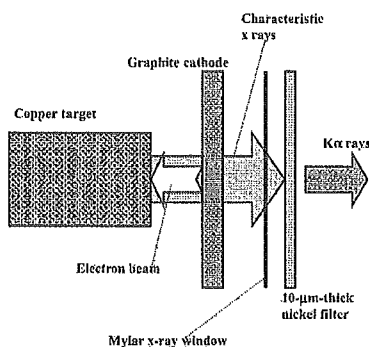


Figure 5: Characteristic x-ray irradiation.

### 3.2 X-ray output

X-ray output pulse was detected using a combination of a plastic scintillator, a photomultiplier, and the filter (Fig. 7). When the charging voltage was increased, the pulse height increased, but the width seldom varied. The widths were approximately 30 ns, and the time-integrated x-ray intensity measured using a thermoluminescence dosimeter (Kyokko TLD Reader 1500 having MSO-S elements without energy compensation) had a value of approximately 1.0  $\mu\text{C}/\text{kg}$  per pulse at 0.5 m from the x-ray source with a charging voltage of  $-70$  kV.

### 3.3 X-ray source

In order to observe the x-ray source, we employed a 100- $\mu\text{m}$ -diameter pinhole camera, an x-ray film (Polaroid XR-7), and the filter (Fig. 8). When the charging voltage was increased, the spot intensity increased, and the intensities corresponded well to the x-ray pulse height. The dimension was almost equal to the target diameter and had a value of approximately 3.0 mm.

### 3.4 X-ray spectra

X-ray spectra were measured by a transmission-type spectrometer with a lithium fluoride curved crystal 0.5 mm in thickness. The spectra were taken using a computed radiography (CR) system<sup>17</sup> with a wide dynamic range, and relative x-ray intensity was calculated from Dicom digital data. Figure 9 shows the measured spectra from the copper target with the filter. We observed clean copper  $K\alpha$  lines, while bremsstrahlung rays were hardly detected at all. The  $K\alpha$  intensity increased with increases in the charging voltage.

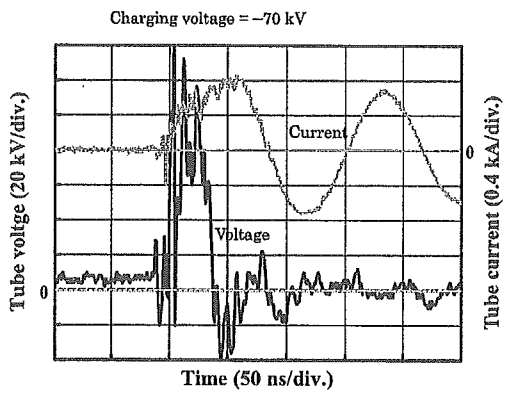
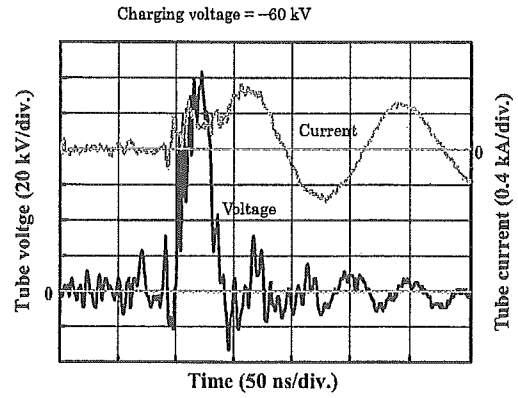
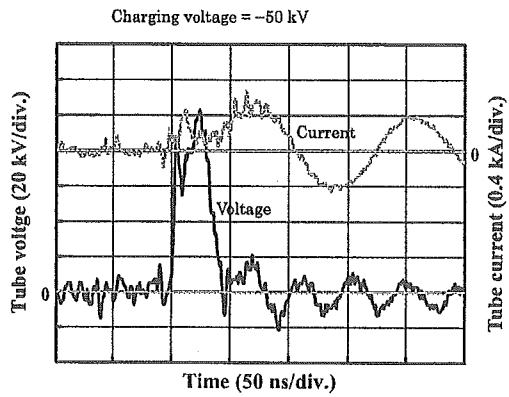


Figure 6: Variations in tube voltage and current with charges in charging voltage.

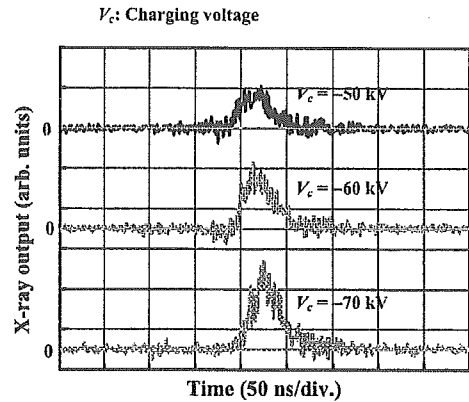


Figure 7: X-ray outputs according to changes charging voltage.

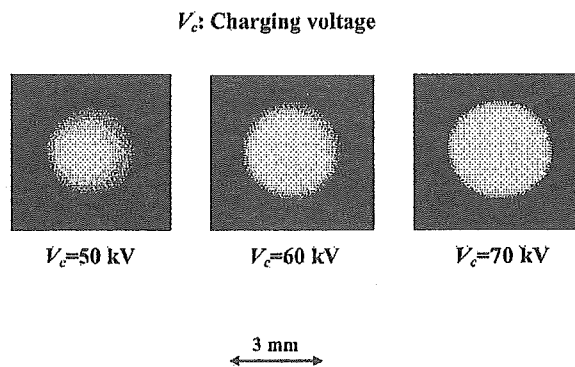


Figure 8: Images of x-ray source with changes in charging voltage.

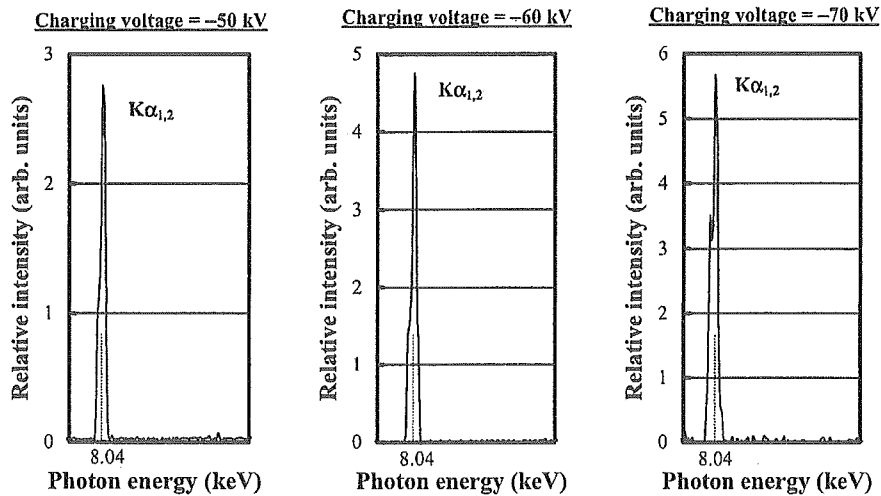


Figure 9: X-ray spectra from copper target according to changes in charging voltage.

#### 4. RADIOGRAPHY

Flash radiography was performed using the CR system (Konica Regius 150) at 0.5 m from the x-ray source, and the charging voltage was  $-70$  kV.

Firstly, rough measurements of spatial resolution were made using wires. Figure 10 shows radiograms of tungsten wires coiled around a pipe made of polymethyl methacrylate. Although the image contrast increased with increasing wire diameter, a  $50\text{-}\mu\text{m}$ -diameter wire could be observed.

Figure 11 shows a radiogram of a vertebra, and fine structures in the vertebra were observed. The image of water falling into a polypropylene beaker from a plastic test tube is shown in Fig. 12. This image was taken with the slight addition of an iodine-based contrast medium. Because the x-ray duration was about  $50$  ns, the stop-motion image of water could be obtained. Figure 13 shows an angiogram of a rabbit heart; iodine-based microspheres of  $15\ \mu\text{m}$  in diameter were used, and fine blood vessels of approximately  $100\ \mu\text{m}$  were visible.

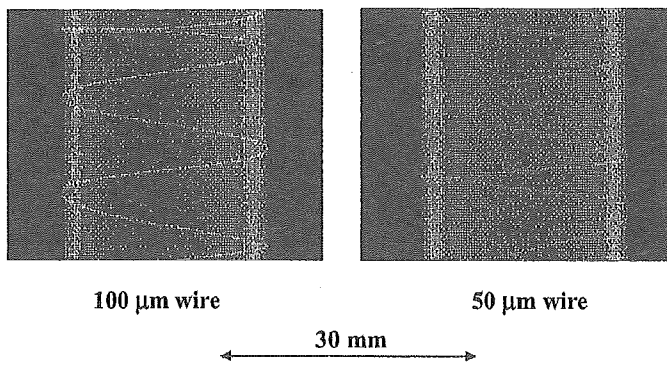


Figure 10: Radiograms of tungsten wires of  $50$  and  $100\ \mu\text{m}$  in diameter coiled around pipe made of polymethyl methacrylate.

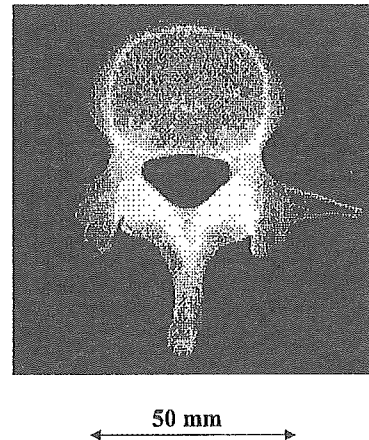


Figure 11: Radiogram of vertebra.



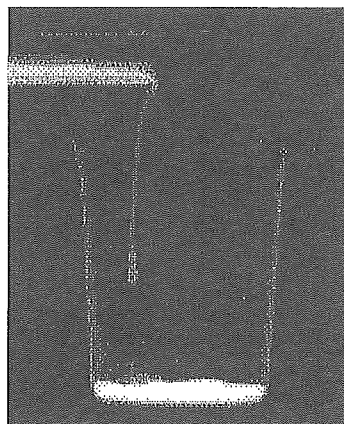


Figure 12: Radiogram of water falling into polypropylene beaker from plastic test tube.

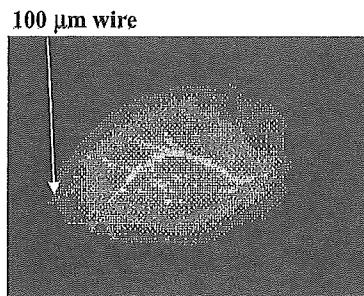


Figure 13: Angiograms of rabbit heart.

## 5. DISCUSSION

Concerning the spectrum measurement, we obtained fairly clean copper  $K\alpha$  rays (8.04 keV). Therefore, we are very interested in the measurement the  $K\alpha$  rays from cerium (34.6 keV), ytterbium (52.0 keV), tantalum (57.1 keV), and tungsten (58.9 keV) targets; the target element should be selected corresponding to the radiographic objectives. In medical applications,  $K\alpha$  rays of cerium are absorbed effectively by an iodine-based contrast medium with a K-edge of 33.2 keV, and K-edge angiography can be performed. In addition, since  $K\alpha$  rays from ytterbium, tantalum, and tungsten targets are absorbed effectively by gadolinium-based contrast media with a K-edge of 50.2 keV, these x rays are very useful for performing enhanced K-edge angiography.

In this research, the instantaneous number of generator-produced  $K\alpha$  photons was approximately  $2.5 \times 10^6$  photons/cm<sup>2</sup> per pulse at 0.5 m from the source. However, the intensity can be increased by increasing the electrostatic energy in condensers in the surge generator, and quasi-monochromatic x rays of both  $K\alpha$  and  $K\beta$  (8.90 keV) lines are produced without using the nickel filter with a K-edge of 8.33 keV.

Using this flash x-ray generator, because the photon energy of characteristic x rays can be selected, a high-speed photon-counting radiography can be performed in order to decrease noise from radiograms. As compared with a steady-state x-ray generator, since the target element can be changed easily using this demountable PMMA tube, demonstrations of monochromatic radiography will be accomplished.

## ACKNOWLEDGMENT

This work was supported by Grants-in-Aid for Scientific Research (13470154, 13877114, and 16591222) and Advanced Medical Scientific Research from MECSST, Health and Labor Sciences Research Grants(RAMT-nano-001, RHGTEFB-genome-005 and RHGTEFB-saisei-003), Grants from Keiryō Research Foundation, The Promotion and Mutual Aid Corporation for Private Schools of Japan, Japan Science and Technology Agency (JST), and New Energy and Industrial Technology Development Organization (NEDO, Industrial Technology Research Grant Program in '03).

## REFERENCES

1. R. Germer, "X-ray flash techniques," *J. Phys. E: Sci. Instrum.*, **12**, 336-350, 1979.
2. A. Mattsson, "Some characteristics of a 600 kV flash x-ray tube," *Physica Scripta*, **5**, 99-102, 1972.

3. E. Sato, H. Isobe and F. Hoshino, "High intensity flash x-ray apparatus for biomedical radiography," *Rev. Sci. Instrum.*, **57**, 1399-1408, 1986.
4. E. Sato, S. Kimura, S. Kawasaki, H. Isobe, K. Takahashi, Y. Tamakawa and T. Yanagisawa, "Repetitive flash x-ray generator utilizing a simple diode with a new type of energy-selective function," *Rev. Sci. Instrum.*, **61**, 2343-2348, 1990.
5. A. Shikoda, E. Sato, M. Sagae, T. Oizumi, Y. Tamakawa and T. Yanagisawa, "Repetitive flash x-ray generator having a high-durability diode driven by a two-cable-type line pulser," *Rev. Sci. Instrum.*, **65**, 850-856, 1994.
6. E. Sato, K. Takahashi, M. Sagae, S. Kimura, T. Oizumi, Y. Hayasi, Y. Tamakawa and T. Yanagisawa, "Sub-kilohertz flash x-ray generator utilizing a glass-enclosed cold-cathode triode," *Med. & Biol. Eng. & Comput.*, **32**, 289-294, 1994.
7. K. Takahashi, E. Sato, M. Sagae, T. Oizumi, Y. Tamakawa and T. Yanagisawa, "Fundamental study on a long-duration flash x-ray generator with a surface-discharge triode," *Jpn. J. Appl. Phys.*, **33**, 4146-4151, 1994.
8. E. Sato, M. Sagae, A. Shikoda, K. Takahashi, T. Oizumi, M. Yamamoto, A. Takabe, K. Sakamaki, Y. Hayasi, H. Ojima, K. Takayama and Y. Tamakawa, "High-speed soft x-ray techniques," *SPIE*, **2869**, 937-955, 1996.
9. H. Mori, K. Hyodo, E. Tanaka, M. U. Mohammed, A. Yamakawa, Y. Shinozaki, H. Nakazawa, Y. Tanaka, T. Sekka, Y. Iwata, S. Honda, K. Umetani, H. Ueki, T. Yokoyama, K. Tanioka, M. Kubota, H. Hosaka, N. Ishizawa and M. Ando, "Small-vessel radiography in situ with monochromatic synchrotron radiation," *Radiology*, **201**, 173-177, 1996.
10. K. Hyodo, M. Ando, Y. Oku, S. Yamamoto, T. Takeda, Y. Itai, S. Ohtsuka, Y. Sugishita and J. Tada, "Development of a two-dimensional imaging system for clinical applications of intravenous coronary angiography using intense synchrotron radiation produced by a multipole wiggler," *J. Synchrotron Rad.*, **5**, 1123-1126, 1998.
11. E. Sato, E. Tanaka, H. Mori, T. Kawai, T. Ichimaru, S. Sato, K. Takayama and H. Ido, "Demonstration of enhanced K-edge angiography using a cerium target x-ray generator," *Med. Phys.*, **31**, 3017-3021, 2004.
12. E. Sato, Y. Hayasi, R. Germer, E. Tanaka, H. Mori, T. Kawai, H. Obara, T. Ichimaru, K. Takayama and H. Ido, "Irradiation of intense characteristic x-rays from weakly ionized linear molybdenum plasma," *Jpn. J. Med. Phys.*, **23**, 123-131, 2003.
13. E. Sato, Y. Hayasi, R. Germer, E. Tanaka, H. Mori, T. Kawai, T. Ichimaru, K. Takayama and H. Ido, "Quasi-monochromatic flash x-ray generator utilizing weakly ionized linear copper plasma," *Rev. Sci. Instrum.*, **74**, 5236-5240, 2003.
14. E. Sato, R. Germer, Y. Hayasi, Y. Koorikawa, K. Murakami, E. Tanaka, H. Mori, T. Kawai, T. Ichimaru, F. Obata, K. Takahashi, S. Sato, K. Takayama and H. Ido: Weakly ionized plasma flash x-ray generator and its distinctive characteristics. *SPIE*, **5196**, 383-392, 2003.
15. E. Sato, Y. Hayasi, R. Germer, E. Tanaka, H. Mori, T. Kawai, T. Ichimaru, S. Sato, K. Takayama and H. Ido, "Sharp characteristic x-ray irradiation from weakly ionized linear plasma," *J. Electron Spectrosc. Related Phenom.*, **137-140**, 713-720, 2004.
16. E. Sato, M. Sagae, E. Tanaka, Y. Hayashi, R. Germer, H. Mori, T. Kawai, T. Ichimaru, S. Sato, K. Takayama and H. Ido: Quasi-monochromatic flash x-ray generator utilizing a disk-cathode molybdenum tube, *Jpn. J. Appl. Phys.*, **43**, 7324-7328, 2004.
17. E. Sato, K. Sato and Y. Tamakawa, "Film-less computed radiography system for high-speed imaging," *Ann. Rep. Iwate Med. Univ. Sch. Lib. Arts and Sci.*, **35**, 13-23, 2000.

\*dresato@iwate-med.ac.jp; phone +81-19-651-5111; fax +81-19-654-9282

# Intense quasi-monochromatic flash x-ray generator utilizing molybdenum-target diode

Michiaki Sagae<sup>\*a</sup>, Eiichi Sato<sup>a</sup>, Haruo Obara<sup>b</sup>, Etsuro Tanaka<sup>c</sup>, Hidezo Mori<sup>d</sup>, Toshiaki Kawai<sup>e</sup>,  
Shigehiro Sato<sup>f</sup>, Hidenori Ojima<sup>g</sup>, Kazuyoshi Takayama<sup>g</sup> and Hideaki Ido<sup>h</sup>

<sup>a</sup> Department of Physics, Iwate Medical University, 3-16-1 Honchodori, Morioka 020-0015, Japan

<sup>b</sup> Department of Radiological Technology, College of Medical Science, Tohoku University, 1-1  
Seiryochō, Sendai 980-0872, Japan

<sup>c</sup> Department of Nutritional Science, Faculty of Applied Bio-science, Tokyo University of  
Agriculture, 1-1-1 Sakuragaoka, Setagaya-ku 156-8502, Japan

<sup>d</sup> Department of Cardiac Physiology, National Cardiovascular Center Research Institute, 5-7-1  
Fujishirodai, Suita, Osaka 565-8565 Japan

<sup>e</sup> Electron Tube Division #2, Hamamatsu Photonics K. K., 314-5 Shimokanzo, Toyooka  
Village, Iwata-gun 438-0193, Japan

<sup>f</sup> Department of Microbiology, School of Medicine, Iwate Medical University, 19-1 Uchimaru,  
Morioka 020-8505, Japan

<sup>g</sup> Shock Wave Research Center, Institute of Fluid Science, Tohoku University, 2-1-1 Katahira,  
Sendai 980-8577, Japan

<sup>h</sup> Department of Applied Physics and Informatics, Faculty of Engineering, Tohoku Gakuin  
University, 1-13-1 Chuo, Tagajo 985-8537, Japan

## ABSTRACT

In the flash x-ray generator, a 150 nF condenser is charged up to 80 kV by a power supply, and flash x rays are produced by the discharging. The x-ray tube is a demountable diode, and the turbomolecular pump evacuates air from the tube with a pressure of approximately 1 mPa. Since the electric circuit of the high-voltage pulse generator employs a cable transmission line, the high-voltage pulse generator produces twice the potential of the condenser charging voltage. At a charging voltage of 80 kV, the estimated maximum tube voltage and current were approximately 160 kV and 40 kA, respectively. When the charging voltage was increased, the K-series characteristic x-ray intensities of molybdenum increased. The K lines were clean and intense, and hardly any bremsstrahlung rays were detected at all. The x-ray pulse widths were approximately 100 ns, and the time-integrated x-ray intensity had a value of approximately 15  $\mu\text{C}/\text{kg}$  at 1.0 m from the x-ray source with a charging voltage of 80 kV.

**Keywords:** flash x-ray, energy-selective radiography, characteristic x rays, quasi-monochromatic x rays, bremsstrahlung x-ray distribution

## 1. INTRODUCTION

In recent years, there have been several investigations dealing with the production of monochromatic x rays in radiology and cardiology. Particularly, monochromatic parallel beams using synchrotrons have been employed to perform enhanced K-edge angiography<sup>1,2</sup> and x-ray phase imaging.<sup>3,4</sup> In angiography, parallel beams with photon energies of approximately 35 keV have been employed, since these beams are absorbed effectively by an iodine-based contrast medium. Subsequently, in cases where phase imaging is employed, the spatial resolution can be improved, and the number of tissues which can be observed using x rays increases.

In order to perform biomedical radiography, we have developed several different soft flash x-ray generators<sup>5-10</sup> corresponding to specific radiographic objectives. Subsequently, electron impact flash x-ray sources can produce quasi-monochromatic x rays, because bremsstrahlung rays are not emitted in the opposite direction to that of electron

acceleration.<sup>11</sup> Therefore, the sources will be conventional x-ray tubes for producing cone-beam K-series characteristic x rays, and monochromatic  $K\alpha$  rays are obtained using a K-edge filter.

We have developed several different plasma flash x-ray generators<sup>12-16</sup> corresponding to specific radiographic objectives, and a major goal in our research is the development of an intense and sharp monochromatic x-ray generator that can impact applications with biomedical radiography. By forming weakly ionized linear plasma, because we have succeeded in producing fairly intense and clean K-series characteristic x rays. Without forming the linear plasma, characteristic x rays can be produced by considering the angle dependence of bremsstrahlung x rays. On the other hand, the electrostatic energy in the main discharge condenser should be increased as much as possible to increase the characteristic x-ray intensity.

In this paper, we describe an intense single flash x-ray generator utilizing a rod-target radiation tube, used to perform a preliminary experiment for generating intense and clean molybdenum K-series characteristic x rays.

## 2. GENERATOR

### 2.1 High-voltage circuit

Figure 1 shows a block diagram of a high-intensity plasma flash x-ray generator. The generator consists of the following essential components: a high-voltage power supply, a high-voltage condenser with a capacity of approximately 150 nF, an air gap switch, a turbomolecular pump, a thyatron pulse generator as a trigger device, and a flash x-ray tube. In this generator, a coaxial cable transmission line is employed in order to increase maximum tube voltage using high-voltage reflection. The high-voltage main condenser is charged up to 80 kV by the power supply, and electric charges in the condenser are discharged to the tube through the four cables after closing the gap switch with the trigger device (Fig. 2).

### 2.2 X-ray tube

The x-ray tube is a demountable cold-cathode diode that is connected to the turbomolecular pump with a pressure of approximately 1 mPa (Fig. 3). This tube consists of the following major parts: a ring-shaped graphite cathode with an inside diameter of 4.5 mm, a stainless-steel vacuum chamber, a nylon insulator, a polyethylene terephthalate (Mylar) x-ray window 0.25 mm in thickness, and a rod-shaped molybdenum target 3.0 mm in diameter. The distance between the target and cathode electrodes can be regulated from the outside of the tube, and is set to 1.5 mm. As electron beams from the cathode electrode are roughly converged to the target by the electric field in the tube, evaporation leads to the formation of weakly ionized plasma, consisting of molybdenum ions and electrons, around the target. Because bremsstrahlung rays are not emitted in the opposite direction to that of electron acceleration (Fig. 4), molybdenum K-series characteristic x rays can be produced without using a filter.

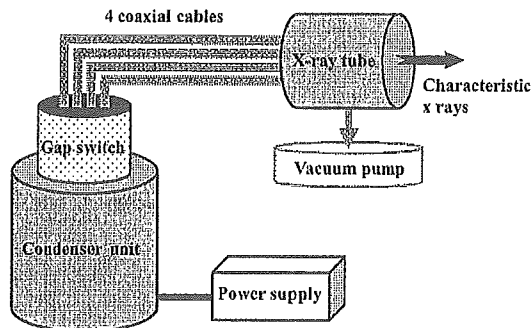


Figure 1: Block diagram of intense quasi-monochromatic flash x-ray generator.

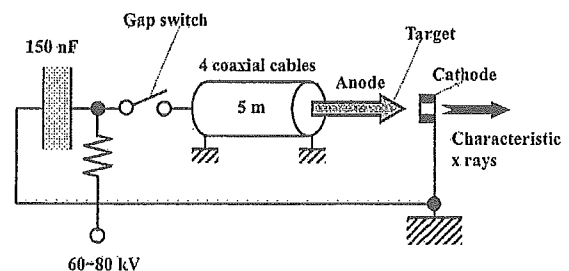


Figure 2: Circuit diagram of flash x-ray generator.