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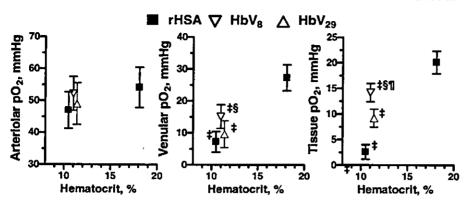


Fig. 7. Intravascular Po₂ after the level 2 and level 3 hemodilutions. Values are presented as means \pm SD. $\ddagger P < 0.05$ compared with level 2 with rHSA; $\ddagger P < 0.05$ compared with level 3 with rHSA; $\ddagger P < 0.05$, level 3 with HbV₃ vs. level 3 with HbV₂₀.

where the anoxic threshold is passed, thus eliminating the inherent variability of oxygen delivery shown by the variability of tissue Po₂.

Considering the significantly improved blood pressure and the trend toward higher flow for HbV₈ (in the absence of vasoconstriction and changes in the rheological properties of blood), it is possible that in conditions of extreme hemodilution the cardiac function should be improved because of the proposed more homogenous heart tissue oxygenation using HbV₈ vs. HbV₂₉.

In summary, the present results show that either HbV₈ or HbV₂₉ are efficient oxygen carriers that do not cause vasoactivity. The experiments were carried out using rHSA as a hemodiluent, and this material was adequate as a plasma volume substitute. Oxygen extraction was similar for both oxygen carriers; however, HbV₈ appeared to be beneficial at the systemic level, because base excess remained at baseline levels, whereas it was decreased for HbV₂₉. This finding suggests that improved tissue Po₂ and microcirculatory oxygen delivery may be efficient in other tissues. The improvement obtained may be specific to the conditions of these experiments

in which the vesicles were tested for their capacity to restore tissue Po₂, FCD, and oxygen extraction in the microcirculation during extreme hemodilution. The significant differences in the tissue oxygen parameters produced by the presence of low-P₅₀ Hbs vs. an identical oxygen carrier with normal P₅₀ suggests that small amounts of Hbs with high oxygen affinity may have therapeutic effects in the treatment of ischemic conditions (6).

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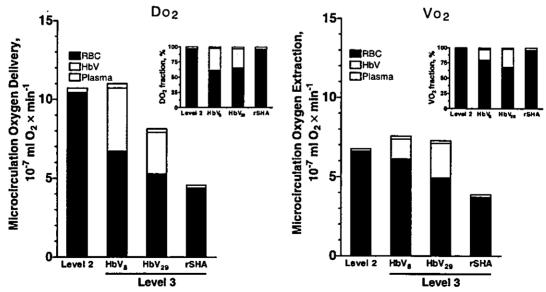


Fig. 8. Arterial oxygen delivery (Do₂) and extraction (Vo₂) before and after the *level 3* hemodilution. Calculations of global oxygen transport are not directly measurable in our model; however, the changes relative to baseline can be calculated using the measured parameters. These calculations can be identified as those presented without standard deviations to focus on their tendencies rather than on the variability of the measurement.



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O2 DELIVERY BY HIGH AND NORMAL OXYGEN AFFINITY HB VESICLES

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Oxygen release from low and normal P₅₀ Hb vesicles in transiently occluded arterioles of the hamster window model

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Sakai, Hiromi, Pedro Cabrales, Amy G. Tsai, Eishun Tsuchida, and Marcos Intaglietta. Oxygen release from low and normal P50 Hb vesicles in transiently occluded arterioles of the hamster window model. Am J Physiol Heart Circ Physiol 288: H000-H000, 2005. First published January 28, 2005; doi:10.1152/ajpheart.01184.2004.—A phospholipid vesicle encapsulating Hb [Hb vesicle (HbV)] has been developed as a transfusion alternative. One characteristic of HbV is that the O2 affinity [Po2 at which Hb is 50% saturated (P50)] of Hb can be easily regulated by the amount of the coencapsulated allosteric effector pyridoxal 5'phosphate. In this study, we prepared two HbVs with different P50s (8 and 29 mmHg, termed HbV8 and HbV29, respectively) and observed their O2-releasing behavior from an occluded arteriole in a hamster skinfold window model. Conscious hamsters received HbV8 or HbV29 at a dose rate of 7 ml/kg. In the microscopic view, an arteriole (diameter: 53.0 ± 6.6 μm) was occluded transcutaneously by a glass pipette on a manipulator, and the reduction of the intra-arteriolar Po2 100 µm down from the occlusion was measured by the phosphorescence quenching of preinfused Pd-porphyrin. The baseline arteriolar Po₂ (50-52 mmHg) decreased to about 5 mmHg for all the groups. Occlusion after HbV8 infusion showed a slightly slower rate of Po2 reduction compared with that after HbV29 infusion. The arteriolar O2 content was calculated at each reducing Po2 in combination with the O2 equilibrium curves of HbVs, and it was clarified that HbVs showed a significantly slower rate of O2 release compared with HbV29 and was a primary source of O2 (maximum fraction, 0.55) overwhelming red blood cells when the Po₂ was reduced (e.g., <10 mmHg) despite a small dosage of HbV. This result supports the possible utilization of Hb-based O2 carriers with lower P₅₀ for oxygenation of ischemic tissues.

blood substitutes; artificial red blood cells; occlusion; microhemodynamics; liposome

PHOSPHOLIPID VESICLES encapsulating concentrated human Hb [Hb vesicles (HbV)] or liposome-encapsulated Hb can serve as a transfusion alternative whose O₂ carrying capacity can be formulated to be comparable to that of blood (1, 5, 8, 16, 24, 30). The capsular structure of HbV (particle diameter ~250 nm) has characteristics similar to those of natural red blood cells (RBCs), because both have membranes that prevent direct contact of Hb with the components of blood and the endothelial lining, mitigating cellular injury due to Hb-mediated prooxidative species (4, 38). Furthermore, Hb encapsulation in vesicles prevents a hypertensive response induced by free Hbs that scavenge the endogenous vasorelaxation factors nitric oxide (NO) and carbon monoxide (12, 18, 26). The safety of HbV has been confirmed in rodent models in terms of the prompt metabolism of the components of HbV in the reticuloendothe-

lial system, which was demonstrated by histopathological analysis and plasma biochemical analysis (28, 29).

One of the characteristics of the capsular HbV is that its physicochemical characteristics such as O2 affinity [O2 tension at which Hb is half-saturated with O2 (P50) can be easily regulated by manipulating the amount of an allosteric effector coencapsulated in HbV. This property provides additional flexibility in formulating the O2 transport properties of HbV by comparison with the chemically modified Hbs whose P50 is modified and fixed by chemical reactions such as cross-linking or polymer conjugation (34). We use pyridoxal 5'-phosphate (PLP) as the allosteric effector (33, 45). For example, coencapsulation of PLP at the molar ratio of PLP to Hb of 2.5:1 yields a P50 of about 29 mmHg. On the other hand, HbVs without PLP have a P50 of 8 mmHg. Historically, P50 was set similar to that of RBCs or about 25-30 mmHg, which theoretically allows sufficient O2 unloading as blood transits the microcirculation. Decreasing O2 affinity (increasing P50) increases O2 unloading in the peripheral blood circulation as shown by the enhanced O2 release and improved exercise capacity in mutant mice that carry high P₅₀ RBCs (36).

Hemoglobin-based O₂ carriers (HBOCs) of molecular dimensions as well as HbV could be effective for the targeted oxygenation of ischemic tissues (6, 43) because the small particle dimension would allow their passage through constricted or partially occluded vessels that do not allow the passage of RBCs (19). Blood flow in these vessels and in collateral vessels is usually slow, thus increasing RBC transit times (7, 11). As a result, tissue Po₂ is low and RBCs release most of their O₂ before reaching the capillary circulation. As an example, if tissue Po₂ is below 5 mmHg, O₂ saturation (Sa_{O2}) of RBCs would be around 5%, and RBCs will have released most of their O₂ before they reach the ischemic tissue. Thus an HBOC with a normal P₅₀ similar to RBCs would not be effective for carrying O₂ to the ischemic tissue.

In this study, we evaluate the rate of O_2 release from HbVs with high and low P_{50} s from arterioles immediately after their occlusion. We selected arterioles with diameters of about 50 μ m because this size of arterioles contributes significantly to tissue oxygenation in normal conditions (13). This model was selected to determine the ability of HbVs to retain or release O_2 in hypoxic conditions and establish their suitability for oxygenating ischemic tissues.

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OXYGEN RELEASE FROM HB VESICLES

MATERIALS AND METHODS

Preparation of HbVs. HbVs with different P50s were prepared under sterile conditions as previously reported (32, 34, 37). Hb was purified from outdated donated human blood provided by the Japanese Red Cross Society (Tokyo, Japan). HbVs with a P₅₀ = 29 mmHg (HbV29) was prepared by adding the allosteric effector pyridoxal 5'-phosphate (PLP; 14.7 mM, Sigma Chemical; St. Louis, MO) to Hb (38 g/dl) at a molar ratio of PLP to Hb = 2.5. HbVs with a $P_{50} = 8$ mmHg (HbV₈) were prepared by adding no allosteric effector to the Hb solution. The Hb solution was encapsulated within vesicles composed of Presome PPG-I [a mixture of 1,2-dipalmitoyl-sn-glycero-3phosphatidylcholine, cholesterol, and 1,5-di-O-octadecyl-N-succinyl-L-glutamate at a molar ratio of 5:5:1 (Nippon Fine Chemicals; Osaka, Japan)], and the particle size of HbVs was regulated by an extrusion method. The surface of the HbVs was modified with polyethylene glycol (molecular mass: 5 kDa, 0.3 mol% of the lipids in the outer surface of vesicles) using 1,2-distearoyl-sn-glycero-3-phosphatidylethanolamine-N-polyethylene glycol (Sunbright DSPE-50H, H-form, NOF; Tokyo, Japan). HbVs were suspended in a physiological salt solution and sterilized with filters (Dismic, Toyo Roshi; Tokyo, Japan; pore size: 0.45 μm) and deoxygenated with N₂ bubbling for storage. The endotoxin content was measured with a modified LAL AQ:1 assay, and the level was less than 0.2 EU/ml (27). The O2 equilibrium curves (OECs) of HbV29 and HbV8 were obtained by a Hemox Analyzer (TCS-Medical Products; Philadelphia, PA), as shown in Fig. 1. The physicochemical parameters of the HbVs are listed in Table 1.

Animal model and preparation. Experiments were carried out in 12 male Syrian golden hamsters (59 ± 12 g body wt, Charles Rivers; Worcester, MA). The dorsal skinfold consisting of two layers of skin and muscle was fitted with two titanium frames with a 15-mm circular opening and surgically installed under intraperitoneal pentobarbital sodium anesthesia (~50 mg/kg body wt, Abbott Laboratory; North Chicago, IL). After the hair on the back skin of the hamster was removed, layers of skin muscle were separated from the subcutaneous tissue and removed until a thin monolayer of muscle including the small artery and vein and one layer of intact skin remained. A coverglass (diameter 12 mm) held by one frame covered the exposed tissue allowing intravital observation of the microcirculation (20, 22, 25).

Polyethylene (PE) tubes (PE-10, Becton-Dickinson; Parsippany, NJ; ~1 cm) were connected to PE-50 tubing (~25 cm) via silicone elastomer medical tubes (~4 cm, Technical Products; Decatur, GA) and were implanted in the jugular vein and the carotid artery. They were passed from the ventral to the dorsal side of the neck and exteriorized through the skin at the base of the chamber. Patency of the catheters was ensured by filling them with heparinized saline (40

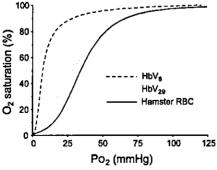


Fig. 1. Oxygen equilibrium curves (OECs) of Hb vesicles (HbVs) at a PO₂ where Hb is half-saturated (P50) of 8 mmHg (HbV8) and 29 mmHg (HbV29) measured with a Hemox Analyzer (TCS Medical Products) at 37°C compared with hamster blood, RBC, red blood cells,

Table 1. Physicochemical properties of HbV₈ and HbV₂₉ compared with hamster blood

Parameters	HbVs	HbV ₂₉	Hamster Blood
Hb concentration, g/dl	10	10	14.8 ± 0.5
Particle diameter, nm	250 ± 64	247 ± 44	5,000-7,000*
P ₅₀ , mmHg	8	29	28
Molar ratio of PLP to Hb	Ó	2.5	
MetHb, %	<3	<1	
НьСО, %	<2	<2	

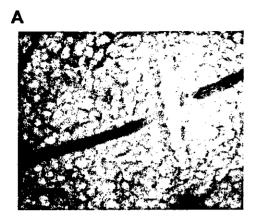
HbV₈ and HbV₂₉, Hb vesicles (HbVs) at 8- and 29-mm Hg Po₂ at which Hb is 50% saturated (Pso); PLP, pyridoxal 5'-phosphate. *Size of hamster red blood cells (RBCs) (39).

IU/ml). Microvascular observations of the awake and unanesthetized hamsters were performed 5 days after chamber implantation to mitigate the effects of surgery. The hamster was placed in a perforated plastic tube from which the window chamber protruded to minimize animal movement without impeding respiration. All animal studies were approved by the Animal Care and Use Committee of University of California-San Diego and performed according to the National Institutes of Health Guide for the Care and Use of Laboratory Animals (Washington, DC: National Academy Press, 1996).

Infusion of HbV₈ and HbV₂₉ and occlusion of an arteriole. The unanesthetized animal was placed in a perforated plastic tube and stabilized under the microscope. Animals were suitable for the experiments if systemic variables were within normal range, namely, heart rate >340 beats/min, mean arterial pressure >80 mmHg, systemic hematocrit >45%, and arterial Po₂ >50 mmHg, and microscopic examination of the tissue in the chamber did not reveal signs of edema or bleeding. Baseline measurements of microvascular parameters and Po₂ (see below) were performed before the infusion of HbV₈ or HbV₂₉ suspended in physiological saline solution into the venous line at 7 ml/kg. Systemic blood volume was estimated as 70 ml/kg. In our previous reports of resuscitation from hemorrhagic shock or hemodilution, HbVs were suspended in an albumin solution to regulate colloid osmotic pressure (30, 33). However, in the present study, we did not use albumin to minimize the hypervolemic effect. For the same reason, the infusion amount was minimized to equal 10% blood volume (7 ml/kg).

After we stabilized the condition and measured the systemic parameters for 20 min, diameter and blood flow of the selected arterioles were measured. Large feeding arterioles or small arcading arterioles (diameter 53.0 \pm 6.6 μ m) were selected for observation. The arterioles were occluded by means of a glass micropipette whose end was drawn into a long fiber by a pipette puller (Fig. 2). The fiber F2 was bent over a flame, and the knee of the bend was used to press on the intact skin of the preparation mounted in an inverted microscope that allowed observation of the opposite side, i.e., the intact microcirculation. Once an arteriole was selected for measurement, the microoccluder is moved to the skin side, between the intact skin and the optics of the substage illumination. The tip of the occluder was placed near the center of the optical field of view of the microscope, and the vessel was similarly placed using the stage micrometric position control. This arrangement allowed for direct microscopic observation of the occluded vessel and the stopped flow as shown in Fig. 2. The duration of occlusion was 30 s.

Measurement of microhemodynamic parameters. Microvessels were observed by transillumination with an inverted microscope (IMT-2, Olympus; Tokyo, Japan). Microscopic images were video recorded (Cohu 4815-2000; San Diego, CA) and transferred to a television videocassette recorder (Sony Trinitron PVM-1271Q monitor; Tokyo, Japan) and Panasonic AG-7355 video recorder (Tokyo, Japan). Arterioles were classified according to their position within the microvascular network according to the previously reported scheme (33). Microvascular diameter and RBC velocity before occlu-



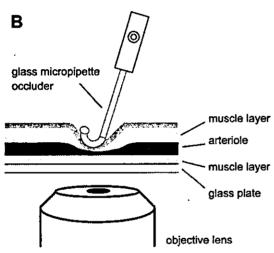


Fig. 2. A: microscopic image of an occluded arteriole in the hamster window chamber. The glass fiber lies across the arteriole. Scale bar = 100 μ m. B: schematic representation of occlusion of A showing the different tissue layers of the skin (not to scale).

sion were analyzed on-line in the arterioles (14, 15). Vessel diameter was measured with an image-shearing system (Digital Video Image Shearing Monitor 908, I.P.M.; San Diego, CA), whereas RBC velocity was analyzed by photodiodes and the cross-correlation technique (Velocity Tracker Mod-102 B, I.P.M.). The blood flow rate (Q) was calculated using the following equation:

$$Q = (RBC \text{ velocity/R}_v) \times (\text{diameter/2})^2$$
 (1)

where $R_{\nu} = 1.6$ and is the ratio of the centerline velocity to average blood velocity according to data from glass tubes (20).

Palladium-porphyrin bound to bovine albumin solution (7.6 wt%, 0.1 ml) was injected intravenously 20 min before the infusion of HbVs. Arteriolar blood Po2 was noninvasively determined by measuring the rate of decay of phosphorescence emitted by the metalloporphyrin complex after pulsed light excitation, which is a function of the local O₂ concentration (17, 40, 44). The relationship between phosphorescence lifetime and Po2 is given by the following Stern-Volmer equation:

$$\tau_o/\tau = 1 + k_o \times \tau_o \times Po_2 \tag{2}$$

where τ_0 and τ are the phosphorescence lifetimes in the absence of molecular O_2 and at a given Po_2 , respectively, and k_q is the quenching constant, with both factors being pH and temperature dependent. Light was gathered from an optical window of 20 \times 5 μm placed longitudinally along the blood vessels. Measurements in the blood compartment were made every second using a single flash.

The Po2 decay curves induced by the occlusion were obtained before the infusion of HbVs and 20 min after the infusion of HbVs. The Sao, of HbVs at every Po2 were obtained from the OECs (Fig. 1), and the total O_2 content in blood (ml O_2 in 1 dl blood) can be estimated using the following equation:

O₂ content =
$$23.6 \times \frac{[Sa_{02}(RBC) + 0.0667 \times Sa_{02}(HbV)]}{100} + 2.42 \times \frac{Po_2}{713}$$
 (3)

In this calculation, we used 15 g/dl as the average Hb concentration in arterial blood (14.8 ± 0.5 g/dl, heme concentration 9.3 mM), which was measured with a handheld photometer (B-Hemoglobin Photometer, Hemocue). One hundred milliliters of blood contain 23.6 ml O₂ bound to Hb when SaO2 is 100% (volume of an ideal gas at 37°C) according to Boyle-Charle's gas law, PV = nRT, where P (in atm) is atmospheric pressure, V (in liters) is gas volume, n is mole number, R is the gas constant (0.082 atm·l·K⁻¹·mol⁻¹), and T is absolute temperature [23.6 (ml) = 9.3×10^{-4} (mol) $\times 0.082 \times (273 + 37) \times$ 1,000]. The physically dissolved O2 content at 1 atm O2 (713 mmHg after subtracting the vapor pressure of water = 47 mmHg) at 37°C was calculated to be 2.42 ml in 100 ml water. Sao₂(RBC) and Sao, (HbV) are Sao, s of RBCs and HbVs, respectively, at each arteriolar Po2 during the experiments.

HbVs were suspended in physiological saline solution ([Hb] = 10 g/dl); therefore, their infusion lowered colloid osmotic pressure, causing the extravasation of plasma fluid. To account for this, we carried out our measurements 20 min after HbV infusion and assumed that this interval was sufficient for normalizing blood volume through the release of extra fluid to the interstitium, thus increasing plasma Hb concentration by 6.7%.

Data analysis. Data are given as means ± SD for the indicated number of animals. Data were analyzed using ANOVA followed by Fisher's protected least-significant difference test between groups according to the previous studies. Student's t-test was used for comparisons within each group. All statistics were calculated using GraphPad Prism 4.01 (Graph Pad Software; San Diego, CA). Changes were considered statistically significant if P < 0.05.

RESULTS

Hemodynamic properties of arterioles. The profiles of the selected arterioles, diameters, centerline RBC velocities, blood flow rates, and intra-arteriolar Po2 values before and after infusion of HbVs are listed in Table 2. There was no significant 72 difference between the groups. The O2 content in blood attributed to hamster RBCs and physically dissolved O2 at the observed arteriolar Po2 was estimated as 18.61 ± 1.23 ml O2/dl blood according to Eq. 3. After the infusion of HbV8 and HbV₂₉, the O₂ content increased to 20.30 \pm 1.18 and 20.17 \pm 1.54 ml O₂/dl blood, respectively, due to the O₂ bound to HbVs. The contributions of HbV8 and HbV29 to whole O2 content were 1.51 \pm 0.01 and 1.25 \pm 0.07 ml O₂/dl blood, respectively. The HbV₈ group showed higher O₂ content than the HbV₂₉ group due to the higher Sa_{O2}(HbV₈), which was $95.9 \pm 0.6\%$ compared with the Sa_{O₂}(HbV₂₉) of 79.6 ± 4.7%.

Changes in Po2 in arterioles after occlusion in the presence of HbVs. Arteriolar Po2 before occlusion was about 50-52 mmHg in average for all groups and started to decrease significantly immediately after occlusion, as shown in Fig. 3. F3 In all groups, Po2 fell to about 10 and 5 mmHg after 10- and

F4

Table 2. Profiles of arterioles for occlusion before and after infusion of HbVs

	Before	After HbV Infusion		
Parameters	Infusion	HbV ₈	HbV₂9	
Arteriolar diameter, µm	53.0±6.6	56.2±6.8	55.8±6.9	
Centerline flow velocity, mm/s	3.1 ± 0.5	3.4 ± 0.7	3.5±0.5	
Blood flow rate, nl/s	6.8 ± 1.6	8.7±3.1	8.5 ± 2.1	
Arteriolar Po2, mmHg	50.7±4.7	51.4±4.8	52.1 ± 5.3	
Sao (RBC), %	78.1 ± 5.1	76.0±7.7	77.9±6.5	
Sao (HbV), %		95.9±0.6†	79.6±4.7	
O ₂ content in whole blood, ml/O ₂ /dl/blood	18.61±1.23	20.30±1.18*	20.17±1.54*	
O ₂ content in HbV, ml/O ₂ /dl/ blood		1.51±0.01	1.25±0.07	

Values are means \pm SD. Arteriolar PO₂, O₂ saturation (SaO₂) and O₂ contents were obtained during 6 s before occlusion. *P < 0.05 vs. before infusion; †P < 0.05 vs. RBCs and HbV₂₉.

30-s occlusion, respectively. When the Po_2 values were expressed as relative to the baseline values (before occlusion), infusion of HbV_8 tended to show a slower rate of reduction of Po_2 compared with the infusion of HbV_{29} and without infusion (Fig. 4). There was a significant difference between the HbV_8 infusion and before infusion groups only at 7 s (P = 0.035).

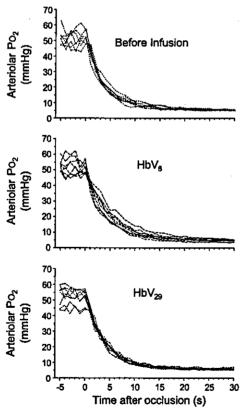


Fig. 3. Time course of Po_2 in the blood of an occluded arteriole (diameter, $53.0\pm6.6~\mu m$) before and after infusion of 7 ml/kg HbVs or HbV29 into hamsters. Measurements were made in blood at a distance of 50 μm from the point of occlusion. Most vessels equilibrate to intravascular partial pressure in the range of 4–6 mmHg about 15–20 s after occlusion.

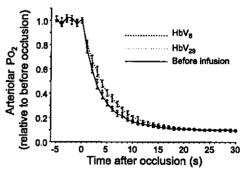


Fig. 4. Changes in Po_2 relative to before occlusion. The data in Fig. 3 were averaged. Baseline values before occlusion were obtained as the average of 6 values before occlusion and fixed as 1.0. There was a significant difference between the HbV₈ infusion and before infusion groups only at 7 s (P = 0.035).

 $Sa_{O_2}(RBC)$ and $Sa_{O_2}(HbV)$ at every arteriolar Po_2 value can be estimated using the OECs in Fig. 1 assuming that the conditions in the arteriole (such as temperature and pH) do not change significantly from the normal condition (37°C, pH 7.4). Figure 5A shows the changes in the whole arteriolar O_2 content F5

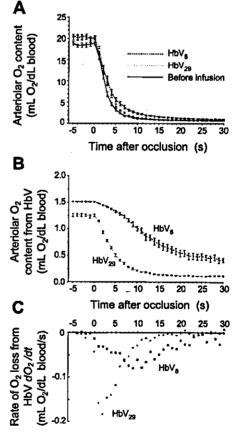


Fig. 5. A: time course of the arteriolar O_2 content in whole blood of an occluded arteriole before and after infusion of 7 ml/kg HbV₈ or HbV₂₉ into hamsters. The O_2 contents were calculated using Eq. 2 and the data of OECs (Fig. 1) and Po₂ changes (Fig. 3). B: time course of the O_2 content derived from HbVs in the blood. The contributions of HbVs are derived from the data in A and magnified in scale. C: rate of O_2 loss from HbVs. The graphs in B were differentiated and plotted.

during the occlusion. Immediately after occlusion, the O2 content decreased rapidly. The HbV8 group showed a slower rate of reduction compared with the HbV29 group and the group before HbV infusion. To demonstrate the contribution of HbVs clearly, only the O2 content of HbVs is shown in Fig. 5B. HbV₈ showed a very slow rate of O₂ release. After 30 s of occlusion, the arteriolar Po₂ decreased to 5.2 ± 0.7 mmHg. However, $Sa_{O_2}(HbV_8)$ was 26.1 \pm 7.3% and did not reach steady state but continued O2 release. HbV29 showed almost no change after 15 s, and $Sa_{O_2}(HbV_{29})$ was 7.4 \pm 1.0% after 30 s. Figure 5C shows the rate of O2 loss from HbVs obtained by the differentiation of the graphs in Fig. 5B. HbV₂₉ showed the fastest O2 loss with the maximum of 0.18 ml O2/dl blood sec after only 2 s of occlusion and did not supply O2 after 17 s. On the other hand, HbV₈ showed a moderate O₂ loss and showed the maximum of 0.08 ml O₂/dl blood after 10 s of occlusion and continued to release O2 until 30 s.

Figure 6 shows the fraction of O2 in blood originating from HbVs. Before occlusion of the arterioles, the fractions of HbV8 and HbV29 are very small and similar because of the small dosage compared with the originally present RBCs. However, after occlusion, the fraction of O2 from HbV8 increased significantly and was about 0.55 after 10 s. This indicated that HbV₈, and not RBCs, was the main source of the O₂ carrier when Po2 attained very low values.

DISCUSSION

The principal finding of this study is that HbV_8 ($P_{50} = 8$ mmHg) with a high O2 affinity (low P50) releases O2 at a slower rate than does HbV29 in occluded arterioles of the hamster dorsal skinfold model. Furthermore, we found that HbV₈, and not HbV₂₉, is the main O₂ source in ischemic conditions.

The immediate occlusion of blood flow in the arterioles caused a rapid reduction of O2 content. Similar phenomena have been observed by Richmond et al. (23) in rat spinotrapezius muscle tissue. There is substantial evidence that the arteriolar wall is a significant O2 sink, consuming O2 at a rate that is much greater than most tissues (9, 35, 42), which explains in part the significant and rapid drop of Po2 found in our study. In our experiments, only one arteriole was occluded at a time in the intact subcutaneous tissue, and arteriolar Po₂ decreased to about 5 mmHg, which was higher than the critical Po_2 (2.9 \pm 0.5 mmHg) in the rat spinotrapezius muscle tissue (23). Although the O2 supply was significantly reduced, diffusion of O2 from the other surrounding arterioles, venules, and

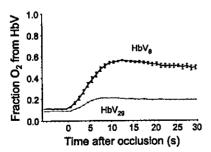


Fig. 6. Time course of the fraction of O2 content from HbVs in whole blood. The extended time of occlusion induced hypoxic conditions and the fraction of O2 content from HbV8 increased significantly compared with HbV29.

capillaries near the occlusion should contribute to maintaining tissue Po2 at a higher value than in the study of Richmond et al. (23), where the supply of blood to the tissue was stopped altogether. Sao, (HbV8) at 5 mmHg is estimated to be about 26% according to the OECs (Fig. 1), which is higher than that for HbV₂₉ (6%) and RBCs (2%); thus HbV₈ remains a source of O2 for a longer period in a prolonged occlusion, because the fraction of O2 from HbV8 was 0.5 or higher, overwhelming the contribution from RBCs, as shown in Fig. 6.

A limitation of our experimental method is that Sao, is estimated under the assumption that conditions in the target arteriole are identical to that of the OEC measurement; however, the O2 affinity of Hb changes as a function of temperature, pH, electrolyte concentration, and CO2 content. Local ischemic conditions caused by the occlusion could affect pH and increase CO₂ tension, resulting in a slight decrease in the O₂ affinity (increased P₅₀); however, it is unlikely that this would introduce a significant error in the measurement of O2 release considering the short duration of the occlusion (30 s).

We have previously demonstrated using an artificial narrow polymer tube (inner diameter: 28 µm) surrounded by a sodium dithionate solution to consume O2 that a Hb solution under continuous flow conditions (1 mm/s) facilitates O2 release when mixed with RBCs. Conversely, HbV did not show this phenomenon (31). This difference is due to the small size of O2-bound acellular Hb molecules, which diffuse and therefore contribute to the facilitated O₂ transport (21, 31), whereas HbVs (diameter, about 250 nm) are too large to show sufficient diffusion for the facilitated O2 transport. In these conditions, O2 affinity (P50) becomes the determining factor for the rate of O2 release and transport to the vessels wall. Thus, in our present results, the presence of HbVs did not facilitate the reduction of Po2 or O2 content but retarded the reduction of Po2 and O2 content.

Our experimental model is designed to characterize the O₂ release behavior of blood from an occluded microvessel and does not directly related to clinical ischemic conditions because the occlusion of the small arteriole for 30 s does not induce tissue ischemia other than the transient event in the proximity of the microvessel. However, our data suggest that HbV₈ could be a significant source of O₂ in an ischemic condition with significantly lowered tissue Po2. Because of the small dosage of HbV8 (10 ml/kg), the O2 content in the blood after occlusion (5 ml O2/dl blood at 5 s) is significantly smaller than the baseline value (20 ml O2/dl blood at 0 s). To enhance the contribution of HbVs, a larger dosage and sustained blood flow would be required. Contaldo et al. (7) recently demonstrated that inducing hemodilution using up to 50% blood exchange with HbV (P₅₀ = 15 mmHg) suspended in dextran effectively oxygenated ischemic collaterized tissue in skin flaps. This phenomenon could be explained by low P50 HbVs retaining O2 in the upstream vessels and delivering it to the ischemic tissue via collateral arterioles, even when these may have significantly slower blood flow. It has been proposed that small-sized HBOCs oxygenate ischemic tissue by being able to pass through constricted or partially occluded vessels that do not allow the passage of RBCs; however, the results from Contaido et al. (17) as well as those from our experimental model do not serve to support this concept, because arterioles were completely ligated or occluded. It should be noted, however, that an advantage of small HBOCs, including HbVs, is that they are homogeneously dispersed in the plasma phase and therefore can deliver O_2 more homogeneously to the periphery than RBCs because microvascular hematocrit is heterogeneous particularly in pathological states. In such conditions, HbVs with a higher O_2 affinity should show a slower O_2 unloading that would be effective for oxygenating ischemic tissues.

In conclusion, HbVs provide the unique feature of allowing for the regulation of P_{50} by modulating the amount of coencapsulated PLP (33, 45). Recent studies showed the effectiveness of HBOCs with a lower P_{50} (higher O_2 affinity) as a means of implementing O_2 delivery targeted to ischemic tissue (2, 3, 41, 43). Thus this experimental method provides data useful for the design and optimization of O_2 carriers and suggests the possible utilization of HbVs for therapeutic approaches aimed at remedying ischemic conditions.

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OXYGEN RELEASE FROM HB VESICLES

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Title: New generation of hemoglobin-based oxygen carriers evaluated for oxygenation of critically ischemic hamster flap tissue

Author(s): Claudio Contaldo MD; Jan Plock MD; Hiromi Sakai PhD; Shinji Takeoka PhD; Eishun Tsuchida PhD; Michael Leunig MD; Andrej Banic MD, PhD; Dominique Erni MD

Objectives: The aim of this study was to investigate and compare the effects of a traditionally formulated, low-viscosity, right-shifted polymerized bovine hemoglobin solution and a highly viscous, left-shifted hemoglobin vesicle solution (HbV-HES) on the oxygenation of critically ischemic peripheral tissue.

Design: Randomized, prospective study.

Setting: University laboratory.

Subject: A total of 40 male golden Syrian hamsters.

Interventions: Island flaps were dissected from the back skin of anesthetized hamsters. The flap included a critically ischemic, hypoxic area that was perfused via a collateralized vasculature. One hour after completion of the preparation, the animals received a 33% blood exchange with 6% hydroxyethyl starch 200/0.5 (HES, n = 9), HbV suspended in HES (HbV-HES, n = 8), or polymerized bovine hemoglobin solution (n = 9).

Measurements and Main Results: Three hours after the blood exchange, microcirculatory blood flow (laser-Doppler flowmetry) was increased to 262% of baseline for HbV-HES (p < .01) and 197% for polymerized bovine hemoglobin solution (p < .05 vs. baseline and HbV-HES). Partial tissue oxygen tension (bare fiber probes) was only improved after HbV-HES (9.4 torr to 14.2 torr, p < .01 vs. baseline and other groups). The tissue lactate/pyruvate ratio (microdialysis) was elevated to 51 in the untreated control animals, and to 34 \pm 8 after HbV-HES (p < .05 vs. control) and 38 \pm 11 after polymerized bovine hemoglobin solution (not significant).

Conclusions: Our study suggests that in critically ischemic and hypoxic collateralized peripheral tissue, oxygenation may be improved by

normovolemic hemodilution with HbV-HES. We attributed this improvement to a better restoration of the microcirculation and oxygen delivery due to the formulation of the solution.

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Exchange transfusion with entirely synthetic red-cell substitute albumin-heme into rats: Physiological responses and blood biochemical tests

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Abstract: Recombinant human serum albumin (rHSA) incorporating 2-[8-{N-(2-methylimidazolyl)}]octanoyloxymethyl]-5,10,15,20-[tetrakis{ $\alpha,\alpha,\alpha,\alpha$ -o-(1-methylcyclohexanoyl)amino}-phenyl]porphinatoiron(II) [albumin-heme (rHSA-heme)] is an artificial hemoprotein which has the capability to transport O_2 in vitro and in vivo. A 20% exchange transfusion with rHSA-heme into anesthetized rats has been performed to evaluate its clinical safety by monitoring the circulation parameters and blood parameters for 6 h after the infusion. Time course changes in all parameters essentially showed the same features as those of the control group (without infusion) and rHSA

group (with administration of the same amount of rHSA). Blood biochemical tests of the withdrawn plasma at 6 h after the exchange transfusion have also been carried out. No significant difference was found between the rHSA-heme and rHSA groups, suggesting the initial clinical safety of this entirely synthetic O₂-carrier as a red-cell substitute. © 2004 Wiley Periodicals, Inc. J Biomed Mater Res 71A: 63–69, 2004

Key words: exchange transfusion; entirely synthetic red-cell substitute; albumin-heme; blood biochemical tests; O₂ carrier.

INTRODUCTION

Although hemoglobin (Hb)-based O_2 carriers are currently undergoing clinical trials as red-cell substitutes or oxygen therapeutics, there are still some concerns about new infectious pathogens in Hb and unresolved side effects such as vasoconstriction. He Recombinant human serum albumin (rHSA) incorporating the synthetic heme albumin-heme is an artificial hemoprotein that has the potential to bind and release O_2 under physiological conditions in the same manner as Hb and myoglobin. In fact, the albumin-heme can transport O_2 through the body and release O_2 to tissues as a red-cell substitute without any acute side effects. For example, rHSA including four molecules of 2-[8-[N-(2-methylimidazolyl)]-octanoyloxymethyl]-5,10,15,20-[tetrakis[$\alpha,\alpha,\alpha,\alpha-o$ -(1-methylcyclohexanoyl)amino]phenyl]porphinatoiron(II)

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(Scheme 1) is one of the promising materials.⁷ Recent study on the 30% exchange transfusion with rHSA-heme after 70% hemodilution with 5 wt % rHSA with the use of anesthetized rats demonstrated that the administration of this material improved the circulatory volume and resuscitated the hemorrhagic shock state.¹⁰ The declined MAP and the mixed venous partial O₂ pressure immediately recovered, and the lowered renal cortical O₂-pressure also significantly increased.

In order to evaluate the initial clinical safety of this albumin-based O₂-carrier, a 20% exchange transfusion with rHSA-heme into anesthetized rats was performed, and the time courses of the circulation parameters (MAP, HR, respiration rate) and blood parameters (paO₂, pvO₂, pH, blood cell numbers) were measured for 6 h, which is adequate time to determine acute toxicity. Blood biochemical tests of the withdrawn plasma were also been carried out.

MATERIALS AND METHODS

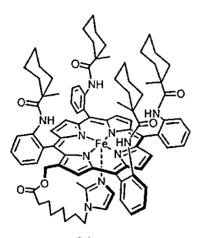
Preparation of rHSA-heme

Recombinant human scrum albumin (rHSA, Albrec*, 25 wt %) was obtained from the NIPRO Corp. (Osaka). The 5

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Scheme 1

g/dL rHSA was made by diluting Albrec* with saline solution (Otsuka Pharmaceutical Co., Ltd.). The rHSA-heme solution ([rHSA]: 4.9 g/dL, pH 7.45, [heme]: 2.8 mM, O_2 -binding affinity ($p_{1/2}O_2$): 37 Torr) used for the experiments was prepared according to a previously reported procedure. The red-colored rHSA-heme solution was filtered with the use of DISMIC 25CS045AS just before use.

Exchange transfusion

The investigations were carried out with 18 male Wister rats (305±3.6 g). The animals were placed on the heating pad under an inhalation anesthesia with sevofluran; its concentration was kept 2.0% for the operations and 1.5% for the experiments. After incision was made in the neck, the heparinized catheter (Natsume Seisakusho SP-55) was introduced into the right common carotid artery for blood withdrawal. Other catheters (SP-31) were inserted into the left femoral artery for a continuous MAP monitoring, and the right femoral vein for sample injection.

After stabilization of the animal condition, the 20% exchange transfusion (total blood volume of rat was estimated to be 64 mL/kg weight) was performed by 1 mL blood withdrawal via the common carotid artery and 1 mL rHSAheme infusion from the femoral vein (each 1 mL/min) with four repeating cycles (n = 6, rHSA-heme group). Blood was taken from the artery (0.3 mL) and vein (0.2 mL) at the following five points; (i) before, (ii) immediately after, (iii) 1 h after, (iv) 3 h after, and (v) 6 h after the exchange transfusion. MAP and HR were recorded with the use of a polygraph system (NIHON KODEN LEG-1000 Ver. 01-02 or PEG-1000 Ver. 01-01) at the same time point as stated above. Withdrawn blood was rapidly applied to a blood gas system (Radio Meter Trading ABL555) to obtain the O2-pressure (paO_2) and pH for the arterial blood, and the O_2 -pressure (pvO₂) for the venous blood. The blood cell numbers were counted by a multisystem automatic blood cell counter (Sysmex KX-21). After 6 h, 4 mL of the venous blood was taken for each animal before sacrifice by sodium pentobarbital overdose. The blood samples were centrifuged at 4°C (Beckman Coulter Co., Optima LE-80K for 3500 × rpm, 10 min), and the plasma phase was frozen (-20°C) for blood biochemical tests. As a reference group, the 5 g/dL rHSA solution was administered similarly into rats (n = 6, rHSA group). Furthermore, six rats without infusion (operation only) were also set as a control group.

All animal handling and care was in accordance with the NIH guidelines. The protocol details were approved by the Animal Care and Use Committee of Keio University.

Blood biochemical tests

A total of 30 analytes, that is, total protein (TP), albumin (Alb), albumin/globulin ratio (A/G), aspartate aminotransferase (AST), alanine aminotransferase (ALT), lactate dehydrogenase (LDH), alkaline phosphatase (ALP), γ -glutamyltransferase (γ -GTP), leucine aminopeptidase (LAP), choline esterase (ChE), total bilirubin (TBil), direct bililubin (DBil), creatinine (CRN), blood urea nitrogen (BUN), uric acid (UA), amylase, lipase, creatine phosphokinase (CPK), total cholesterol (TCho), free cholesterol (FCho), cholesterol ester (ECho), β -lipoprotein (β -LP), high-density lipoprotein (HDL)-cholesterol, neutral fat (triglyceride, TG), total lipid, free fatty acid (FFA), phospholipids (PhL), K⁺, Ca²⁺ and Fe³⁺, were measured by Kyoto Microorganism Institute (Kyoto).

Data analysis

MAP, HR, respiration rate, paO_2 and pvO_2 were represented as percent ratios of the basal values with mean \pm standard error of mean (SEM). Body temperature, pH, blood cell numbers and the data of blood biochemical tests were shown as mean \pm SEM.

Statistical analysis were performed by repeated-analysis measures of variance (ANOVA) followed by the paired t-test for comparison with a basal value (body temperature), by the Bartlett test followed by the Tukey-Kramer multiple comparison test for pH, blood cell numbers, and the results of the blood biochemical tests, and by the Kruskal-Wallis test followed by the Tukey-Kramer multiple comparison test for more than three groups (MAP, HR, respiration rate, paO_2 , and pvO_2). Values of p < 0.05 were considered significant. The statistical analytical software used was StatView (SAS Institute, Inc.).

RESULTS

Circulation parameters

The basal values of some measurements, the data values of which are represented by percent ratios, are summarized in Table I. There are no significant differences between the three groups (control, rHSA, and rHSA-heme groups).

The body temperature of each group was constantly

TABLE I Basal Values of Each Group

	Control	rHSA	rHSA-heme
MAP (mmHg)	99 ± 2.8	101 ± 2.8	100 ± 6.1
HR (beats/min)	404 ± 19	435 ± 19	420 ± 13
Respiration rate			
(breaths/min)	66 ± 0.7	75 ± 4.0	70 ± 2.1
paO ₂ (mmHg)	84.7 ± 3.1	84.9 ± 3.7	80.8 ± 2.2
pvO ₂ (mmHg)	51.0 ± 1.5	45.7 ± 1.1	51.0 ± 1.7
Body weight (g)	305 ± 4.0	304 ± 2.8	305 ± 4.1

maintained within 36.9-37.4°C during the experiments [Fig. 1(a)].

The MAP time course in the control group demonstrated only a small deviation within 83.8–100.0% for 6 h. In the rHSA and rHSA-heme groups, the observed changes in MAP were almost the same as those of the control group. They ranged within 93.2–100 and 89.3–100%, respectively. It is remarkable that no vasoactive reaction was seen after the infusion of rHSA-heme [Fig. 1(b)].

The HR of the control, rHSA, and rHSA-heme groups remained unaltered for 6 h. The values of the control, rHSA, and rHSA-heme groups were in the range of 98.3–103.9, 96.9–108.8, and 85.7–100.0%, respectively [Fig. 1(c)].

The respiration rates also remained stable during

the measurements. No significant difference was recognized among the three groups [Fig. 1(d)].

Blood-gas parameters

No difference in the pH changes was observed in the three groups. The pH values of the control, rHSA, and rHSA-heme groups were constant in the narrow ranges of 7.42–7.45, 7.42–7.44, and 7.42–7.44, respectively [Fig. 2(a)].

The paO_2 values of the control, rHSA, and rHSA-heme groups were also constant in the range of 100–108.1, 100–109.1, and 100–110.8%, respectively, by the end of measurements [Fig. 2(b)].

The pvO_2 of the control, rHSA and rHSA-heme groups demonstrated only small changes within 81.5–100.0, 84.9–108.4, and 81.9–100.0%, respectively [Fig. 2(c)].

Blood cell numbers

The Hct values of the control group were unchanged from 34.8–37.0% during the experiment. On the other hand, the 20% exchange transfusion with the

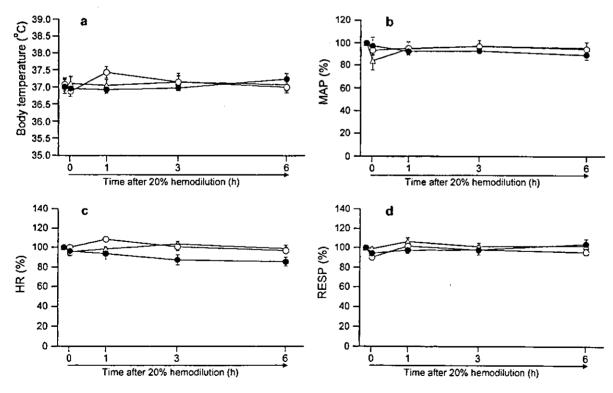


Figure 1. (a) Time courses of body temperature, (b) mean arterial pressure (MAP), (c) heart rate (HR), and (d) respiration rate (RESP) in anesthetized rats after 20% exchange transfusion with rHSA-heme or rHSA solution. Each value represents the mean ± SEM of six rats (triangles, control group without infusion; open circles, rHSA group; solid circles, rHSA-heme group).

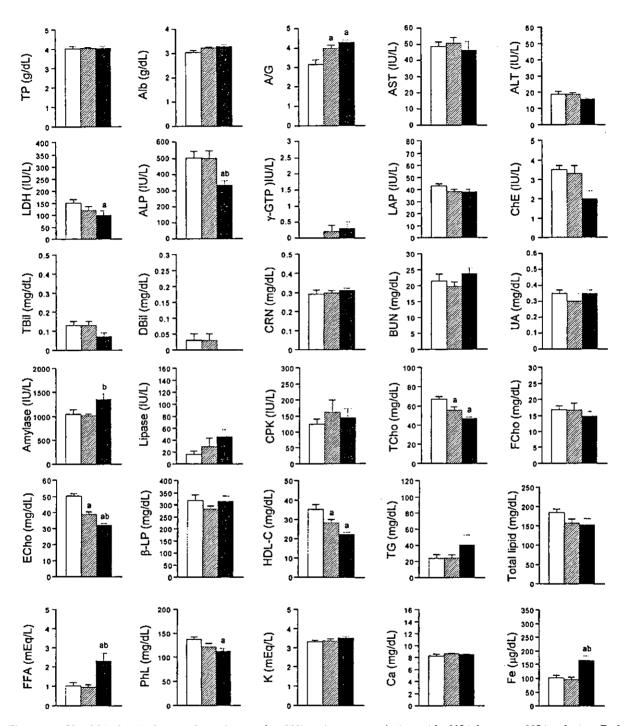


Figure 4. Blood biochemical tests of rat plasma after 20% exchange transfusion with rHSA-heme or rHSA solution. Each value represents the mean \pm SEM of six rats (white bar, control group without infusion; diagonal bar, rHSA group; black bar, rHSA-heme group). $^{a}p < 0.05$ versus control group (Tukey-Kramer test), $^{b}p < 0.05$ versus rHSA group (Tukey-Kramer test).

with rHSA-heme. These results showed the initial clinical safety of the rHSA-heme solution, which allows us to undergo further advanced preclinical testing of this synthetic O_2 -carrying hemoprotein as a new class of red-cell substitutes. Biochemical tests and histopathological observations for 7 days after the exchange

transfusion with rHSA-heme will be reported in a forthcoming article.

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Synthesis of protoheme IX derivatives with a covalently linked proximal base and their human serum albumin hybrids as artificial hemoprotein

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The simple one-pot reaction of protoporphyrin IX and ω -(N-imidazolyl)alkylamine or O-methyl-L-histidyl-glycine with benzotriazol-1-yl-oxytris(dimethylamino)phosphonium hexafluorophosphate at room temperature produced a series of protoporphyrin IX species with a covalently linked proximal base at the propionate side-chain. The central iron was inserted by the general FeCl₂ method, converting the free-base porphyrins to the corresponding protoheme IX derivatives. Mesoporphyrin IX and diacetyldeuteroporphyrin IX analogues were also prepared by the same procedure. The Fe(II) complexes formed dioxygen (O₂) adducts in dimethylformamide at 25 °C. Some of them were incorporated into the hydrophobic domain of recombinant human serum albumin (rHSA), providing albumin-heme hybrids (rHSA-heme), which can bind and release O₂ in aqueous media (pH 7.3, 25 °C). The oxidation process of converting the dioxygenated heme in rHSA to the inactive Fe(III) state obeyed first-order kinetics, indicating that the μ -oxo dimer formation was prevented by the immobilization of heme in the albumin scaffold. The rHSA-heme, in which the histidylglycil tail coordinates to the Fe(II) center, showed the most stable O₂ adduct complexes.

Introduction

Numerous model compounds of hemoglobin (Hb) and myoglobin (Mb) have already been prepared and their O2-binding equilibria and kinetics were extensively studied. In particular, synthetic hemes having a sterically encumbered porphyrin platform can form stable O2 adducts in organic solvent at room temperature. If we are to reproduce or mimic any biochemical reaction, the aqueous medium is particularly important. The dioxygenated complexes of highly-modified hemes are unfortunately oxidized to the ferric state in water. Human serum albumin (HSA) is the most abundant plasma protein in our circulatory system and solubilizes hydrophobic small molecules.2 We have found that synthetic hemes are also spontaneously incorporated into HSA, which provides unique albumin-heme hybrids (HSAhemes) and allows their Fe(11) states to remain stable in aqueous solution.3 Actually, recombinant HSA4 (rHSA) including tetrakis(a,a,a,a-o-pivalamidophenyl)porphinatoiron(II) with a covalently linked proximal base can reversibly bind and release O2 under physiological conditions, and acts as an artificial O2 transporter in the blood stream.5 Our next target is to realize O2 coordination to rHSA-heme involving protoheme IX in the same manner as natural Hb and Mb. The dioxygenation of protoheme IX has several advantages. (1) Synthetic procedures are rather simplified with respect to the highly modified tetraphenylporphyrin. (2) It has the same structure and thus the same spectra as do hemoproteins; this makes possible the study of subtle changes in the protein nanostructure. (3) Its metabolism process has been clarified,6 which is an advantage for medical use as an artificial O2 carrier.

We report herein the simple synthetic methodology of protoheme IX derivatives with a covalently-linked proximal imidazolyl arm and the O₂-binding properties of the obtained rHSA-hemes.

Results and discussion

Synthesis

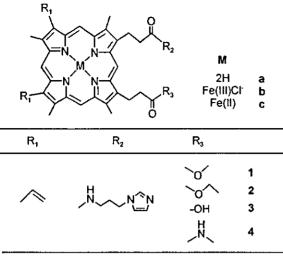
The free-base porphyrins with a covalently linked proximal base (1a-8a, Scheme 1) were synthesized by the one-pot reaction of protoporphyrin IX, ω -(N-imidazolyl)alkylamine

[R₂H; 3-(N-imidazolyl)propylamine, 4-(N-(2-methylimidazolyl))butylamine or O-methyl-L-histidyl-glycine] for one propionic acid group, and a capping alcohol or amine on the other side (R3H; MeOH, EtOH or MeNH2) in the presence of benzotriazol-1-yl-oxytris(dimethylamino)phosphonium hexafluorophosphate (BOP) at 25 °C in pyridine [or dimethylformamide (DMF)] (Scheme 2). The carbonyl attachment was made through either an ester or an amide function. After the reaction, the mixture was poured into 10% NaCl solution, which led to the precipitation of the crude porphyrin. Centrifugation at 7000 g for 30 min gave a purple pellet. The pyridine (or DMF), BOP, R₂H and R₃H in the supernatant were all discarded at this point. The obtained precipitate was dissolved in CHCl₃ and showed several spots on a thin layer chromatograph. The anpolar band corresponds to the double R3-substituted component (ex. protoporphyrin IX diethyl ester in the cases of 2, 5, 6) and the second band is the desired porphyrin, which is purified by a silica gel chromatographic separation (yield: 20-30%). The iron was then inserted by the general FeCl2 method with 2,6-lutidine in DMF solution, giving the corresponding hemins. Mesoporphyrin IX and diacetyldeuteroporphyrin IX also gave similar analogues (7b and 8b). We obtained a mixture of two isomeric compounds that we were unable to separate.

Traylor and co-workers reported many pioneering studies on "chelated hemes". They synthesized compound 1b, for instance, using an acid anhydride procedure directly from protohemin chloride. First, the protohemin dimethyl ester was partially hydrolyzed and, after purification, the mono acid was coupled to a 3-(N-imidazolyl)propylamine by the pivaloyl chloride method. Nevertheless, reaction mixtures involving the diacid and monoacid are normally insoluble in common organic solvents, therefore, the yield of this reaction largely depends on the separation techniques. In contrast, our simple procedure makes it possible to synthesize a series of new protoporphyrins with a wide variety of proximal bases and end-capping groups of the other propionic acid.

Dioxygenation of heme in DMF solution

The obtained hemin complexes 1b-8b in DMF solution were reduced to the corresponding Fe(11) complexes using a solution



Scheme 1

of the crown ether-dithionite as reducing agent.8 The UV-vis absorption spectrum of 2c [Fe(II) complex] under a nitrogen (N_2) atmosphere showed a single broad band in the α,β region around 520-580 nm. This indicates the formation of a typical five-N-coordinate high-spin complex,7 in which the proximal imidazole group intramolecularly coordinates to the central Fe(II) ion in the non-coordinating solvent (DMF) (Fig. 1). Because 2-methyl-imidazole significantly inhibits a sixth ligand binding to the trans-position, 6c also demonstrated a similar 5coordinated spectrum in DMF solution. Upon bubbling of the O2 gas through the solution of 2c, the spectral pattern immediately changed to that of the O2 adduct complex. After adding carbon monoxide (CO) gas, the heme changed to a very stable carbonyl complex. Similar absorption changes were observed for all the heme derivatives, 1c-8c. The absorption maxima (λ_{max}) of compounds 1c-8c in DMF solution under N_2 , O_2 and CO atmospheres are summarized in Table 1.

The positions and the relative intensities of all peaks were independent of the temperature changes from 5 to 25 °C. In general, the electron density of the porphyrin ring systematically changes the λ_{max} of the B-band and Q-band. The replacement of the vinyl groups at the 3,8-positions of protoheme IX with ethyl groups (from 2c to 7c) produced a hypsochromic shift. In contrast, changing the vinyl groups to electron withdrawing acetyl groups (from 2c to 8c) produced a bathochromic shift.

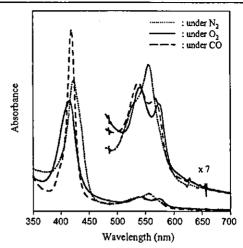


Fig. 1 UV-vis spectra of 2c in DMF at 25 °C.

Table 1 Absorption maxima (λ_{max}) of heme derivatives in DMF under various conditions

	λ_{max}/nm				
Compound	Under N ₂	Under O2	Under CO		
1c (15 °C)	427, 530, 558	414, 543, 575	420, 540, 569		
1c (25 °C)	424, 532, 559	412, 542, 575	420, 539, 567		
2c (5 °C)	422, 531, 556	415, 541, 574	419, 537, 567		
2c (25 °C)	421, 533, 557	409, 539, 571	418, 537, 565		
3c (25 °C)	426, 537, 559	415, 543, 575	420, 539, 567		
4c (5 °C)	421, 527, 555	413, 540, 572	417, 536, 564		
5c (5 °C)	419, 529, 551	406, 537, 569	412, 534, 562		
5c (25 °C)	423, 533, 557	408, 539, 573	419, 538, 567		
6c (5 °C)	430, 555	413, 547, 576	418, 538, 561		
7c (25 °C)	414, 523, 548	407, 531, 563	409, 529, 556		
8c (5 °C)	440, 541, 571	432, 552, 579	434, 549, 576		
8c (25 °Ć)	439, 545, 569	431, 552, 580	433, 548, 577		

We could not find any significant difference in the absorption maxima of 1c-6c, because modification of the propionic acids did not affect the electron density of the porphyrin macrocycle.

Preparation of rHSA-heme

Aqueous solutions of rHSA-heme were prepared by injecting an ethanol solution of the carbonylated heme into an aqueous solution of rHSA. The inclusion of heme into rHSA was confirmed by the following results: (1) Sepharose gel column chromatography showed the elution peaks of heme and rHSA coincided at the same position, (2) during dialysis of the rHSA-heme solution against phosphate buffer, the outer aqueous phase did not contain the heme component. The UV-vis absorption spectra of the obtained solution showed that the heme was retained as a CO adduct complex.

The binding number of heme in one rHSA was determined to be 0.9-1.1 (mol/mol) by assaying the iron and rHSA concentrations. The binding constant of 1b for rHSA was estimated to be ca. 4×10^6 M⁻¹, which is approximately 1/25 of that for protohemin IX itself to albumin (ca. 1×10^8 M⁻¹). Polar heme derivatives 3c with monopropionic acid and 4c with a methyl-

 $BOP: benzotriazol-1-yl-oxytris (dimethylamino) phosphonium \ hexafluorophosphate$

Scheme 2 Synthesis of protoheme IX derivatives.

Table 2 Absorption maxima (λ_{mix}) of rHSA-hemes in phosphate buffer solution (pH 7.3) at 25 °C

Compounds	λ _{max} /nm			
	Under N ₂	Under O2	Under CO	
tHSA-1c	420, 536, 561	414, 540, 567	419, 541, 566	
rHSA-2c	420, 538, 561	416, 540, 567	421, 543, 567	
rHSA-5c	422, 539, 561	418, 540, 571	422, 541, 569	
rHSA-8c	444, 549, 571	432, 551, 580	440, 555, 578	

amide capping group at the porphyrin periphery were partially oxidized to the Fe(III) state during the inclusion process. Since the binding force of the heme derivative to rHSA is a hydrophobic interaction, ¹¹ relatively polar porphyrins may not be incorporated into a certain domain of rHSA and easily oxidized compared to more apolar ones.

The circular dichroism spectra of the rHSA-hemes (rHSA-1c, -2c, -5c, -7c and -8c) are almost identical to that of rHSA itself (not shown). This suggests that the secondary structure of the albumin host molecule did not change after incorporation of the hemes. Furthermore, the isoelectric points of these rHSA-hemes were all 4.8, which is the original value of rHSA. The surface net charges of rHSA remained unaltered after heme incorporation.

Dioxygenation of rHSA-heme in aqueous solution

Light irradiation of the CO adduct complex of rHSA-heme (rHSA-1c, -2c, -5c, -6c, -7c and -8c) under an N_2 atmosphere led to CO dissociation and demonstrated new spectral patterns with well-defined α and β bands. For example, the typical absorption spectral changes of rHSA-2c are shown in Fig. 2.

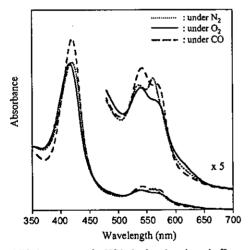


Fig. 2 UV-vis spectra of rHSA-2c in phosphate buffer solution (pH 7.3) at 25 °C.

From the nature of these spectra, we concluded that the obtained Fe(II) complexes are a mixture of Fe(II) 5-coordinated (high-spin) and 6-coordinated (low spin) species. It implies that the sixth coordinate position of the heme might be partially occupied by some amino acid residue of the protein scaffold. Upon exposure of O₂ to the Fe(II) complex of rHSA-1c, the spectrum changed to that of the O₂ adduct species. Although the aqueous micelle solution of 1c with 5% surfactant (cetyl-trimethylammonium bromide) forms a CO adduct complex, dioxygenation was not stable enough to measure the spectrum at 25 °C. In contrast, rHSA-1c, -2c, -5c, and -8c formed O₂ adduct complexes at 25 °C (pH 7.3) except for rHSA-6c and -7c (Table 2). The introduction of a methyl group to the 2-position of the imidazole ring is widely recognized to reduce the O₂ and CO binding affinities. In this case, the strength of the imidazole

Table 3 Half-life $(\tau_{1/2})$ and O_2 binding affinity $(P_{1/2})$ of rHSA-hemes in phosphate buffer solution (pH 7.3) at 25 °C

Compounds	τ ₁₀ /min	$P_{1/2}$ /Torr	
rHSA-1c	20	0.1	
rHSA-2c	50	0.1	
rHSA-5c	90	0.1	
rHSA-8c	50	0.4	

coordination to the Fe(II) center is too weak to produce a stable O_2 adduct complex.

The oxidation process of dioxygenated rHSA-heme to the inactive Fe(III) state obeyed first-order kinetics. This indicates that the μ -oxo dimer formation was prevented by the immobilization of heme in the albumin structure. The half-life of the O_2 adduct complexes ($\tau_{1/2}$) and the O_2 binding affinities ($P_{1/2}$) of rHSA-hemes are summarized in Table 3. The histidylglycyl tail coordinated protoheme (5c) in rHSA showed the most stable O_2 adduct complex ($\tau_{1/2}$: 90 min) with respect to the imidazole bound ones. The more hydrophobic ethylpropionate (2c) also contributed to prolong the stability of the O_2 adduct complex relative to the methylpropionate protoheme (1c).

The $P_{1/2}$ values of rHSA-1c, -2c and -5c are 0.1 Torr at 25 °C. On the other hand, rHSA-8c showed a higher $P_{1/2}$ value (low O_2 -binding affinity) compared to the others. The acetyl groups at the 3,8-positions of 8c decrease the electron density of the porphyrin macrocycle, therefore $P_{1/2}$ could be significantly reduced. Traylor and co-workers found that the O_2 binding affinity of the chelated heme was sensitive to the electron density at Fe(II) and thus to the substituents at the heme periphery. The O_2 binding constant decreased by 1/6 upon changing the substituent from a vinyl to an acetyl group. 12 Our experimental data of hemes in rHSA are quite consistent with their observations.

Conclusion

A convenient one-pot synthesis of protoporphyrin IX derivatives with a covalently linked proximal base has been described. rHSA successfully incorporates the protoheme derivatives, providing an artificial hemoprotein, which can form an O_2 adduct complex at 25 °C. The rHSA-heme, in which the histidylglycil tail intramolecularly coordinates to the Fe(11) center, showed the most stable O_2 adduct complex with the relatively high O_2 binding affinity of 0.1 Torr.

Experimental

Materials and apparatus

All reagents were used as supplied commercially unless otherwise noted. All solvents were normally purified by distillation before use. DMF was distilled under reduced pressure in N_2 . Pyridine was refluxed over and distilled from P_2O_5 . The water was deionized using an ADVANTEC GS-200 system. The rHSA (Albrec*, 25 wt%) was obtained from NIPRO Corp. (Osaka).

Thin-layer chromatography was carried out on 0.2 mm precoated plates of silica gel 60 F254 (Merck). Purification was performed by silica gel 60 (Merck) column chromatography. The infrared spectra were measured with a JASCO FT/IR-410 spectrometer. The UV-vis absorption spectra were recorded by a JASCO V-570 spectrophotometer. The 'H-NMR spectra were recorded using a JEOL Lambda 500 spectrometer. Chemical shifts were expressed in parts per million downfield from Me₄Si as the internal standard. The FAB-MS spectra were obtained using a JEOL JMS-SX102A spectrometer.

Synthesis of porphyrin derivatives

O-Methyl-L-histidyl-glycine¹³ and 4-(N-(2-methylimidazolyl))-butylamine¹⁴ were synthesized according to the reported procedures.

3,18-Divinyl-8-(3-methoxycarbonyl)ethyl-12-(3-(N-imidazolyl)propylamido)ethyl-2,7,13,17-tetramethylporphyrin (1a). A pyridine (7 mL) solution of 3-(N-imidazolyl)propylamine (35 µL, 0.29 mmol) was added dropwise to protoporphyrin IX (200 mg, 0.36 mmol) and benzotriazol-1-yloxytris-(dimethylamino)phosphonium hexafluorophosphate (411 mg, 0.93 mmol) in pyridine (20 mL) and stirred for 30 min at room temperature. The mixture was reacted for 4 h at 40 °C. After the addition of methanol (10 mL), the solution was stirred for another 12 h at 40 °C. The mixture was then poured into a 10% NaCl solution (1 L, 4 °C) and the suspension was centrifuged for 30 min at 7000g. The supernatant was discarded and the precipitate was collected and dried in vacuo. The residue was chromatographed on a silica gel column using CHCl₃/CH₃OH = 8/1 (v/v) as the eluent. The main band was collected and dried at room temperature for several hours in vacuo, giving compound 1a as a purple solid (75 mg, 20%). $R_f = 0.3$ $(CHCl_3/CH_3OH = 8/1 (v/v))$; IR (NaCl) v = 1731 (C=O, ester), 1646 (C=O, amide) cm⁻¹; UV-vis (CHCl₃) $\lambda_{max} = 408, 506, 542,$ 575, 630 nm; ¹H-NMR (CDCl₃) δ: -4.0 (s, 2H, inner), 1.8-2.4 $(m, 4H, -(CH_2)-Im), 2.7 (m, 4H, -CH_2-COO-, NH-CH_2-), 3.2$ $(t, 2H, -CONH-CH_{2-}), 3.3-3.7 \text{ (m, 18H, por-CH₃, -CH₂-CO-,$ -COOCH₃), 4.2 (d, 4H, por-CH₂-), 5.4 (s, 1H, Im), 6.0-6.3 (m, 4H, =CH₂ (vinyl)), 6.4 (d, 1H, Im), 6.6 (d, 1H, Im), 8.0-8.4 (m, 2H, -CH = (vinyl), 9.7 (m, 4H, meso); MS m/z: 681.67.

Fe(111) complex of 1a (1b). Iron(11) chloride tetrahydrate (106 mg, 0.53 mmol) was added to a dry DMF (10 mL) solution of 1a (36 mg, 53 µmol) and 2,6-lutidine (30 µL, 0.27 mmol) under an N2 atmosphere. The reaction mixture was stirred at 70 °C for 3 h. After confirming the disappearance of the porphyrin's fluorescence (600-800 nm, ex. 400 nm), the solution was cooled to room temperature and poured into 10% NaCl solution (1 L, 4 °C). The suspension was centrifuged for 30 min at 7000g and the supernatant was discarded. The precipitate was dried in vacuo and chromatographed on a silica gel column using CHCl₃/CH₃OH = 8/1 (v/v) as the eluent. The main band was collected and dried at room temperature for several hours in vacuo to give compound 1b as a brown solid (27 mg, 68%). $R_f = 0.3$ (CHCl₃/CH₃OH = 8/1); IR (NaCl) $\nu = 1728$ (C=O, ester), 1646 (C=O, amide) cm⁻¹; UV-vis (CHCl₃) $\lambda_{max} = 389$, 513, 641 nm; HR-MS m/z: calcd for C41H43O3N7Fe: 737.2777, found: 737.2778 [M+].

3,18-Divinyl-8-(3-ethoxycarbonyl)ethyl-12-(3-(N-imidazolyl)-propylamido)ethyl-2,7,13,17-tetramethylporphyrin (2a). The synthetic procedure of compound 2a was the same as that used for 1a except for using ethanol instead of methanol. Yield 30%; $R_{\rm f} = 0.4$ (CHCl₃/CH₃OH = 10/1); IR (NaCl) $\nu = 1650$ (C=O, amide), 1732 (C=O, ester) cm⁻¹; UV-vis (CHCl₃) $\lambda_{\rm max} = 409$, 544, 580, 633 nm; ¹H-NMR (CDCl₃) δ : -4.1 (s, 2H, inner-NH), 0.8-0.9 (t, 3H, -COO-CH₂-CH₃), 1.3-1.5 (t, 2H, -CONH-CH₂-CH₂-), 3.0-3.1 (t, 2H, -CH₂-Im), 3.1-3.3 (m, 4H, -CH₂-COO), 3.5-3.7 (m, 12H, por-CH₃), 3.8-3.9 (m, 2H, -COO-CH₂-CH₃), 4.2-4.4 (d, 4H, por-CH₂-), 6.1 (s, 1H, Im), 6.1-6.4 (q, 5H, =CH₂ (vinyl), Im), 6.6-6.7 (d, 1H, Im), 6.9-7.0 (d, 1H, Im), 8.1-8.3 (m, 2H, -CH= (vinyl)), 9.8-10.2 (m, 4H, meso); MS m/z: 695.29.

Fe(III) complex of 2a (2b). Iron insertion to 2a was carried out by the same procedure as in the 1b preparation. Yield 80%; $R_f = 0.3$ (CHCl₃/CH₃OH = 8/1); IR (NaCl) $\nu = 1651$ (C=O, amide), 1725 (C=O, ester) cm⁻¹, UV-vis (CHCl₃) $\lambda_{max} = 406$, 520, 578 nm; HR-MS m/z: calcd. for $C_{42}H_{45}O_3N_7Fe$: 751.2933, found: 751.2953 [M*].

3,18-Divinyl-8-(3-carboxy)ethyl-12-(3-(N-imidazolyl)propylamido)ethyl-2,7,13,17-tetramethylporphyrin (3a). Sodium hydroxide (2 N, 4.5 mL) was added to the methanol (10 mL) solution of 2a (266 mg, 0.38 mmol) and the mixture was stirred

for 12 h at room temperature. It was brought to dryness in vacuo. Methanol was added to the residue and the mixture was added dropwise to 10% NaCl solution (pH 2, 4 °C). It was centrifuged for 30 min at 7000g and the precipitate was collected and dried in vacuo, affording compound 3a as a brown solid (187 mg, 78%), IR (KBr) $\nu = 1652$ (C=O, amide), 1707 (C=O, -COOH) cm⁻¹; UV-vis (DMSO) $\lambda_{max} = 409$, 508, 543, 578, 631 nm; ¹H-NMR (dg-DMSO) δ : -3.5 (s, 2H, inner-NH), 1.6-1.7 (t, 2H, -CONH-CH₂-CH₂-), 2.8-2.9 (t, 2H, -CH₂-Im), 3.1-3.3 (m, 2H, -CONH-CH₂-), 3.5-3.9 (m, 12H, por-CH₃), 4.2-4.4 (d, 4H, por-CH₂-), 6.1 (s, 1H, Im), 6.1-6.4 (q, 5H, =CH₂ (vinyl), Im), 6.6-6.7 (d, 1H, Im), 6.9-7.0 (d, 1H, Im), 8.5-8.6 (m, 2H, -CH= (vinyl)), 10.2-10.4 (m, 4H, meso); MS m/z: 670.41.

Fe(III) complex of 3a (3b). Iron insertion to 3a was carried out by the same procedure as in the 1b preparation. Yield 80%; IR (KBr) $\nu = 1646$ (C=O, amide), 1707 (C=O, -COOH) cm⁻¹; UV-vis (DMSO) $\lambda_{max} = 403$, 508, 631 nm; HR-MS m/z: calcd. for $C_{40}H_{41}O_3N_7Fe$: 723.2620, found: 724.2668 [M + H⁺].

3,18-Divinyl-8-(3-methylamido)ethyl-12-(3-(N-imidazolyl)-propylamido)ethyl-2,7,13,17-tetramethylporphyrin (4a). Compound 4a was synthesized according to the same procedure as for 1a except for using methyl amine instead of methanol. Yield 20%; $R_f = 0.5$ (CHCl₃/CH₃OH = 3/1); IR (NaCl) $\nu = 1631$ (C=O, amide) cm⁻¹; UV-vis (CHCl₃) $\lambda_{\text{max}} = 409$, 509, 543, 579, 632 nm; ¹H-NMR (CD₃OD, CDCl₃) δ : -4.0 (s, 2H, inner), 1.8-2.4 (m, 4H, -(CH₂)₂-Im), 2.5 (t, 3H, -CONH-CH₃), 2.9 (m, 2H, -CONH-CH₂-), 3.3 (m, 4H, -CH₂-CONH-), 3.4-3.6 (m,12H, por-CH₃), 5.5 (s, 1H, Im), 6.0 (s, 1H, Im), 6.1-6.4 (m, 4H, =CH₂ (vinyl)), 6.8 (m, 1H, Im), 8.1-8.3 (m, 2H, -CH= (vinyl)), 9.7-9.9 (q, 4H, meso); MS m/z: 680.69.

Fe(III) complex of 4a (4b). Iron insertion to 4a was carried out by the same procedure as in the 1b preparation. Yield 67%; $R_f = 0.3$ (CHCl₃/CH₃OH = 5/1); IR (NaCl) $\nu = 1646$ (C=O, amide) cm⁻¹; UV-vis (CHCl₃) $\lambda_{max} = 408$, 521, 565 nm; HR-MS m/z: calcd. for C₄)H₄₄O₃N₇Fe: 736.2937, found: 736.2938 [M⁺].

3,18-Divinyl-8-(3-ethoxycarbonyl)ethyl-12-(((3-N-glycyl-Lhistidinyl)-9-oxymethyl)carbonyl)ethyl-2,7,13,17-tetramethyl-porphyrin (5a). The synthetic procedure of compound 5a was same as that used for 1a. DMF was used instead of pyridine, because it dissolves O-methyl-t-histidyl-glycine. Yield 15%; $R_{\rm f}=0.4$ (CHCl₃/CH₃OH = 15/1); IR (NaCl) $\nu=1635$ (C=O, amide), 1725 (C=O, ester) cm⁻¹; UV-vis (CHCl₃) $\lambda_{\rm max}=405$, 505, 541, 577, 627 nm; ¹H-NMR (CDCl₃) $\delta:-4.6$ (s, 2H, inner-NH), 2.7-2.9 (m, 2H, Im-CH₂-), 3.0-3.5 (m, 18H, por-CH₃, -CH₂-CO-NH-, -CH₂-COO-CH₂-CH₃), 3.6 (s, 2H, -CONH-CH₂-CONH-), 3.8 (s, 3H, -OCH₃), 4.0-4.3 (d, 4H, por-CH₂-), 4.3-4.5 (m, 1H, α -CH), 6.0-6.4 (m, 4H, =CH₂ (vinyl)), 7.4 (s, 1H, Im-H), 8.0-8.3 (m, 5H, -CH= (vinyl), Im-H), 9.8-10.0 (m, 4H, meso-H); MS m/z: 782.68.

Fe(III) complex of 5a (5b). Iron insertion to 5a was carried out by the same procedure as in the 1b preparation. Yield 75%; $R_{\rm f} = 0.5$ (CHCl₃/CH₃OH = 8/1); IR (NaCl) $\nu = 1660$ (C=O, amide), 1734 (C=O, ester) cm⁻¹; UV-vis (CHCl₃) $\lambda_{\rm max} = 388$, 508, 637 nm; HR-MS mlz: calcd. for C₄₄H₄₆O₆N₈Fe: 838.2890, found: 839.2929 [M + H⁺].

3,18-Divinyl-8-(3-ethoxycarbonyl)ethyl-12-(4-(N-(2-methyl-imidazolyl))butylamido)ethyl-2,7,13,17-tetramethylporphyrin (6a). Compound 6a was synthesized by the same procedure as for 1a except for using 4-(N-(2-methylimidazolyl))butylamine instead of 3-imidazolylpropylamine. Yield 20%; R_f : 0.1 (CHCl₃/CH₃OH = 8/1); IR (NaCl) ν = 1732 (C=O, ester), 1651 (C=O, amide) cm⁻¹; UV-vis (CHCl₃) λ_{max} = 408, 506, 542, 576, 630 nm; ¹H-NMR (CDCl₃) δ : -4.2 (s, 2H, inner-H), 0.4-0.6 (m, 4H, CONH-CH₂-(CH_2)₂-), 1.4-1.5 (d, 3H, Im-CH₃), 2.2-2.4 (m,